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(54) **METHODS AND SYSTEMS FOR DETECTING AN ANALYTE OR CLASSIFYING A SAMPLE**

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CPC **G01N 33/581** (2013.01); **B01L 3/502715** (2013.01); **C12Q 1/66** (2013.01); **G01N 21/76** (2013.01); **G01N 21/763** (2013.01); **G01N 33/5308** (2013.01); **G01N 33/542** (2013.01); **B01L 2300/0636** (2013.01); **B01L 2300/0654** (2013.01); **B01L 2300/0816** (2013.01); **B01L 2300/0867** (2013.01); **B01L 2300/1822** (2013.01); **B01L 2300/1827** (2013.01); **B01L 2400/0487** (2013.01); **G01N 2333/726** (2013.01); **G01N 2333/90241** (2013.01)

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None
See application file for complete search history.

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(57) **ABSTRACT**

The present invention relates to methods and systems for detecting one or more analytes in a sample and/or for classifying a sample. In particular, the present invention relates to methods and systems which can be used to detect the analytes in real time and which rely on flowing through a microfluidic device one or more types of sensor molecule each comprising a domain that binds one or more analytes, a chemiluminescent donor domain and an acceptor domain, wherein the separation and relative orientation of the chemiluminescent donor domain and the acceptor domain, in the presence and/or the absence of analyte, is within $\pm 50\%$ of the Forster distance.

19 Claims, 58 Drawing Sheets

Specification includes a Sequence Listing.

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Figure 1

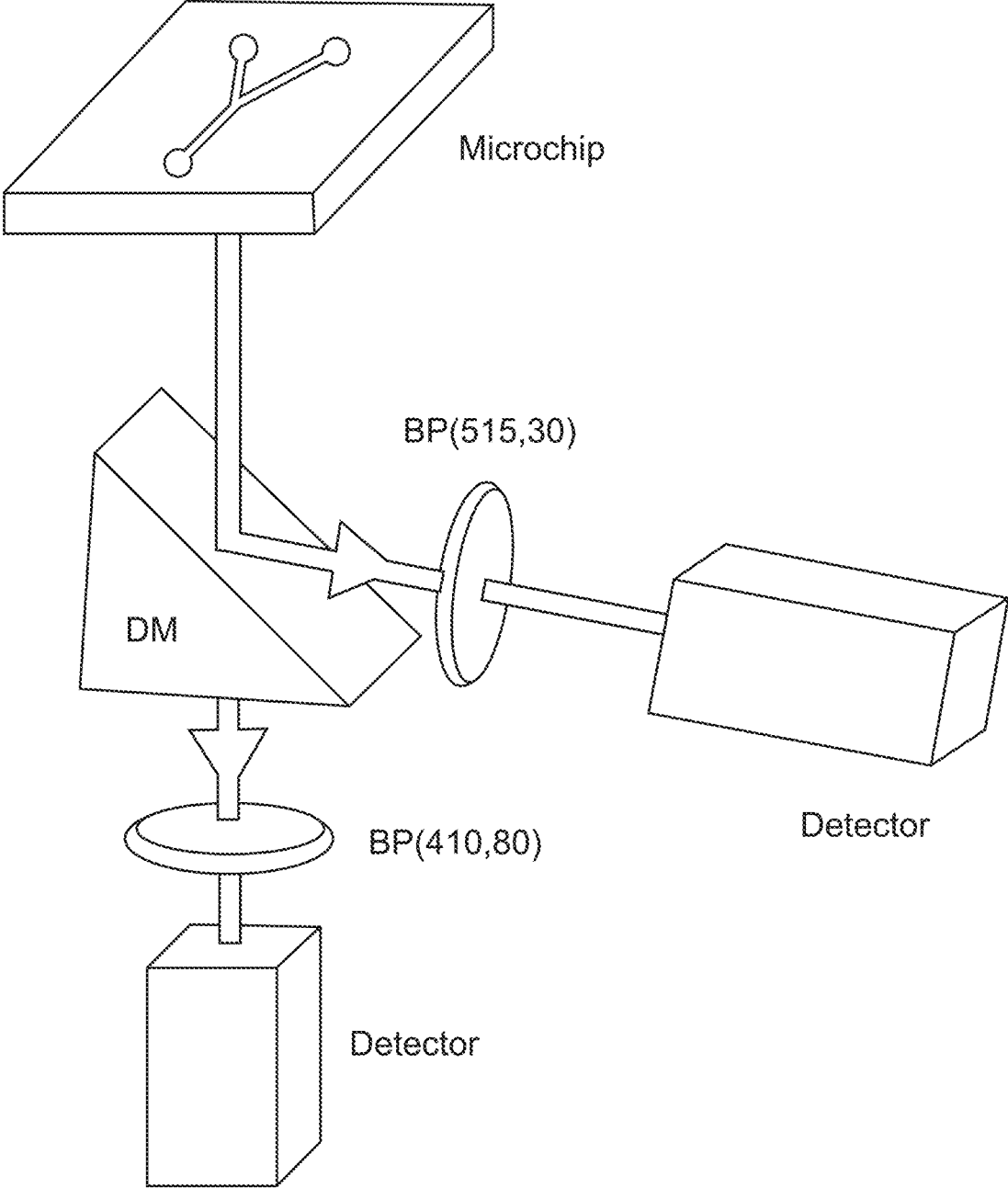


Figure 2

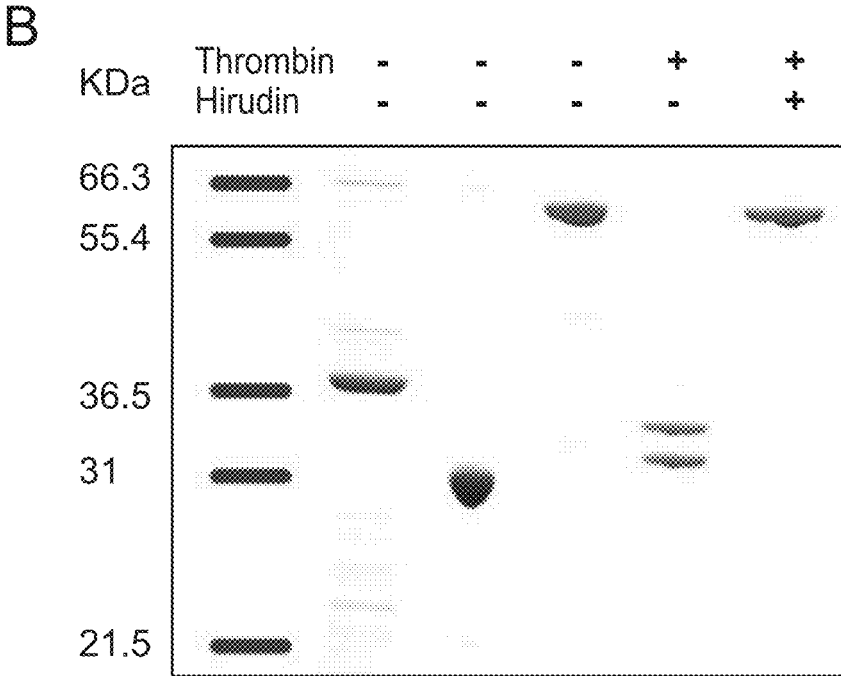
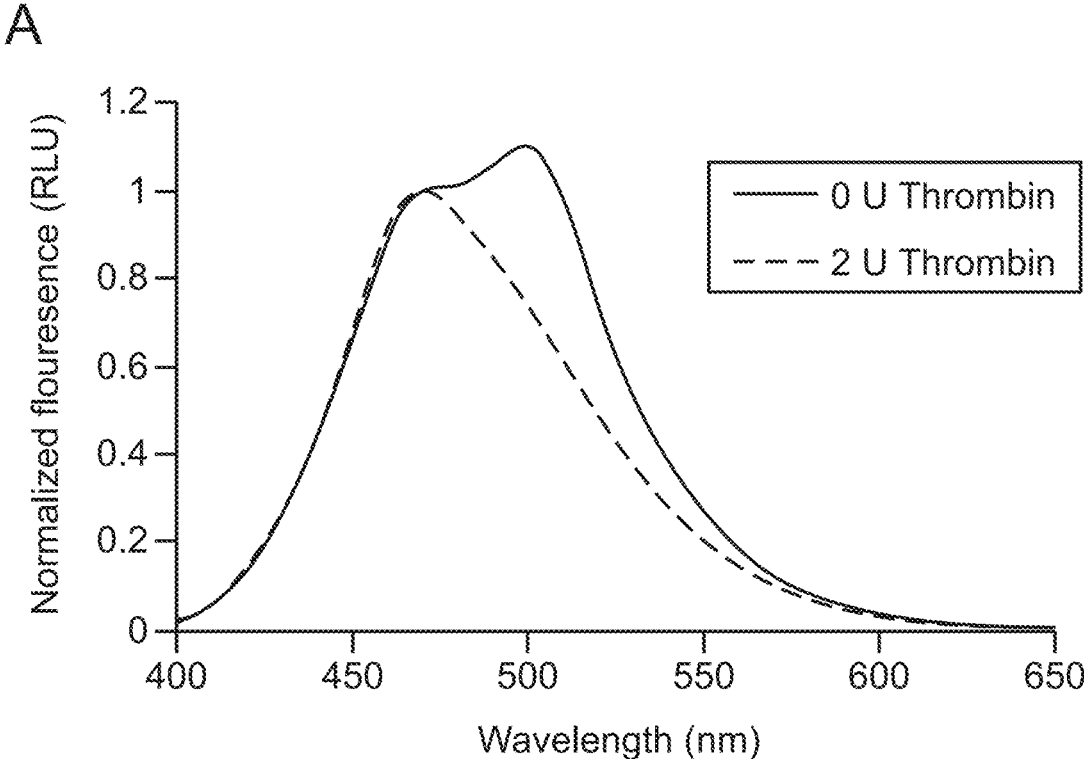


Figure 3

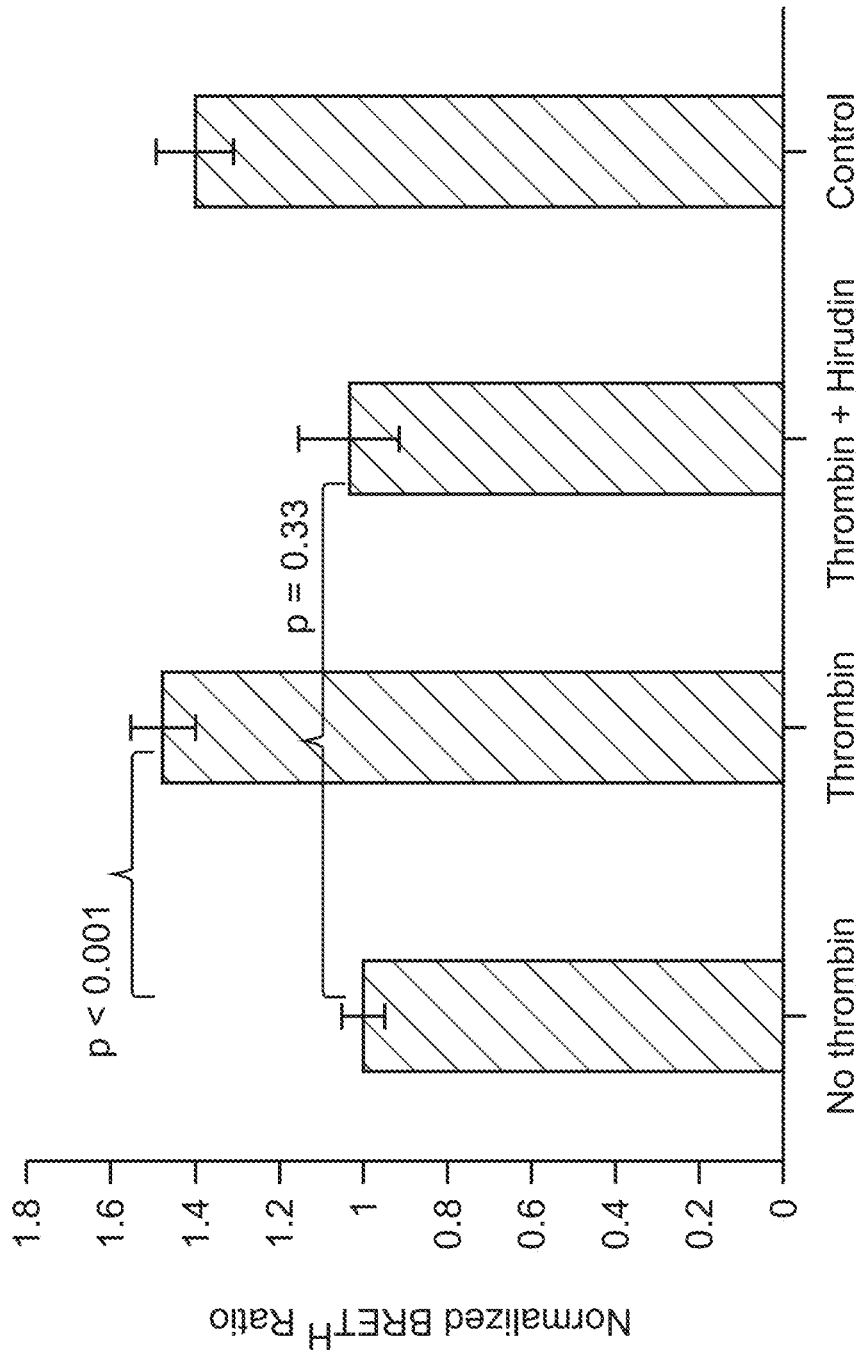


Figure 4

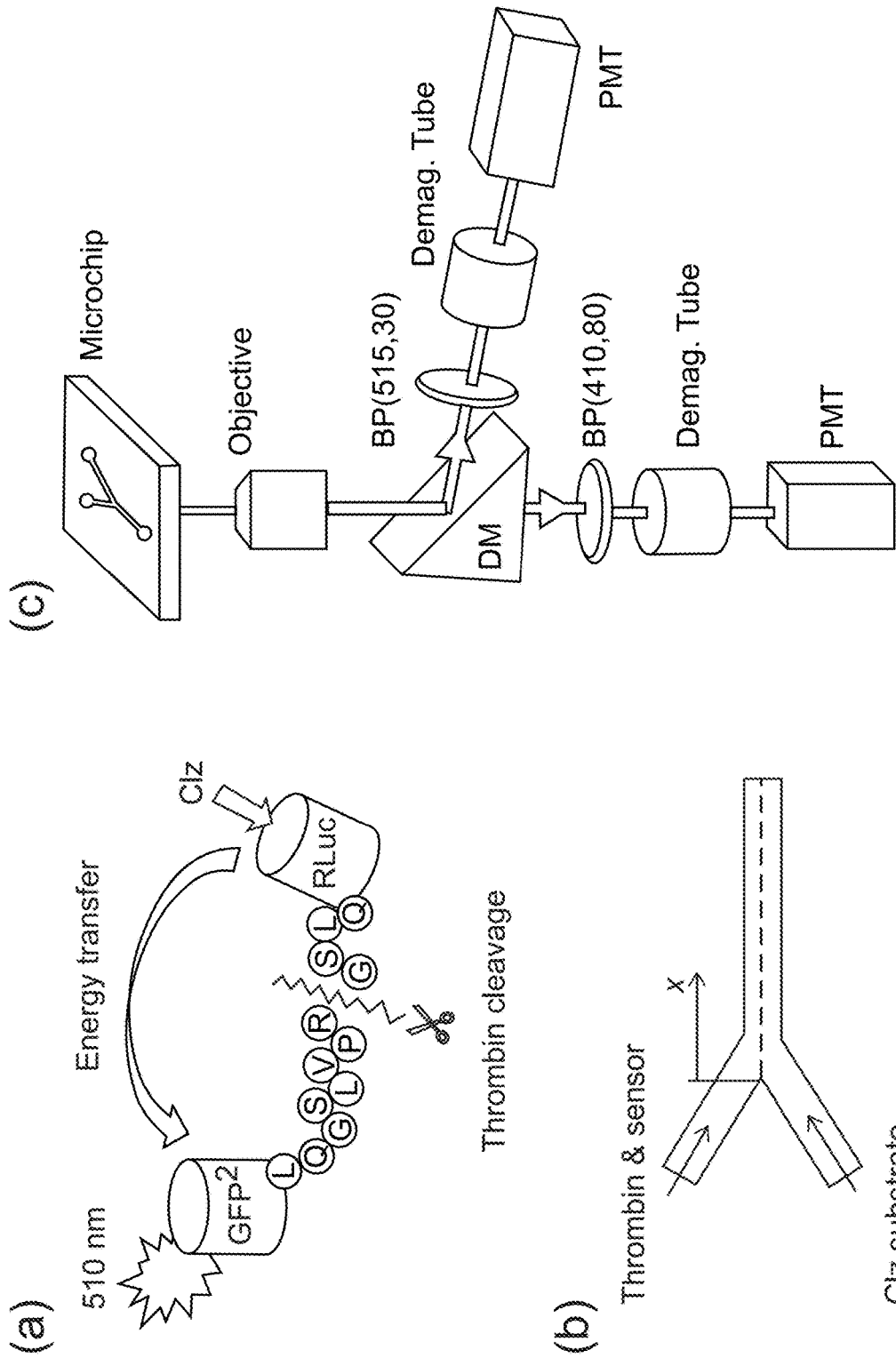


Figure 5

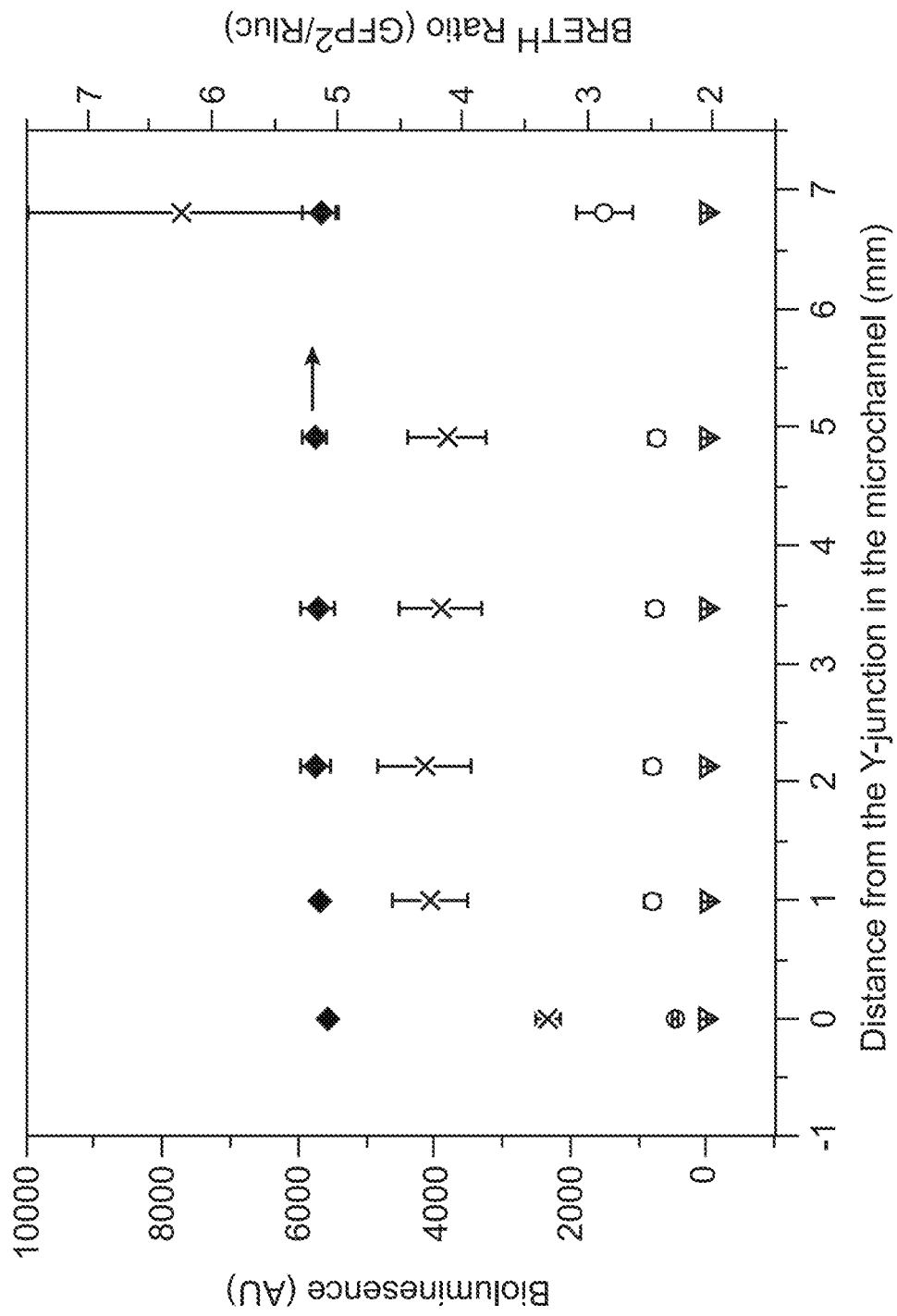


Figure 6

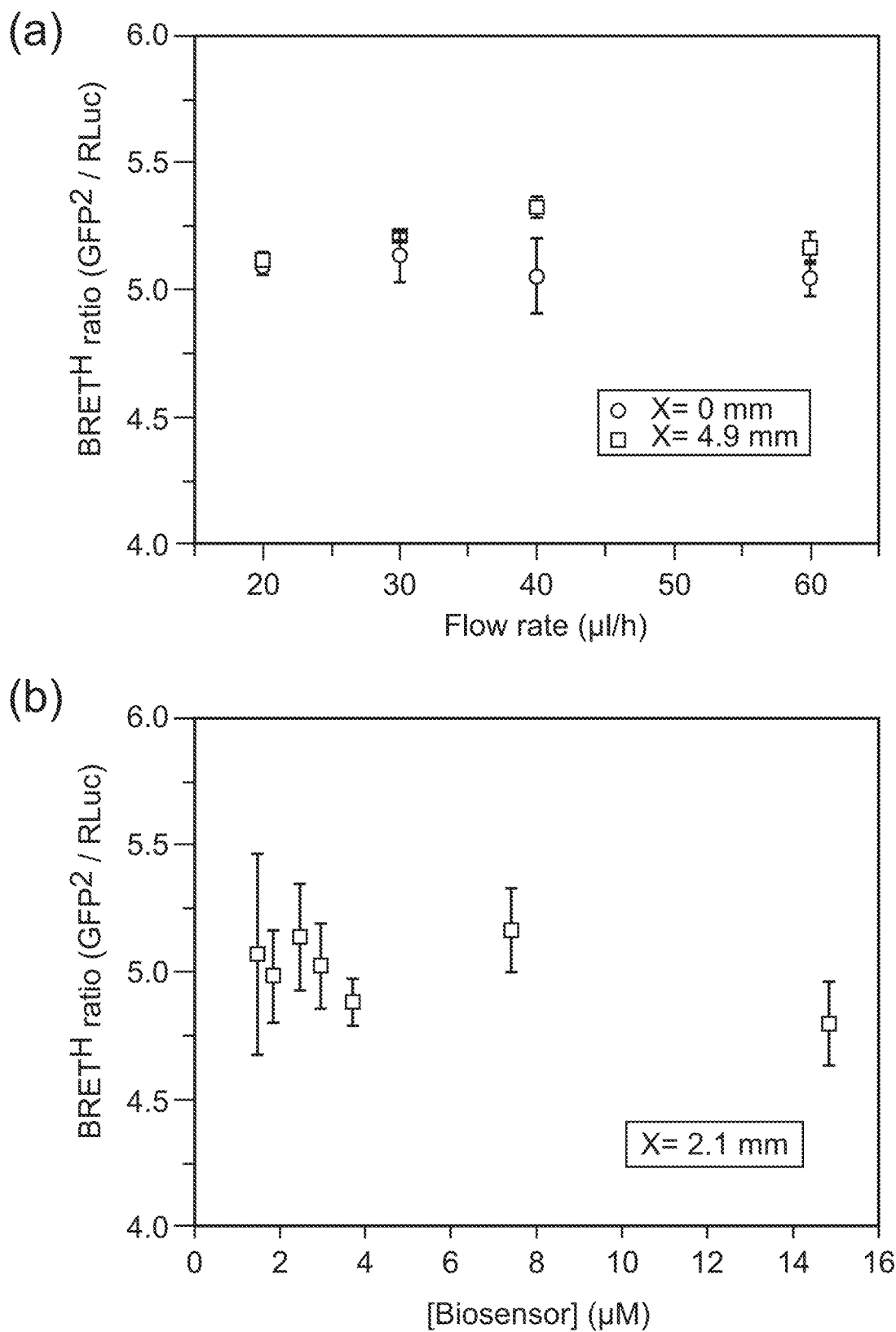


Figure 7

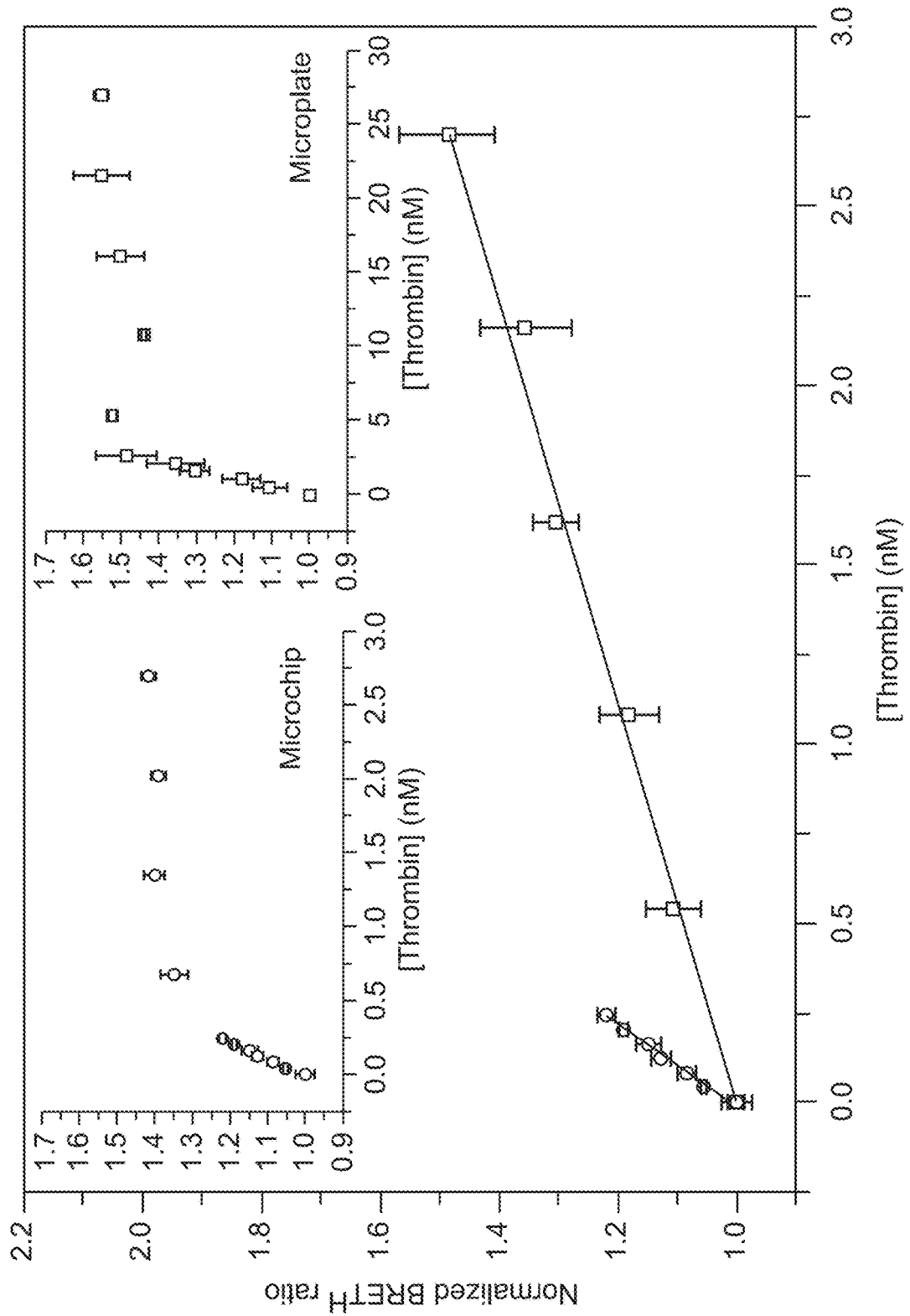


Figure 8

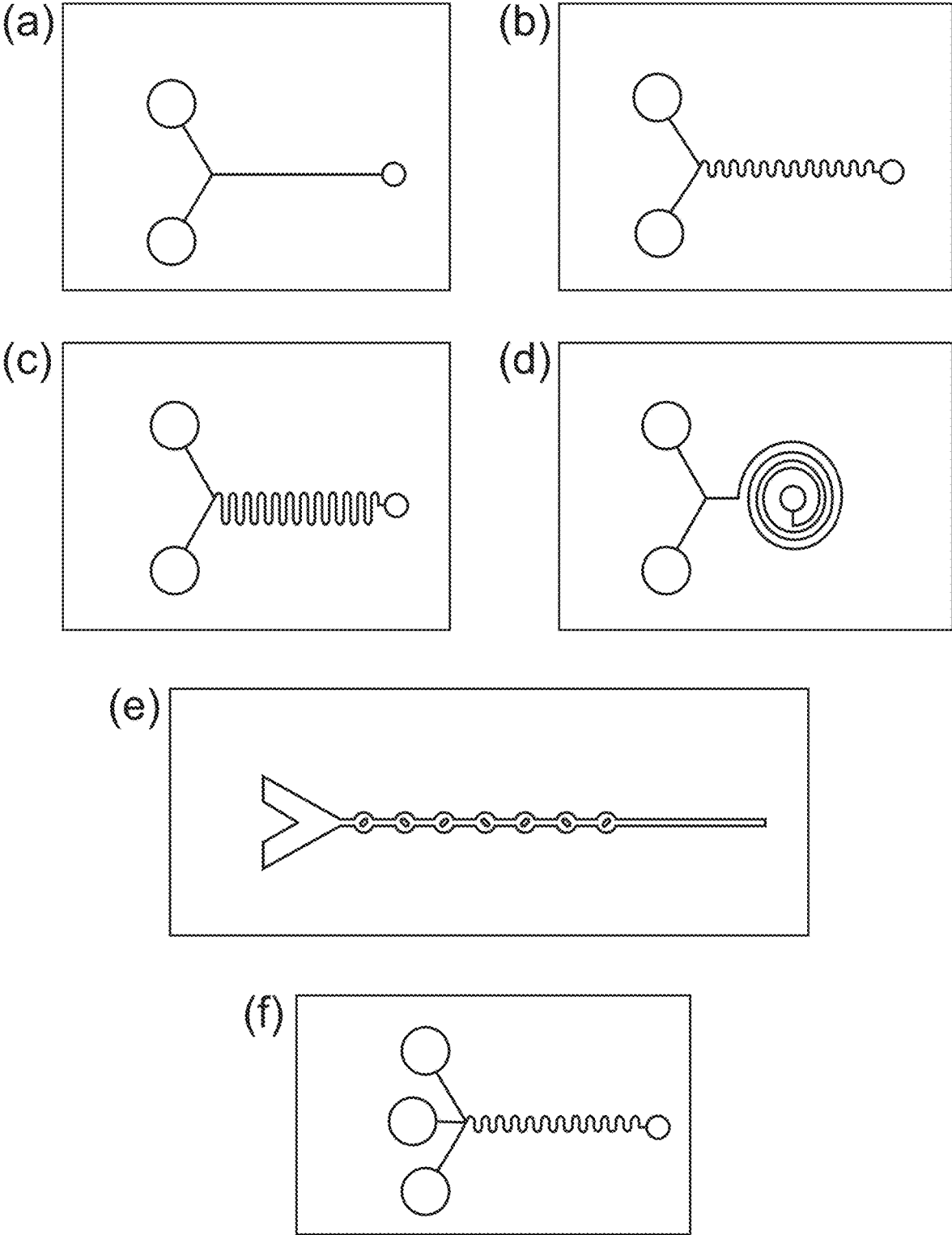


Figure 9

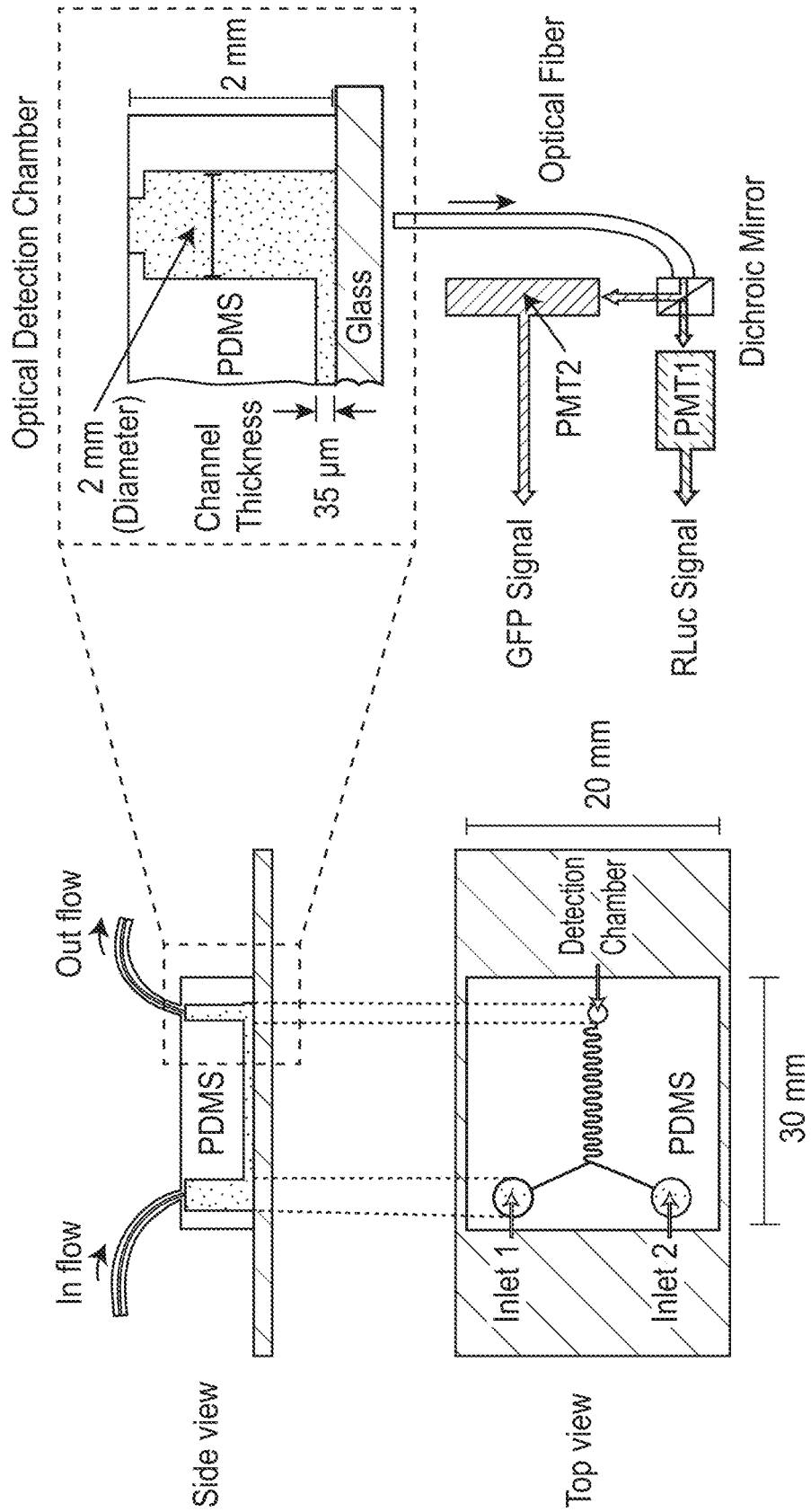


Figure 10

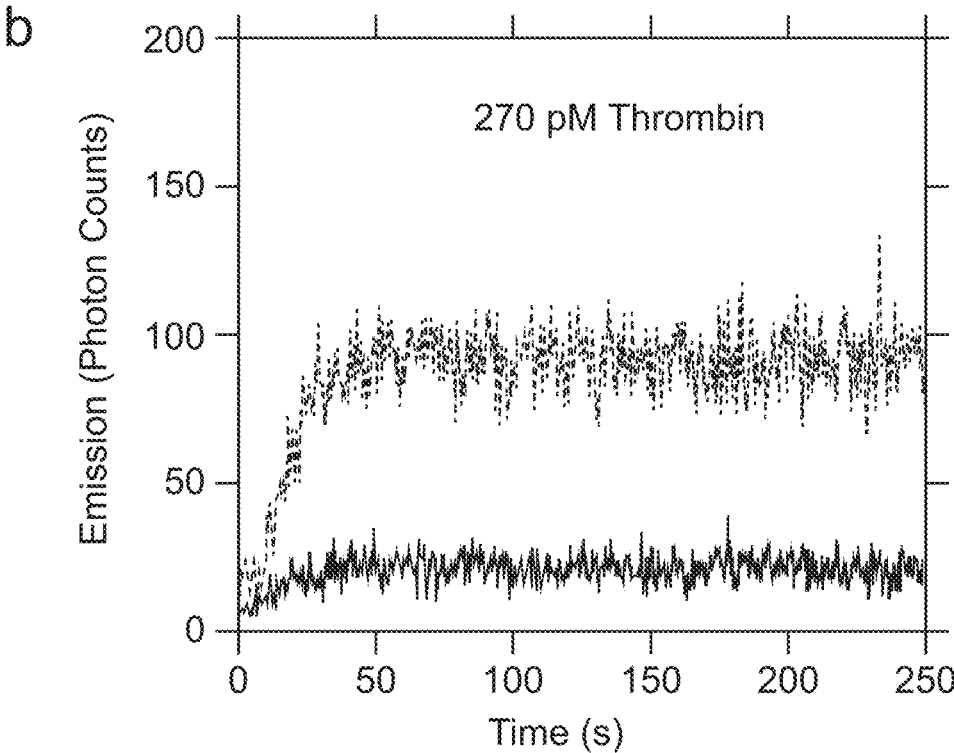
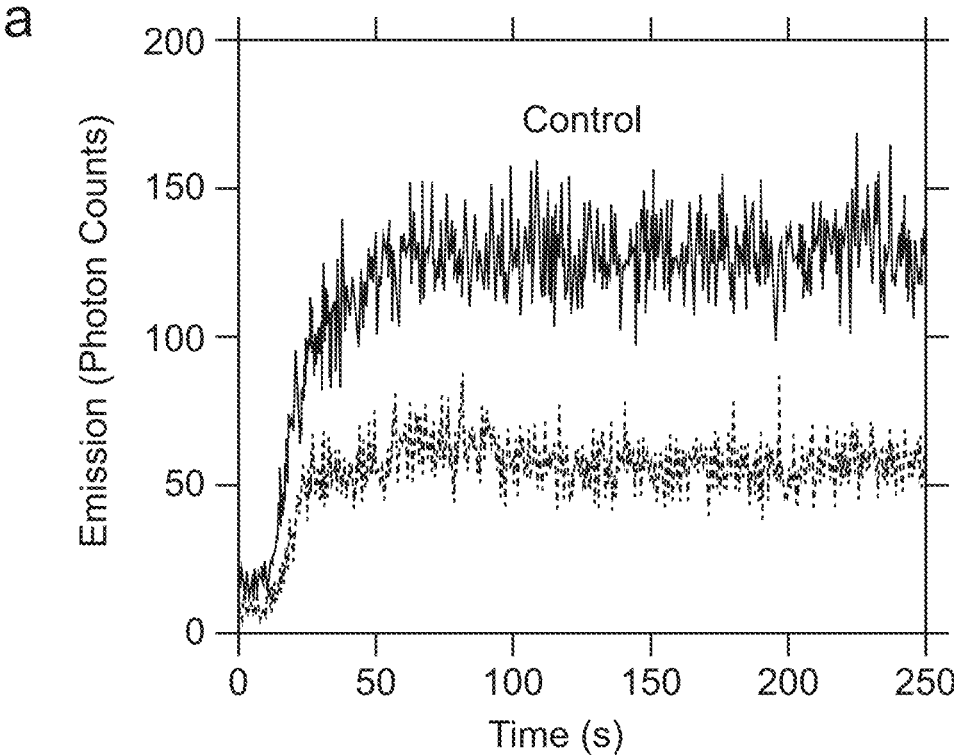


Figure 10 (Cont.)

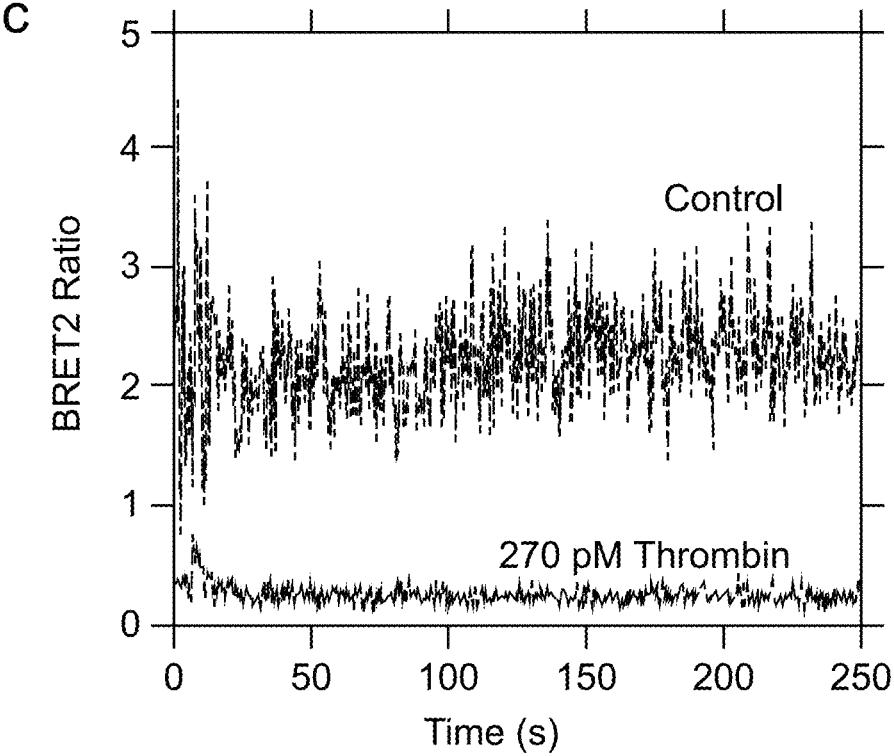


Figure 11

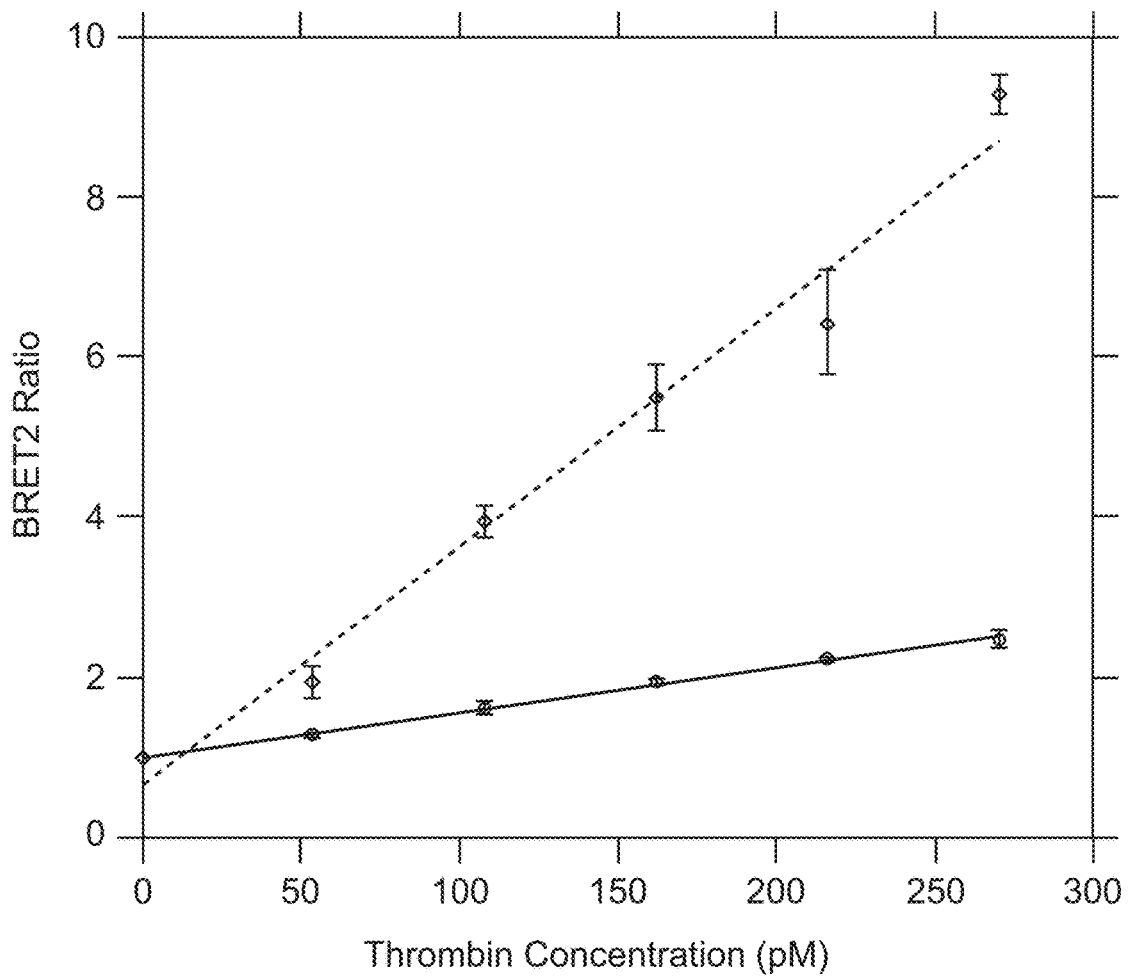
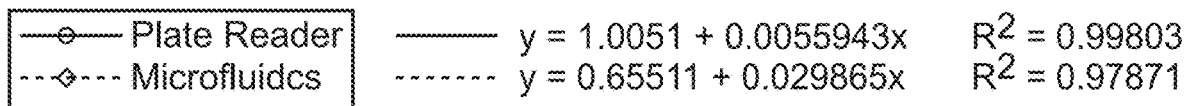


Figure 12

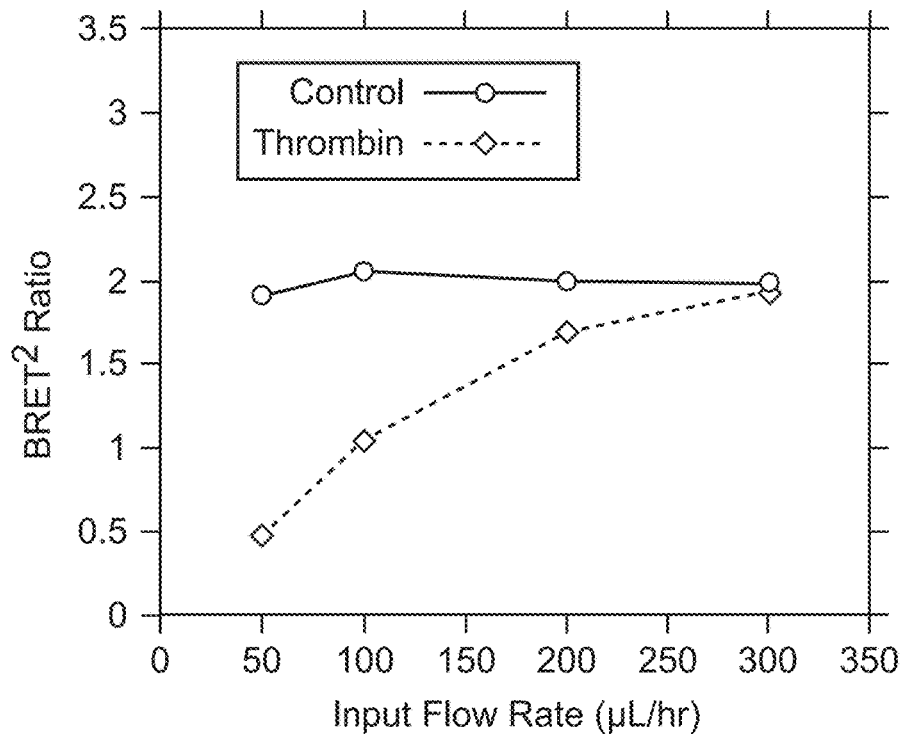


Figure 13

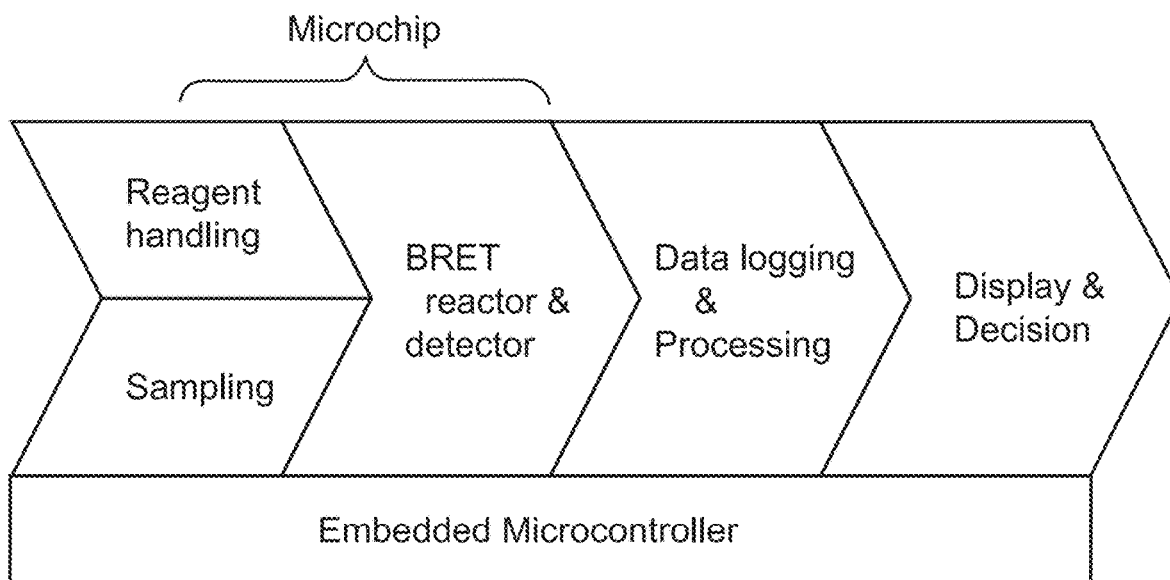


Figure 14

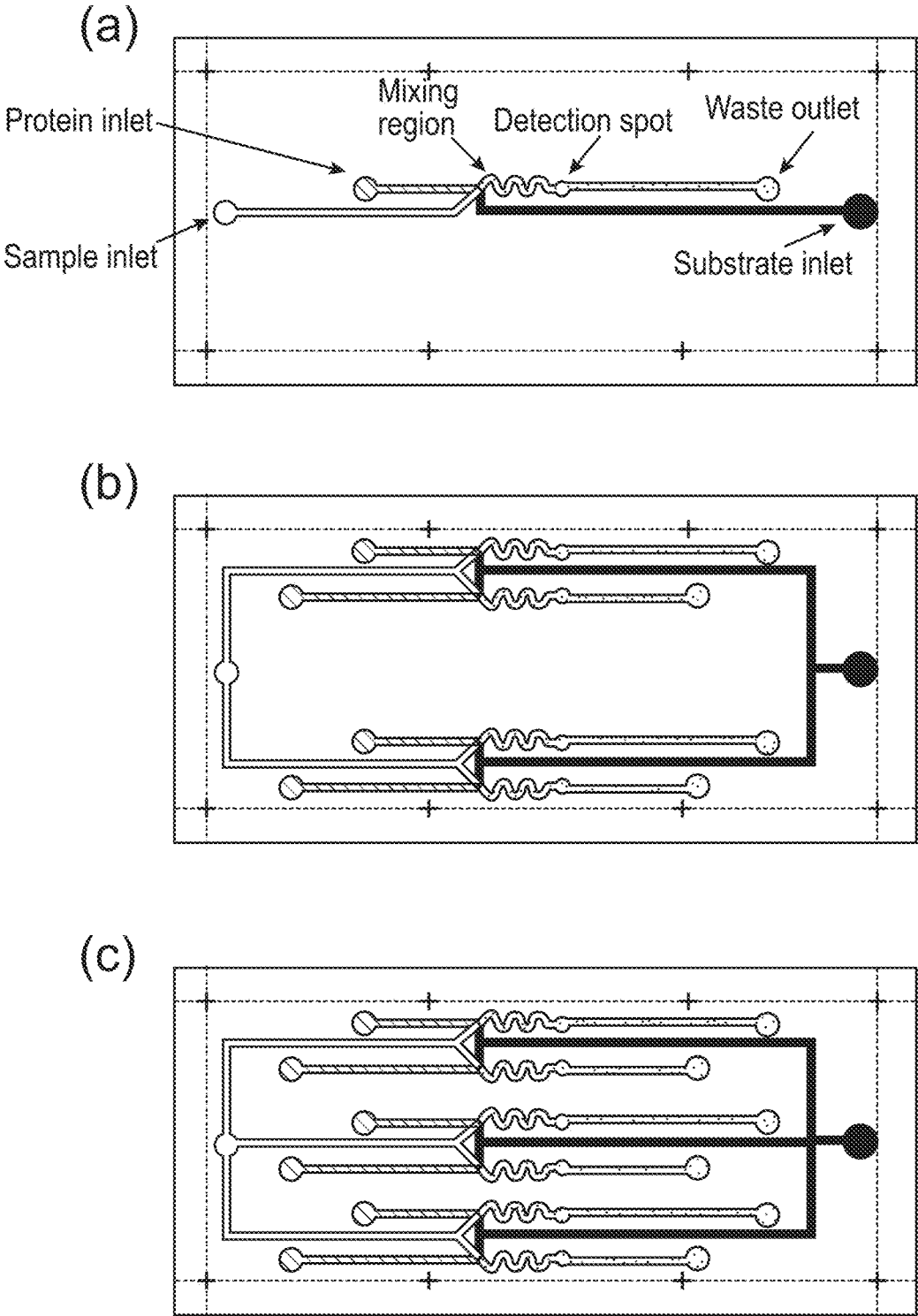


Figure 15

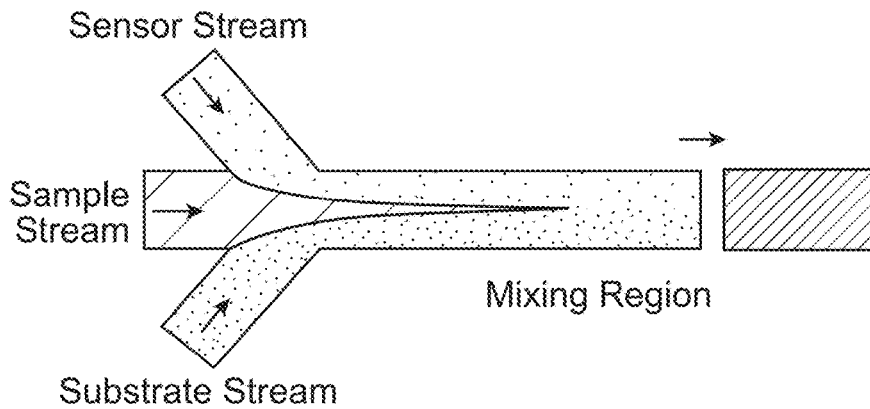


Figure 16

Disposable COC chip ($n = 1.53$, standard size $1 \times 25 \times 75 \text{ mm}^3$), hot embossed by a metal mold, with 5 BRET optical detection elements

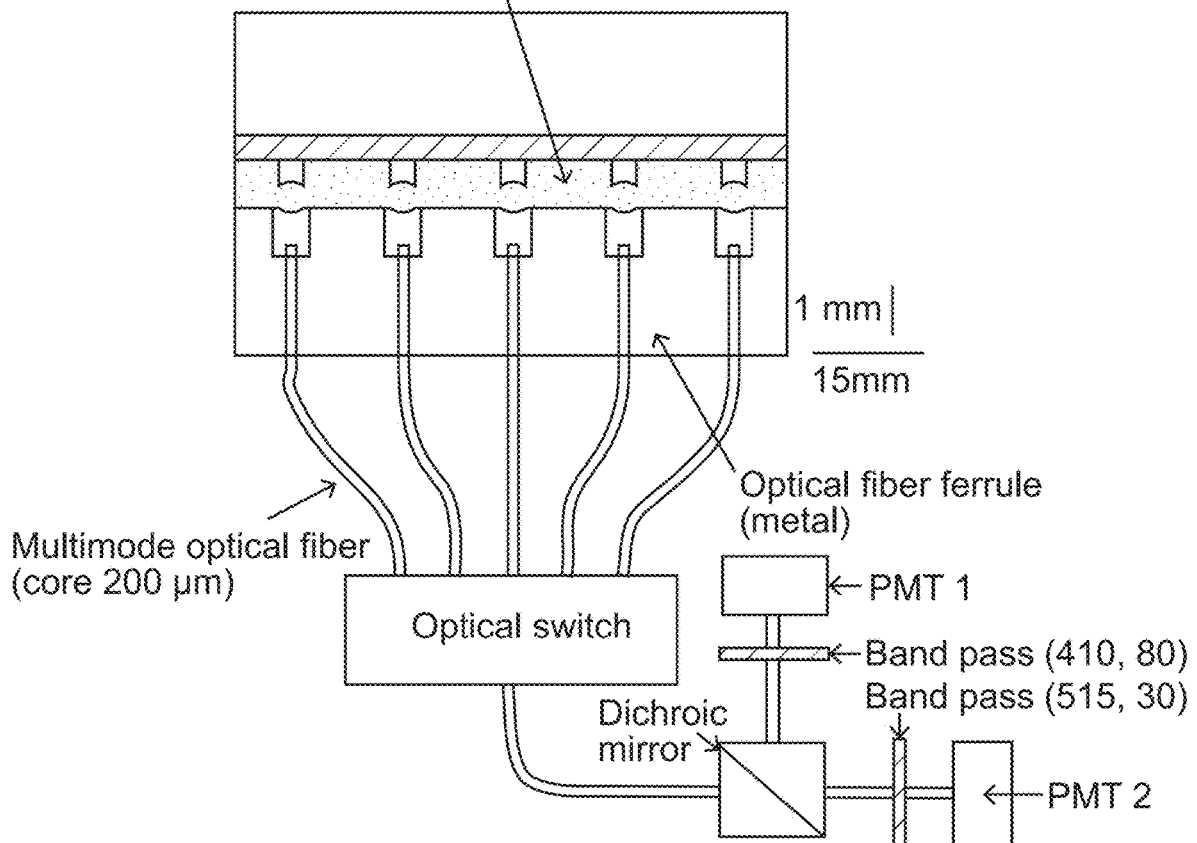


FIG. 17

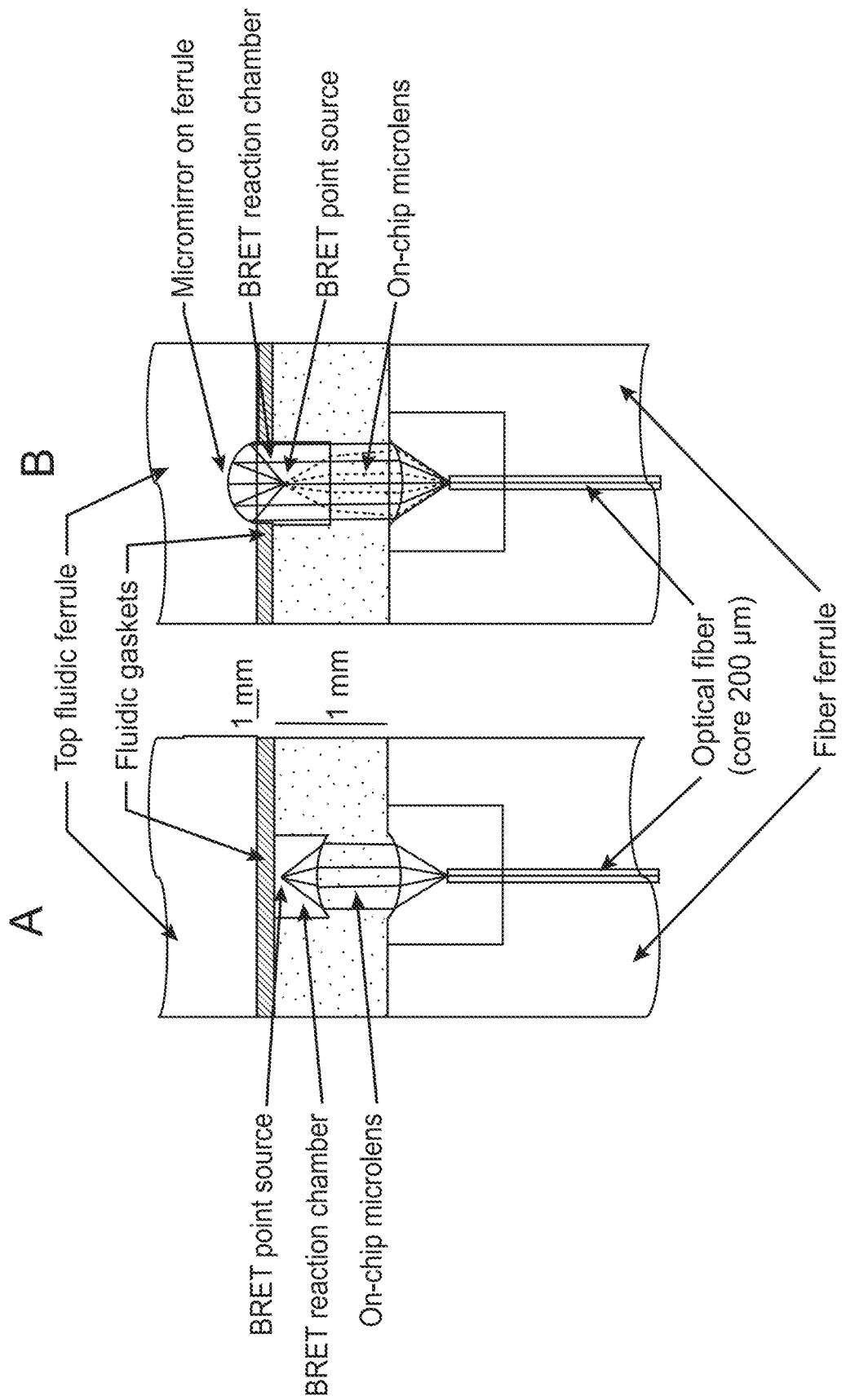


FIG. 18

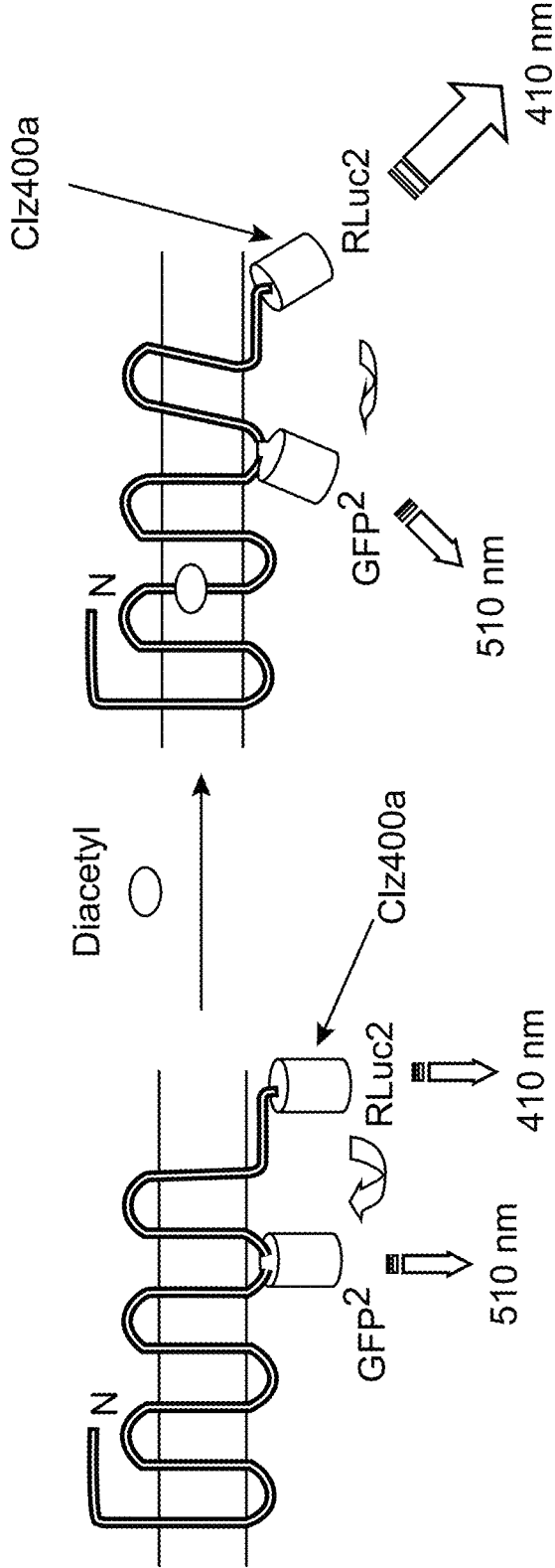


Figure 19

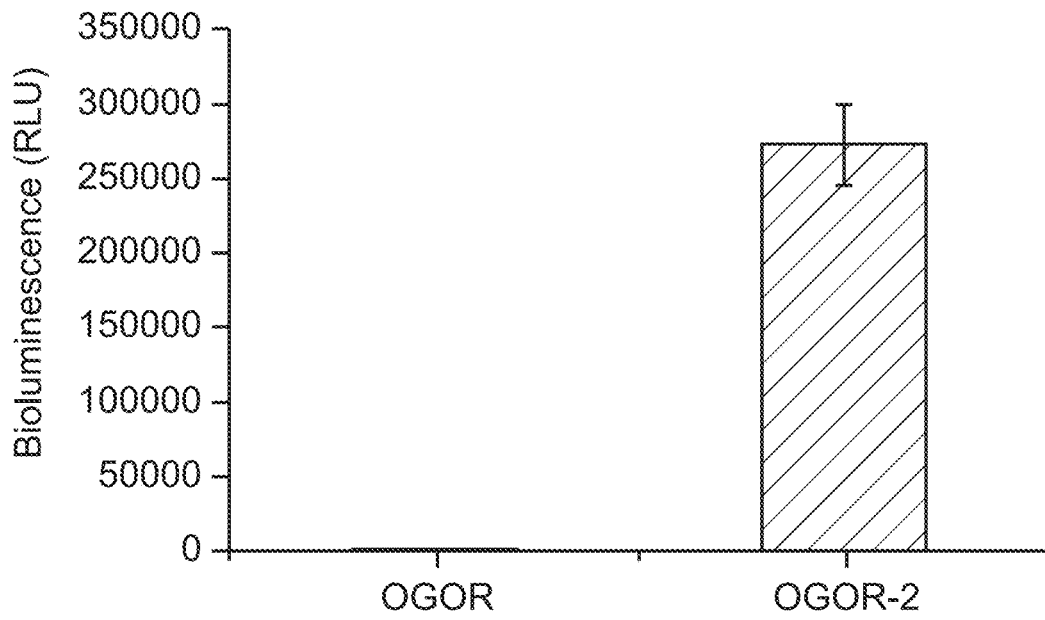


Figure 20

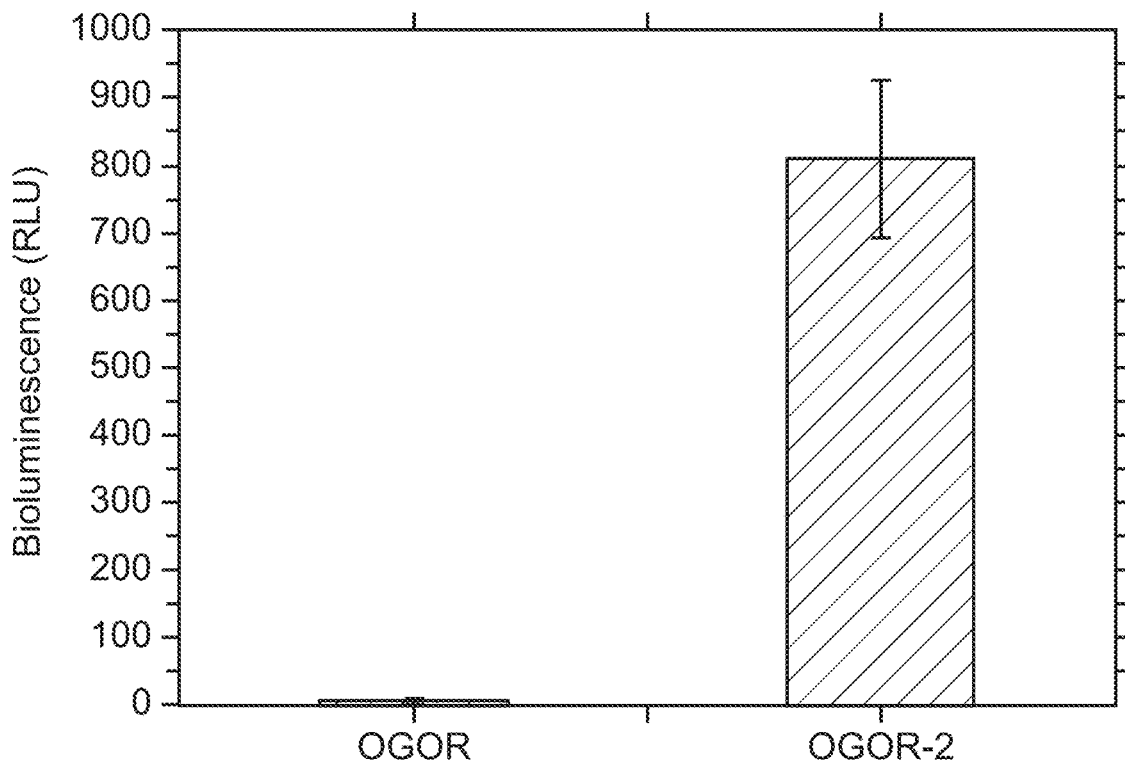


Figure 21

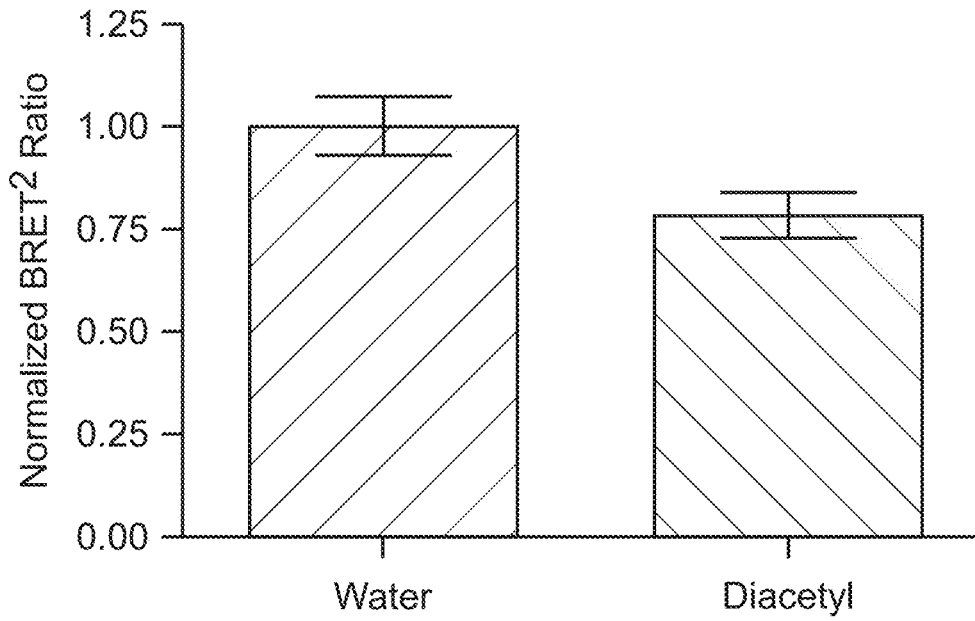


Figure 22

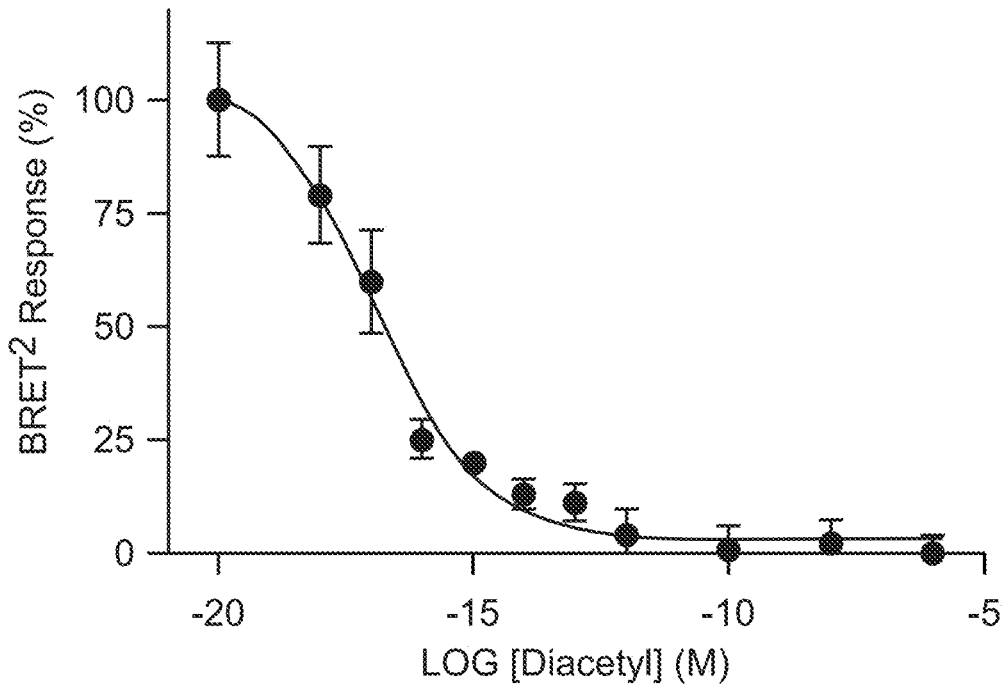


Figure 23

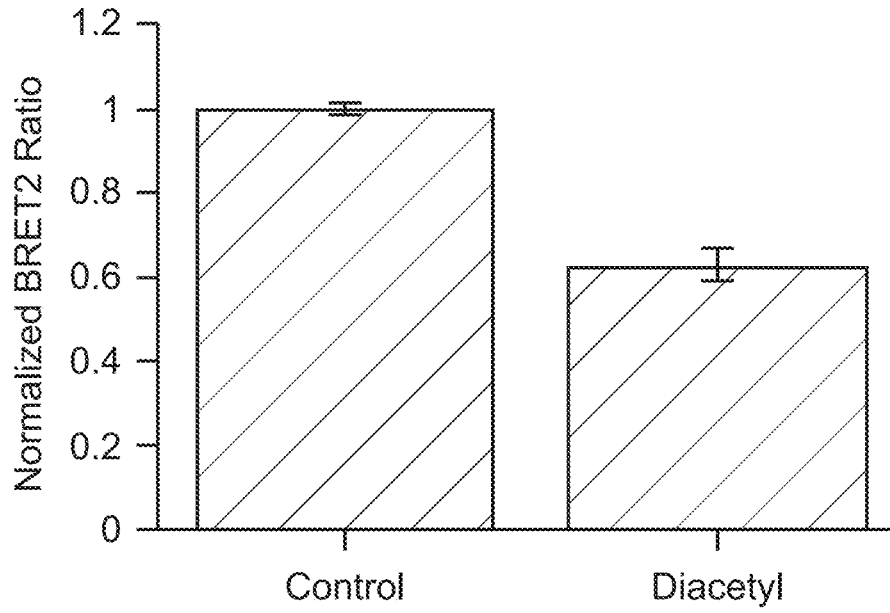


Figure 24

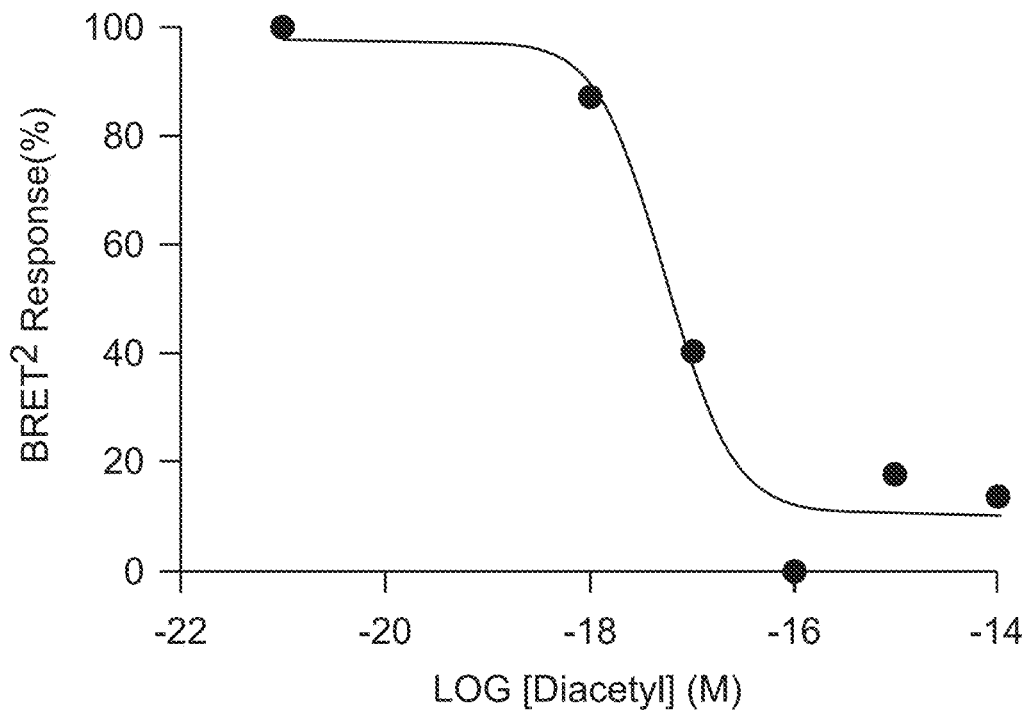


Figure 25

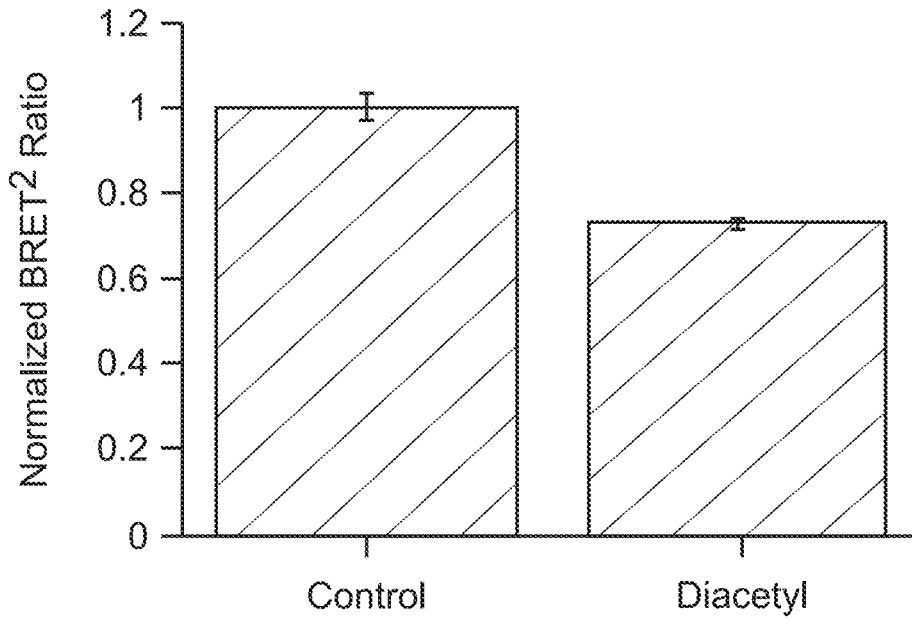


Figure 26

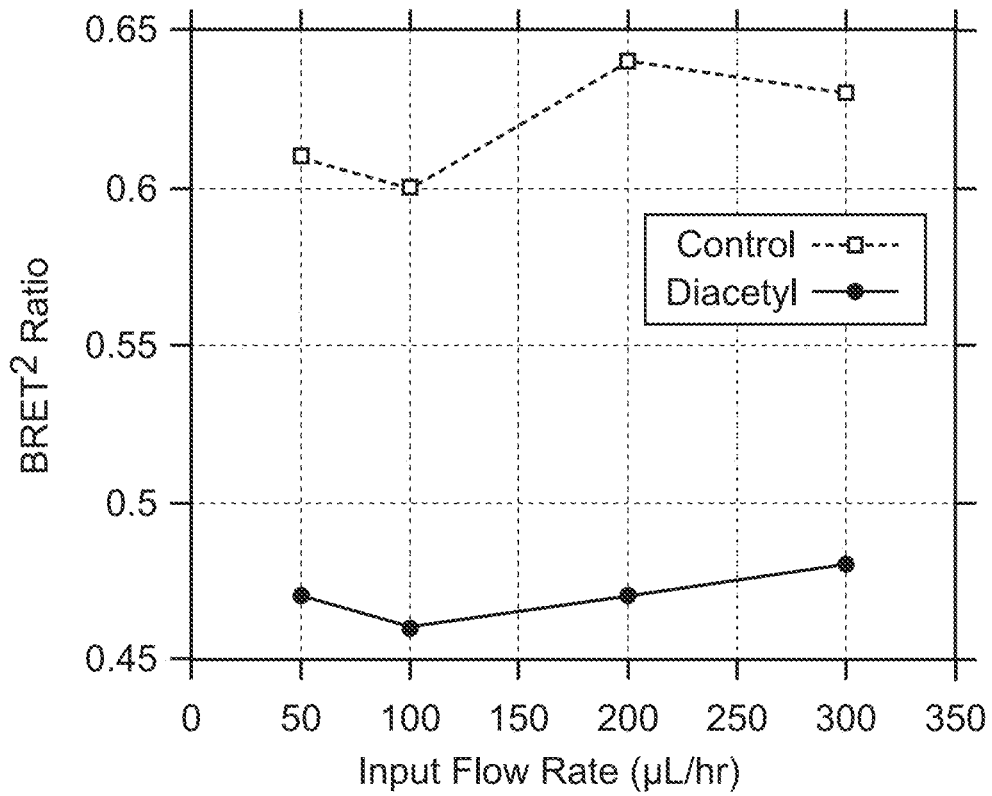


Figure 27

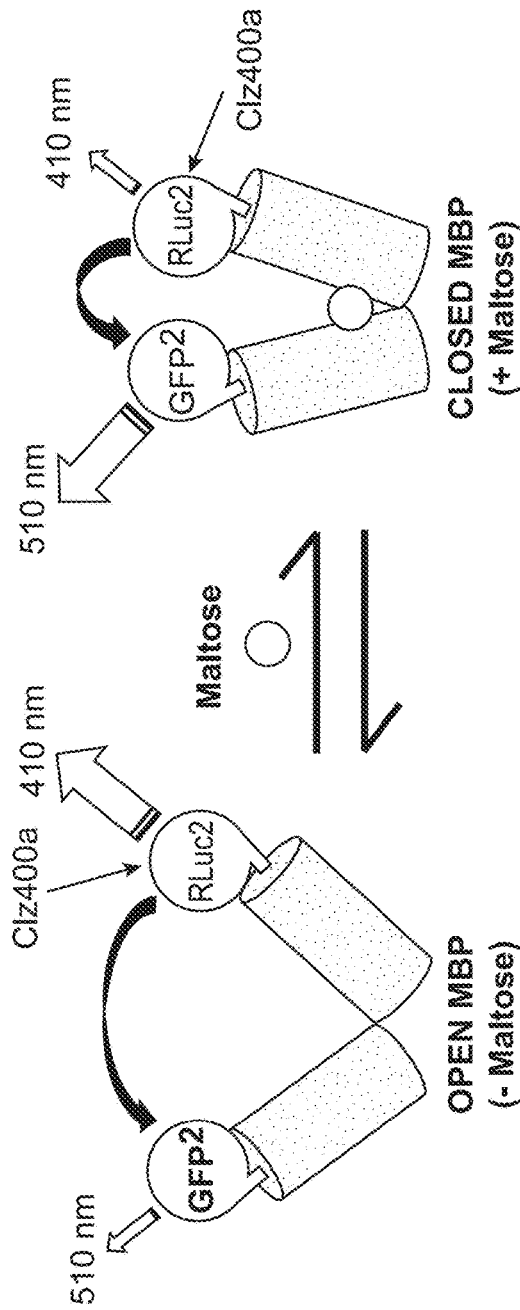


Figure 28

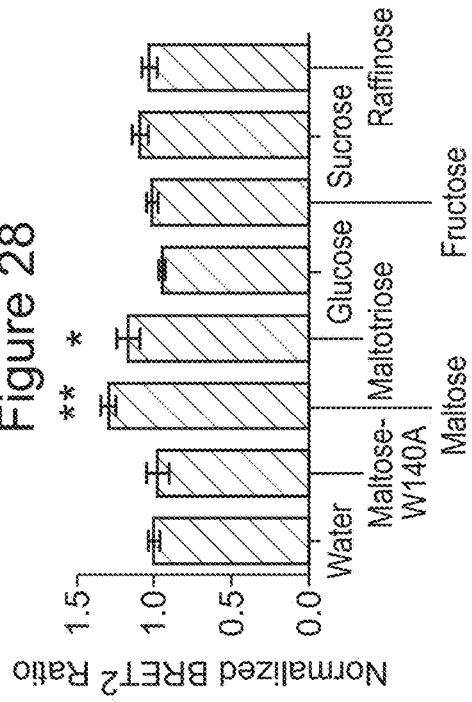


Figure 29

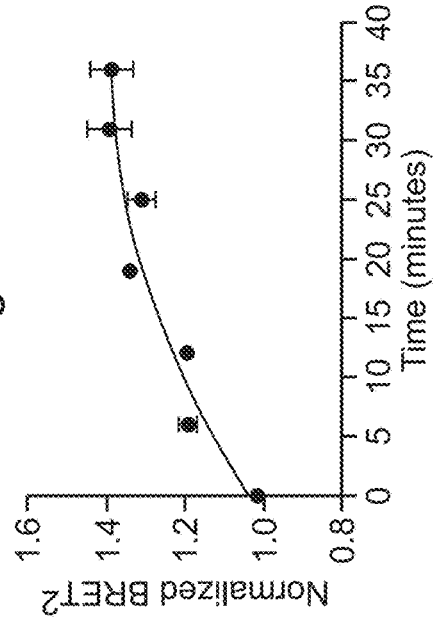


Figure 30

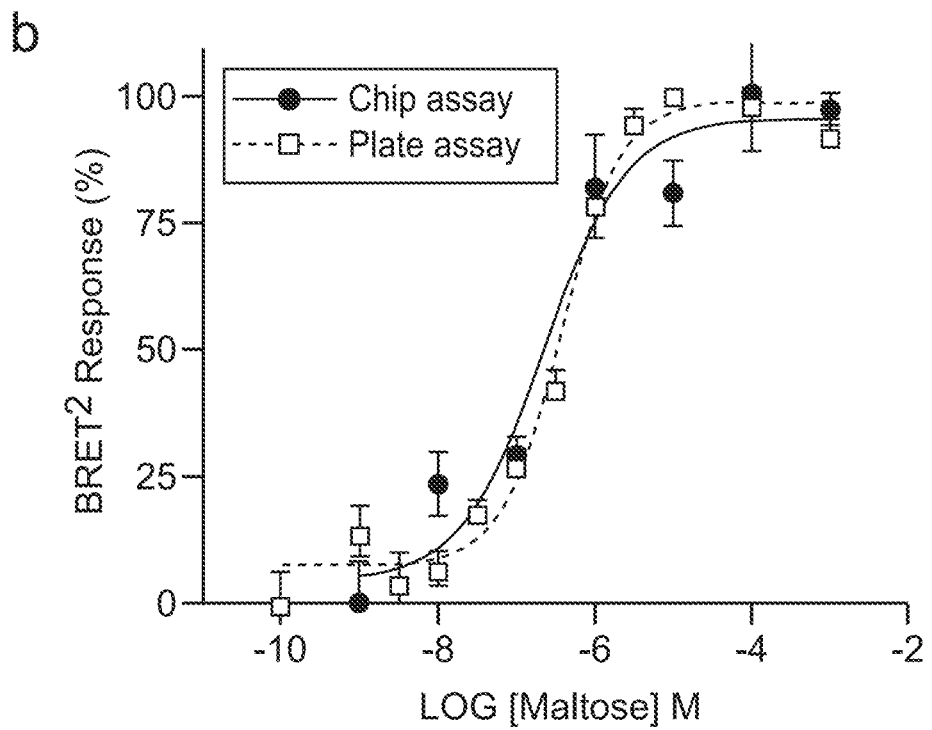
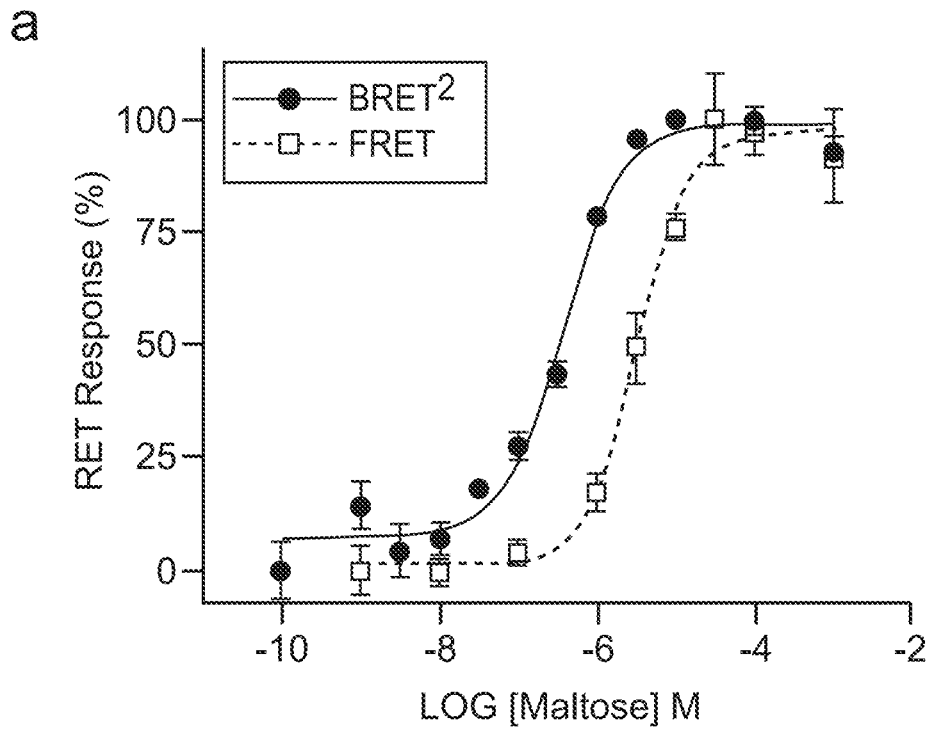


FIG. 31

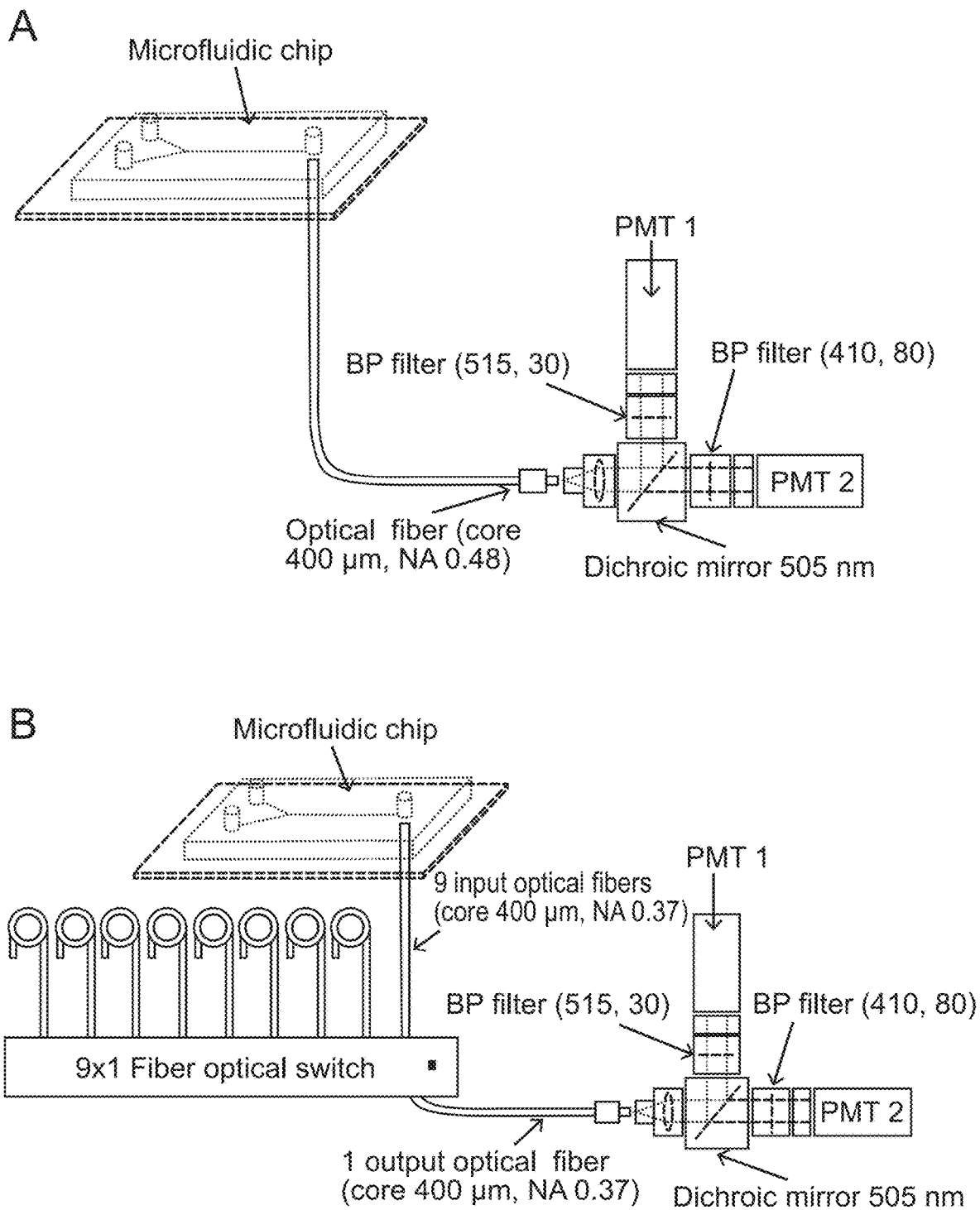


Figure 32

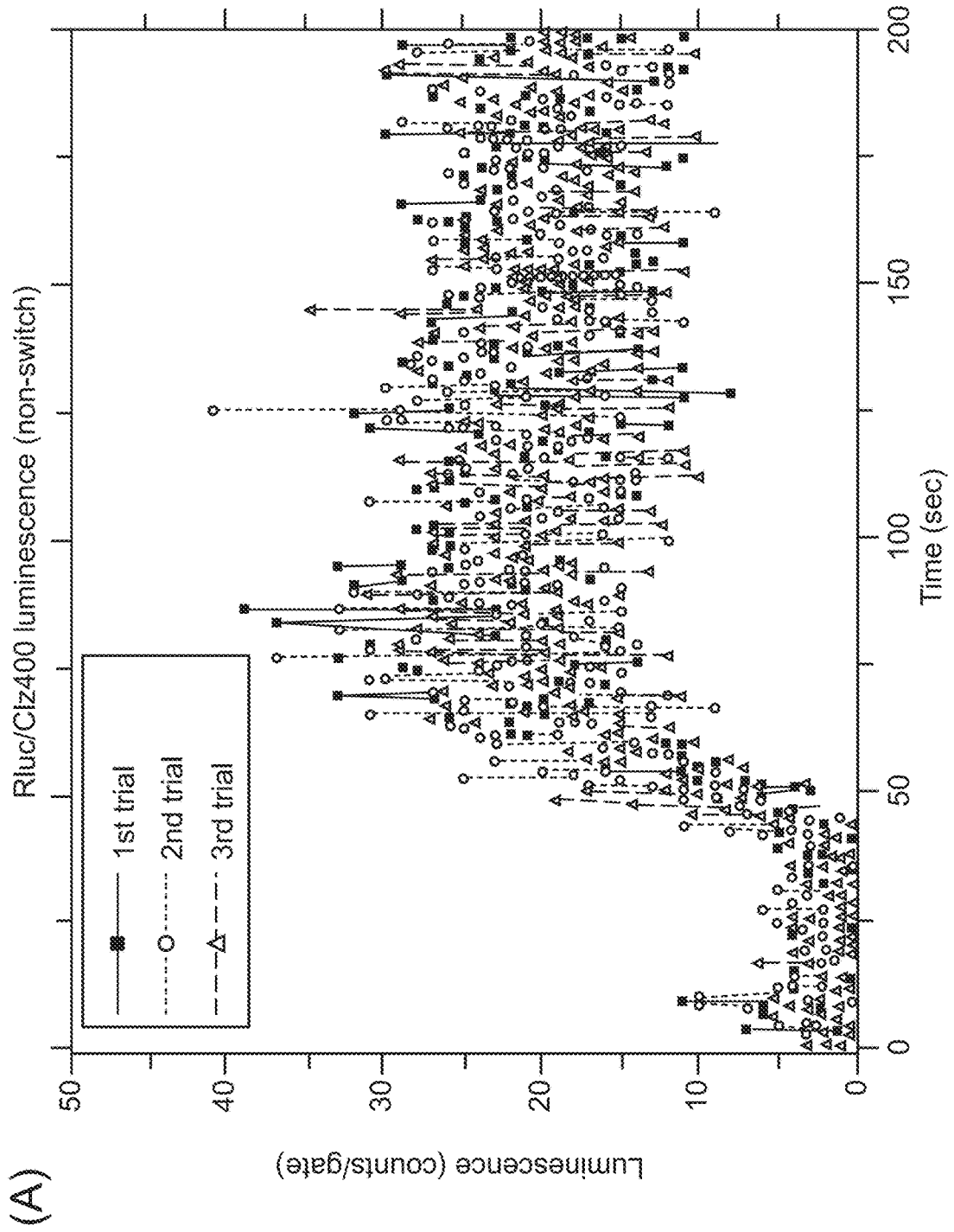


Figure 32 (Cont.)

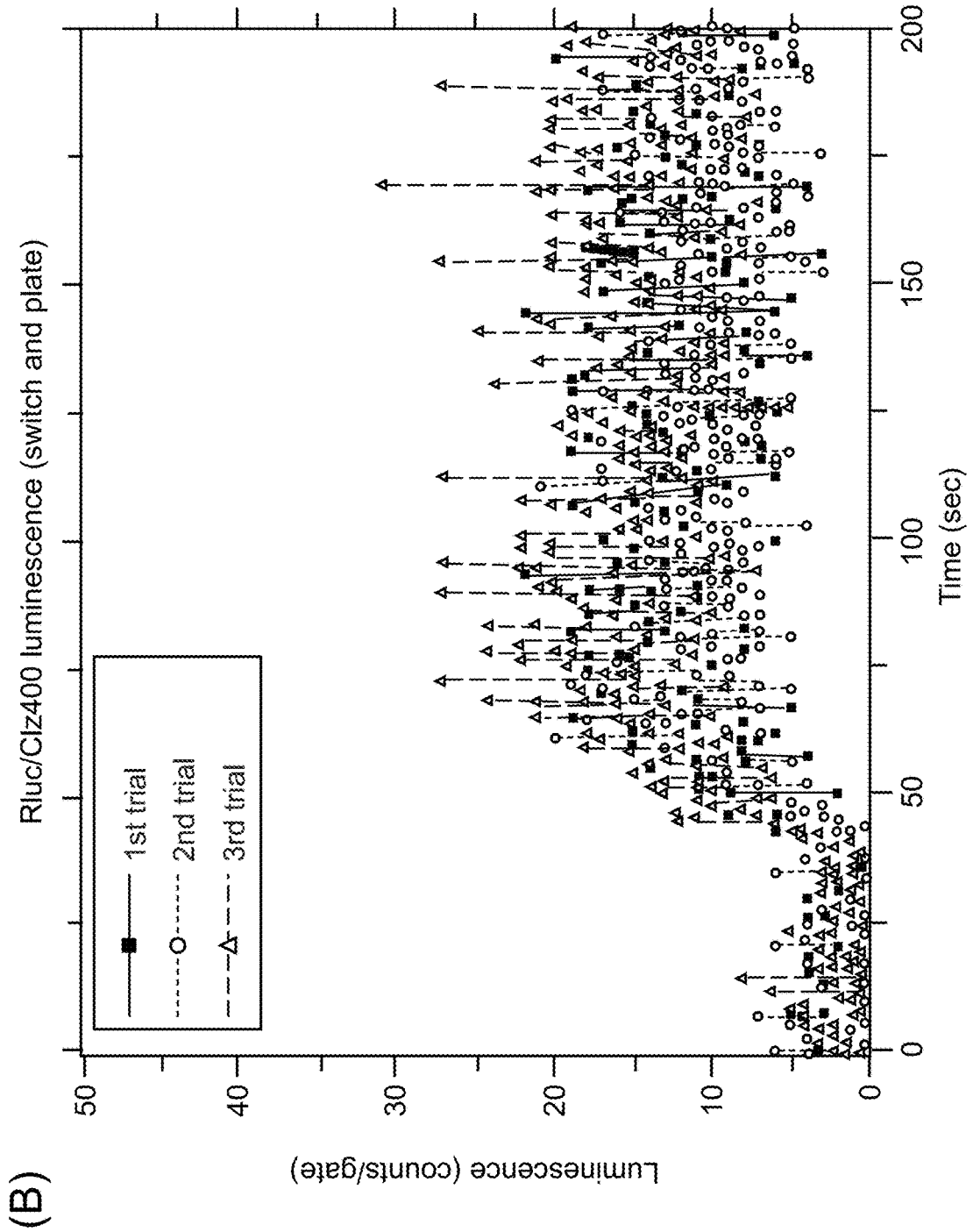


Figure 33

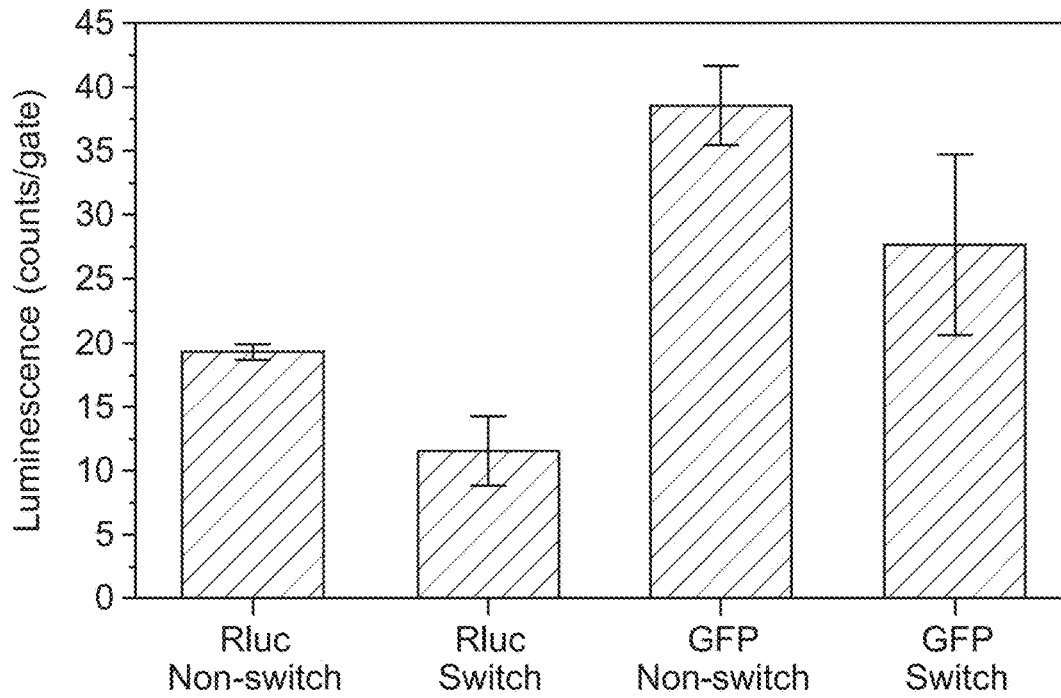


Figure 34

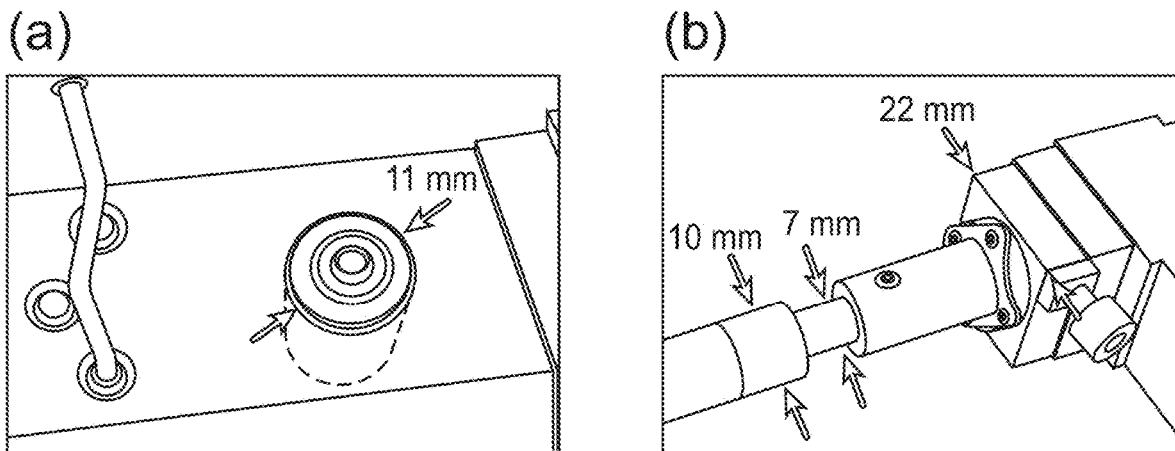


Figure 35

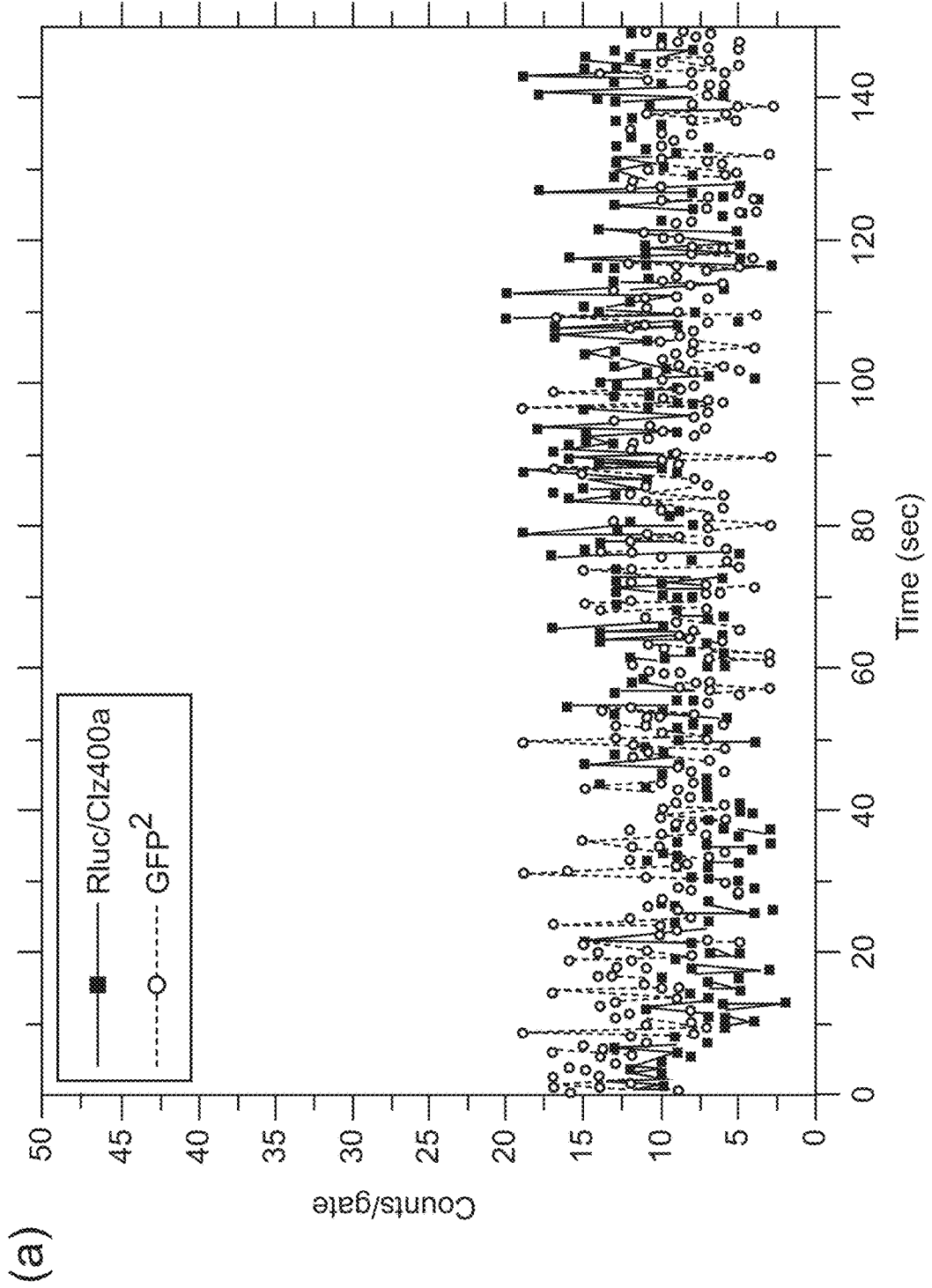


Figure 35 (Cont.)

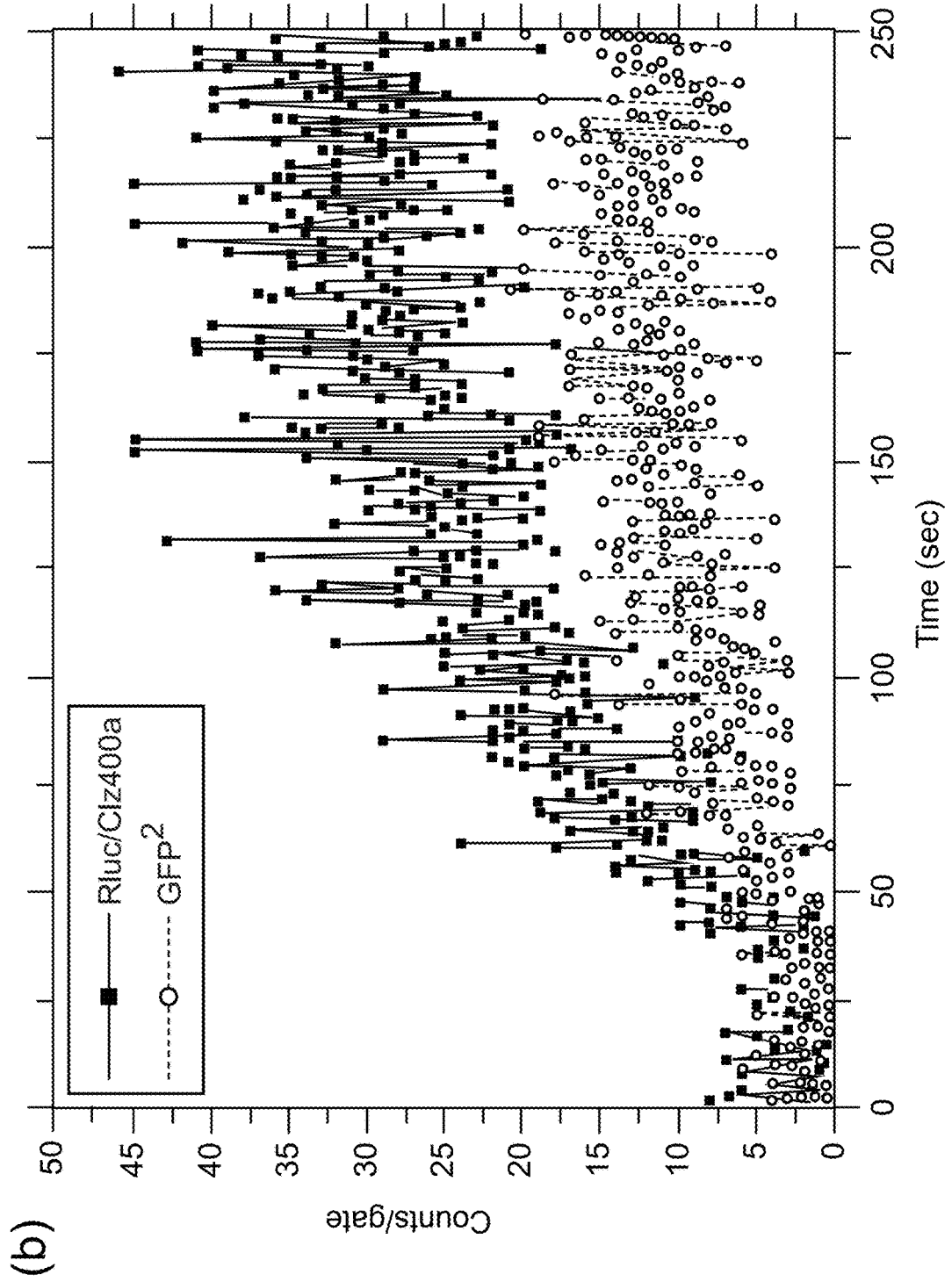


Figure 36

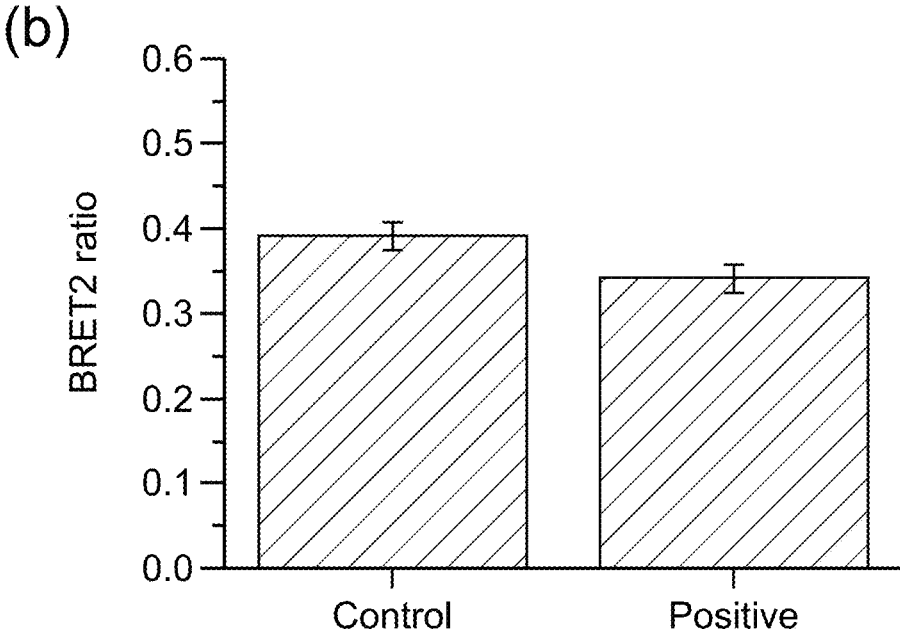
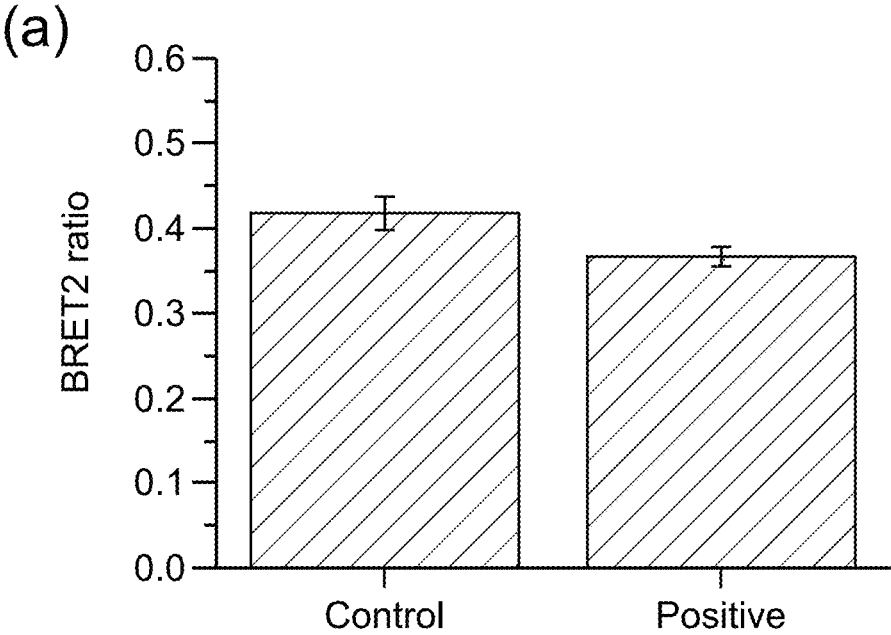


Figure 37

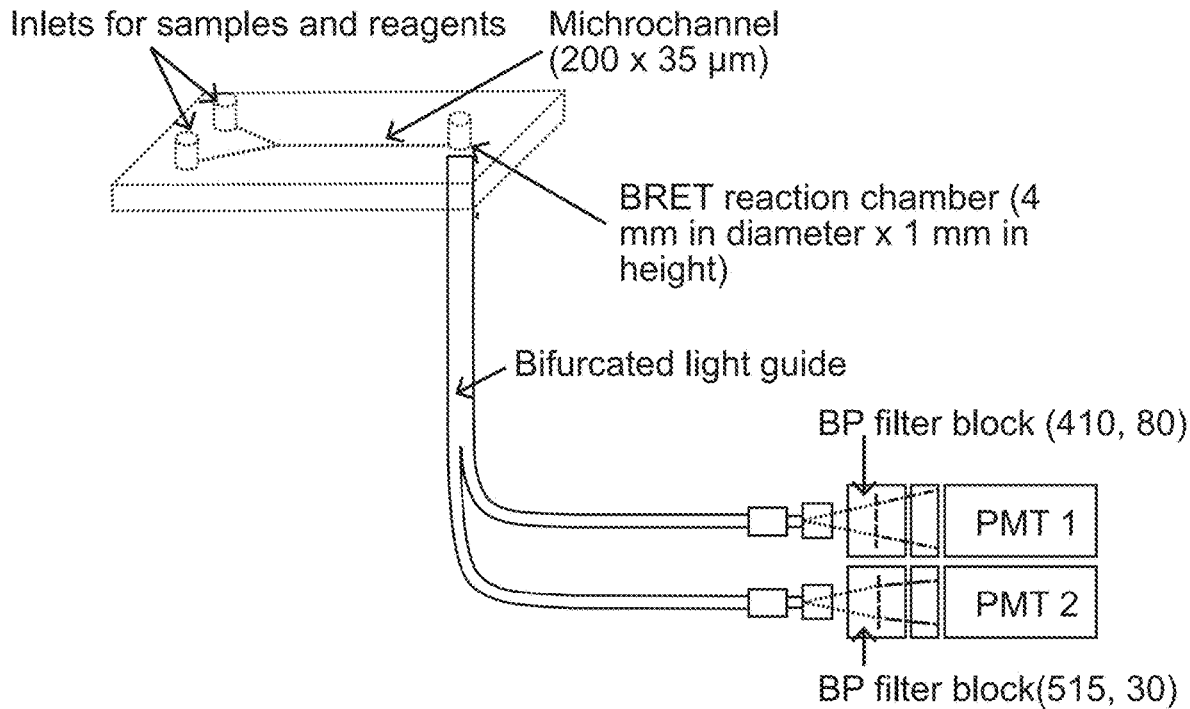


Figure 38

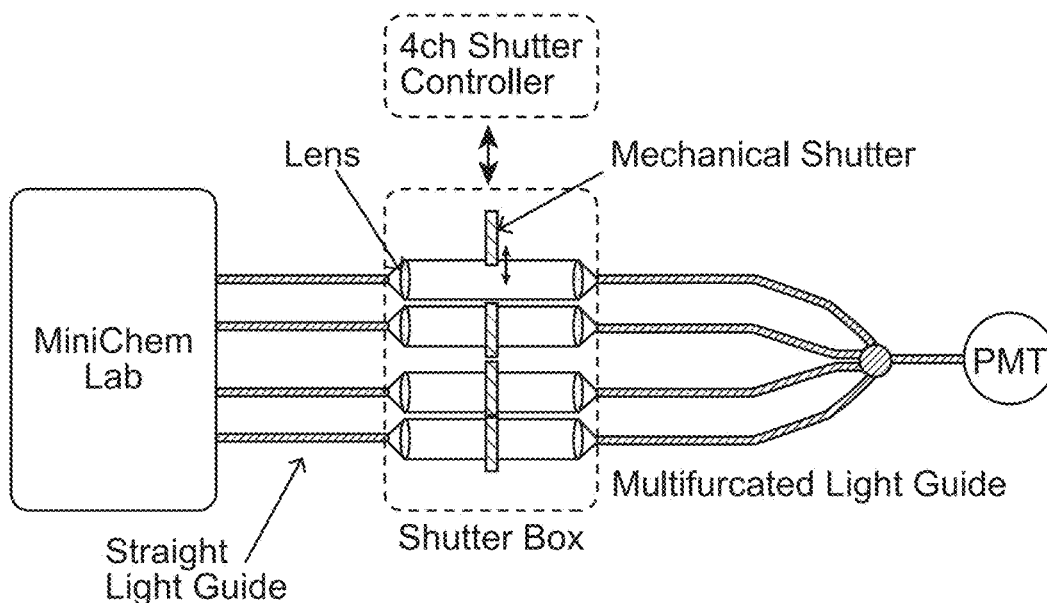


Figure 39

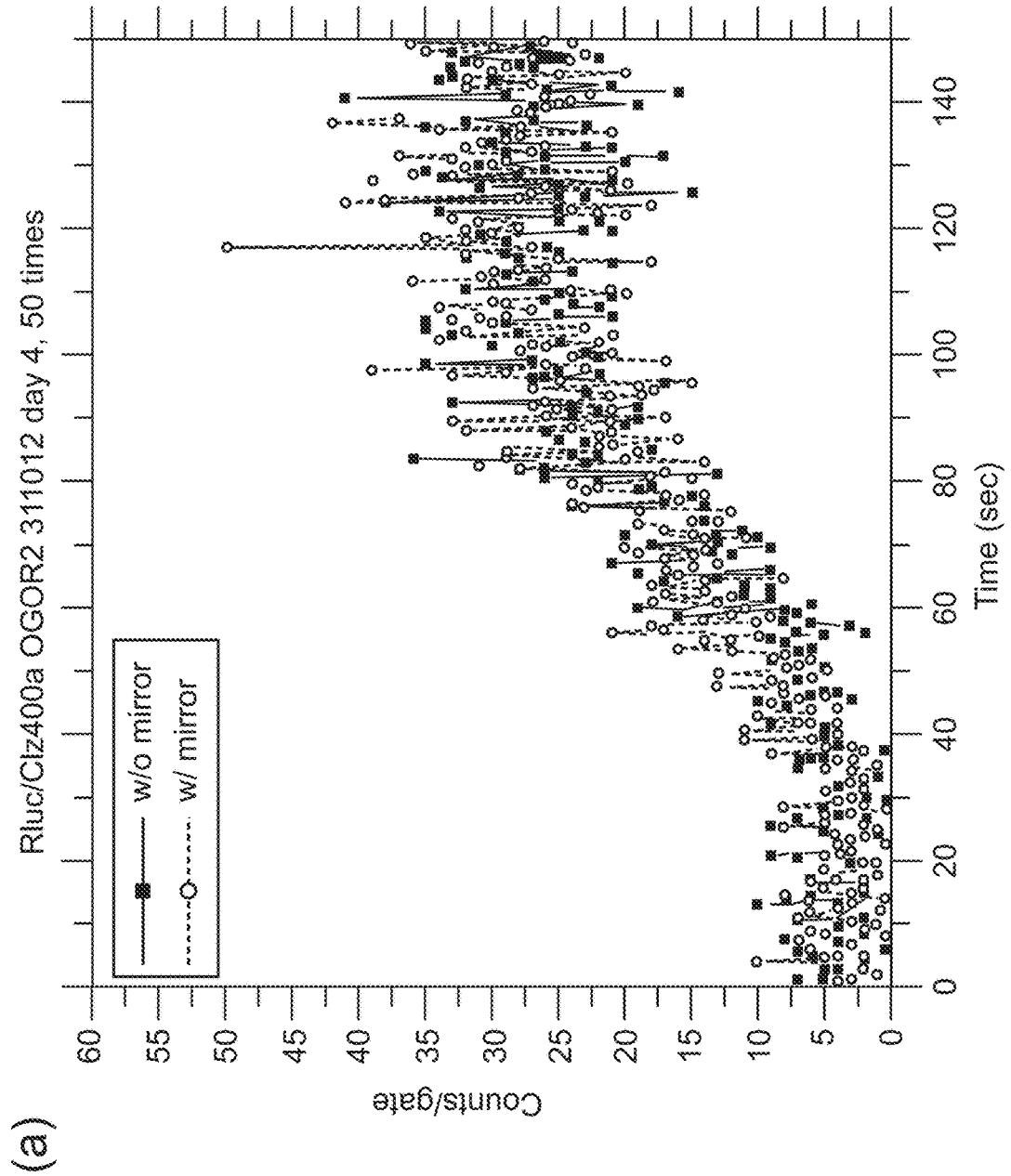


Figure 39 (Cont.)

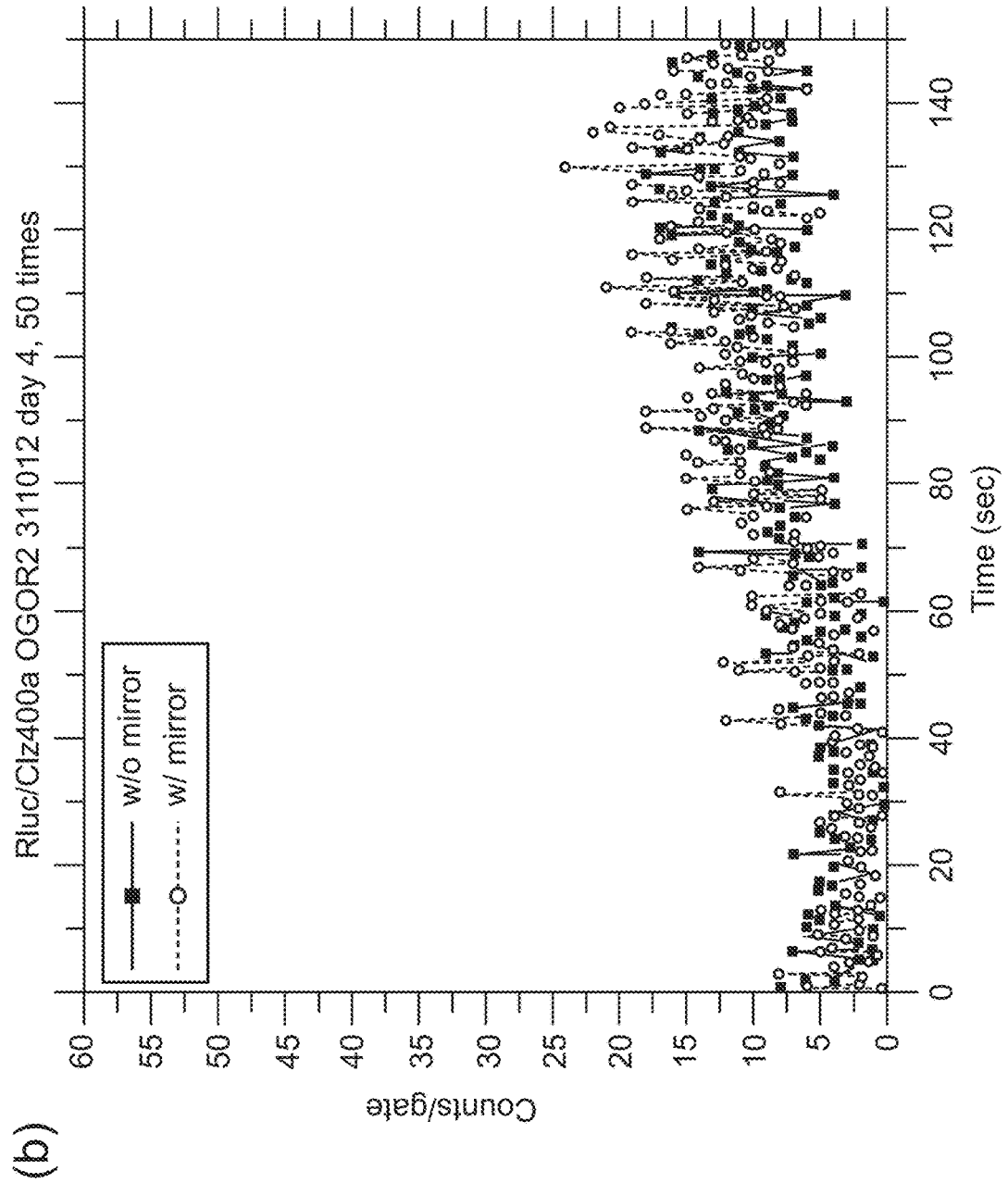


Figure 39 (Cont.)

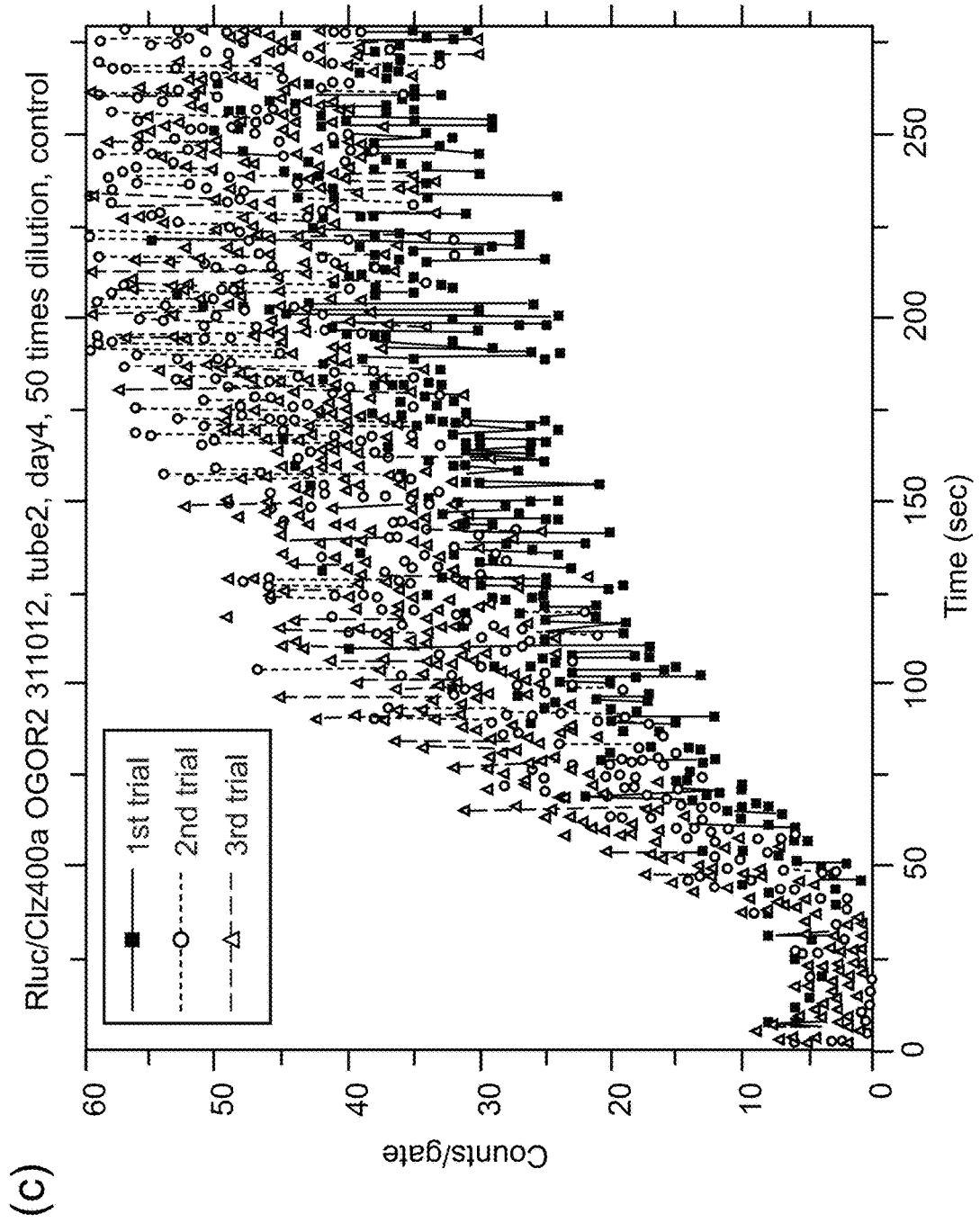


Figure 39 (Cont.)

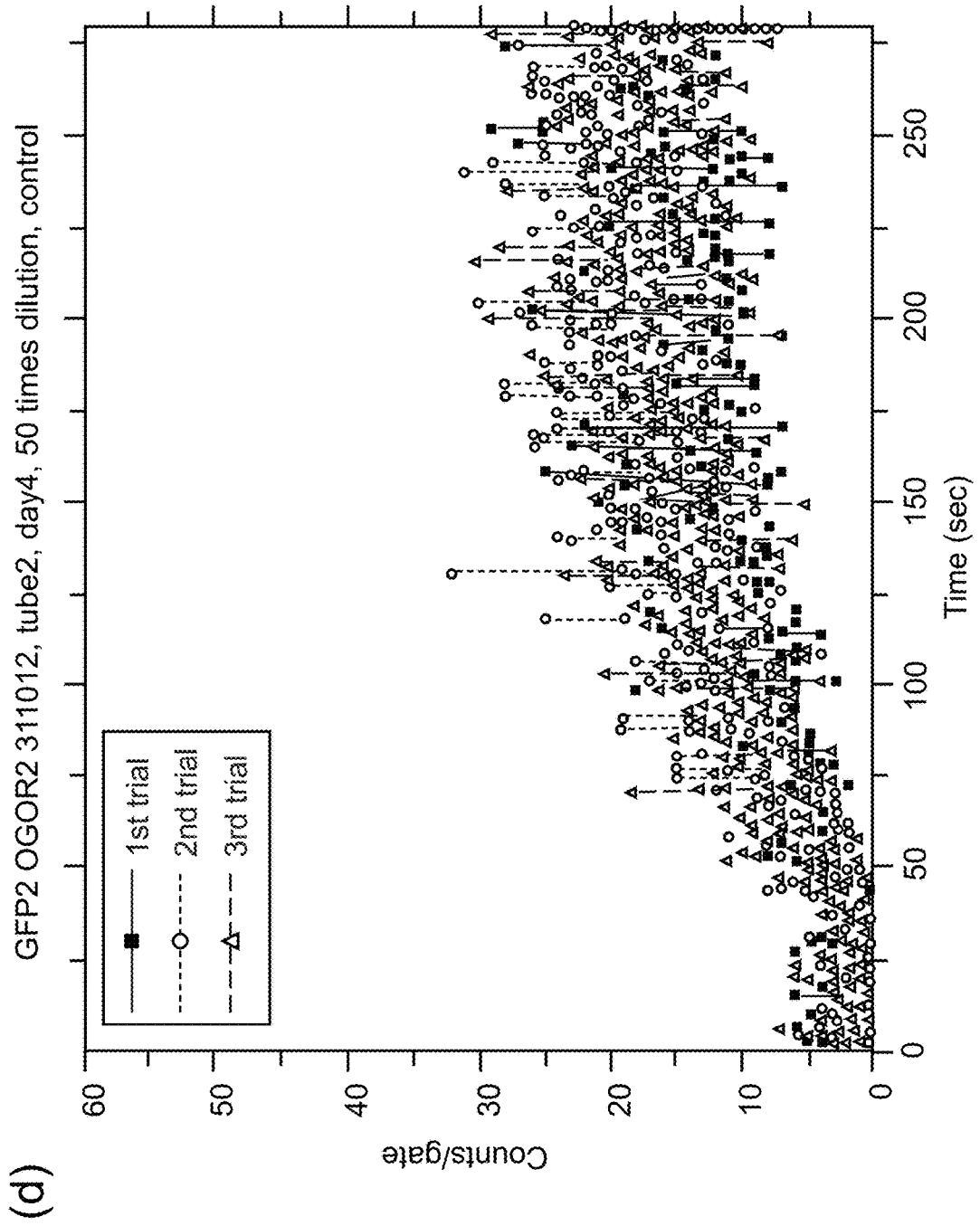


Figure 40

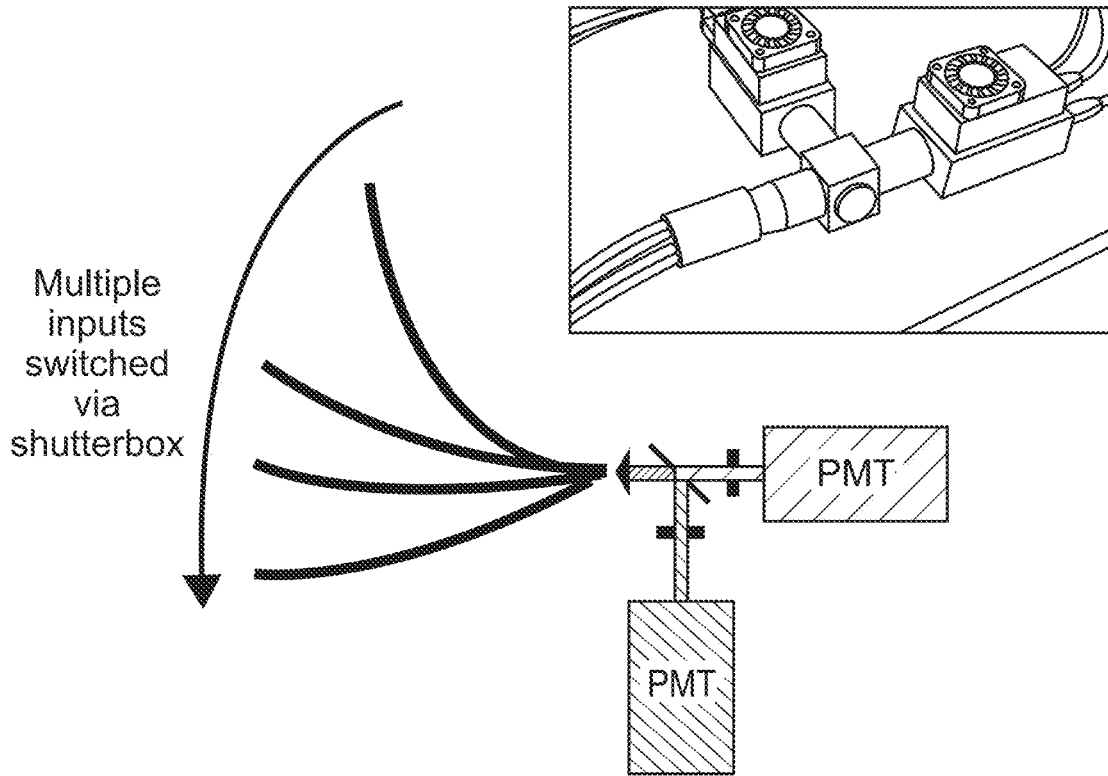


Figure 41

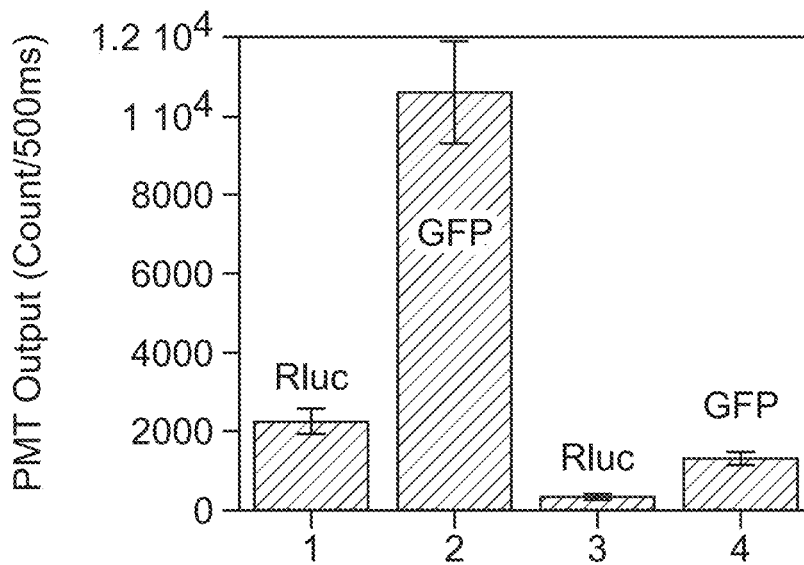


Figure 42

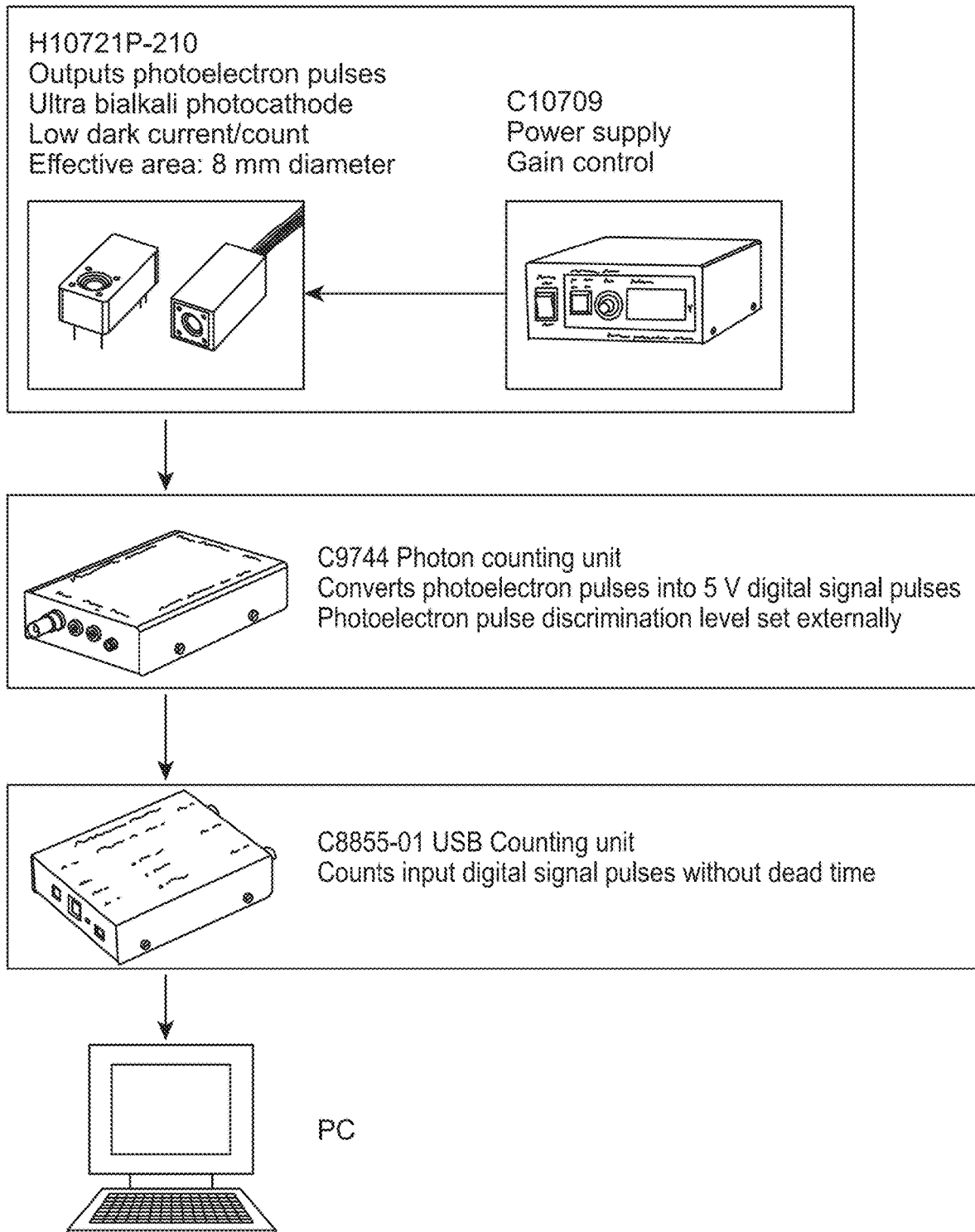


Figure 43

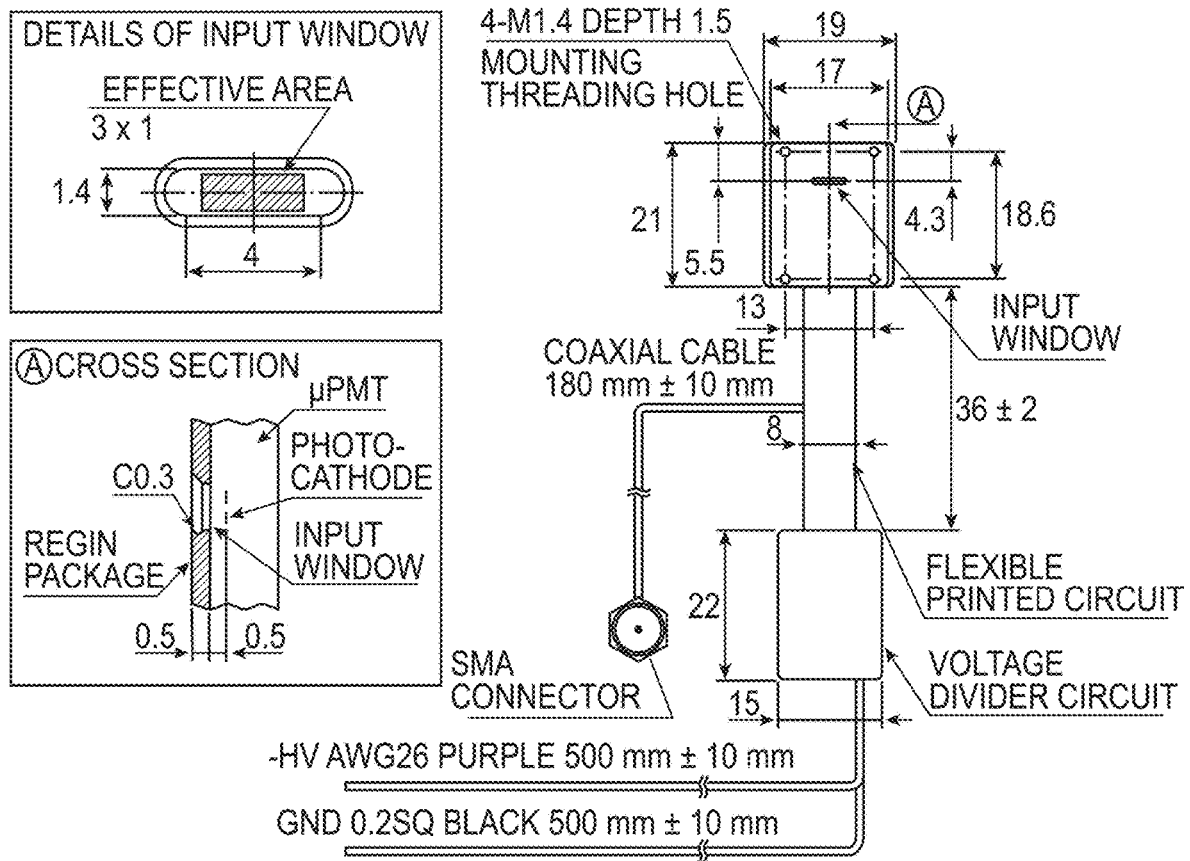


Figure 44

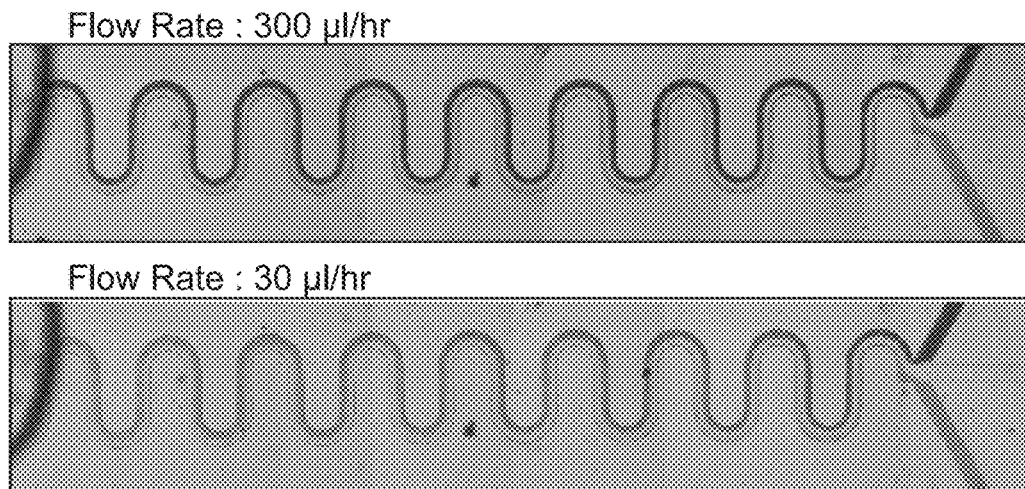


Figure 45

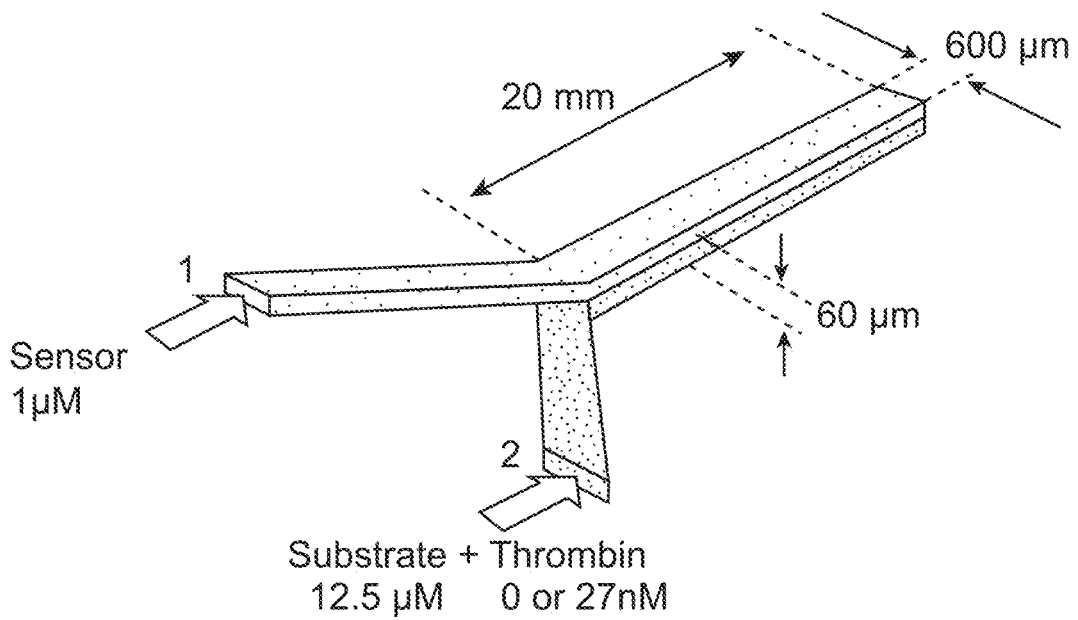


Figure 46

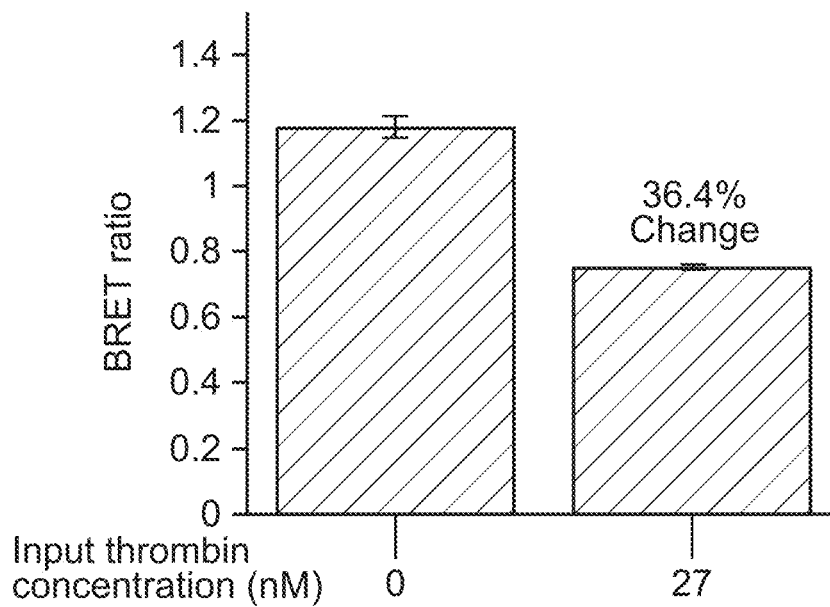


Figure 47

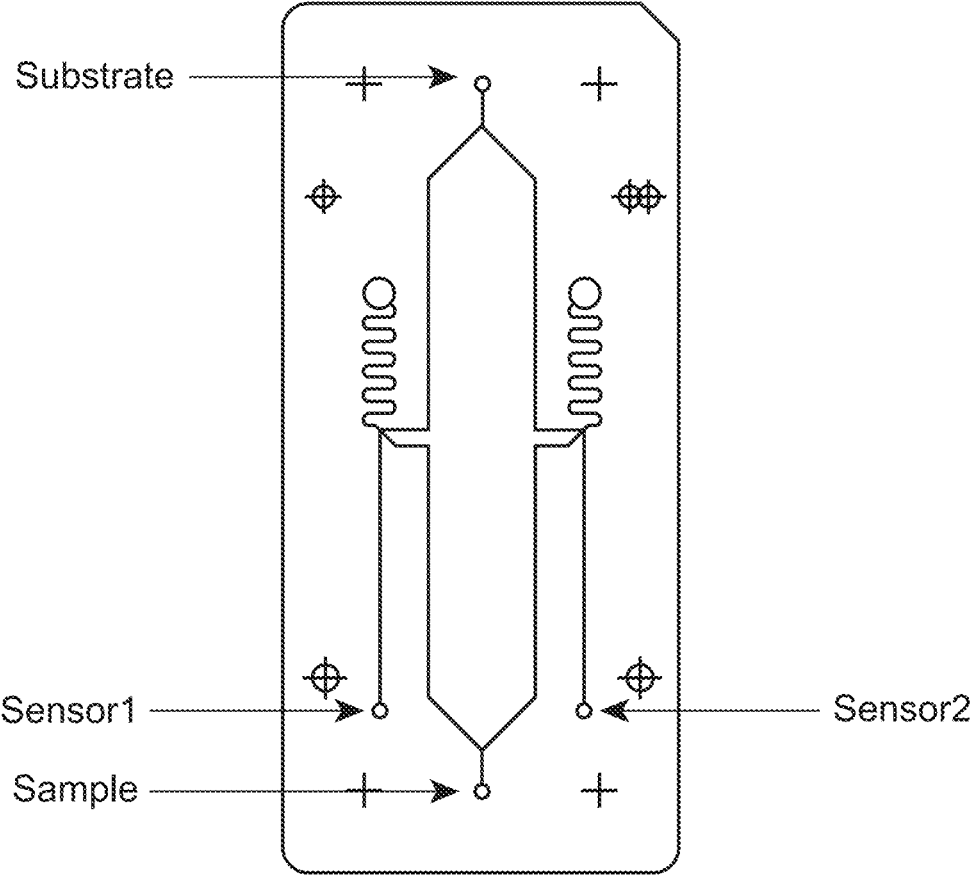


Figure 48

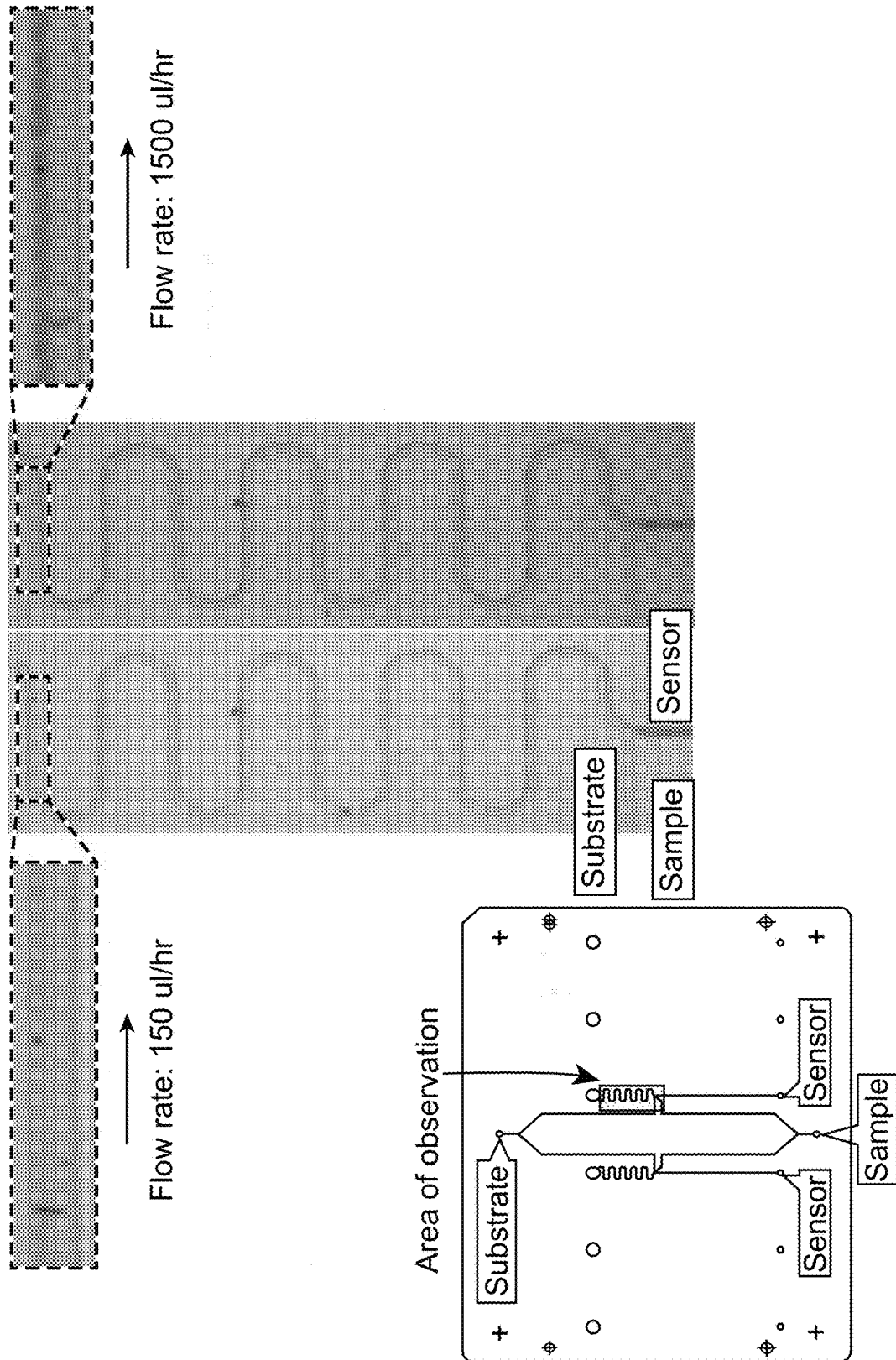


Figure 49

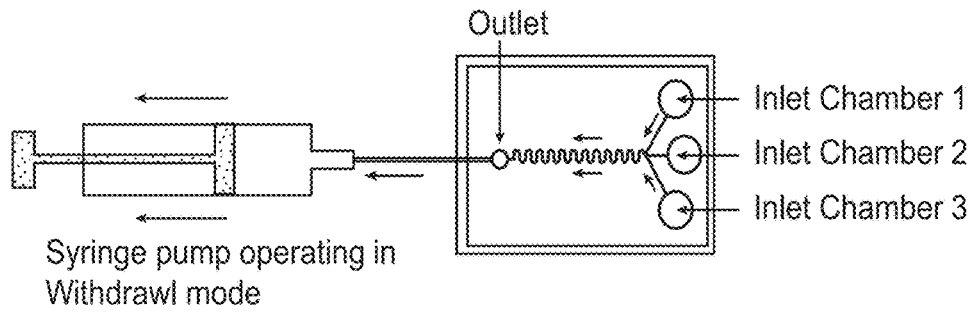


Figure 50

Possibility of independent operation with different flow rates in each mixing channel

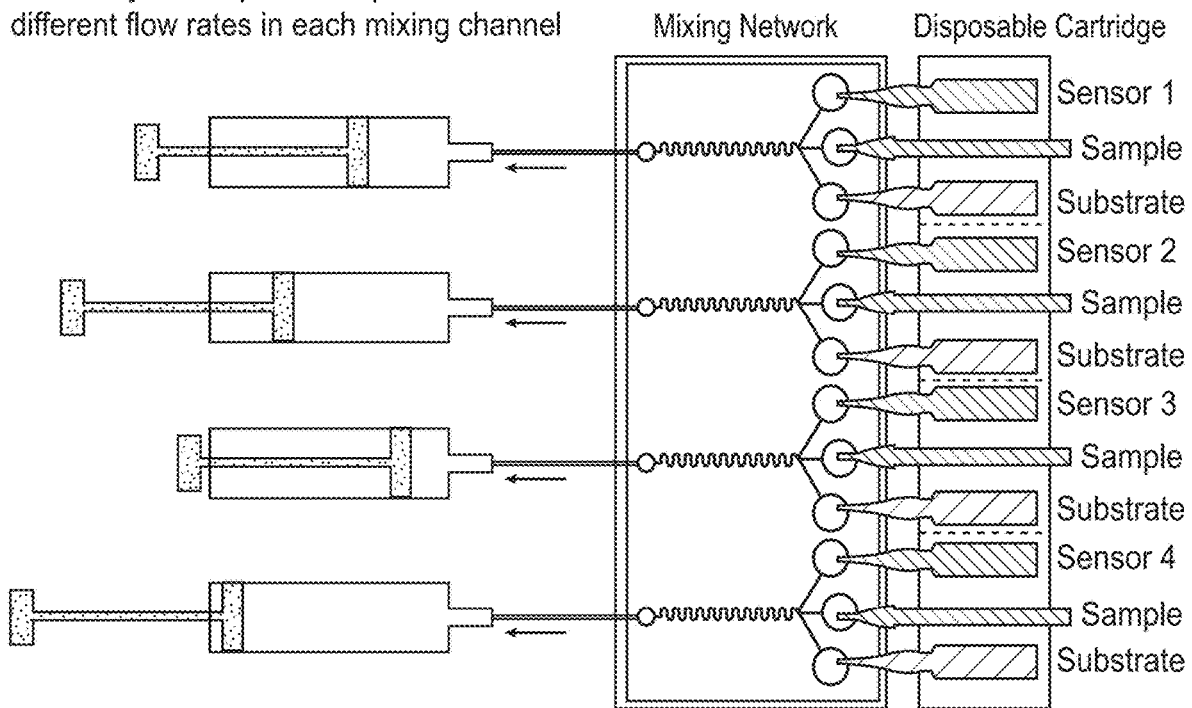


Figure 51

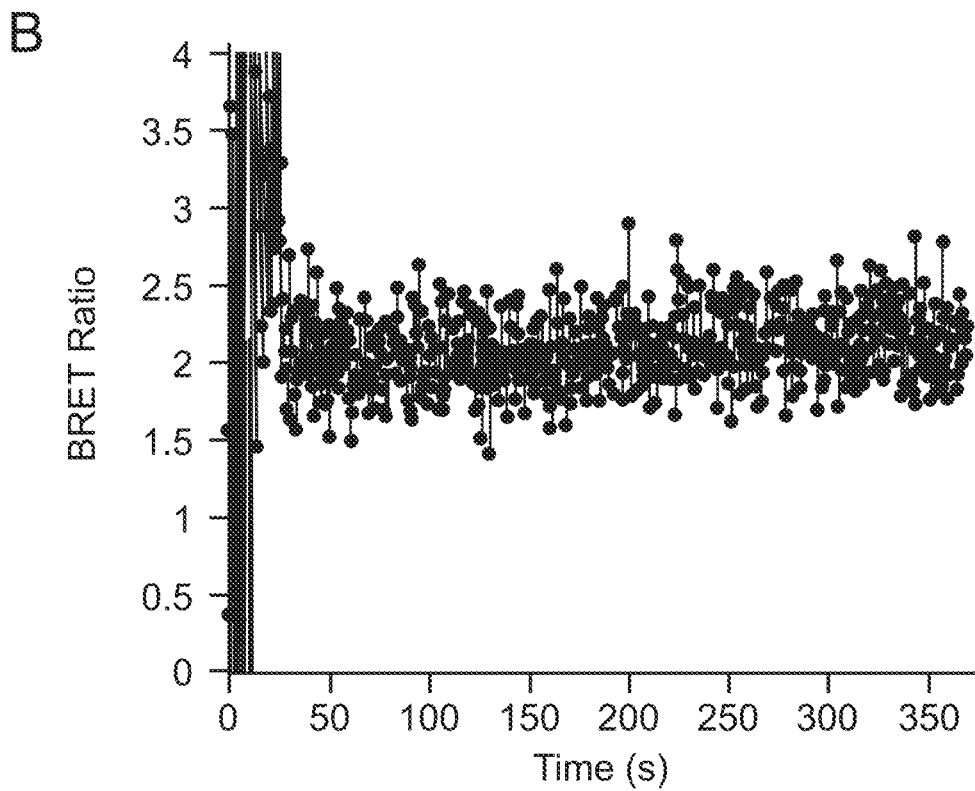
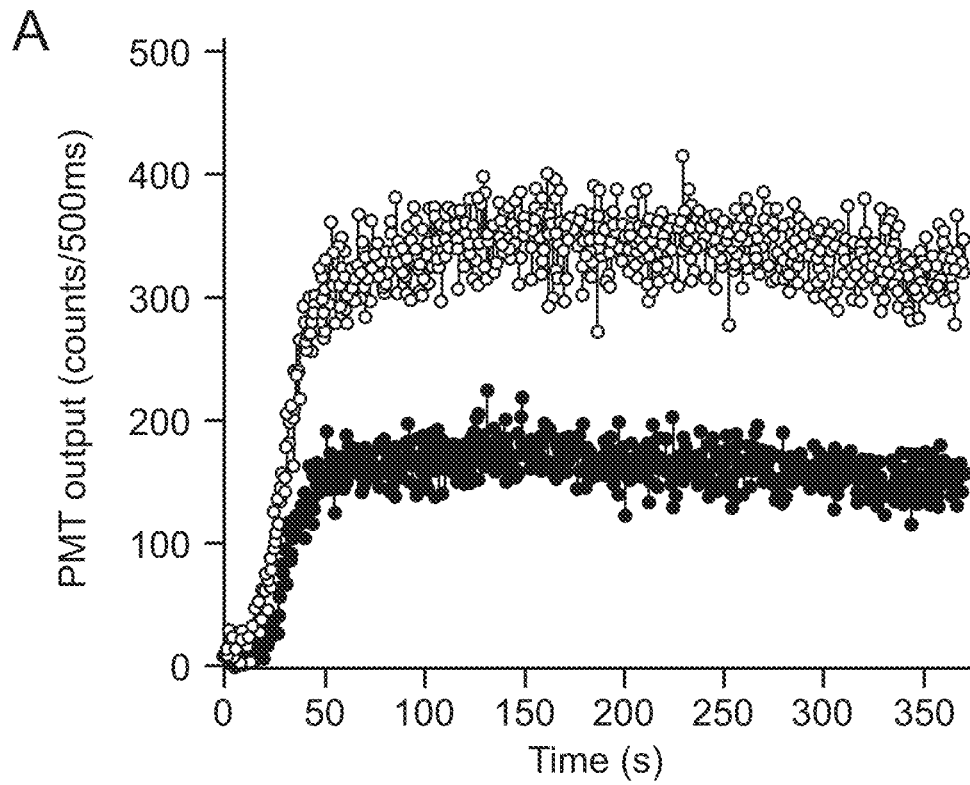


Figure 51 (Cont.)

C

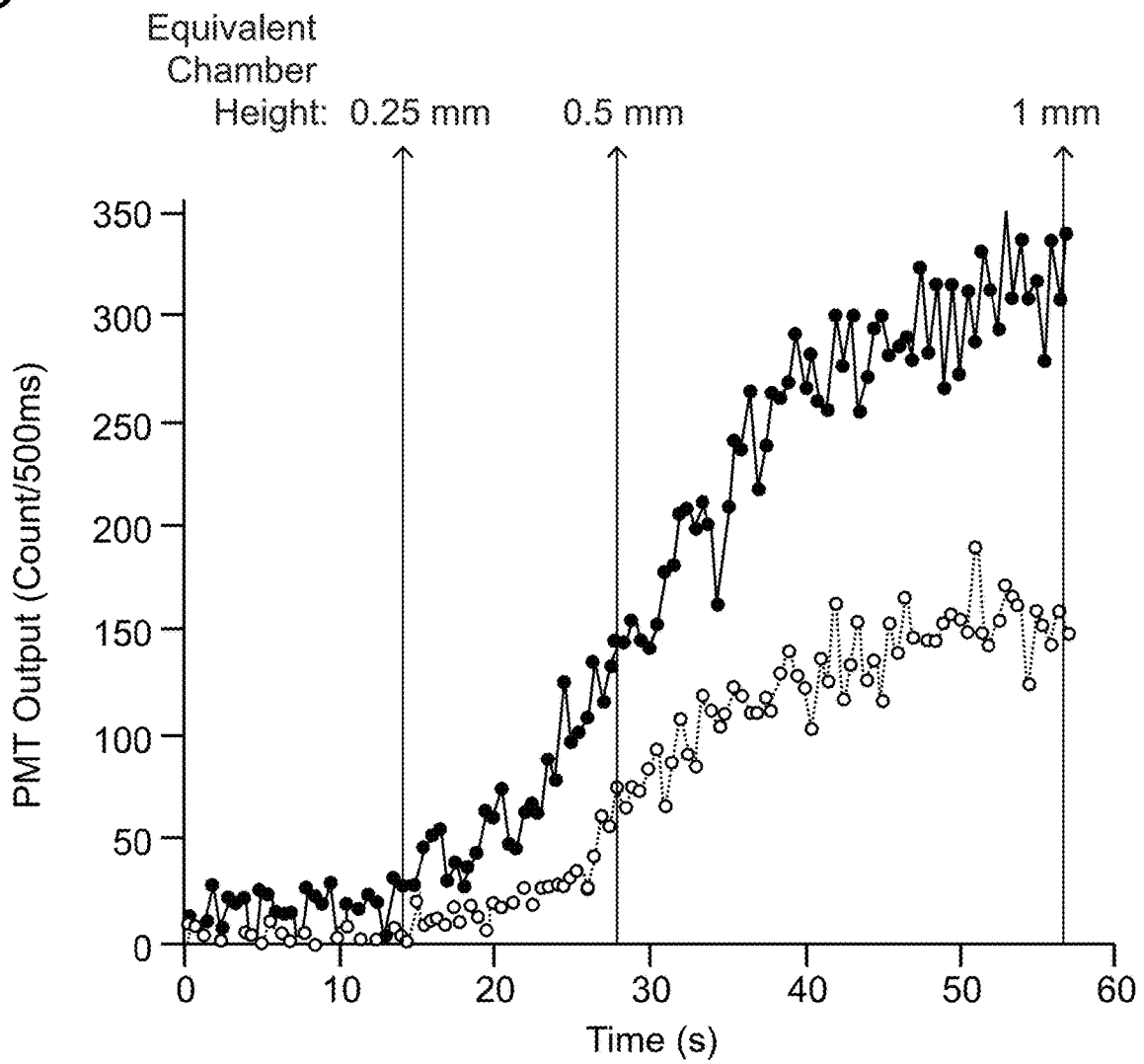


Figure 52

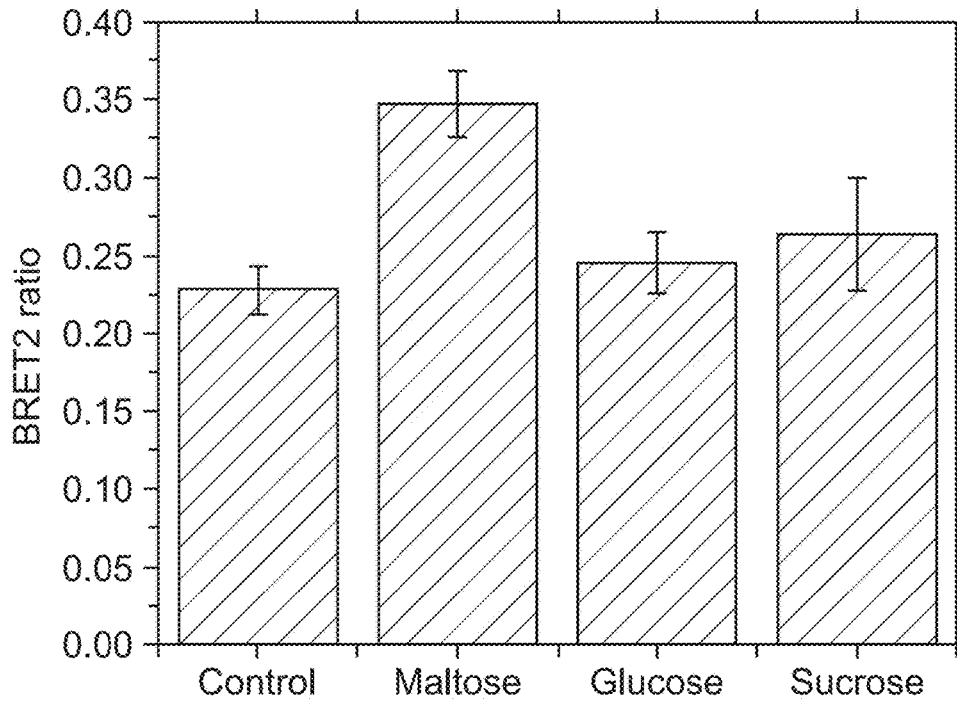


Figure 53

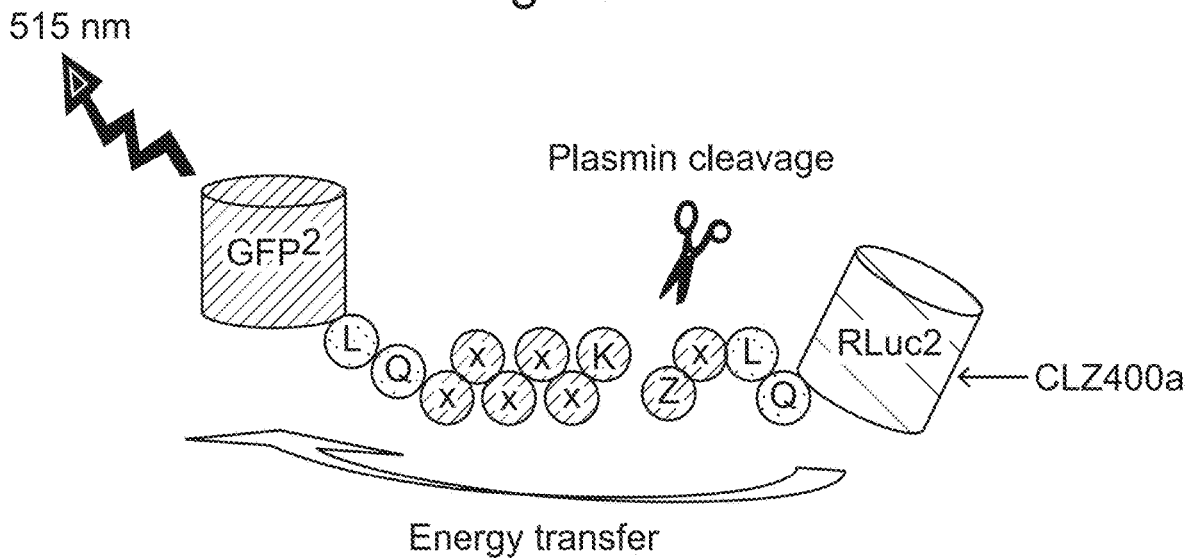


Figure 54

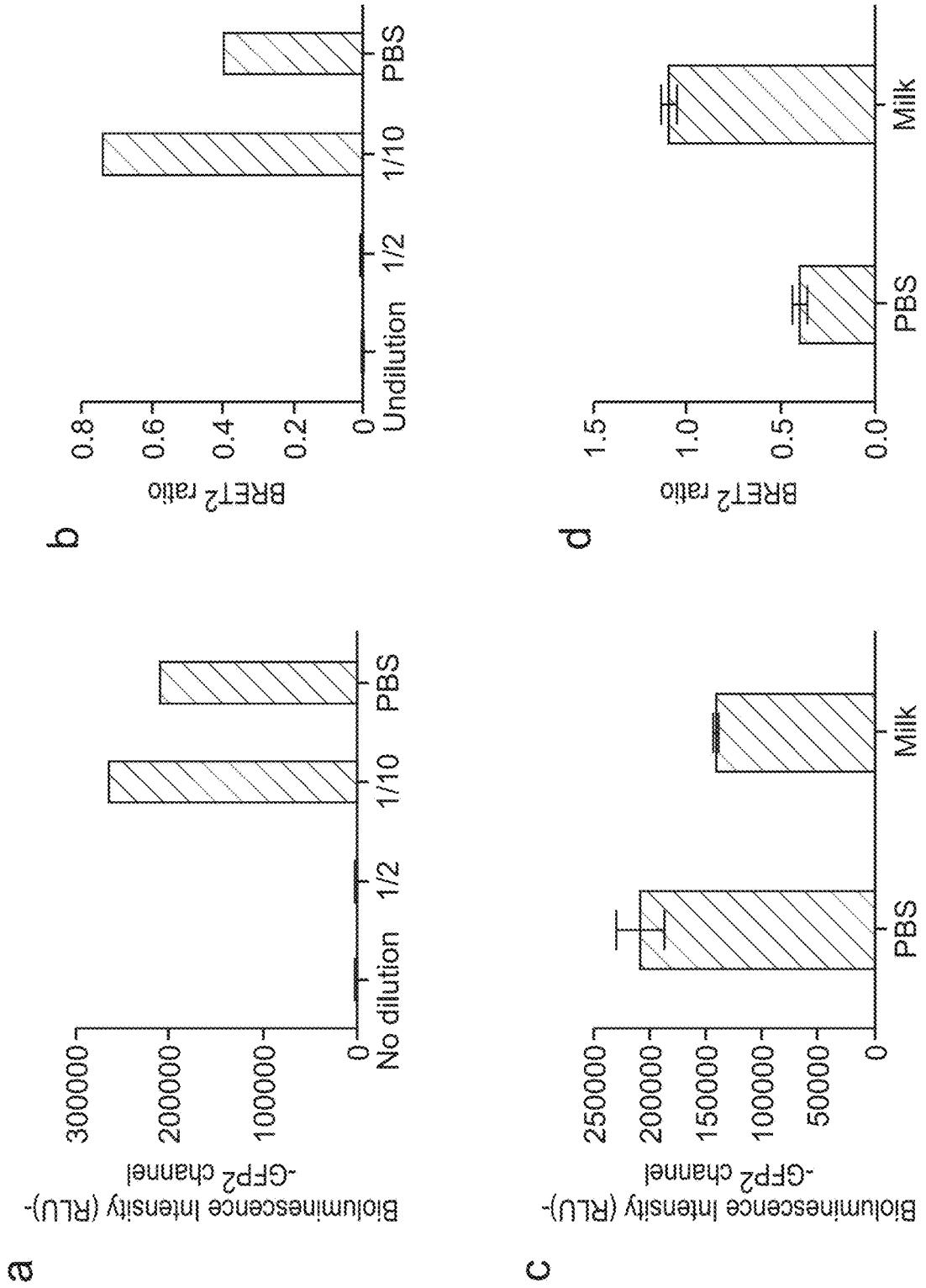
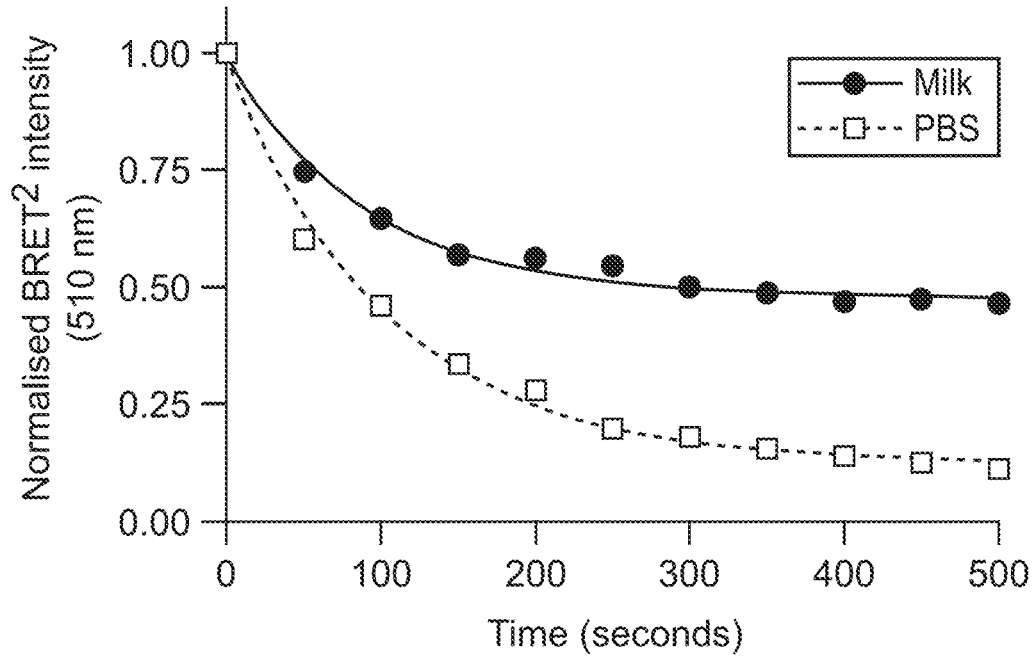


Figure 55

a.



b.

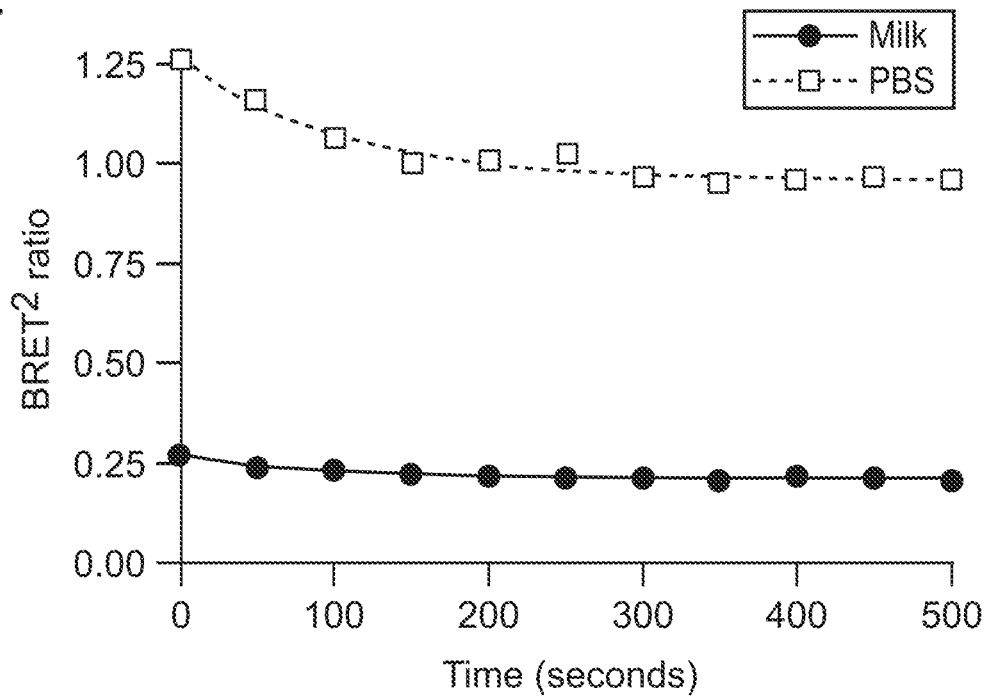


Figure 56

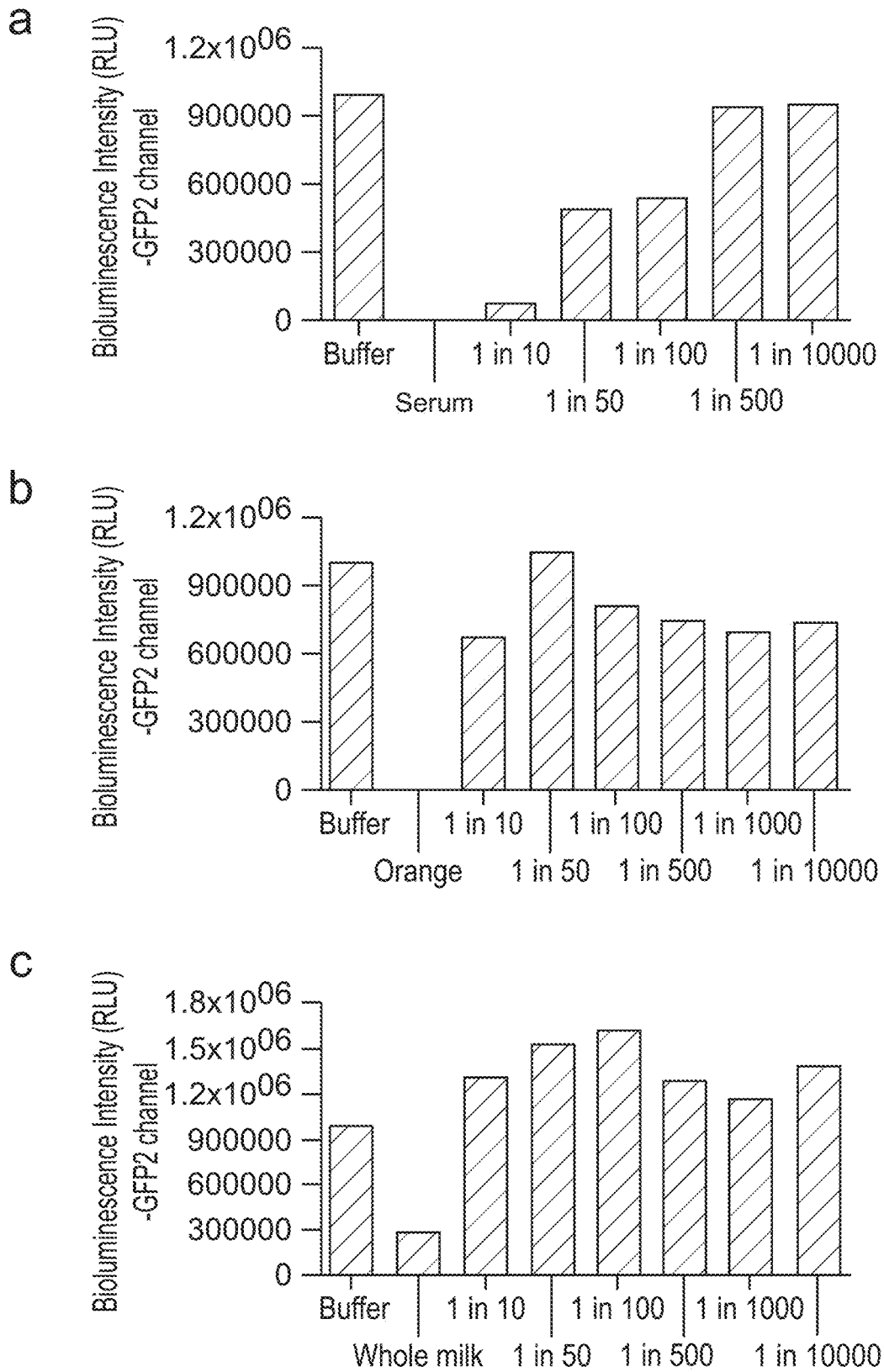


Figure 57

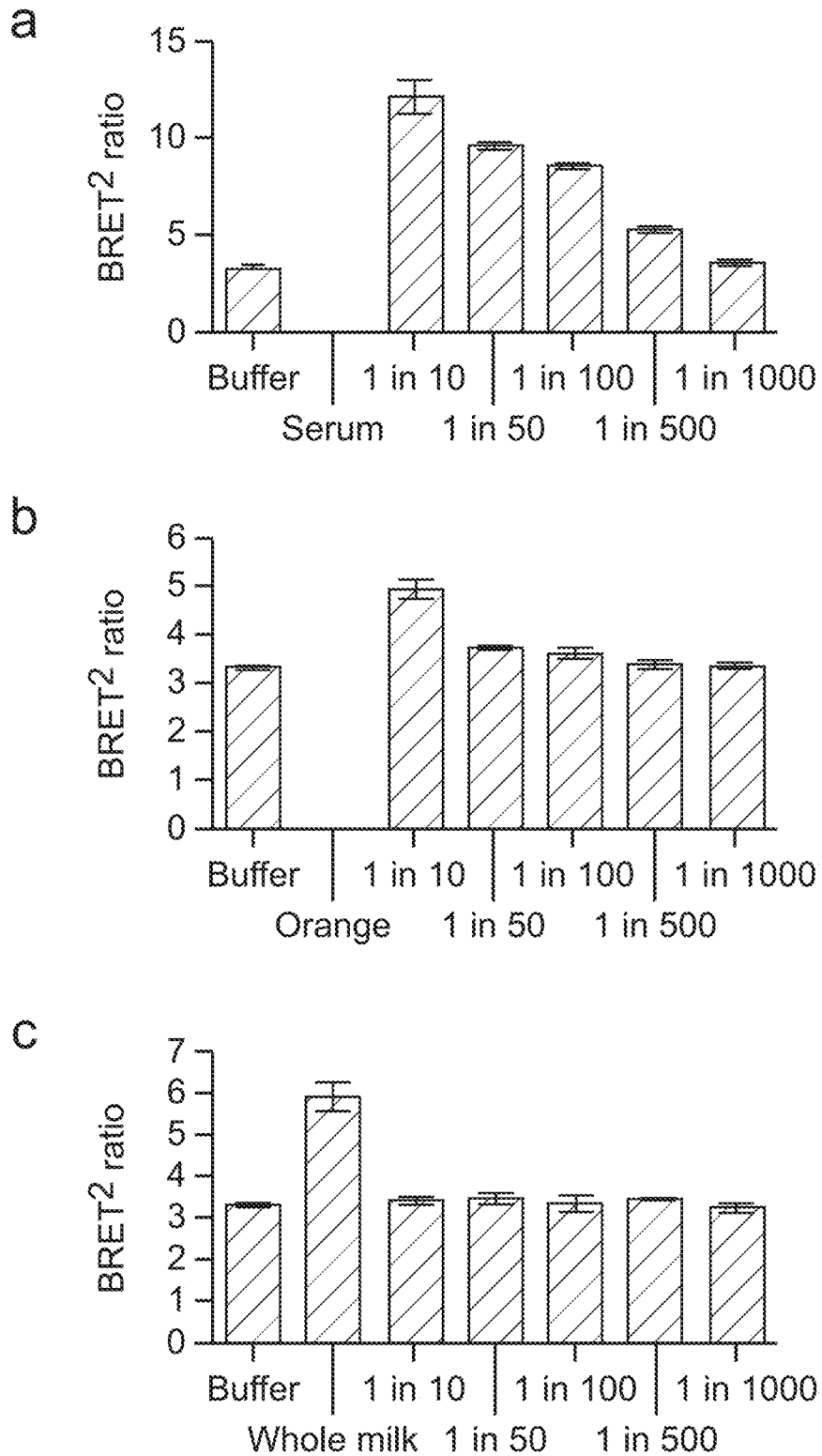


Figure 58

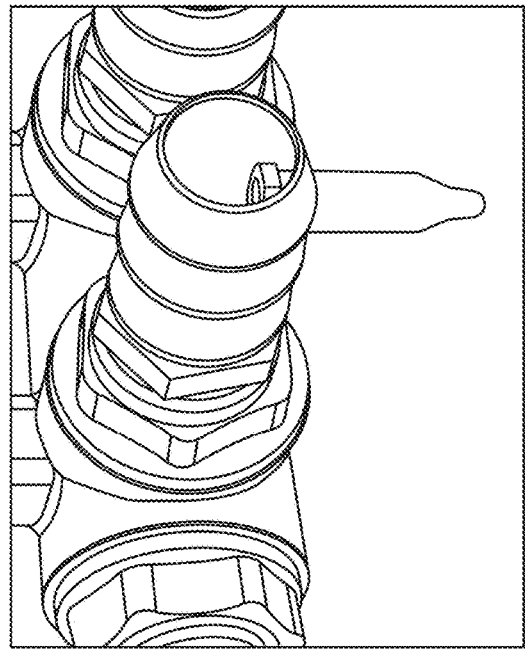
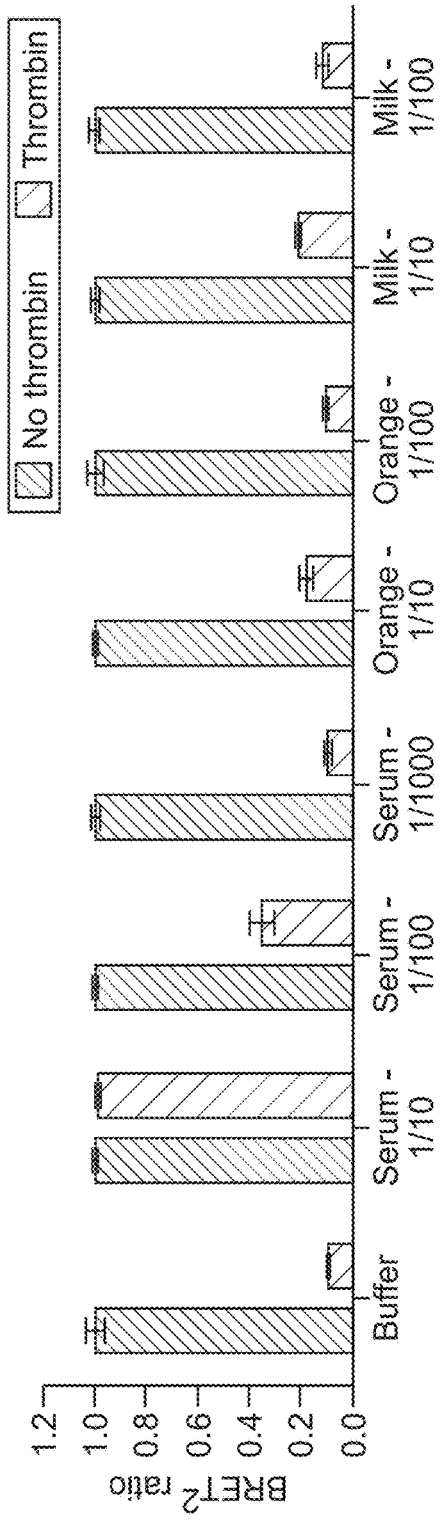


Figure 59

Figure 60

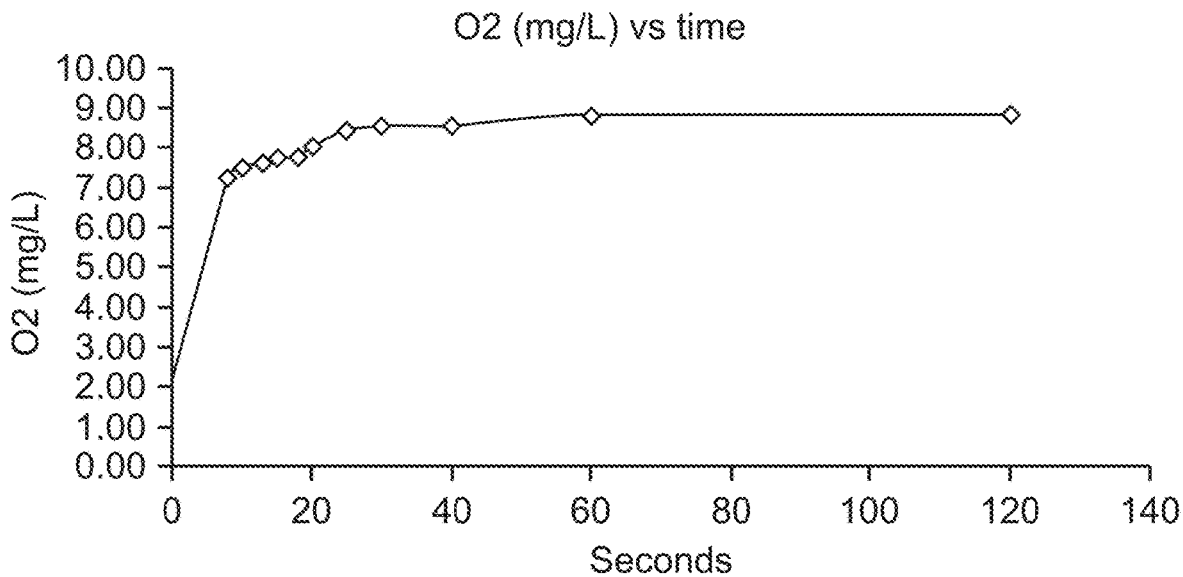


Figure 61

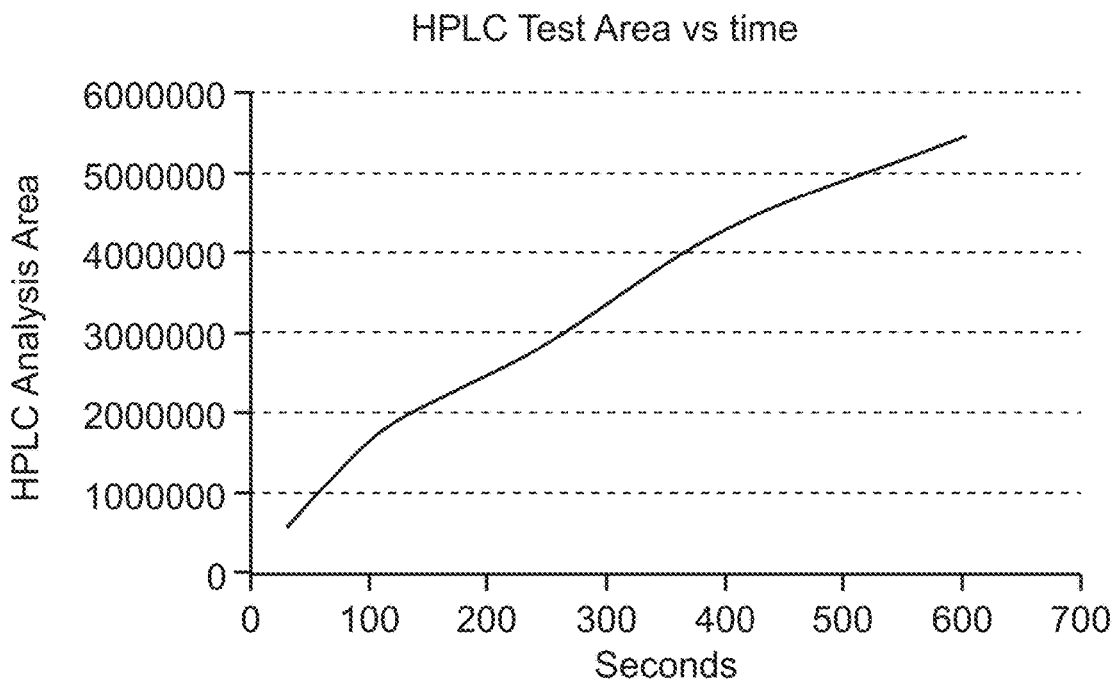


Figure 62

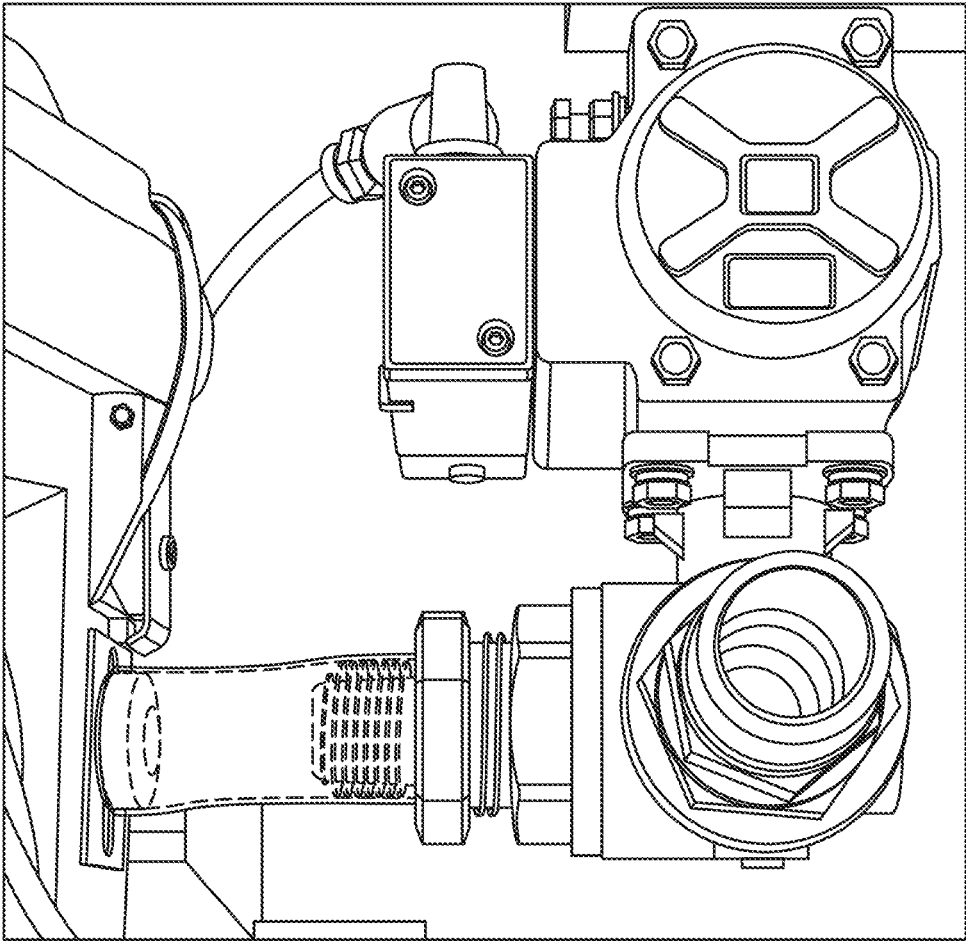


Figure 63

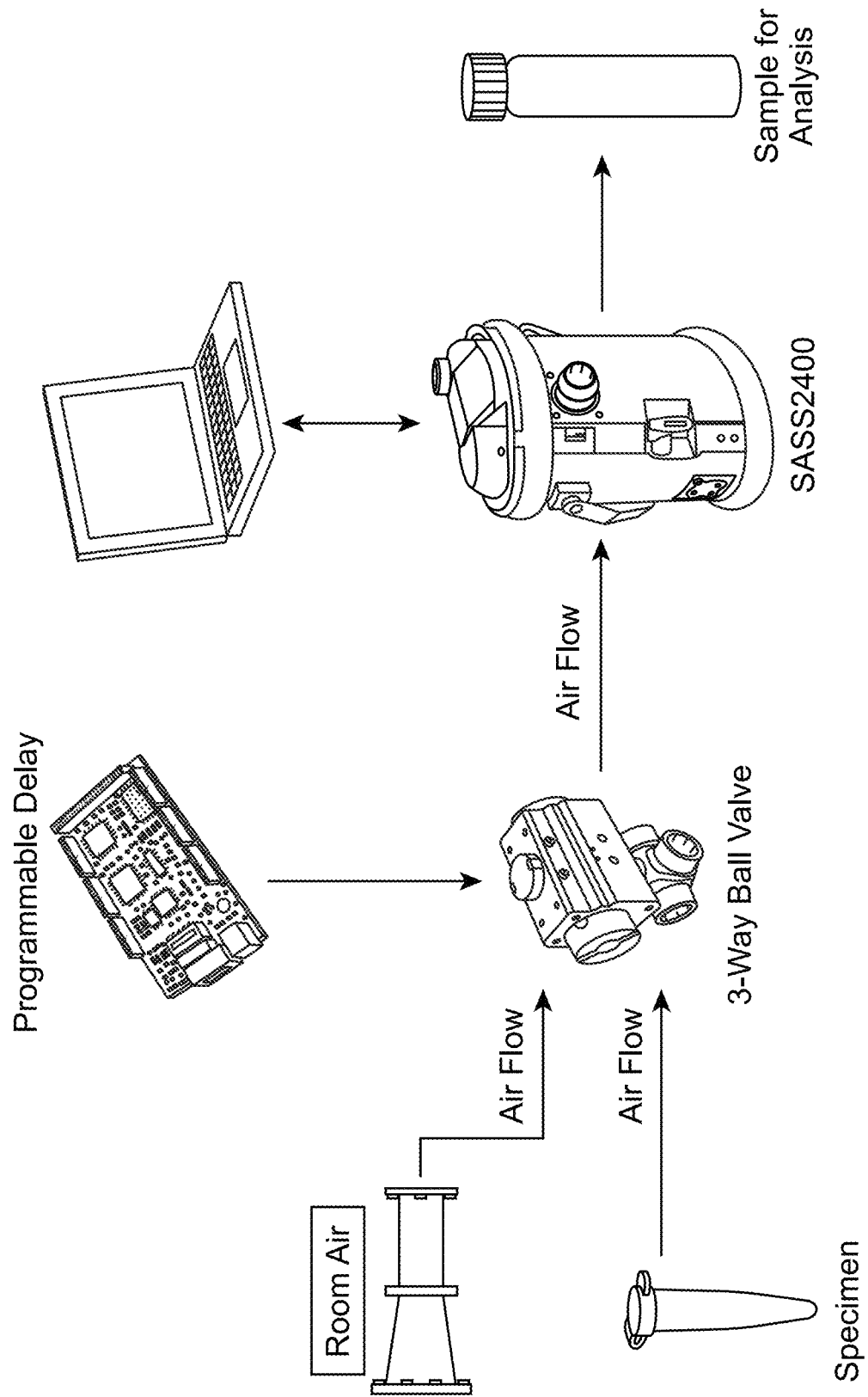


Figure 64

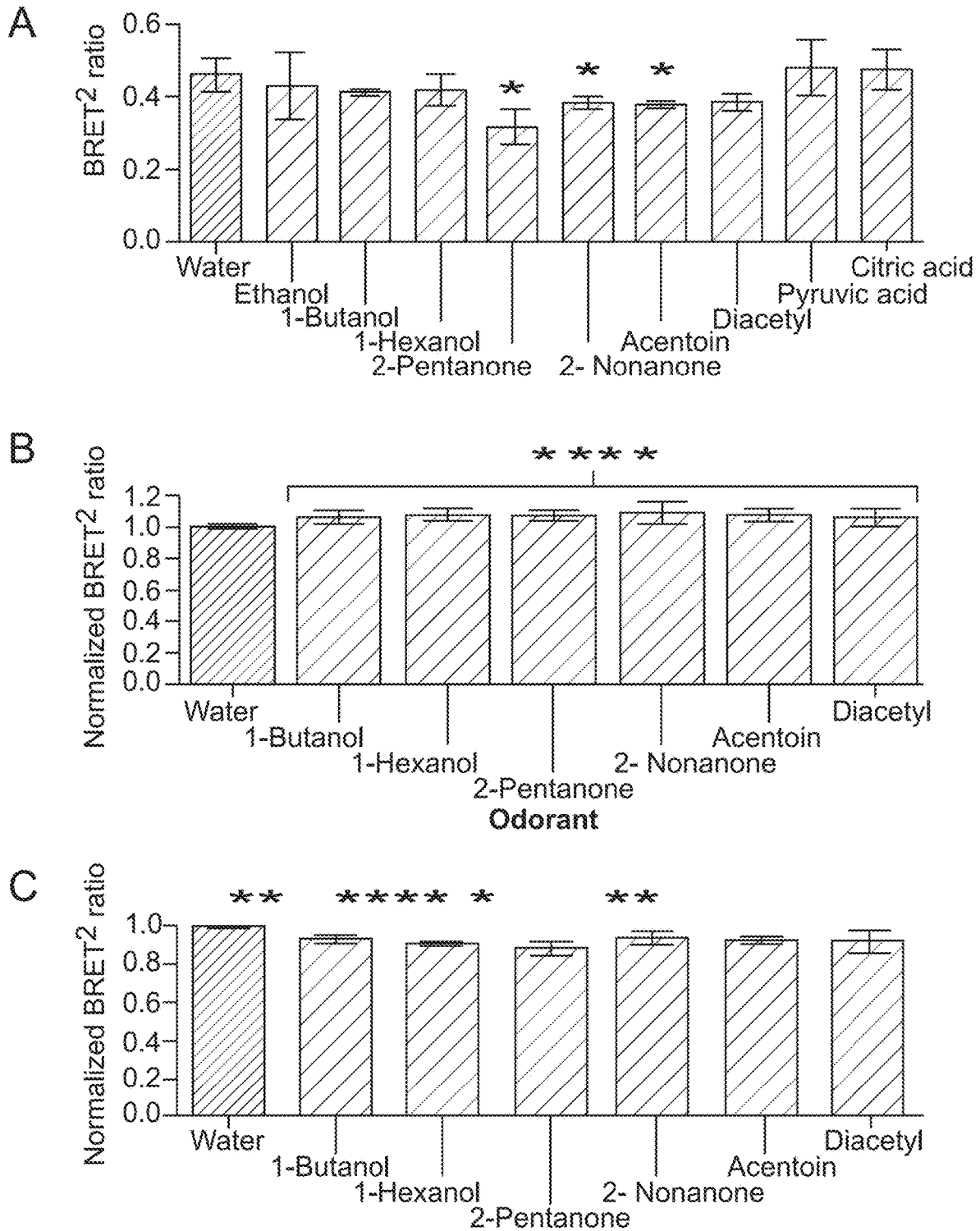


Figure 65

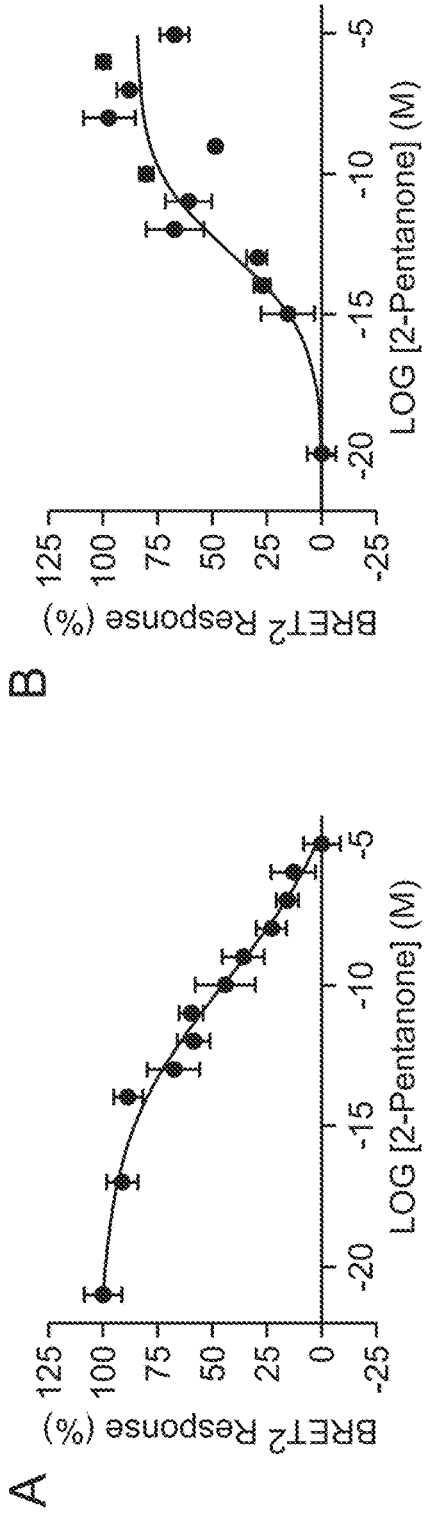


Figure 66

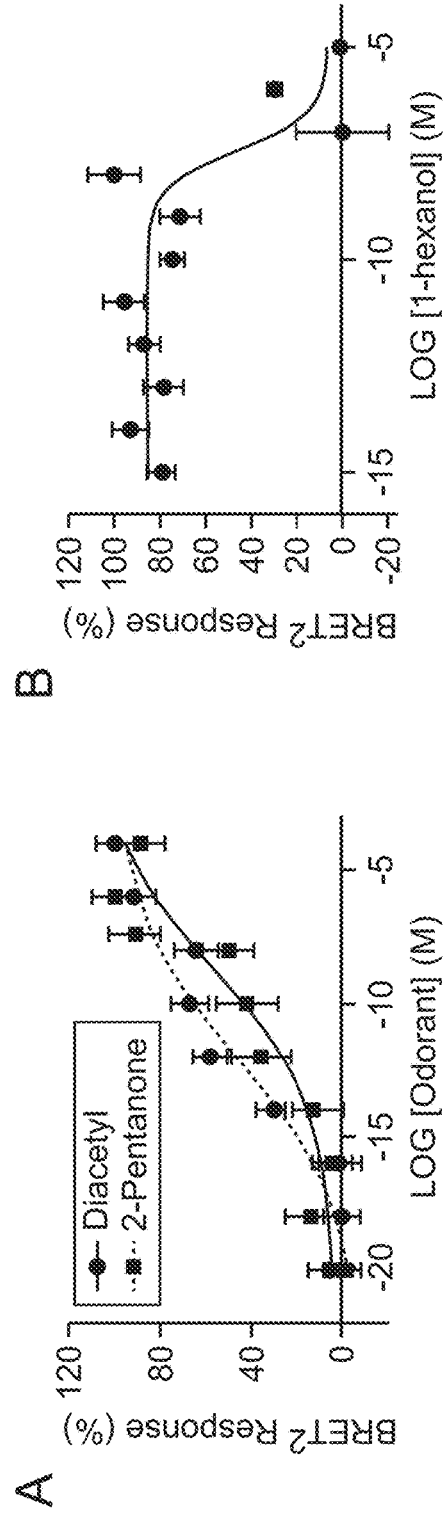


Figure 67

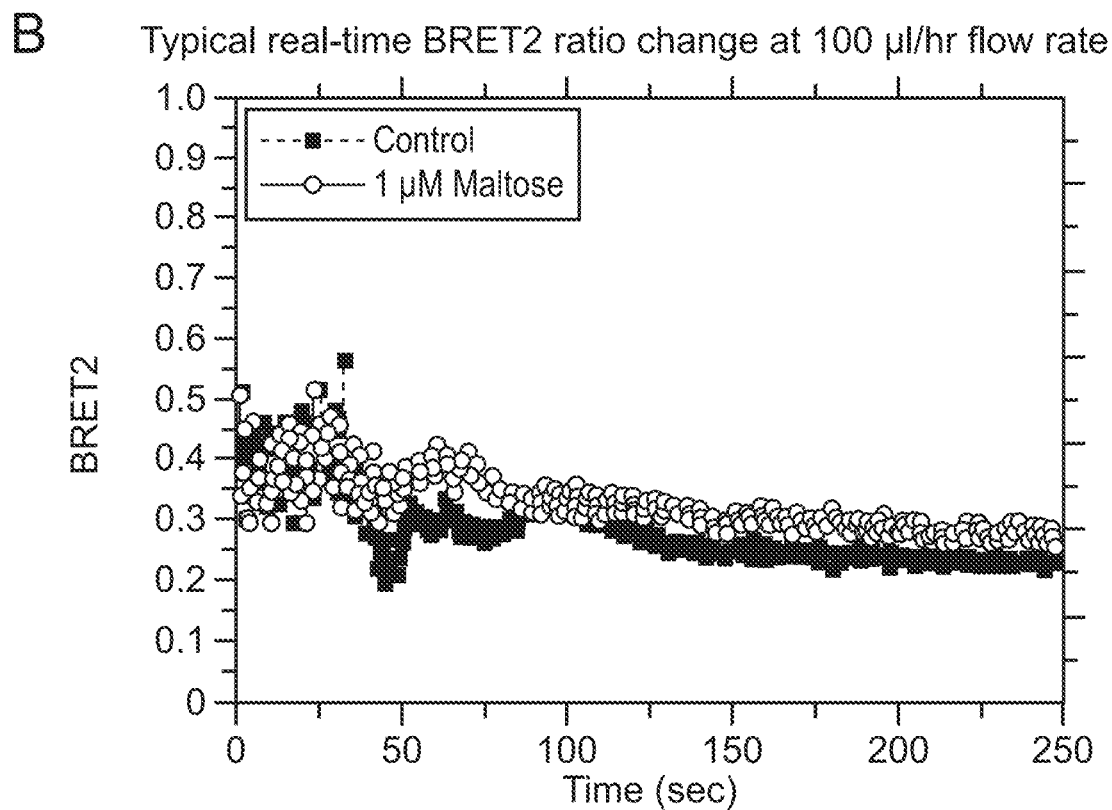
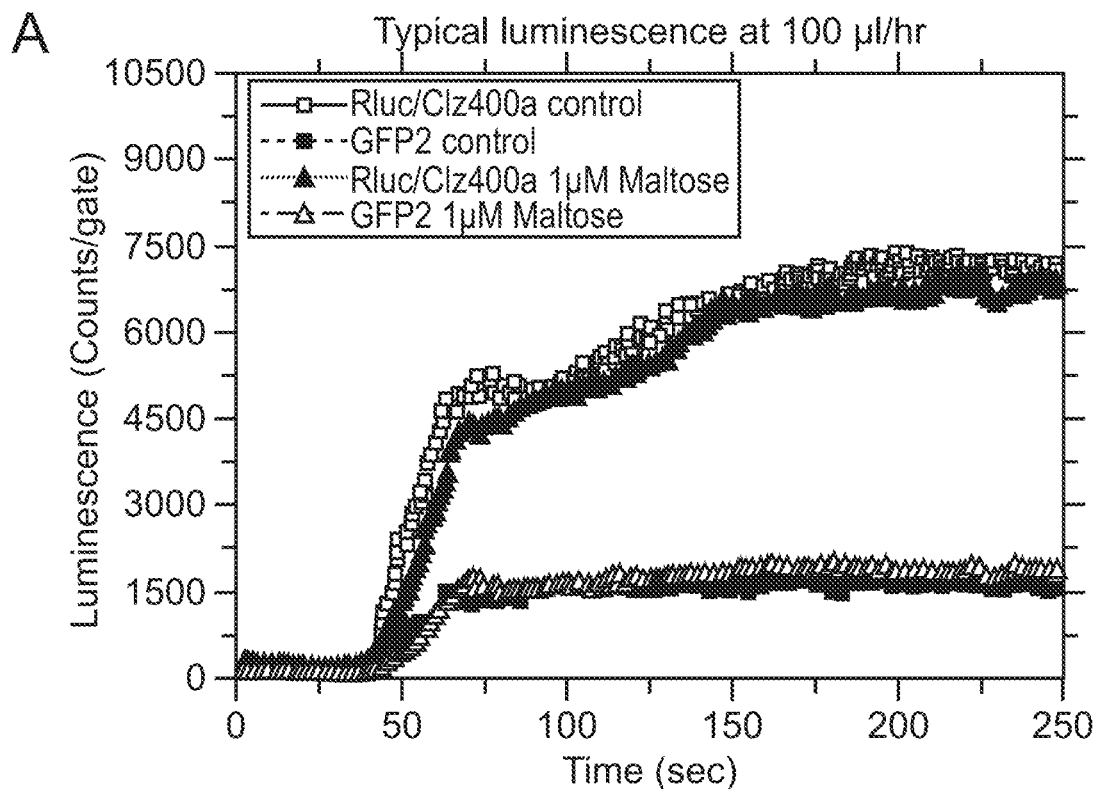
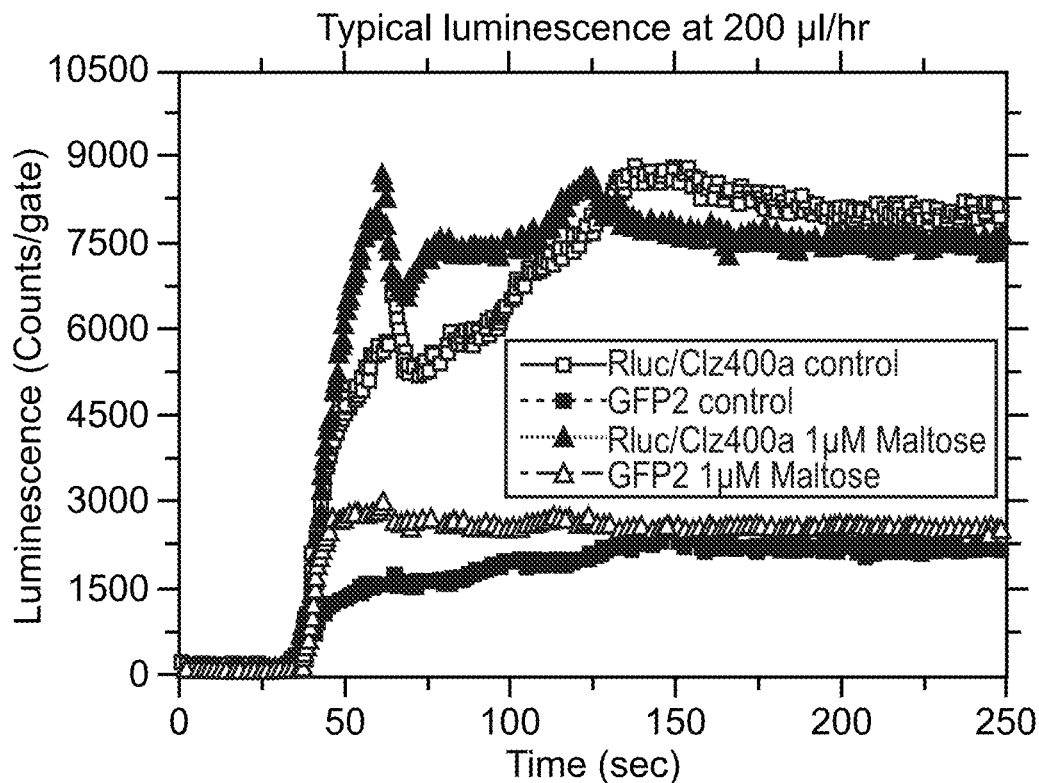


Figure 67 (Cont.)

C



D

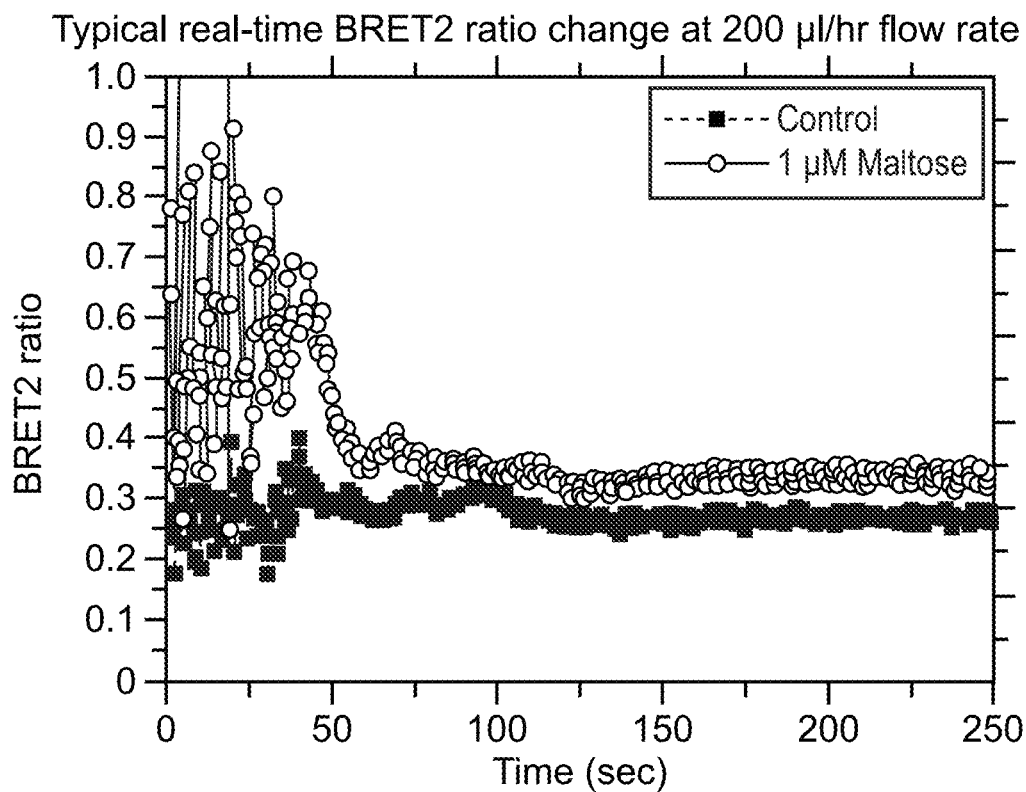
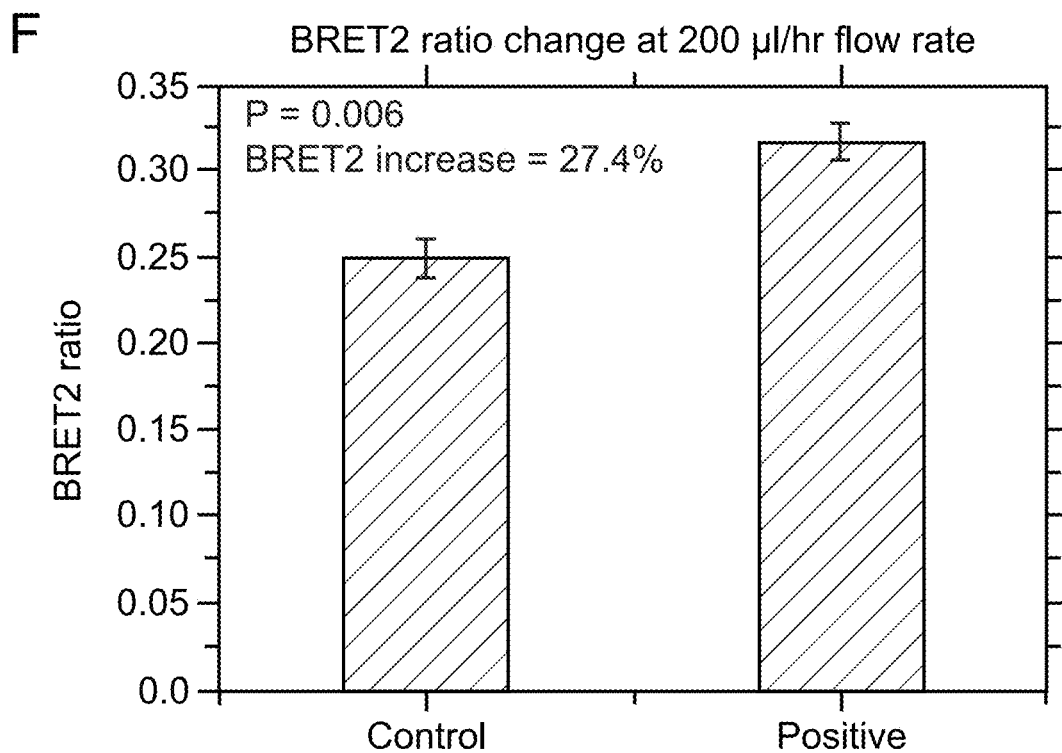
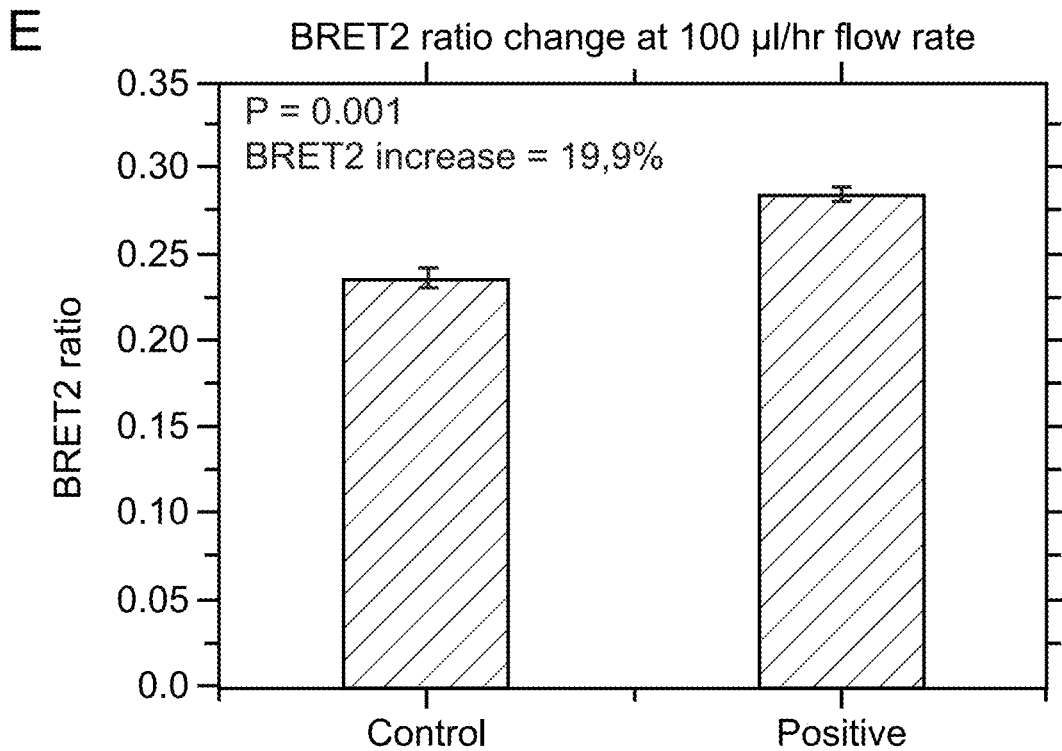


Figure 67 (Cont.)



METHODS AND SYSTEMS FOR DETECTING AN ANALYTE OR CLASSIFYING A SAMPLE

The present application is a continuation of U.S. application Ser. No. 14/387,197, filed Sep. 22, 2014, which application is a national phase application under 35 USC § 371 of International Patent Application No. PCT/AU2013/000378, filed Apr. 15, 2013, which application claims priority from Provisional Patent Application No. 61/624,899 filed on Apr. 16, 2012 and claims priority to Australian Provisional Patent Application No 2013204332 filed on Apr. 12, 2013, the content of which is incorporated herein by reference.

FIELD OF THE INVENTION

The present invention relates to methods and systems for detecting one or more analytes in a sample and/or for classifying a sample. In particular, the present invention relates to methods and systems which can be used to detect the analytes in real time and which rely on flowing through a microfluidic device one or more types of sensor molecule each comprising a domain that binds one or more analytes, a chemiluminescent donor domain and an acceptor domain, wherein the separation and relative orientation of the chemiluminescent donor domain and the acceptor domain, in the presence and/or the absence of analyte, is within $\pm 50\%$ of the Forster distance.

BACKGROUND OF THE INVENTION

Bioluminescence resonance energy transfer (BRET) occurs naturally in marine organisms such as *Aequorea victoria* and *Renilla reniformis* (Morin and Hastings, 1971). BRET is a form of Förster resonance energy transfer (RET), which is the non-radiative transfer of energy from an excited state donor to a ground state acceptor. There are two commonly used forms of the BRET principle, i.e., BRET¹ and BRET². Both use *Renilla* luciferase (RLuc) as the energy donor. In BRET¹, the substrate is native coelenterazine (CLZ) or coelenterazine h (CLZh). RLuc and a yellow fluorescent protein (YFP) are the energy donor and acceptor, respectively, giving peak donor emission at 475 nm and peak acceptor emission at 535 nm. In BRET², YFP is replaced with GFP² and a modified CLZ substrate, i.e. coelenterazine-400a or (CLZ400a) is used. The peak donor emission and acceptor emission are shifted to 395 nm and 515 nm, respectively (Dacres et al., 2009a, b; Pflieger and Eidne, 2006). A third form of BRET, i.e., BRET³, has recently been developed. It used CLZh as the substrate and RLuc8 as the energy donor and mOrange as the acceptor, resulting in improved spectral resolution (De et al., 2009).

RET is a ratiometric technique which can eliminate data variability caused by fluctuations in light output due to variations in assay volume, assay conditions and signal decay across different wells in a plate. RET-based reactions are homogeneous, generally occurring in solution without solid-phase attachment. This allows for detection of analytes in different forms such as liquid, gas and even particulates without separation. The avoidance of solid-phase attachment eliminates the process of surface regeneration used in many surface-based techniques such as Surface Plasmon Resonance (SPR) (Fang et al., 2005) and, in conjunction with the fast reaction rate, allows it to be used for on-line monitoring.

So far, however, uses of BRET have been restricted to research laboratories using sophisticated detection equipment. Microfluidic technologies are attracting interest in

many fields, including chemistry, biology, medicine, sensing and materials. Their advantages over conventional technologies include reduced reagent consumption, fast reaction rate, short analysis time, and amenability to automation and mass production (Holden and Cremer, 2005).

There have been substantial research and development in microfluidic technologies. Examples include an integrated biochip design with fluorescence light collection (EP 2221606), on-chip biosensing using Raman spectroscopy (WO 20091020479), a biosensing device (WO 20091018467) for detecting GPCR-ligand binding using surface plasmon resonance techniques, a light detection chip (US 201110037077 and US 2008085552) with mirrors as light reflectors, an assay device with a cartridge format (WO 2009/044088), a chemiluminescence-based microfluidic biochip (US 2002/0123059) and so on. Many of these device have the disadvantages of high cost per chip due to integration of multiple components, inability to perform real-time monitoring due to the requirement for surface regeneration and slow reaction of reagents, limited detection sensitivity, or signal drift.

Furthermore, there is considerable background art in the fields of electronic noses and electronic tongues, which contact a gaseous or liquid sample with an array of solid state sensors in order to detect analytes and/or classify the samples. Electronic noses and tongues have been bedeviled by poor performance due to limited selectivity of the sensors, poor sensitivity, sensor saturation and slow regeneration and sensor drift over time.

There is therefore a need for further methods of detecting analytes and classifying samples based on the analytes they contain, particularly methods that can be performed in real time and with increased sensitivity and that do not suffer from downtime due to the need to regenerate the sensing surface and that resist the confounding effects of sensor drift. Multiple channel microfluidic systems deploying an array of biologically derived sensors electro-optically coupled to a detection system offer a novel solution to these problems.

SUMMARY OF THE INVENTION

The present inventors have identified an improved method of detecting an analyte in a sample.

In one aspect, the present invention provides a method of detecting an analyte in a sample, the method comprising

- i) flowing through a microfluidic device comprising one or more microchannels,
 - a) the sample,
 - b) a sensor molecule comprising a domain that binds the analyte, a chemiluminescent donor domain and an acceptor domain, wherein the separation and relative orientation of the chemiluminescent donor domain and the acceptor domain, in the presence and/or the absence of analyte, is within $\pm 50\%$ of the Forster distance,
 - c) a substrate of the chemiluminescent donor,
- ii) mixing the sensor molecule, sample and substrate in the device, and
- iii) detecting modification of the substrate by the chemiluminescent donor using an electro-optical sensing device, wherein the spatial location and/or dipole orientation of the chemiluminescent donor domain relative to the acceptor domain is altered when the analyte binds the sensor molecule.

In a preferred embodiment, the sensor molecule is not fixed to the device.

In a further preferred embodiment, the method can be used to detect the analyte in real time.

In another preferred embodiment, the sensor molecule and substrate enter the device through different microchannels. In an alternate embodiment, the sensor molecule and substrate enter the device through the same microchannel, however, in this embodiment it is preferred that the sensor molecule and substrate are mixed shortly before (for example 10 seconds, more preferably 1 second, or less) before entering the microchannel.

In a preferred embodiment, the Förster distance of the chemiluminescent donor domain and the acceptor domain is at least 5.6 nm, or at least 6 nm. In another preferred embodiment, the Förster distance of the chemiluminescent donor domain and the acceptor domain is between about 5.6 nm and about 10 nm, or is between about 6 nm and about 10 nm.

In a further preferred embodiment, the analyte binding or releasing from the sensor molecule results in a change in BRET ratio which is $\geq 15\%$, $\geq 20\%$, $\geq 30\%$, $\geq 35\%$, about 15% to about 50%, or about 15% to about 40%, of the maximum observed BRET ratio. A change in the BRET ratio of 15% or more increases the signal to noise ratio of analyte detection. This results in a superior limit of detection for any given sampling time and more precise coding of the level of concentration of analyte. Alternatively, at a fixed limit of detection, the greater change in BRET ratio facilitates shorter signal integration times and therefore more rapid detection.

In a further preferred embodiment, the quantum yield detected by the electro-optical sensing device is less than about 8%, or less than about 5%, or less than about 2%.

In another preferred embodiment, the acceptor domain has a Stokes Shift of between about 50 nm and about 150 nm. In an embodiment, the acceptor domain has a Stokes Shift of about 100 nm.

An advantage of the method of the present invention is that it is highly time resolved. Thus, in a preferred embodiment, the method is performed within about 1s to about 100 s.

The sample can be in any form that is capable of being flowed through a microfluidic device. Examples include, but are not necessarily limited to, a liquid, gas, emulsion or suspension. In an embodiment, the sample is a liquid which has been pre-equilibrated with a gas.

In one embodiment, the suspension is, or comprises, a cell-free composition. In an alternate embodiment, the suspension comprises cells.

In an embodiment, the flow rate through the microfluidic device is between about 1 l/hour to about 10 ml/hour, or 1 μ l/hour to about 1 ml/hour, or 1 μ l/hour to about 1.5 ml/hour, or about 20 μ l/hour to about 0.5 ml/hour, and the preferred flow rate is between about 200 μ l/hour to about 1 ml/hour.

In a preferred embodiment, the flow rate and length of the section of the microchannel comprising the sample, sensor molecule and substrate is such that the sample, sensor molecule and substrate are in the section for at least about 5 sec, at least about 10 sec, at least about 15 sec, at least about 20 sec, about 5 sec to about 50 sec, or about 10 sec to about 30 sec.

In one embodiment, for instance when the sensor molecule comprises a protein receptor such as a G coupled protein receptor, the concentration of the sensor molecule following step ii) is between about 1 nM to about 10 μ M or between about 1 nM to about 1 μ M. In another embodiment, for instance when the sensor molecule comprises a cleavable peptide-derived or periplasmic binding protein, the concen-

tration of the sensor molecule following step ii) is between about 0.1 μ M to about 10 μ M.

In an embodiment, the flow through the microfluidic device is continuous flow, batch flow or stop flow.

The sample, sensor molecule and substrate may be actively mixed using mechanical, electrokinetic, acoustical or other suitable means. In a preferred embodiment, the mixing is achieved by diffusion over dimensions perpendicular to the direction of flow through a microchannel comprising the sample, sensor molecule and substrate. For example, efficient mixing (? 20%) of sample, sensor molecule and substrate can be conveniently achieved by predominantly passive diffusional (non-turbulent) processes. The typical conditions include, flow rates of approximately no more than 1,000 microlitres per hour, common microchannel lengths of approximately 10 mm or more and that the summed height of the stacked inputs when they are flowing in contact with each other in the common channel is approximately 200 micrometres or less (measured perpendicular to the direction of flow).

The sample, sensor molecule and substrate can be flowed through the microfluidic device by any suitable means such as, but are not necessarily limited to, one or more of pumping, vacuum, hydraulics, suction, electrokinesis, chemiosmosis, capillary force, acoustics, electromagnetics, piezoelectrics. Pumping mechanisms can be realised in compact, miniaturised and micron-size pumps. In a preferred embodiment, the sample, sensor molecule and substrate is flowed through the microfluidic device by suction (negative pressure), for example using a syringe pump in withdrawal mode.

In an embodiment, each microchannel has a cross-sectional area of about 1 μ m² to about 1 mm².

In a further embodiment, the microchannel for the sample, sensor molecule and substrate each have a width of ≥ 300 μ m and height ≥ 60 μ m, width of ≥ 600 μ m and height ≥ 30 μ m or width of ≥ 1200 μ m and height ≥ 15 μ m. In an embodiment, the height is no greater than about 1 mm or about 0.5 mm. In another embodiment, the height is about 15 μ m to about 1 mm or about 15 μ m to about 0.5 mm. In a further embodiment, the width is no greater than about 1.5 mm. In yet a further embodiment, the width is about 300 μ m to about 1.5 mm or about 300 μ m to about 1.2 mm.

The lengths of the input microchannels for substrate, sensor molecule and sample are as short as possible, preferably less than 10 mm, and more preferably less than 5 mm.

The length of the common microchannel where the substrate, sensor molecule and sample are allowed to mix and react may be between 5 mm and 100 mm, or between 10 mm and 100 mm, preferably between 20 mm and 50 mm and may be linear, serpentine or any suitable combination of straight curved geometries. In an alternate embodiment, the common microchannel may be dispensed with entirely and the sensor molecule, substrate and sample may be introduced directly into the reaction chamber with or without active mixing.

In a further embodiment, step iii) is performed in a reaction chamber with a volume of about 1 pl (i.e. picoliter or a trillionth of a liter) to about 200 μ l and the preferred volume is 0.5 μ l to about 8 μ l, or 0.5 μ l to about 2 μ l.

In yet another embodiment, step iii) comprises processing at least one signal from the electro-optical sensing device to determine whether the analyte is absent or present in the sample, and if present optionally determining the concentration of the analyte in the sample.

In an embodiment, the domain that binds the analyte is a protein (which may be a peptide) or a nucleic acid. In a

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preferred embodiment, the domain is a protein. In an embodiment, the protein is a naturally occurring protein, which binds one or more analytes (ligand), or a variant of the protein which retains analyte (ligand) binding activity. Examples include, but are not necessarily limited to, a receptor, odorant binding protein, pheromone-binding protein, enzyme, ligand carrier or bacterial periplasmic binding protein. In an embodiment, the receptor is a G protein coupled receptor such as an odorant receptor or a taste receptor. In a further embodiment, the odorant receptor or taste receptor is from a nematode or vertebrate or is a mutant thereof.

In an embodiment, the chemiluminescent donor domain is a bioluminescent protein. Examples include, but are not necessarily limited to, a luciferase, β -galactosidase, a lactamase, a horseradish peroxidase, an alkaline phosphatase, a β -glucuronidase or a β -glucosidase. Examples of luciferases include, but are not necessarily limited to, a *Renilla* luciferase, a Firefly luciferase, a Coelenterate luciferase, a North American glow worm luciferase, a click beetle luciferase, a railroad worm luciferase, a bacterial luciferase, a *Gaussia* luciferase, Aequorin, an *Arachnocampa* luciferase, or a biologically active variant or fragment of any one, or chimera of two or more, thereof. In a preferred embodiment, the *Renilla* luciferase variant is RLuc2 or RLuc8.

In an embodiment, the substrate is luciferin (such as a beetle luciferin), calcium, coelenterazine, or a derivative or analogue of coelenterazine.

In a preferred embodiment, the acceptor domain is a fluorescent acceptor domain.

In a further embodiment, the fluorescent acceptor domain is a protein. Examples include, but are not necessarily limited to, green fluorescent protein (GFP), blue fluorescent variant of GFP (BFP), cyan fluorescent variant of GFP (CFP), yellow fluorescent variant of GFP (YFP), enhanced GFP (EGFP), enhanced CFP (ECFP), enhanced YFP (EYFP), GFPS65T, Emerald, Venus, mOrange, Topaz, GFPuv, destabilised EGFP (dEGFPX), destabilised ECFP (dECFP), destabilised EYFP (dEYFP), HcRed, t-HcRed, DsRed, DsRed2, t-dimer2, t-dimer2(12), mRFPI, pociilorporin, *Renilla* GFP, Monster GFP, paGFP, Kaede protein or a Phycobiliprotein, or a biologically active variant or fragment of any one thereof.

In an alternate embodiment, the fluorescent acceptor domain is a non-protein. Examples include, but are not necessarily limited to, an Alexa Fluor dye, Bodipy dye, Cy dye, fluorescein, dansyl, umbelliferone, fluorescent microsphere, luminescent microsphere, fluorescent nanocrystal, Marina Blue, Cascade Blue, Cascade Yellow, Pacific Blue, Oregon Green, Tetramethylrhodamine, Rhodamine, Texas Red, rare earth element chelates, or any combination or derivatives thereof.

In an embodiment, the method further comprises providing a co-factor of the bioluminescent protein. Examples of co-factors include, but are not necessarily limited to, ATP, magnesium, oxygen, FMNH₂, calcium, or a combination of any two or more thereof.

In a preferred embodiment,

- i) the bioluminescent protein is a luciferase or a biologically active variant or fragment, and/or
- ii) the substrate is luciferin, coelenterazine, or a derivative or analogue of coelenterazine, and/or
- iii) the acceptor domain is green fluorescent protein (GFP), Venus, mOrange, or a biologically active variant or fragment of any one thereof.

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In a further preferred embodiment,

- i) the luciferase is a *Renilla* luciferase, the acceptor domain is GFP², and the substrate is coelenterazine 400a,
 - ii) the luciferase is a *Renilla* luciferase 2, the acceptor domain is GFP², and the substrate is coelenterazine 400a,
 - iii) the luciferase is a *Renilla* luciferase 8, the acceptor domain is GFP², and the substrate is coelenterazine 400a,
 - iv) the luciferase is a *Renilla* luciferase 2, the acceptor domain is Venus, and the substrate is coelenterazine,
 - v) the luciferase is a *Renilla* luciferase 8, the acceptor domain is Venus, and the substrate is coelenterazine,
 - vi) the luciferase is a *Renilla* luciferase 8.6-535, the acceptor domain is mOrange, and the substrate is coelenterazine, or
 - vii) the luciferase is a *Renilla* luciferase 8, the acceptor domain is mOrange, and the substrate is coelenterazine.
- More preferably,

- i) the luciferase is a *Renilla* luciferase, the acceptor domain is GFP², and the substrate is Coelenterazine 400a,
- ii) the luciferase is a *Renilla* luciferase 2, the acceptor domain is GFP², and the substrate is Coelenterazine 400a,
- iii) the luciferase is a *Renilla* luciferase 8, the acceptor domain is GFP², and the substrate is Coelenterazine 400a,
- iv) the luciferase is a *Renilla* luciferase 8.6-535, the acceptor domain is mOrange, and the substrate is Coelenterazine, or
- v) the luciferase is a *Renilla* luciferase 8, the acceptor domain is mOrange, and the substrate is Coelenterazine.

Even more preferably,

- i) the luciferase is a *Renilla* luciferase, the acceptor domain is GFP², and the substrate is Coelenterazine 400a,
- ii) the luciferase is a *Renilla* luciferase 2, the acceptor domain is GFP², and the substrate is Coelenterazine 400a, or
- iii) the luciferase is a *Renilla* luciferase 8, the acceptor domain is GFP², and the substrate is Coelenterazine 400a.

In an embodiment, the method comprises simultaneously or sequentially detecting two or more different analytes using the same microfluidic device, for example using a device as shown in FIGS. 14b and 14c.

In an embodiment, the microfluidic device comprises one or more sets of

- a) three input microchannels, one each for the sensor molecule, substrate and sample, or
- b) two input microchannels, one for the substrate and the other for a pro-mixture of the sensor molecule and sample, or
- c) two input microchannels, one for the sensor molecule and the other for a pre-mixture of the substrate and sample.

In a further embodiment, at least one microchannel comprises a reaction chamber which has a different volume to at least one other microchannel.

In another embodiment, at least one microchannel comprises two or more reaction chambers of the same or different volume.

In a preferred embodiment, the electro-optical sensing device has at least two different wavelength channels, which may detect overlapping or non-overlapping wavelengths. In

an alternate embodiment, the electro-optical sensing device has a single wavelength channel, wherein in this embodiment the donor quenches emission from the acceptor.

In an embodiment, the electro-optical sensing device comprises fibre bundle or liquid light guides. In an embodiment, diameter of the fibre bundle or liquid light guide is between about 1 mm and about 10 mm, or about 1 mm and about 6 mm. In an embodiment, the electro-optical sensing device further comprises a shutter box.

In an embodiment, the electro-optical sensing device comprises a bifurcated light guide, and no dichroic block.

In a preferred embodiment, the sensor molecule is present in a cell-free extract. In an alternate embodiment, the sensor molecule is expressed by cells (for example present on the surface of the cells or secreted by the cells) and provided as a cell suspension where the cells are intact.

The method can be used to sort cells. Thus, in an embodiment, the analyte is exposed on the surface of a cell and the method further comprises diverting cells comprising the analyte through a different microchannel than cells in the sample lacking the analyte, and collecting the cells comprising the analyte and/or collecting the cells lacking the analyte, wherein if both cell types are collected they are collected in separate containers.

In another aspect, the present invention provides a microfluidic system for detecting an analyte in a sample, the system comprising

- i) at least one reservoir suitable for containing (or comprising) a sensor molecule comprising a domain that binds the analyte, a chemiluminescent donor domain and an acceptor domain, wherein the separation and relative orientation of the chemiluminescent donor domain and the acceptor domain, in the presence and/or the absence of analyte, is within $\pm 50\%$ of the Forster distance,
- ii) a microfluidic device comprising one or more microchannels,
- iii) means for mixing the sensor molecule, the sample and a substrate of the chemiluminescent donor domain in the device,
- iv) a reaction chamber for detecting binding of the analyte to the sensor molecule, and
- v) an electro-optical sensing device, wherein the spatial location and/or dipole orientation of the chemiluminescent donor domain relative to the acceptor domain is altered when the analyte binds the sensor molecule.

In a preferred embodiment, the sensor molecule is not fixed to the microfluidic device.

In a further preferred embodiment, the system can be used to detect the analyte in real time.

In another preferred embodiment, the sensor molecule and substrate enter the device through different microchannels.

In a further preferred embodiment, the microfluidic device comprises at least two input microchannels, wherein one of the input microchannels is for flowing the sensor molecule into the device.

As the skilled addressee will appreciate, each of the preferred embodiments relating to the method of the invention also relate to the system of the invention and/or how the system can operate.

In an embodiment, the electro-optical sensing device comprises at least two different wavelength channels.

In a particularly preferred embodiment, the electro-optical sensing device is capable of simultaneously, or in rapid succession, detecting two different wavelength channels.

For example, the electro-optical sensing device is capable of detecting two different wavelength channels in less than 1 second.

In a further embodiment, the microfluidic device is designed to enable the detection of two or more analytes. In an embodiment, the device comprises a separate microchannel for flowing each different sensor molecule into the device.

In an embodiment, the mixing occurs in the reaction chamber.

The present invention can also be used to classify a sample. For this purpose it is not essential that it already be known which analyte(s) in a sample actually bind(s) one or more sensor molecules. Thus, in another aspect the present invention provides a method of classifying a sample, the method comprising

- i) flowing through a microfluidic device comprising one or more microchannels,
 - a) the sample,
 - b) a sensor molecule comprising a domain that binds one or more analytes, a chemiluminescent donor domain and an acceptor domain, wherein the separation and relative orientation of the chemiluminescent donor domain and the acceptor domain, in the presence and/or the absence of analyte(s), is within $\pm 50\%$ of the Forster distance,
 - c) a substrate of the chemiluminescent donor,
- ii) mixing the sensor molecule, sample and substrate in the device,
- iii) detecting modification of the substrate by the chemiluminescent donor using an electro-optical sensing device,
- iv) processing at least one signal from the electro-optical sensing device and correlating the pattern of electro-optical responses with one or more pre-determined characteristics of one or more samples of interest, and
- v) classifying the sample based on the correlation of the pattern of responses, wherein the spatial location and/or dipole orientation of the chemiluminescent donor domain relative to the acceptor domain is altered when the one or more analytes binds the sensor molecule.

In a preferred embodiment, the above method comprises two or more different sensor molecules each of which binds a different analyte (which may be a different set of analytes) or range of analytes, and step v) comprises classifying the sample based on the presence, absence or concentration of each of the analytes or range of analytes.

In an embodiment, one or more of the analytes are unknown.

In a further embodiment, the method can be used to classify the sample in real time.

In another embodiment, the sensor molecule is not fixed to the device.

In yet a further embodiment, the sensor molecule and substrate enter the device through different microchannels.

Also provided is a microfluidic system for classifying a sample, the system comprising

- i) at least one reservoir suitable for containing (or comprising) a sensor molecule comprising a domain that binds one or more analytes, a chemiluminescent donor domain and an acceptor domain, wherein the separation and relative orientation of the chemiluminescent donor domain and the acceptor domain, in the presence and/or the absence of analyte, is within $\pm 50\%$ of the Forster distance,
- ii) a microfluidic device comprising one or more microchannels,

- iii) means for mixing the sensor molecule, the sample and a substrate of the chemiluminescent donor domain in the device,
- iv) a reaction chamber for detecting binding of the analyte to the sensor molecule, and
- v) an electro-optical sensing device, wherein the spatial location and/or dipole orientation of the chemiluminescent donor domain relative to the acceptor domain is altered when the one or more analytes binds the sensor molecule.

In an embodiment, the system comprises two or more different sensor molecules each of which binds a different analyte, which may be a different set of analytes, or range of analytes.

In an embodiment, the system comprises two or more different sensor molecules each of which binds the same analyte at a different site and/or with a different level of affinity.

In another embodiment, one or more of the analytes, or range of analytes, are unknown.

In a further embodiment, the system can be used to classify samples in real time.

In an embodiment, the sensor molecule is not fixed to the device.

In a further embodiment, the sensor molecule and substrate enter the device through different microchannels.

In another embodiment, the microfluidic device comprises at least two input microchannels, wherein one of the input microchannels is for flowing the sensor molecule into the device.

In a further aspect, the present invention provides a method of screening for a compound that binds a molecule of interest, the method comprising

- i) flowing through a microfluidic device comprising one or more microchannels,
 - a) a candidate compound,
 - b) a sensor molecule comprising the molecule of interest, a chemiluminescent donor domain and an acceptor domain, wherein the separation and relative orientation of the chemiluminescent donor domain and the acceptor domain, in the presence and/or the absence the candidate compound, is within $\pm 50\%$ of the Forster distance,
 - c) a substrate of the chemiluminescent donor,
- ii) mixing the sensor molecule, the candidate compound and substrate in the device,
- iv) detecting modification of the substrate by the chemiluminescent donor using an electro-optical sensing device,
- v) processing at least one signal from the electro-optical sensing device to determine whether the candidate compound binds the sensor molecule, and
- vi) selecting the compound if it binds the sensor molecule, wherein the spatial location and/or dipole orientation of the chemiluminescent donor domain relative to the acceptor domain is altered when the candidate compound binds the sensor molecule.

In a preferred embodiment, the method can be used to detect binding of the candidate compound to the sensor molecule in real time.

In a further preferred embodiment, the sensor molecule is not fixed to the device.

In another preferred embodiment, the sensor molecule and substrate enter the device through different microchannels.

In a preferred embodiment, the method further comprises confirming that the candidate compound binds the binding

domain of the molecule of interest and not other domains of the sensor molecule. As the skilled person would appreciate, this can be performed using any one of a wide variety of techniques in the art such as using the molecule of interest on a column to capture the candidate compound, competitive binding assays, determining whether following incubation of the candidate compound with the molecule of interest modifies the migration of the molecule of interest using gel chromatography and so on.

The candidate compound and the molecule of interest can be the same type of substance, for example, both could be nucleic acids, proteins (including peptides) or small molecules. In one embodiment, the molecule of interest is a protein such as, but not limited to, a receptor, odorant binding protein, pheromone-binding protein, enzyme, ligand carrier or bacterial periplasmic binding protein. The molecule of interest may be naturally occurring or a mutant/variant thereof.

In a further aspect, the present invention provides a microfluidic system for screening for a compound that binds a molecule of interest, the system comprising

- i) at least one reservoir suitable for containing (or comprising) a sensor molecule comprising the molecule of interest, a chemiluminescent donor domain and an acceptor domain, wherein the separation and relative orientation of the chemiluminescent donor domain and the acceptor domain, in the presence and/or the absence of a candidate compound, is within $\pm 50\%$ of the Forster distance,
- ii) a microfluidic device comprising one or more microchannels,
- iii) means for mixing the sensor molecule, the candidate compound, and a substrate of the chemiluminescent donor domain in the device,
- iv) a reaction chamber for detecting binding of the candidate compound to the sensor molecule, and
- v) an electro-optical sensing device, wherein the spatial location and/or dipole orientation of the chemiluminescent donor domain relative to the acceptor domain is altered when the candidate compound binds the sensor molecule.

In a preferred embodiment, the system can be used to detect binding of the candidate compound to the sensor molecule in real time.

In a further preferred embodiment, the sensor molecule is not fixed to the device.

In another preferred embodiment, the sensor molecule and substrate enter the device through different microchannels.

In a further embodiment, the microfluidic device comprises at least two input microchannels, wherein one of the input microchannels is for flowing the sensor molecule into the device

The present inventors have also identified a hybrid BRET (BRET²) detection system that does not suffer from the low luminescence trait of BRET2. Thus, in a further aspect, the present invention provides a method of detecting an analyte in a sample, the method comprising

- i) contacting the sample, in the presence of coelenterazine, with a sensor molecule comprising
 - a) a domain that binds the analyte,
 - b) *Renilla* luciferase, and
 - c) green fluorescent protein 2, and
- ii) determining whether bioluminescent resonance energy transfer (BRET) between the bioluminescent protein and the acceptor molecule is modified, wherein the spatial location and/or dipole orientation of the biolu-

minescent protein relative to the acceptor molecule is altered when the analyte binds the domain.

Naturally, the above method can readily be used in a method of the invention using a microfluidic device.

In a further aspect, the present invention provides an isolated sensor molecule comprising a domain that binds one or more analytes, *Renilla* luciferase, and green fluorescent protein 2.

The present inventors have identified polypeptides which bind 2-pentanone, and hence these polypeptides can be used to detect this compound.

Accordingly, in a further aspect the present invention provides a method of detecting 2-pentanone in a sample, the method comprising

- i) contacting the sample with a polypeptide which is *C. elegans* str-112 (SEQ ID 41) or str-113 (SEQ ID NO:42), or a variant thereof which binds 2-pentanone, and
- ii) detecting whether any of the polypeptide is bound to 2-pentanone.

As the skilled person would appreciate, there is an enormous array of different assays that can be configured once a new ligand/polypeptide binding pair has been identified. In one embodiment, the methods of the invention are used to detect 2-pentanone in a sample.

In an embodiment, the variant of str-113 is a str-114/str-113 fusion (SEQ ID NO:43).

In an embodiment, the polypeptide is detectably labelled. Examples of such detectably labelled polypeptides include, but are not limited to, those provided as SEQ ID NOs 13, 14, 18, 27, 28 and 30.

2-pentanone is produced by bacteria, and hence the above method can be used to detect, for example, bacterial infections or contaminations.

Thus, in a further aspect the present invention provides a method of detecting bacteria in a sample comprising detecting 2-pentanone using the method of the invention.

In an embodiment, the bacteria is *Escherichia sp.* such as *E. coli*.

Any embodiment herein shall be taken to apply *mutatis mutandis* to any other embodiment unless specifically stated otherwise.

The present invention is not to be limited in scope by the specific embodiments described herein, which are intended for the purpose of exemplification only. Functionally-equivalent products, compositions and methods are clearly within the scope of the invention, as described herein.

Throughout this specification, unless specifically stated otherwise or the context requires otherwise, reference to a single step, composition of matter, group of steps or group of compositions of matter shall be taken to encompass one and a plurality (i.e. one or more) of those steps, compositions of matter, groups of steps or group of compositions of matter.

The invention is hereinafter described by way of the following non-limiting Examples and with reference to the accompanying figures.

BRIEF DESCRIPTION OF THE ACCOMPANYING DRAWINGS

FIG. 1—Generic arrangement for performing the claimed method, showing the microfluidic chip (microchip) and a BRET detection system. DM=dichroic mirror, BP=band pass filter (wavelength centre in nm, width in nm).

FIG. 2—Thrombin cleavage of GFP²-RG-RLuc fusion protein sensor molecule monitored by (A) Spectral change

of the hybrid BRET system upon addition 5 μM of native coelenterazine to GFP²-RG-RLuc fusion protein with and without the addition of 2 units of thrombin and (B) SDS-PAGE analysis of purified His-tagged BRET proteins. 2.5 μg protein loaded per lane. From left to right; Molecular markers (kDa), RLuc, GFP², GFP²-RG-RLuc, GFP²-RG-RLuc following incubation with 54 nM thrombin for 90 minutes at 30° C.; GFP²-RG-RLuc same conditions as previous lane except that thrombin has been pre-incubated with 2 units of hirudin for 10 minutes at room temp.

FIG. 3—Change in normalised BRET^{Hz} ratio following thrombin cleavage (mean±S.D., n=3) of 1 μM of fusion proteins upon addition of 5 μM of native coelenterazine; GFP²-RG-RLuc following treatment (90 minutes, 30° C.) with 54 nM thrombin or 54 nM of thrombin following pre-treatment (10 minutes, room temperature) with 2 units of hirudin. Controls consist of 1 μM of RLuc and GFP² proteins. p≤0.001 indicates a highly significant difference, p=0.33 indicates the changes are not significant.

FIG. 4—Experimental set-up for on-chip detection. (a) A schematic drawing of the hybrid BRET reaction, and (b and c) the microfluidic chip system for BRET signal detection (Clz=Native coelenterazine, DM=dichroic mirror, BP=band pass, PMT=photomultiplier tube).

FIG. 5—Bioluminescence intensity (AU) of GFP²-RG-RLuc thrombin sensor protein upon the addition of coelenterazine substrate and the BRET^{Hz} ratio as a function of distance x from the Y-junction as labelled in FIG. 4b. The symbols + and ∇ represent bioluminescence background of RLuc and GFP² channel, respectively. ○ and × represent bioluminescence intensity of RLuc and GFP² channel, respectively. ♦ represents the BRET ratio. The fusion protein concentration was 3.0 μM. Native coelenterazine concentration was 58.6 μM; each aqueous flow rate was 20 μl/h; a 20× objective was used; filter band pass for GFP² and RLuc channel are 515 nm-555 nm and 430 nm-455 nm respectively; an internal gate time of 200 ms was used for data acquisition.

FIG. 6—BRET^{Hz} ratios as a function of total flow rate of the aqueous streams (a) and the thrombin sensor concentration (b). (a) Thrombin sensor protein concentration was 3.0 μM and native coelenterazine concentration was 58.6 μM; (b) Native coelenterazine concentration was 58.6 μM; each aqueous flow rate was 20 μl/h; a 20× objective was used; filter band pass for GFP² and RLuc channel are 515 nm-555 nm and 430 nm-455 nm respectively; an internal gate time of 200 m was used for data acquisition.

FIG. 7—Calibration curves for the BRET^{Hz} thrombin sensors in microfluidic and microplate formats (mean±SD, n=5). All microfluidic measurements were obtained at x=2.1 mm. ○ and □ represent data for microchip and microplate measurements, respectively. The main graph shows the data at low thrombin concentrations while the insets show the corresponding full-range measurements. The lines are the linear regressions, which are y=0.835x+1.019 (R²=0.996) for the microchip data and y=0.1797x+1.001 (R²=0.995) for the microplate data. For the microchip method, the fusion protein concentration was 3.0 μM and native coelenterazine concentration was 58.6 μM, each aqueous flow rate was 20 μl/h. For the microplate method, the fusion protein and native coelenterazine concentrations were 1 μM and 5 μM, respectively

FIG. 8—Examples of passive mixing designs (a) Y-shape with linear contact region (b) narrow serpentine, (c) wide serpentine, (d) spiral, (e) Y-shape channel with size variations and baffles, and (f) three inlet with narrow serpentine contact region.

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FIG. 9—Schematics of a particular example of a chip and on-chip optical detection system of the invention. PMT-photomultiplier tube. PDMS-polydimethylsiloxane chip matrix.

FIG. 10—Sample data indicates detection of thrombin by the change in BRET² ratio of a GFP²-RG-RLuc thrombin sensor. a. GFP (green-top) and *Renilla* luciferase (blue-bottom) channel emission intensities with no thrombin present. b. GFP (green-bottom) and *Renilla* luciferase (blue-top) channel emission intensities following incubation of the sensor with 270 μM thrombin. c. BRET² ratio for the no thrombin and 270 μM thrombin conditions.

FIG. 11—Direct comparison of the sensitivity of thrombin detection by BRET² measurement, using a GFP²-RG-RLuc thrombin sensor in the microfluidic device of FIG. 9 (blue line) compared with the results from a commercially available plate reader instrument (red line).

FIG. 12—BRET² ratio measured with a two inlet microfluidic device upon mixing thrombin biosensor (1 μM) with a preparation containing thrombin (540 nM) and coelenterazine 400a substrate (12.5 μM).

FIG. 13—Example of the subsystems of a system of the invention.

FIG. 14—Example of single and multiple sensor chip designs.

FIG. 15—Example of the zone of passive or diffusion-based reagent mixing when three microfluidic flows come into contact.

FIG. 16—Example of electro-optical detection system.

FIG. 17—Designs of two BRET optical detection elements (a) a double-convex microlens serves at the bottom of the reaction chamber to collect fluorescence from many BRET point sources inside the reaction chamber and focus onto a multimode optical fiber (core 200 μm) (b) a plano-convex microlens also serve as the bottom of the reaction chamber. However an aspherical micro mirror on top (micro-machined on the ferrule) will collect fluorescence from the top of the BRET point sources and collimate onto the microlens. Similar to (a), the plano-convex microlens will then focus the fluorescence into the core of the optical fiber.

FIG. 18—Principle of resonance energy transfer in ODR-10 receptor constructs fused to RLuc2 and GFP². GFP² is inserted in the third intracellular loop of ODR-10 and RLuc2 at the C-terminus (OGOR2). Diacetyl binding causes a conformational change in the OGOR2 biosensor resulting in an increase in distance, or a change in the orientation of dipole moments, between the BRET² components. Clz400a=Coelenterazine 400a substrate.

FIG. 19—Bioluminescence intensity of OGOR and OGOR2 sensors upon addition of 5 μM Clz400a to 20 nM of the sensor.

FIG. 20—Bioluminescence intensity of OGOR and OGOR2 sensors upon on-chip mixing of 12.5 μM Clz400a to 1 μM of the sensor.

FIG. 21—BRET² signal from OGOR2 in the wells of a 96-well plate following incubation with 1 μM diacetyl in water, or a water only control (mean±SD, n=3).

FIG. 22—Diacetyl concentration response curve for BRET² signal of OGOR2 in a microwell plate format.

FIG. 23—Change in BRET² signal detected with on-chip microfluidic assay of OGOR2 signal following incubation with 10 fM diacetyl in PBS or a PBS only as control (mean±SD, n=3).

FIG. 24—Dose response of OGOR2 with on-chip (microfluidic) assay measurements.

FIG. 25—Averaged change in BRET² signal detected using real-time microfluidic measurement upon on-chip

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contact of OGOR2 over a range of flow rates. 1 fM diacetyl in PBS or PBS only and 12.5 μM Clz400a substrate (mean±SD of BRET² ratio at four different flow rates).

FIG. 26—BRET² ratio measured at different common flow rates with a three-inlet microfluidic device upon contacting OGOR2 (290 nM) with 1 femtomolar diacetyl solution in PBS and with 12.5 μM coelenterazine 400a.

FIG. 27—Principle of BRET in MBP receptor constructs fused to BRET² components GFP² and RLuc2. Maltose binding causes a conformational change in the BRET² tagged MBP receptor bringing the BRET² components in closer proximity causing an increase in the efficiency of energy transfer from RLuc2 to GFP². Clz400a=Coelenterazine 400a substrate.

FIG. 28—Effect of 0.1 mM of various sugars on the BRET² ratio of the GFP²—MBP—RLuc2 sensor. BRET² ratio (Mean±SD, n=3) was recorded following addition of 16.7 μM coelenterazine 400a to 1 μM GFP²—MBP—RLuc2 or W140A mutant (hatched bar) following incubation with water (grey bar) or 0.1 mM of the stated sugars for 30 minutes at 28° C. BRET² ratios were normalized by the water response. ** P<0.01 and P* <0.05.

FIG. 29—Response time (minutes, mean±S.D., n=3) of 1 μM GFP²—MBP—RLuc2 to 0.1 mM Maltose upon addition of 16.67 μM coelenterazine 400a. The BRET² response following incubation with maltose for any time period was normalized by the BRET² response following incubation with water for the same time period.

FIG. 30—(A) FRET vs BRET². Maltose concentration dependence of the BRET² response (mean±SD, n=11) of 1 μM GFP²—MBP—RLuc2 fusion protein upon addition of 16.67 μM coelenterazine 400a compared to the FRET response (mean±SD, n=3) of FLIPmal-2μ (530/485-nm ratio). The latter dose-response curve was re-plotted from data presented by Fehr et al. (2002). Data was fitted to a log [Agonist] vs response. BRET² EC50=0.4 μM and FRET EC50=3.2 μM. (B) Comparison of BRET²-based MBP assay for maltose on a microfluidic chip versus using a microplate assay.

FIG. 31—Experimental setup for collecting data from a microfluidic chip system without (A) and with (B) an in-line optical fibre switch. BP-band pass, PMT-photomultiplier; NA-numerical aperture.

FIG. 32—Real-time RLuc/Clz400a bioluminescent signal collected without (A) and with optical switch (B) for three runs.

FIG. 33—Mean bioluminescent signal comparison for RLuc/Clz400a and GFP channels without and with optical switch.

FIG. 34—Example showing arrangement of increased diameter BRET reaction chamber (Ø=4 mm, h=2 mm) coupled through a liquid light guide to the photodetector.

FIG. 35—Comparison of performance of narrow vs wide bore BRET detection chamber/optical system. In both cases BRET emissions are measured from a 1/100 dilution of an OGOR2 sensor flowing through the microfluidic channel. (a) narrow bore system (chamber size Ø=2 mm, h=2 mm; fiber core diameter=1 mm, NA=0.48). (b) wide bore system (chamber size Ø=4 mm, h=2 mm, light guide core diameter=5 mm, NA=0.59).

FIG. 34—Demonstration of detection of 1 μM diacetyl using highly diluted OGOR2 sensors, using a more efficient light capture system based on a wider diameter BRET reaction chamber (4 mm) and a wide bore liquid light guide. (a) 100 times sensor dilution. Diacetyl-dependent reduction in BRET² ratio=13.7% and (b) 50 times sensor dilution,

Diacetyl-dependent reduction in BRET² ratio=14.7%. Error bars represent the standard deviation for 3 experiments (N=3).

FIG. 37—Example of a single microfluidic channel and BRET light collection system using bifurcated light guide and without dichroic block. Additional sets of bifurcated light guides with filters and pairs of photodetectors can be added to accommodate one or more additional microfluidic channels and/or BRET reaction chambers.

FIG. 38—Optical architecture with a shutter box facilitating multichannel measurements

FIG. 39—Comparison of the strength of BRET signals detected with a bifurcated light guide or a dichroic block. a, b: bifurcated light guide, reaction chamber dimensions Ø=4 mm; h=1 mm, with and without reflective lid. c,d: single light guide with dichroic block, reaction chamber dimensions Ø=4 mm; h=2 mm (i.e. double the volume of a, b). All panels show the increase in signal with time, following initiation of flow at t=0. Panels a & c blue channel, panels b & d green channel

FIG. 40—Multifurcated light guide arrangement suitable for measuring BRET outputs from a shutterbox.

FIG. 41—Comparison of multifurcated light guide converging on a single dichroic block against bifurcated light guides diverging to two separate colour filters. Relative light intensity collected in the blue (RLuc; 1, 3) and green (GFP; 2, 4) channels 1, 2: Multifurcated light guide with inputs allocated to different microfluidic channels and output directed to a pair of PMTs via an optimised dichroic filter as per FIGS. 38 & 40. 3, 4: Bifurcated light guide with output allocated to different spectral channels, as per FIG. 37.

FIG. 42—Example of an ultra low level light photodetector using vacuum photomultiplier technology. Source Hamamatsu

FIG. 43—Example of an ultra low light level photodetector implemented using solid state technology. Dimensions in mm. Source: Hamamatsu

FIG. 44—Direct visualisation of laminar flow and diffusional mixing in a three-inlet microfluidic device operating at two different flow rates. Two of the three aqueous inputs are colored with blue or red food colouring. The device was operated with a single syringe pump working in withdrawal mode. Direction of flow: right to left.

FIG. 45—Passive mixing example design based on vertically stacked streams. The width of the channel is starting from 600 µm up to 2 mm, the thickness is 20-60 µm. The length is flexible starting from 20 mm to 100 mm, the angle is 45 degrees (which may be varied over a wide range, from 0° to close to approximately 170° or indeed at an angle to the plane of the microfluidic chip).

FIG. 46—Comparison of BRET ratio measurements. Error bars reflect the standard deviation (n=3).

FIG. 47—Microfluidic chip design example for multiplexed detection. The inlet at the top is designated for substrate while the three inlets at the bottom are used for introducing sensor 1, sample and sensor 2.

FIG. 48—Microfluidic chip design example for parallel detection. Flow direction is bottom to top. Flow rates were 150 µl/hr and 1500 µl/hr. Red food dye was introduced from the substrate inlet and blue dye was introduced from the sensor inlet. No food coloring was used for the sample inlet.

FIG. 49—Three inlet microfluidic device operated by a single suction pump in withdrawal mode. A pump in suction mode creates negative pressure at the device outlet. Sample, sensor and substrate streams are sucked into the common channel (shown as a serpentine arrangement) and are passively mixed. A BRET reaction chamber is situated just

before the outlet. The pump used here is a syringe pump, a wide variety of pumping methods could also be used.

FIG. 50—Architecture for parallel independent operation using syringe pumps working in withdrawal mode. An example in which four sensor channels are operated independently, in parallel, by using four separate syringes. This enables the operation of the sensor channels at different flow rates to meet a range of different requirements.

FIG. 51—a. RLuc and GFP signals from on chip thrombin sensor operating in suction mode with multifurcated light guide and optimised dichroic block. Reaction chamber Ø=2 mm, H=1 mm. b. BRET² signal from "a". c. Demonstration of expected signal for chambers of the same diameter and varying heights based on the equivalent residence times.

FIG. 52—Specific maltose detection achieved in a microfluidic format. Comparison of the BRET² responses of a BRET²-MBP sensor to 0.1 mM maltose, glucose and sucrose.

FIG. 53—BRET² thrombin sensor with GFP² at the N-terminus and RLuc2 at the C-terminus has been modified to mimic plasmin's κ-casein target sequence: XKZX, where Z=K, Y, V or E. Prior to cleavage, the modified BRET² thrombin sensor includes the amino acid sequence: LQXXXXXXXXKZXLQ (SEQ ID NO:47).

FIG. 54—BRET² signal intensity and ratio generated in various dilutions of PBS, milk c) and d) or orange juice (a and b) using the GFP²-FL₁-RLuc2 sensor in the presence of 5 µM coelenterazine

FIG. 55—Time course of a BRET² signal generated in undiluted whole milk using the GFP²-FL₁-RLuc2 sensor in the presence of 5 µM coelenterazine A. a. Intensity. b. BRET² ratio.

FIG. 56—Bioluminescent intensity (GFP² channel -515 nm bandpass 30 nm) for GTR2 protein in thrombin cleavage buffer or various dilutions of (a) serum (b) orange or (c) milk.

FIG. 57—BRET² ratio GTR2 protein in thrombin cleavage buffer or various dilutions of (a) serum (b) orange or (c) milk.

FIG. 58—Detection of thrombin protease activity (2 units) in thrombin cleavage buffer, diluted milk, orange juice or serum using GTR2. Results are presented as normalised BRET² ratios because the absolute BRET² ratios vary according to the sample and its dilution. Note that the absence of an effect in the 1/10 dilution of serum is possibly due to the inactivation of added thrombin by residual activated antithrombin III generated by the heparin used in serum preparation.

FIG. 59—Specimen holder for gas-liquid partition experiments

FIG. 60—Timecourse of uptake of oxygen into deoxygenated SASS2400 sample fluid following fan start up at time=0.

FIG. 61—Timecourse of phenol uptake into SASS2400 sample fluid following fan start up at time=0. Relative phenol concentration indicated using arbitrary units.

FIG. 62—3-way L port pneumatically operated ball valve. This allows rapid (≤1 s) switching of the volatile headspace into the SASS2400 air inflow during active sampling.

FIG. 63—Schematic showing set up for SASS2400 testing with three way valve for rapid switching of air intake

FIG. 64—Selectivity of Str 112 (A), Str114/113 (B) and Str113 (C). BRET² response of Str112 (mean±SD, n=3), Str114/113 (mean±SD, n=14) and Str113 (mean±SD, n=6) to 1 µM of odorant or water (grey bar), **** P<0.0001, ** P<0.001 and * P<0.05.

FIG. 65—BRET responses of BRET tagged SGSR-112 (A) and SGSR-114/113 (B) nematode odorant receptors to 2-pentanone.

FIG. 66—BRET response of BRET tagged (A) Str114/113 nematode odorant receptor to diacetyl and 2-pentanone and (B) Str-113 nematode odorant receptor to 1-hexanol.

FIG. 67—Real time, continuous, on-chip detection of 1 μ M maltose using GMR BRET²-based sensor. A) Channel luminance changing with time at 100 μ L/hour input rate B) BRET² ratio changing with time at 100 μ L/hour input rate C) Channel luminance changing with time at 200 μ L/hour input rate D) BRET² ratio changing with time at 200 μ L/hour input rate. E) Comparison of BRET² ratio between water control and 1 μ M maltose averaged from 200-250 seconds at 100 μ L/hour. F) Comparison of BRET² ratio between water control and 1 μ M maltose averaged from 200-250 seconds at 200 μ L/hour.

KEY TO SEQUENCE LISTING

SEQ ID NO:1—Nucleotide sequence encoding OGOR2 fusion protein.

SEQ ID NO:2—OGOR2 fusion protein.

SEQ ID NO:3—Nucleotide sequence encoding GFP²—MBP—RLuc2 fusion protein.

SEQ ID NO:4—GFP²—MBP—RLuc2 fusion protein.

SEQ ID NO:5—Nucleotide sequence encoding GFP²—MBP—RLuc2 W140A fusion protein.

SEQ ID NO:6—GFP²—MBP—RLuc2 W140A fusion protein.

SEQ ID NOS:7 to 12—Oligonucleotide primers.

SEQ ID NO:13—GFP²-str-112 SGSR—RLuc fusion protein.

SEQ ID NO:14—GFP²-str-113 SGSR—RLuc fusion protein.

SEQ ID NO:15—GFP²-str-114 SGSR—RLuc fusion protein.

SEQ ID NO:16—GFP²-str-115 SGSR—RLuc fusion protein.

SEQ ID NO:17—GFP²-str-116 SGSR—RLuc fusion protein.

SEQ ID NO:18—GFP²-str-114/113 SGSR—RLuc fusion protein.

SEQ ID NO:19—Nucleotide sequence encoding GFP²-str-112 SGSR—RLuc fusion protein.

SEQ ID NO:20—Nucleotide sequence encoding GFP²-str-113 SGSR—RLuc fusion protein.

SEQ ID NO:21—Nucleotide sequence encoding GFP²-str-114 SGSR—RLuc fusion protein.

SEQ ID NO:22—Nucleotide sequence encoding GFP²-str-115 SGSR—RLuc fusion protein.

SEQ ID NO:23—Nucleotide sequence encoding GFP²-str-116 SGSR—RLuc fusion protein.

SEQ ID NO:24—Nucleotide sequence encoding GFP²-str-114/113 SGSR—RLuc fusion protein.

SEQ ID NO:25—GFP²-OGOR-RLuc2 fusion protein.

SEQ ID NO:26—GFP²-OGOR mutant-RLuc2 fusion protein.

SEQ ID NO:27—GFP²-str-112 SGSR—RLuc2 fusion protein.

SEQ ID NO:28—GFP²-str-113 SGSR—RLuc2 fusion protein.

SEQ ID NO:29—GFP²-str-114 SGSR—RLuc2 fusion protein.

SEQ ID NO:30—GFP²-str-114/113 SGSR—RLuc2 fusion protein.

SEQ ID NO:31—GFP²-str-115 SGSR—RLuc2 fusion protein.

SEQ ID NO:32—GFP²-str-116 SGSR—RLuc2 fusion protein.

5 SEQ ID NO:33—Nucleotide sequence encoding GFP-OGOR-RLuc2 fusion protein.

SEQ ID NO:34—Nucleotide sequence encoding GFP²-OGOR mutant-RLuc2 fusion protein.

10 SEQ ID NO:35—Nucleotide sequence encoding GFP²-str-112 SGSR—RLuc2 fusion protein.

SEQ ID NO:36—Nucleotide sequence encoding GFP²-str-113 SGSR—RLuc2 fusion protein.

SEQ ID NO:37—Nucleotide sequence encoding GFP²-str-114 SGSR—RLuc2 fusion protein.

15 SEQ ID NO:38—Nucleotide sequence encoding GFP²-str-114/113 SGSR—RLuc2 fusion protein.

SEQ ID NO:39—Nucleotide sequence encoding GFP²-str-115 SGSR—RLuc2 fusion protein.

20 SEQ ID NO:40—Nucleotide sequence encoding GFP²-str-116 SGSR—RLuc2 fusion protein.

SEQ ID NO:41—*C. elegans* str-112.

SEQ ID NO:42—*C. elegans* str-113.

SEQ ID NO:43—*C. elegans* str-114/113 chimeric protein.

SEQ ID NO:44—Open reading frame encoding *C. elegans* str-112.

SEQ ID NO:45—Open reading frame encoding *C. elegans* str-113.

SEQ ID NO:46—Open reading frame encoding *C. elegans* str-114/113 chimeric protein.

DETAILED DESCRIPTION OF THE INVENTION

General Techniques and Definitions

Unless specifically defined otherwise, all technical and scientific terms used herein shall be taken to have the same meaning as commonly understood by one of ordinary skill in the art (e.g., in cell culture, molecular genetics, immunology, immunohistochemistry, protein chemistry, and biochemistry).

Unless otherwise indicated, the recombinant protein, cell culture, and immunological techniques utilized in the present invention are standard procedures, well known to those skilled in the art. Such techniques are described and explained throughout the literature in sources such as, J. Perbal, *A Practical Guide to Molecular Cloning*, John Wiley and Sons (1984), J. Sambrook et al., *Molecular Cloning: A Laboratory Manual*, Cold Spring Harbour Laboratory Press (1989), T. A. Brown (editor), *Essential Molecular Biology: A Practical Approach*, Volumes 1 and 2, IRL Press (1991), D. M. Glover and B. D. Hames (editors), *DNA Cloning A Practical Approach*, Volumes 1-4, IRL Press (1995 and 1996), and F. M. Ausubel et al. (editors), *Current Protocols in Molecular Biology*, Greene Pub. Associates and Wiley-Interscience (1988, including all updates until present), Ed Harlow and David Lane (editors) *Antibodies: A Laboratory Manual*, Cold Spring Harbour Laboratory, (1988), and J. E. Coligan et al. (editors) *Current Protocols in Immunology*, John Wiley & Sons (including all updates until present).

The term "and/or", e.g., "X and/or Y" shall be understood to mean either "X and Y" or "X or Y" and shall be taken to provide explicit support for both meanings or for either meaning.

65 Unless the context suggests otherwise, the mention of a term in singular such a sensor molecule and substrate clearly means the plural as well. For instance, logically many

individual sensor molecules will be flowed through the device rather than a single molecule.

As used herein, the term about, unless stated to the contrary, refers to $\pm 20\%$, more preferably $\pm 10\%$, even more preferably $\pm 5\%$, of the designated value.

Throughout this specification the word “comprise”, or variations such as “comprises” or “comprising”, will be understood to imply the inclusion of a stated element, integer or step, or group of elements, integers or steps, but not the exclusion of any other element, integer or step, or group of elements, integers or steps.

Detection/Classification/Screening System

The present invention relates to a method of detecting an analyte in a sample, the method comprising

- i) flowing through a microfluidic device comprising one or more microchannels,
 - a) the sample,
 - b) a sensor molecule comprising a domain that binds the analyte, a chemiluminescent donor domain and an acceptor domain, wherein the separation and relative orientation of the chemiluminescent donor domain and the acceptor domain, in the presence and/or the absence of analyte, is within $\pm 50\%$ of the Forster distance,
 - c) a substrate of the chemiluminescent donor,
- ii) mixing the sensor molecule, sample and substrate in the device, and
- iii) detecting modification of the substrate by the chemiluminescent donor using an electro-optical sensing device, wherein the spatial location and/or dipole orientation of the chemiluminescent donor domain relative to the acceptor domain is altered when the analyte binds the sensor molecule.

The present invention also relates to a microfluidic system for performing the method of the invention, the system comprising

- i) at least one reservoir suitable for containing (or comprising) a sensor molecule comprising a domain that binds the analyte, a chemiluminescent donor domain and an acceptor domain, wherein the separation and relative orientation of the chemiluminescent donor domain and the acceptor domain, in the presence and/or the absence of analyte, is within $\pm 50\%$ of the Forster distance,
- ii) a microfluidic device comprising one or more microchannels,
- iii) means for mixing the sensor molecule, the sample and a substrate of the chemiluminescent donor domain in the device,
- iv) a reaction chamber for detecting binding of the analyte to the sensor molecule, and
- v) an electro-optical sensing device, wherein the spatial location and/or dipole orientation of the chemiluminescent donor domain relative to the acceptor domain is altered when the analyte binds the sensor molecule.

As the skilled person would appreciate, the methods and systems of the invention can be used to detect the presence or absence of an analyte in a sample, and if present may also be used to determine the concentration of the analyte.

The present invention has numerous advantages over the prior art, particularly when compared to methods and systems where the sensor molecule is fixed to the device. First, there is no need to regenerate (re-set) the device. Second, there is less drift in signal in the methods and systems of the invention. Third, costs are reduced because the device can be

re-used many more times than when the sensor molecule is fixed. Fourth, the invention avoids the problem of low signal with fixed configurations due to surface area and density of sensor molecule. Fifth, the current technique is a volume-based detection technique, not a surface-based technique such as surface plasmon resonance in which the sensor molecules need to be attached to the surface. The sensor-analyte reaction happens much more rapidly, thereby reducing analysis time even without active control.

Furthermore, BRET has several advantages over fluorescence based technologies because it does not require excitation of the donor with an external light source. BRET does not suffer from autofluorescence, light scattering, photobleaching and/or photoisomerization of the donor moiety or photo damage to cells. The absence of an external light source in BRET assays results in a very low background and consequently increased detection sensitivity. For example, BRET is 50 times more sensitive than FRET for monitoring thrombin-catalysed proteolytic cleavage (Dacres et al., 2009b).

With regard to the use of a method of the invention for classifying a sample, a sensor molecule, more typically a set of sensor molecules, can be used to detect patterns of substances (analytes) that are representative for a specific sub-population. As an example, the method can be used to classify different types, age, quality etc. of beer, wine, cheese or other consumables. The method can also be used broadly with samples of foods, beverages, perfumes, fragrances and the like to classify or quantify their organoleptic properties such as sweetness, bitterness, umami character, “heat” for example in relation to capsaicin or hydroxy- α -sanshool, “coolness” for example in relation to menthol and/or any olfactory notes for which suitable sensor molecules can be isolated or engineered. The method can also be used to classify a wide range of other samples based on chemical signatures, for example the health, nutritional or disease status of humans, animals or plants based on samples of headspace, breath, sweat, urine, other biological fluids. Another use of the method is to classify samples based on their toxicity or noxiousness, such as the presence of explosives or explosive-associated components, toxic industrial chemicals, chemical or biological warfare agents or pathogenic microbes. The method can also be used for monitoring of industrial processes including conformity to specifications or the presence, absence of levels of any group or groups of chemicals. The method can also be used to classify environmental samples either in real time or in batch mode, for example to determine air quality, presence or level of unpleasant odours or toxic chemicals or, similarly, the quality of natural or reticulated water systems, sewerage systems or ground water or to classify fluids in contact with soils or rocks.

Classification of samples is usually performed by generating a discriminating function or classifier based on the pattern of electro-optical responses to a training set of samples representing or encompassing all the classes of samples that one wishes to discriminate. This may be achieved routinely using multivariate statistical approaches, such as principal components analysis, linear discriminant analysis, stepwise discrimination analysis and the like. Alternately, a wide variety of machine learning approaches may be used, one example being support vector machines. A similar approach is to use Bayesian networks or train an artificial neural network to make such discriminations among samples of the test set. One viable approach is then to capture a pattern of electro-optical responses from the test or unknown sample(s) process them in real time and com-

pare them with saved patterns, obtained with the training set of samples, assigning them to known classes according to the best matches or assigning them to a novel class or classes if a similar pattern has not previously been observed. For classification methods it is not essential that the actual analyte(s) be known, simply that a sensor molecule (or group of sensor molecules) reproducibly produce a different pattern of signals with different classes of sample, which enables the user to classify the sample(s) being analysed.

With regard to sensitivity, concentrations of analyte as low as micromolar, nanomolar, femtomolar, attomolar or even lower can be detected. In an embodiment, the method of the invention is at least 5 fold, or at least 10 fold, or a 5 fold to 1,000 fold, or 5 fold to 100 fold, or 5 fold to 50 fold, or 5 fold to 20 fold, or and in some circumstances up to 100 to 1,000 fold more sensitive than if the method was performed on a microwell plate with the same concentration of reagents.

The present invention is particularly useful for detecting an analyte in real time. As used herein, the term "real time" means that a certain state is substantially simultaneously displayed in another form (e.g., as an image on a display or a graph with processed data). In such a case, the "real time" lags behind an actual event by the time required for data processing. Such a time lag is included in the scope of "real time" if it is substantially negligible. Such a time lag may be typically within 10 seconds, and preferably within 1 second, without limitation. In a preferred embodiment, the method of the invention is performed within about 1s to about 100s.

As used herein, the "Förster distance" is the distance between the donor and acceptor at which the energy transfer is (on average) 50% efficient. Förster distance (R_0) is dependent on a number of factors, including the quantum yield of the donor in the absence of acceptor, the refractive index of the solution, the dipole angular orientation of each domain, and the spectral overlap integral of the donor and acceptor.

As used herein, "quantum yield" refers to a measure of final emission of original energy donation.

As used herein, "Stokes shift" is the difference in wavelength between positions of the band maxima of the absorption and emission spectra of the same electronic transition.

In an embodiment, the invention is used to analyse, on the device, an increasing (for example, through synthesis of the analyte on the chip) or decreasing (for example, degradation or modification of the analyte on the chip) concentration of the analyte. Typically, this will require detecting modification of the substrate at two different points on the device, for instance in a first and second reaction chamber through which the analyte flows. Thus, in an embodiment, the analyte releasing from the sensor molecule results in a change in BRET ratio which is $\geq 15\%$, $\geq 20\%$, $\geq 30\%$, $\geq 35\%$, about 15% to about 50%, or about 15% to about 40%, of the maximum observed BRET ratio.

In a further embodiment, the sensor molecule may enter the input microchannel bound to a ligand, and the analyte to be detected (for example catalytic enzyme) cleaves and/or modifies the ligand such that the modified ligand releases from (is no longer bound) to the sensor molecule.

The BRET sensing in the methods and systems of the invention is realized in a microfluidic device. In one configuration, the system comprises several modules which include (1) sample delivery, (2) reagent storage and handling, (3) microfluidic chip and loading system, (4) optionally temperature control, (5) electro-optical system for light

collection, (6) electro-optical detection system, (7) data acquisition and processing, and (8) software and embedded control system (FIG. 13).

Sample Delivery

The "sample" can be any substance or composition known or suspected of comprising the analyte to be detected or from which it is expected or required that a particular substance, set of substances or composition is absent. Examples of samples include air, liquid, and biological material. The sample may be obtained directly from the environment or source, or may be at least partially purified by a suitable procedure before a method of the invention is performed.

The sample can be in any form that is capable of being flowed through a microfluidic device. Examples include, but are not necessarily limited to, a liquid, gas, emulsion or suspension. In an embodiment, the sample is a liquid, which has been pre-equilibrated with a gas. Examples of suspensions include, but are not necessarily limited to, water-in-oil, oil-in-water and gas in liquid.

In a more specific embodiment, ambient air or other gases from a location of interest or the headspace from any object or sample of interest is brought into close contact with water or an aqueous solution so that rapid mass transfer of analytes may occur from the gas phase to the liquid phase based on the gaseous concentration, solubility and partition coefficients of the analytes and the composition of the liquid phase. Any method that generates a gas-liquid interface with a large area, relative to the volume of the liquid, is potentially suitable. Example methods include wetted wall cyclones, misting or bubbling systems. The SASS2400 wetted wall cyclone is a specific example of a suitable device for accelerating the partition of volatiles from air into an aqueous phase. Preferably, the method allows a large volume of air to come into contact with a smaller volume of liquid, thereby permitting large volumes of the gas phase to be sampled and providing a concentration step. Based on the published specifications of the SASS2400 it is possible to contact 1 volume of water or aqueous solution with 40,000 volumes of gas at standard temperature and pressure per minute. Depending on the dimensions and operational characteristics of equipment used, much lower or higher gas-liquid ratios may be sampled.

In one embodiment, the suspension is, or comprises, a cell-free extract. In an alternate embodiment, the suspension comprises cells.

The sample (and the sensor molecule and substrate) can be flowed through the microfluidic device by any suitable means such as, but are not necessarily limited to, one or more of pumping, vacuum, hydraulics, suction, electrokinesis, chemiosmosis, capillary force, acoustics, electromagnetics, piezoelectrics and so on. Pumping mechanisms can be realised in compact, miniaturised and micron-size pumps for the applications. There may be a pre-conditioning device to filter out debris such as particles, organic droplets and so on from the sample, and/or a condition monitoring device which measures some basic parameters of the samples such as temperature, humidity, flow rate and volume of samples.

Reagent Storage and Handling

A disposable and retractable liquid storage system for multiple reagents (BRET reagent, cleaning DI water, substrate etc.) storage can be used. The device can be pre-loaded in the laboratory and be inserted into the sensing device during operation.

Microfluidic Device and Loading System

Microfluidic devices (also referred to in the art as a chip or "lab-on-a-chip") perform chemical or biochemical reac-

tions or analyses by manipulating fluid reagents in chambers and passages which are generally sized in cross-section from approximately 10 to 50 μm (micrometers) up to approximately 100 to 1000 μm , and which are formed on or in a usually flat substrate having linear dimensions from approximately 1 mm to approximately 20 cm. A microfluidic device may manipulate fluid reactants as they flow through the passages and chambers of the device, either as continuous flows from input reservoirs through the device to outlet ports, or as semi-continuous flows of fluid aliquots substantially filling the passages and chambers of the device during operation. Alternatively, microfluidic devices may manipulate fluid reagents as separate and discrete micro-droplets that are characterized by having lengths that are approximately an order of magnitude or more smaller than the dimensions of the device.

The microfluidic device may maintain connection with all sample and reagent delivery outlet once it is inserted into a chip loading system. This loading system can form part of the temperature control and optical components. Single to multiple reactors can be integrated into a chip (FIG. 14). Three reagent (sample, sensor molecule and substrate) flows can be pumped into the chip and mixed in the mixing region. In an alternate configuration, there are two input microchannels, one for the substrate and the other for a pre-mixture of the sensor molecule and sample. In a further configuration, there are two input microchannels, one for the sensor molecule and the other for a pre-mixture of the substrate and sample.

The mixed reagents will undergo BRET reactions and the products can be continuously pumped through the detection chamber before being collected from the waste outlets (FIG. 15).

As used herein, the term "mixing" or variations thereof mean that the analyte(s), sensor molecule and substrate come into contact through any kind of means whether it be diffusion (for example resulting from linear (laminar) flow) and/or through some sort of active mixing means. Thus, in one embodiment the "means for mixing" can be passive diffusion in a linear (laminar) flow. In this embodiment, although complete mixing is not achieved, the present inventors have found that a sufficient amount of mixing occurs for the methods of the invention to function properly. In an embodiment, the diffusion mixing results in at least 20% of the microchannel comprising the sample, sensor molecule and substrate having a homogeneous mixture of these components.

The angle at least two microchannels converge to form the common microchannel can vary from 0° to close to approximately 170° or indeed at an angle to the plane of the microfluidic chip (device).

As used herein, the term "common microchannel" or variations thereof refers to a microchannel, or section thereof, comprising the sample, sensor molecule and the substrate.

As used herein, the term "input microchannel" or variations thereof refers to the microchannel through which a particular reagent such as the sample, sensor molecule or the substrate, or combination of reagents, enters the microfluidic device.

In at least some embodiments, due to the existence of a laminar flow region, a mixing means is preferably implemented in the mixing region for enhancing the contact of the reactants. The mixing means may include passive mixing (FIG. 8 and FIG. 44) and/or active mixing such as with an acoustic mixer (for example as described in WO 2006/

105616). Other mixing techniques can also be implemented for such a purpose such as that described in WO 2003/015923.

As used herein, the term "mixing the sensor molecule, sample and substrate in the device" and variations thereof encompasses mixing the sensor molecule, sample and substrate in a reservoir of the device, mixing the sensor molecule, sample and substrate in tubes which flow into the microchannels of the device, mixing the sensor molecule, sample and substrate in the microchannels of the device or mixing the sensor molecule, sample and substrate in a reaction chamber, or a combination or two or more thereof. In a preferred embodiment, the sensor molecule, sample and substrate are mixed in a microchannel. Preferably, if the sensor molecule and sample are not mixed in the microchannels they are mixed shortly before (for example 10 seconds, more preferably 1 second, or less) before entering the microchannels.

In an embodiment, the mixing step results in the sensor molecule, substrate and analyte forming a mixture which is at least 20%, at least 30%, at least 40%, at least 50%, at least 60%, at least 70%, at least 80%, at least 90%, or at least 95%, homogeneous. As indicated above, active mixing will result in greater levels of homogeneity for any given flow rate and channel architecture, but this is not necessarily required to perform the invention.

The methods of the invention can be used to simultaneously or sequentially detect two or more different analytes using the same microfluidic device, for example using a device as shown in FIGS. 14b and 14c. In an embodiment, different sensor molecules are flowed into the device using different microchannels. For convenience, if the sample to be analysed is the same for each of the analytes there may be a single flow of sample into the device which then branches and joins with other channels comprising different sensor molecules (see FIGS. 14b and 14c). The same applies if the substrate for each of the sensor molecules is the same. The skilled person can readily design a suitable configuration for the microchannels depending on the number of samples to be analysed, the number of sensor molecules required to detect each target analyte, and the number of corresponding substrates required in light of the different sensor molecules being used.

Microfluidic devices can be fabricated from any material that has the necessary characteristics of chemical compatibility and mechanical strength. Examples of such substances include, but are not necessarily limited to, silicon, glass (e.g. fused silica, fused quartz, boro-silicate, or any type of glass with different additives), polydimethylsiloxane, polyimide, polyethylene terephthalate, polymethylmethacrylate, polyurethane, polyvinylchloride, polystyrene polysulfone, polycarbonate, polymethylpentene, polypropylene, a polyvinylidene fluoride, polysilicon, polytetrafluoroethylene, polysulfone, acrylonitrile butadiene styrene, polyacrylonitrile, polybutadiene, poly(butylene terephthalate), poly(ether sulfone), poly(ether ketones), poly(ethylene glycol), styrene-acrylonitrile resin, poly(trimethylene terephthalate), polyvinyl butyral, polyvinylidenedifluoride, poly(vinyl pyrrolidone), cyclic olefin-copolymer and any combination thereof.

The device (chip) can be constructed using standard techniques in the art such as single and multilayer soft lithography (MSL) techniques and/or sacrificial-layer encapsulation methods (see, e.g., Unger et al. (2000); WO 01/01025). Further methods of fabricating microfluidic devices include micromachining, micromilling, laser-based machining, chemical etching, (deep) reactive ion etching,

imprinting techniques. These techniques can be used in conjunction with hot embossing and/or injection moulding techniques for mass production of the microdevices. There is a large body of prior art in fabrication techniques. Some of these are also described in U.S. Pat. Nos. 5,858,195, 5,126,022, 4,891,120, 4,908,112, 5,750,015, 5,580,523, 5,571,410, 5,885,470 and 6,793,753. Freestanding structures can be made to have very thin or very thick walls in relation to the channel width and height. The walls, as well as the top and bottom of a channel can all be of different thickness and can be made of the same material or of different materials or a combination of materials such as a combination of glass, silicon, and a biologically-compatible material such as PDMS. Sealed channels or chambers can be made entirely from biologically-compatible material such as PDMS.

Devices useful for the invention can have one or more channels and/or reaction chambers. For example, the device can comprise 2, 3, 4, 5, 6, 7, 8, 9, 10 or more channels. Furthermore, the device can comprise 2, 3, 4, 5, 6, 7, 8, 9, 10 or more reactions chambers.

The reaction chamber and microchannels can be any suitable shape known in the art such as, but are not limited to, cylindrical, rectangular, semi-spherical or trapezoidal.

In an embodiment, where the device is capable of performing more than one reaction the channel design is such that each component flows through channels with the same length, size and configuration such as the bilaterally symmetrical parallel channel layout provided in FIG. 47.

In another embodiment, the function of the microchannels and the functions of the reaction chamber may be fulfilled by a single combined microfluidic element in which mixing occurs and from which light is collected.

The microfluidic device will typically have one or more reaction chamber volumes of about 1 pl (i.e. picoliter or a trillionth of a liter) to about 200 μ l. However, reaction chamber volumes of between about 0.01 nl (i.e. nanoliter or a billionth of a liter) to about 100 nl, or between about 0.01 nl and 10 nl may be advantageous in certain applications. Some embodiments may optimally perform when the volume of each reaction chambers is between about 0.20 nl to about 5 nl. An additional embodiment is where the volume of each reaction chambers is between about 0.25 nl to about 2 nl. In a further embodiment, the reaction chamber(s) have a volume of about 1 μ l to about 12 μ l. Other possible reaction chamber volumes may be used where appropriate.

In a preferred embodiment, the reaction chamber is wider than it is short. In one example, the reaction chamber has a cross-sectional area of about 1 mm² to 1 cm² and a height of no more than about 5 mm.

In some circumstances it may be desirable to use reaction chambers of more than one size and shape. For example, the present inventors have observed that larger reaction chambers generate more light and allow the detection of more weakly emitting sensor molecules, often at the expense of a slower response time (time to peak change in BRET ratio) upon presentation of a sample containing a target analyte and a longer off-time when the analyte is removed. Different channels may therefore be equipped with reaction chambers of different sizes in order to match the sensitivity, precision and time dynamics of particular combinations of sensor molecules and analytes or sets of analytes. It would also be possible, and may in some cases be desirable, to implement more than one reaction chamber per sensor channel. This would allow near simultaneous detection of samples with higher luminance and quantitative precision (large chamber) and higher time resolution (smaller chamber). This could easily be achieved by fitting the large and smaller chambers

with their own light path to the detector via an optical switch or equivalent, or fitting each with separate solid state light detectors.

Dimensions of the microchannels can be chosen based on the specific application of the device. Accordingly, width of the microchannel can range from, for example, about 0.1 mm to about 10 mm. In some embodiments, the width of the microchannel is from about 0.5 mm to about 5 mm. In some embodiments, the width of the microchannel is from about 1 mm to about 4 mm. In some embodiments, the width of the microchannel is about 2.5 mm. Depth or height of the microchannel can also be chosen based on the specific application of the device. Accordingly, the depth of the microchannel can range from, for example, about 5 μ m to about 2000 μ m. In some embodiments, the depth of the microchannel is from about 100 μ m to about 1000 μ m. In some embodiments, the depth of the microchannel is from about 250 μ m to about 750 μ m. In some embodiments, the depth of the microchannel is about 560 μ m. In another embodiment, each microchannel has a cross-sectional area of about 1 μ m² to about 1 mm².

As the skilled person will understand, the device will have suitable inlet ports and outlet ports to enable the relevant components to flow through the device.

The skilled artisan is well aware that the flow through a microfluidic device is dependent on various factors including, but not limited to, dimensions of the microchannels, viscosity of the fluid, and the detection and method employed. Accordingly, the sample (sensor molecule and substrate) can flow through the chip microchannel at a rate of about 1 μ l/hr to about 10 ml/hr. In some embodiments, the sample (sensor molecule and substrate) can flow through the device microchannel at a rate of about 1 μ l/hr to about 100 μ l/hr, about 5 μ l/hr to about 200 μ l/hr, from about 7.5 μ l/hr to about 500 μ l/hr, or about 10 μ l/hr to about 1 ml/hr.

In one embodiment, the device comprises multiple reaction chambers for sensing, for example, different analytes in the same source (sample). Due to the likely need to use different sensor molecules to detect different analytes, in some instances it may be desirable to modify the flow rate in different, preferably parallel, channels. In this regard, each individual flow rate can be set to optimize the sensitivity for each individual sensor molecule.

In one embodiment, in a device comprising multiple reaction chambers the flow rate to and from each reaction chamber is controlled by separate means, for instance a separate suction pump controls the flow rate to and from each reaction chamber. This configuration allows the simultaneous operation of multiple sensor channels independently of each other with potentially different flow rates and consequently different balances between speed and sensitivity.

The surface of the microfluidic channels may be passivated by exposure to a solution of a suitable reagent, such as a 0.1-5% (w/v) aqueous solution of bovine serum albumin, diluted mammalian serum, fish-skin gelatin, fat free milk proteins and/or using a solution of a non-ionic detergent, such as Tween-20 or by using a suspension of yeast microsomes.

After the reagents (sample, sensor molecule, substrate) have passed through the device, the device can be washed by flowing an appropriate fluid, e.g., a washing fluid such as a buffer, through the microchannels. This enables the device to be re-used. According, in some embodiments, the method further comprises the step of flowing a fluid, such as a buffer, through the microdevice after the analyte has been detected. The amount of fluid to be flown through the microdevice can

be any amount and can be based on the volume of the chip. In some embodiments, the amount of the washing fluid is from about 0.5× to about 10× total volume of the microchannels in the device. In one embodiment, the amount of the washing fluid is from about 1.5× to about 2.5× total

Temperature Control

If present, this module is used to maintain desired temperatures for reagent storage, 1-8° C., preferably 2-4° C. and BRET reactions, 20-37° C., preferably 25-28° C. The BRET temperature control can be integrated with the loading mechanism and the electro-optical collection device. In particular they are constructed according to a technology that uses local resistive heating or Peltier-device cooling for control functions. For example, a thermally-controlled processor can be maintained at baseline temperature by a temperature-controlled heat sink or a cooling element, such as a Peltier device, with actuators controlled by localized heating above the baseline. Alternatively, cooling may be provided using a miniature heat pump. Localized heating may preferably be provided by low power resistive heaters of less than approximately 1 to 2 W, advantageously controlled by low voltages, for example, less than 50, 25, 15 or 10 V.

Electro-Optical System for Light Collection

The term “signal” as used herein refers to luminescence measured as a change in absorbance. In some embodiments, the signal will be “emitted light”, wherein the step of detecting the signal will be the detection of photons of specific wavelengths of light by one or more photodetectors. Example photodetectors include photomultiplier tubes (PMTs), photodiodes, avalanche photodiodes, silicon or other solid state photomultipliers (http://en.wikipedia.org/wiki/Silicon_photomultiplier) or CCD cameras, which may be cooled. Preferably, the photodetector has a photon detecting efficiency of $\geq 10\%$, more preferably $\geq 30\%$ and most preferably $\geq 50\%$. Preferably these efficiencies operate in the blue and green bands of the optical spectrum. The detector further comprises a means of restricting the detected light to specific wavelength(s) or specific ranges of wavelengths. This can be, for example, suitable filters optionally mounted to a filter wheel or a filter slide or a monochromator or a dichroic mirror or a combination of two or more of these devices.

The electro-optical system may mainly consist of optical fibres and an optical switch (FIG. 16). The optical fibre can be replaced by fibre bundles or liquid light guides. The fibres with core diameters from about 10 μm to about 3000 μm can be fixed into the loading system. For fibre bundles or liquid light guides, the core diameter can be in the range from 0.5 mm to 10 mm. The flat ends of the fibres may be located right below the reaction chambers, each fibre collecting light from a particular chamber. Two BRET electro-optical detection elements can be designed which can be integrated with the reaction chamber (see FIG. 17). A spherical microlens might be incorporated into the reaction chamber to help focus BRET light into the core of the optical fiber.

In another embodiment, the optical fibre/liquid light guide system can be replaced by a set of lenses and mirrors so that light from each chamber is relayed to the detectors. The switching for multiple channel system can be realised by a mechanical chopper or other switching mechanisms.

To further increase the BRET signal collected, a flat or aspherical mirror might be placed on top of the reaction chamber (FIG. 17b). In this case, most of the BRET light emitted to the top will be reflected back into the optical fibers. For multi-channel detection, an optical switch can be

used to collect lights from all channels. The material for this element can be in glass or polymeric materials, which have excellent optical, chemical properties such as polydimethylsiloxane, cyclic olefin co-polymer (COC) and so on. The BRET reaction chamber will be connected to the microfluidic network designed above for sample delivery and mixing.

Digital Photon Integration

Ultra low level light detection requires a highly sensitive photomultiplier tube (PMT) and digital signal processing unit to eliminate the dark current FIG. 42 illustrates an example system for use in the invention composed of three units: PMT, Photon counting unit, USB counting unit. H10721P-210 is a current output PMT with ultrabialkali photocathode providing high sensitivity in visible wavelengths. The photosensitive area is round shape with a diameter of 8 mm. When a photon reaches to the ultrabialkali photocathode, photoelectrons are generated. The photoelectrons are accelerated towards a series of cascaded electrode structures at which the number of electrons increased exponentially at each stage. At the final stage the PMT outputs the sum of the generated electrons as a photoelectron pulse or current.

The dark current is defined as the current output appearing from a PMT in the absence of incident light. By identifying and eliminating the so-called the “dark pulses” it is possible to minimize the dark current. In this example, a signal processing unit (C9744 Photon counting unit) is used to eliminate the dark pulses. The unit allows implementation of a user set threshold value such that only the pulses with amplitude higher than the threshold value are sent to output. The remaining pulses are filtered out of the output signal. In this unit, the pulses which pass the discrimination criteria are converted to 5 V digital signal pulses and sent to the output terminal.

C8855-01 is a USB interface counting unit designed to count digital signal pulses without dead time. The signal generated in C9744 Photon counting unit is input to the counting unit and results are sent to a PC with a USB connection.

Optical Detection System

Detection can be achieved using detectors that are incorporated into the device or that are separate from the device but aligned with the region of the device to be detected.

The optical detection system samples the light output from each microfluidic channel, including each BRET reaction chamber. Each microfluidic channel may be equipped with a dedicated photodetector. For example, a fraction of the optical output of a single BRET reaction chamber may be channeled through a blue band-pass filter, while the remainder may be channeled through a green band-pass filter (or other suitable band-pass characteristics depending on the type of BRET in use). Light from these filters may be directed to separate photomultipliers using optical fibres, bundles of optical fibres or liquid light guides. Alternatively, silicon or other highly sensitive solid-state photomultipliers may be placed in close proximity to the band pass filters so as to sample the light emissions directly from each microfluidic channel and BRET reaction chamber. In an other embodiment, an aspherical lens or set of aspherical lenses might be placed at the end of the optical fibre, bundles of optical fibre or liquid light guide to collimate the output beam before entering the PMTs, thus reducing the optical loss due to rays diverging outside the sensitive area of the PMTs. In a preferred embodiment, the bandpass filters are placed on opposite sides of the microfluidic chip and in close contact with it and solid state photomultipliers or other

photodetectors are placed in close contact with both of the bandpass filters on each of the microfluidic channels. The advantages of providing a dedicated detection system for each microfluidic channel are that it minimises the complexity of the optical system and minimise potential photon losses, including those due to the switching dead time, where each microfluidic channel is optically silent for the majority of the polling cycle.

Alternatively, each microfluidic channel may be polled sequentially by one or more shared photodetectors.

In one embodiment, the detection system may consist of an optical or optomechanical switching device, which receives light via an optical fiber or light guide from each of the microfluidic channels and sequentially outputs the optical signal of each of these inputs via a single optical fiber or light guide. The switching time from chamber to chamber could be in the range of nanoseconds to a few seconds (for example 2 or 3), preferably in the range of a 10-500 milliseconds or less. The output of the optical switching device impinges on and a photodetector such as a dichroic mirror to split the light into two wavelength ranges corresponding to the emissions of BRET donor and acceptor, respectively and two photomultiplier tubes for simultaneously detecting the light in each of these wavelength ranges (FIG. 16). Optionally, the dichroic block may be augmented by band pass filters tuned to the BRET donor and acceptor emission spectra.

In an alternative embodiment, a shutter box may be used instead of the optical switch. In such an arrangement, the output of the shutter box may be a many-to-one multifurcated light guide, which constrains the output of all optical channels into a single light guide that directs light to the photodetector. In this arrangement the shutters are operated so that the light from each single microfluidic channel is passed to the photodetector sequentially. The potential advantage of a switching system is that it allows a smaller number of photodetectors to sample the optical output of a larger number of microfluidic channels with cost, weight and power savings.

In another embodiment, the operating characteristics of the paired solid state photodetectors may be chosen so that their peak photon detection efficiencies (PDEs) are selective or semi-selective for the peak emissions of the BRET donor and acceptor. In this case, it is possible to dispense with the spectral filters and dichroic block and rely on the inherent differential spectral sensitivities different types of solid state photodetector to generate a BRET ratio.

Data Acquisition and Processing

The BRET signal of donors and acceptors in terms of counts/gate versus time will be collected by suitable software. A BRET ratio is calculated based on the ratio of light collected from the acceptors channel to the light collected from the donor channel. This BRET ratio should be constant if the ratio of flows of the sensor molecule and substrate remains constant and without the analyte to be detected in the BRET chamber. However, in the presence of the analyte, the BRET ratio will change corresponding to the amount of reagent in the reaction chambers.

Software and Embedded Control System

Preferably, the system comprises a trainable data processing and output software algorithm that can learn and discriminate the response patterns characteristic of different chemical samples. The software will capture salient features of the signal from each microfluidic channel, such as the baseline BRET ratio, the steady state BRET ratio when exposed to a sample and various features of the time course of changes in BRET ratio. These features from each channel

will be input into a variety of discriminating algorithms, such as principle components analysis, linear discriminant analysis, stepwise discriminant analysis, machine learning algorithms such as support vector machines, Bayesian network analysis or neural network algorithms and compared with the results of previously learned sample classifications. Tentative sample analysis or classification is provided to the operator, preferably through a GUI and/or acoustical output. Alternatively, the signal strength in each channel may be output visually and/or acoustically so that the operator may match response patterns with those they have previously been trained to recognise.

In one embodiment, GUI software is used for controlling all in-device compositions such as the speed and concentration ratio of the sampling subsystem, the rate of flow of the microfluidic channels, the timing of flushing and purging cycles, pumps, the rate and intensity of any active mixing, the sensitivity and integration time of the photodetector systems, the temperature of the reagent reservoirs and the reaction changer and all aspects of data acquisition and processing. Optionally many of these functions may be carried out through an embedded microcontroller. Some or all of the functions may be carried out on a laptop or tablet computer or equivalent device.

Chemiluminescence Resonance Energy Transfer

Chemiluminescence is the emission of energy with limited emission of heat (luminescence), as the result of a chemical reaction. The term "chemiluminescence" is used herein to encompass bioluminescence, which relies upon the activity of an enzyme.

As used herein, bioluminescent resonance energy transfer (BRET) is a proximity assay based on the non-radioactive transfer of energy between the bioluminescent protein donor and the acceptor molecule.

As used herein, the term "spatial location" refers to the three dimensional positioning of the donor relative to the acceptor molecule which changes as a result of the analyte binding or releasing from the sensor molecule.

As used herein, the term "dipole orientation" refers to the direction in three-dimensional space of the dipole moment associated either with the donor and/or the acceptor molecule relative their orientation in three-dimensional space. The dipole moment is a consequence of a variation in electrical charge over a molecule.

Using BRET as an example, in an embodiment the energy transfer occurring between the bioluminescent protein and acceptor molecule is presented as calculated ratios from the emissions measured using optical filters (one for the acceptor molecule emission and the other for the bioluminescent protein emission) that select specific wavelengths (see equation 1).

$$E_a/E_d = \text{BRET ratio} \quad (1)$$

where E_a is defined as the acceptor molecule emission intensity (emission light is selected using a specific filter adapted for the emission of the acceptor) and E_d is defined as the bioluminescent protein emission intensity (emission light is selected using a specific filter adapted for the emission of the bioluminescent protein).

It should be readily appreciated by those skilled in the art that the optical filters may be any type of filter that permits wavelength discrimination suitable for BRET. For example, optical filters used in accordance with the present invention can be interference filters, long pass filters, short pass filters, etc. Intensities (usually in counts per second (CPS) or relative luminescence units (RLU)) of the wavelengths passing through filters can be quantified using either a

photo-multiplier tube (PMT), photodiode, including a cascade photodiode, photodiode array or a sensitive camera such as a charge coupled device (CCD) camera. The quantified signals are subsequently used to calculate BRET ratios and represent energy transfer efficiency. The BRET ratio increases with increasing intensity of the acceptor emission.

Generally, a ratio of the acceptor emission intensity over the donor emission intensity is determined (see equation 1), which is a number expressed in arbitrary units that reflects energy transfer efficiency. The ratio increases with an increase of energy transfer efficiency (see Xu et al., 1999).

Energy transfer efficiencies can also be represented using the inverse ratio of donor emission intensity over acceptor emission intensity (see equation 2). In this case, ratios decrease with increasing energy transfer efficiency. Prior to performing this calculation the emission intensities are corrected for the presence of background light and auto-luminescence of the substrate. This correction is generally made by subtracting the emission intensity, measured at the appropriate wavelength, from a control sample containing the substrate but no bioluminescent protein, acceptor molecule or polypeptide of the invention.

$$Ed/Ea=BRET \text{ ratio} \quad (2)$$

where Ea and Ed are as defined above.

The light intensity of the bioluminescent protein and acceptor molecule emission can also be quantified using a monochromator-based instrument such as a spectrofluorimeter, a charged coupled device (CCD) camera or a diode array detector. Using a spectrofluorimeter, the emission scan is performed such that both bioluminescent protein and acceptor molecule emission peaks are detected upon addition of the substrate. The areas under the peaks represent the relative light intensities and are used to calculate the ratios, as outlined above. Any instrument capable of measuring lights for the bioluminescent protein and acceptor molecule from the same sample, can be used to monitor the BRET system of the present invention.

In an alternative embodiment, the acceptor molecule emission alone is suitable for effective detection and/or quantification of BRET. In this case, the energy transfer efficiency is represented using only the acceptor emission intensity. It would be readily apparent to one skilled in the art that in order to measure energy transfer, one can use the acceptor emission intensity without making any ratio calculation. This is due to the fact that ideally the acceptor molecule will emit light only if it absorbs the light transferred from the bioluminescent protein. In this case only one light filter is necessary.

In a related embodiment, the bioluminescent protein emission alone is suitable for effective detection and/or quantification of BRET. In this case, the energy transfer efficiency is calculated using only the bioluminescent protein emission intensity. It would be readily apparent to one skilled in the art that in order to measure energy transfer, one can use the donor emission intensity without making any ratio calculation. This is due to the fact that as the acceptor molecule absorbs the light transferred from the bioluminescent protein there is a corresponding decrease in detectable emission from the bioluminescent protein. In this case only one light filter is necessary.

In an alternative embodiment, the energy transfer efficiency is represented using a radiometric measurement which only requires one optical filter for the measurement. In this case, light intensity for the donor or the acceptor is determined using the appropriate optical filter and another measurement of the samples is made without the use of any

filter (intensity of the open spectrum). In this latter measurement, total light output (for all wavelengths) is quantified. Ratio calculations are then made using either equation 3 or 4. For the equation 3, only the optical filter for the acceptor is required. For the equation 4, only the optical filter for the donor is required.

$$Ea/Eo-Ea=BRET \text{ ratio or } =Eo-Ea/Ea \quad (3)$$

$$Eo-Ed/Ed=BRET \text{ ratio or } =Ed/Eo-Ed \quad (4)$$

where Ea and Ed are as defined above and Eo is defined as the emission intensity for all wavelengths combined (open spectrum).

It should be readily apparent to one skilled in the art that further equations can be derived from equations 1 through 4. For example, one such derivative involves correcting for background light present at the emission wavelength for bioluminescent protein and/or acceptor molecule.

In performing a BRET assay, light emissions can be determined from each well using the BRETCount. The BRETCount instrument is a modified TopCount, wherein the TopCount is a microtiterplate scintillation and luminescence counter sold by Packard Instrument (Meriden, Conn.). Unlike classical counters which utilise two photomultiplier tubes (PMTs) in coincidence to eliminate background noise, TopCount employs single-PMT technology and time-resolved pulse counting for noise reduction to allow counting in standard opaque microtiter plates. The use of opaque microtiterplates can reduce optical crosstalk to negligible level. TopCount comes in various formats, including 1, 2, 6 and 12 detectors (PMTs), which allow simultaneous reading of 1, 2, 6 or 12 samples, respectively. Beside the BRETCount, other commercially available instruments are capable of performing BRET: the Victor 2 (Wallac, Finland (Perkin Elmer Life Sciences)) and the Fusion (Packard Instrument, Meriden). BRET can be performed using readers that can detect at least the acceptor molecule emission and preferably two wavelengths (for the acceptor molecule and the bioluminescent protein) or more.

Chemiluminescence

Non-enzymatic chemiluminescence is the result of chemical reactions between an organic dye and an oxidizing agent in the presence of a catalyst. Chemiluminescence emission occurs as the energy from the excited states of organic dyes, which are chemically induced, decays to ground state. The duration and the intensity of the chemiluminescence emission are mostly dependent on the extent of the chemical reagents present in the reaction solution.

As used herein, the term "bioluminescent protein" refers to any protein capable of acting on a suitable substrate to generate luminescence.

It is understood in the art that a bioluminescent protein is an enzyme which converts a substrate into an activated product which then releases energy as it relaxes. The activated product (generated by the activity of the bioluminescent protein on the substrate) is the source of the bioluminescent protein-generated luminescence that is transferred to the acceptor molecule.

There are a number of different bioluminescent proteins that can be employed in this invention (see, for example, Table 1). Light-emitting systems have been known and isolated from many luminescent organisms including bacteria, protozoa, coelenterates, mollusks, fish, millipedes, flies, fungi, worms, crustaceans, and beetles, particularly click beetles of genus *Pyrophorus* and the fireflies of the genera *Photinus*, *Photuris*, and *Luciola*. Additional organ-

isms displaying bioluminescence are listed in WO 00/024878, WO 991049019 and Viviani (2002).

One very well known example is the class of proteins known as luciferases which catalyze an energy-yielding chemical reaction in which a specific biochemical substance, a luciferin (a naturally occurring fluorophore), is oxidized by an enzyme having a luciferase activity (Hastings, 1996). A great diversity of organisms, both prokaryotic and eukaryotic, including species of bacteria, algae, fungi, insects, fish and other marine forms can emit light energy in this manner and each has specific luciferase activities and luciferins which are chemically distinct from those of other organisms. Luciferin/luciferase systems are very diverse in form, chemistry and function. Bioluminescent proteins with luciferase activity are thus available from a variety of sources or by a variety of means. Examples of bioluminescent proteins with luciferase activity may be found in U.S. Pat. Nos. 5,229,285, 5,219,737, 5,843,746, 5,196,524, and 5,670,356. Two of the most widely used luciferases are: (1) *Renilla* luciferase (from *R. reniformis*), a 35 kDa protein, which uses coelenterazine as a substrate and emits light at 480 nm (Lorenz et al., 1991); and (ii) Firefly luciferase (from *Photinus pyralis*), a 61 kDa protein, which uses luciferin as a substrate and emits light at 560 nm (de Wet et al., 1987).

Gaussia luciferase (from *Gaussia princeps*) has been used in biochemical assays (Verhaegen et al., 2002). *Gaussia*

luciferase is a 20 kDa protein that oxidises coelenterazine in a rapid reaction resulting in a bright light emission at 470 nm.

Luciferases useful for the present invention have also been characterized from *Anachnocampa* sp (WO 2007/019634). These enzymes are about 59 kDa in size and are ATP-dependent luciferases that catalyze luminescence reactions with emission spectra within the blue portion of the spectrum.

Biologically active variants or fragments of naturally occurring bioluminescent protein can readily be produced by those skilled in the art. Three examples of such variants useful for the invention are RLuc2 (Loening et al., 2006), RLuc8 (Loening et al., 2006) and RLuc8.6-535 (Loening et al., 2007) which are each variants of *Renilla* luciferase. In a further preferred embodiment, the sequence of the BRET chemiluminescent donor is chosen to have greater thermal stability than sensor molecules incorporating native *Renilla* luciferase sensors. RLuc2 or RLuc8 are convenient examples of suitable choices, which consequently exhibit $\geq 5\times$ or $\geq 10\times$ higher luminance than sensors incorporating the native *Renilla* luciferase sequence. Such enhanced luminance has significant benefits as it permits the use of lower detection chamber volumes and/or faster on-chip flow rates with concomitant improvement in time resolution at any given combination of detection chamber volume and flow rate. Alternatively, it permits more economical use of reagents for any given time resolution.

TABLE 1

Exemplary bioluminescent proteins.					
Species	Name	Organism	MW kDa $\times 10^{-3}$	Emission (nm)	Example of Substrate
Insect	FFluc	<i>Photinus pyralis</i> (North American Firefly)	~61	560	D-(-)-2-(6'-hydroxybenzothiazolyl)- Δ^2 -thiazoline-4-carboxylic acid, HBTTCa (C ₁₁ H ₈ N ₂ O ₃ S ₂) (luciferin)
Insect	FF'luc	<i>Luciola cruciata</i> (Japanese Firefly)		560-590 (many mutants)	Luciferin
Insect		Phengodid beetles (railroad worms)			Luciferin
Insect		<i>Arachnocampa</i> sp.			Luciferin
Insect		<i>Orphelia fultoni</i> (North American glow worm)			Luciferin
Insect	Cluc	<i>Pyrophorus plagiophthalmus</i> (click beetle)		546, 560, 578 and 593	Luciferin
Jellyfish	Aequorin	<i>Aequorea</i>	44.9	460-470	Coelenterazine
Sea pansy	Rluc	<i>Renilla reniformis</i>	36	480	Coelenterazine
Sea pansy (modified)	Rluc8	<i>Renilla reniformis</i> (modified)	36	487 (peak)	Coelenterazine/ Deep Blue C
Sea pansy (modified)	Rluc2	<i>Renilla reniformis</i> (modified M185V/Q235A)	36	480	Coelenterazine
Sea pansy (modified)	RLuc8.6-535	<i>Renilla reniformis</i> (modified)	36	535	Coelenterazine
Sea pansy	Rmluc	<i>Renilla mullerei</i>	36.1	~480	Coelenterazine
Sea pansy		<i>Renilla kollikeri</i>			
Crustacea (shrimp)	Vluc	<i>Vargula hilgendorffii</i>	~62	~460	coelenterazine *
Crustacea		Cypridina (sea firefly)	75	460	coelenterazine **
Dinofagellate (marine alga)		<i>Gonyaulax polyedra</i>	130	~475	Tetrapyrrole
Mollusc		<i>Latia</i> (fresh water limpet)	170	500	Enol formate, terpene, aldehyde
Hydroid		<i>Obelia bicuspidata</i>	~20	~470	Coelenterazine
Shrimp		<i>Oplophorus gracilorostris</i>	31	462	Coelenterazine

TABLE 1-continued

Exemplary bioluminescent proteins.					
Species	Name	Organism	MW kDa $\times 10^{-3}$	Emission (nm)	Example of Substrate
Others	Ptluc	Ptilosarcus		~490	Coelenterazine
	Gluc	Gaussia	~20	~475	Coelenterazine
	Plluc	Pleuromamma	22.6	~475	Coelenterazine

As used herein, a “biologically active fragment” is a portion of a polypeptide as described herein which maintains a defined activity of the full-length polypeptide. As used herein, a “biologically active variant” is a molecule which differs from a naturally occurring and/or defined molecule by one or more amino acids but maintains a defined activity, such as defined above for biologically active fragments. Biologically active variants are typically least 50%, more preferably at least 80%, more preferably at least 90%, more preferably at least 95%, more preferably at least 97%, and even more preferably at least 99% identical to the naturally occurring and/or defined molecule.

Alternative, non-luciferase, bioluminescent proteins that can be employed in this invention are any enzymes which can act on suitable substrates to generate a luminescent signal. Specific examples of such enzymes are β -galactosidase, lactamase, horseradish peroxidase, alkaline phosphatase, β -glucuronidase and β -glucosidase. Synthetic luminescent substrates for these enzymes are well known in the art and are commercially available from companies, such as Tropix Inc. (Bedford, Mass., USA).

An example of a peroxidase useful for the present invention is described by Hushpulian et al. (2007).

In a preferred embodiment, a bioluminescent protein with a small molecular weight is used to prevent an inhibition of the interaction due to steric hindrance. The bioluminescent protein preferably consists of a single polypeptide chain. Also the bioluminescent proteins preferably do not form oligomers or aggregates. The bioluminescent proteins *Renilla* luciferase, *Gaussia* luciferase and Firefly luciferase meet all or most of these criteria.

Substrates

As used herein, the term “substrate” refers to any molecule that can be used in conjunction with a chemiluminescent donor to generate or absorb luminescence. The choice of the substrate can impact on the wavelength and the intensity of the light generated by the chemiluminescent donor.

A widely known substrate is coelenterazine which occurs in cnidarians, copepods, chaetognaths, ctenophores, decapod shrimps, mysid shrimps, radiolarians and some fish taxa (Greer and Szalay, 2002). For *Renilla* luciferase for example, coelenterazine analogues/derivatives are available that result in light emission between 418 and 512 nm (Inouye et al., 1997). A coelenterazine analogue/derivative (400A, DeepBlueC) has been described emitting light at 400 nm with *Renilla* luciferase (WO 01/46691). Other examples of coelenterazine analogues/derivatives are EnduRen and ViviRen.

As used herein, the term “luciferin” refers to a class of light-emitting biological pigments found in organisms capable of bioluminescence, which are oxidised in the presence of the enzyme luciferase to produce oxyluciferin and energy in the form of light. Luciferin, or 2-(6-hydroxybenzothiazol-2-yl)-2-thiazoline-1-carboxylic acid, was first isolated from the firefly *Photinus pyralis*. Since then, various

forms of luciferin have been discovered and studied from various different organisms, mainly from the ocean, for example fish and squid, however, many have been identified in land dwelling organisms, for example, worms, beetles and various other insects (Day et al., 2004; Viviani, 2002).

There are at least five general types of luciferin, which are each chemically different and catalysed by chemically and structurally different luciferases that employ a wide range of different cofactors. First, is firefly luciferin, the substrate of firefly luciferase, which requires ATP for catalysis (EC 1.13.12.7). Second, is bacterial luciferin, also found in some squid and fish, that consists of a long chain aldehyde and a reduced riboflavin phosphate. Bacterial luciferase is FMN-dependent. Third, is dinoflagellate luciferin, a tetrapyrrolic chlorophyll derivative found in dinoflagellates (marine plankton), the organisms responsible for night-time ocean phosphorescence. Dinoflagellate luciferase catalyses the oxidation of dinoflagellate luciferin and consists of three identical and catalytically active domains. Fourth, is the imidazolopyrazine vargulin, which is found in certain ostracods and deep-sea fish, for example, *Porichthys*. Last, is coelenterazine (an imidazolopyrazine), the light-emitter of the protein aequorin, found in radiolarians, ctenophores, cnidarians, squid, copepods, chaetognaths, fish and shrimp. Acceptor Molecules

As used herein, the term “fluorescent acceptor domain” (also referred herein to as “acceptor molecule”) refers to any compound which can accept energy emitted as a result of the activity of a chemiluminescent donor, and re-emit it as light energy. There are a number of different acceptor molecules that can be employed in this invention. The acceptor molecules may be a protein or non-proteinaceous. Examples of acceptor molecules that are protein include, but are not limited to, green fluorescent protein (GFP), blue fluorescent variant of GFP (BFP), cyan fluorescent variant of GFP (CFP), yellow fluorescent variant of GFP (YFP), enhanced GFP (EGFP), enhanced CFP (ECFP), enhanced YFP (EYFP), GFP65T, Emerald, Venus, mOrange, Topaz, GFPuv, destabilised EGFP (dEGFP), destabilised ECFP (dECFP), destabilised EYFP (dEYFP), HcRed, t-HcRed, DsRed, DsRed2, t-dimer2, t-dimer2(12), mRFP1, pociilorporin, *Renilla* GFP, Monster GFP, paGFP, Kaede protein or a Phycobiliprotein, or a biologically active variant or fragment of any one thereof. Examples of acceptor molecules that are not proteins include, but are not limited to, Alexa Fluor dye, Bodipy dye, Cy dye, fluorescein, dansyl, umbelliferone, fluorescent microsphere, luminescent microsphere, fluorescent nanocrystal, Marina Blue, Cascade Blue, Cascade Yellow, Pacific Blue, Oregon Green, Tetramethylrhodamine, Rhodamine, Texas Red, rare earth element chelates, or any combination or derivatives thereof.

One very well known example is the group of fluorophores that includes the green fluorescent protein from the jellyfish *Aequorea victoria* and numerous other variants (GFPs) arising from the application of molecular biology, for example mutagenesis and chimeric protein technologies

(Tsien, 1998). GFPs are classified based on the distinctive component of their chromophores, each class having distinct excitation and emission wavelengths: class 1, wild-type mixture of neutral phenol and anionic phenolate: class 2, phenolate anion: class 3, neutral phenol: class 4, phenolate anion with stacked s -electron system: class 5, indole: class 6, imidazole: and class 7, phenyl.

A naturally occurring acceptor molecule which has been mutated (variants) can also be useful for the present invention. One example of an engineered system which is suitable for BRET is a *Renilla* luciferase and enhanced yellow mutant of GFP (EYFP) pairing which do not directly interact to a significant degree with one another alone in the absence of a mediating protein(s) (in this case, the G protein coupled receptor) (Xu et al., 1999).

In another embodiment, the acceptor molecule is a fluorescent nanocrystal. Nanocrystals, or "quantum dots", have several advantages over organic molecules as fluorescent labels, including resistance to photodegradation, improved brightness, non-toxicity, and size dependent, narrow emission spectra that enables the monitoring of several processes simultaneously. Additionally, the absorption spectrum of nanocrystals is continuous above the first peak, enabling all sizes, and hence all colors, to be excited with a single excitation wavelength.

Fluorescent nanocrystals may be attached, or "bioconjugated", to proteins in a variety of ways. For example, the surface cap of a "quantum dot" may be negatively charged with carboxylate groups from either dihydrolipoic acid (DHLA) or an amphiphilic polymer. Proteins can be conjugated to the DHLA-nanocrystals electrostatically, either directly or via a bridge consisting of a positively charged leucine zipper peptide fused to recombinant protein. The latter binds to a primary antibody with specificity for the intended target. Alternatively, antibodies, streptavidin, or other proteins are coupled covalently to the polyacrylate cap of the nanocrystal with conventional carbodiimide chemistry.

There are colloidal methods to produce nanocrystals, including cadmium selenide, cadmium sulfide, indium arsenide, and indium phosphide. These quantum dots can contain as few as 100 to 100,000 atoms within the quantum dot volume, with a diameter of 10 to 50 atoms. Some quantum dots are small regions of one material buried in another with a larger band gap. These can be so-called core-shell structures, for example, with CdSe in the core and ZnS in the shell or from special forms of silica called ormosil. The larger the dot, the redder (lower energy) its fluorescence spectrum. Conversely, smaller dots emit bluer (higher energy) light. The coloration is directly related to the energy levels of the quantum dot. Quantitatively speaking, the bandgap energy that determines the energy (and hence color) of the fluoresced light is inversely proportional to the square of the size of the quantum dot. Larger quantum dots have more energy levels which are more closely spaced. This allows the quantum dot to absorb photons containing less energy, i.e. those closer to the red end of the spectrum.

In an alternate embodiment, the acceptor molecule is a fluorescent microsphere. These are typically made from polymers, and contain fluorescent molecules (for example fluorescein GFP or YFP) incorporated into the polymer matrix, which can be conjugated to a variety of reagents. Fluorescent microspheres may be labelled internally or on the surface. Internal labelling produces very bright and stable particles with typically narrow fluorescent emission spectra. With internal labelling, surface groups remain available for conjugating ligands (for example, proteins) to the

surface of the bead. Internally-labelled beads are used extensively in imaging applications, as they display a greater resistance to photobleaching.

Carboxylate-modified fluorescent microspheres are suitable for covalent coupling of proteins using water-soluble carbodiimide reagents such as 1-ethyl-3-(3-dimethylamino-propyl) carbodiimide hydrochloride (EDAC). Sulfate fluorescent microspheres are relatively hydrophobic and will passively and nearly irreversibly adsorb almost any protein. Aldehyde-sulfate fluorescent microspheres are sulfate microspheres that have been modified to add surface aldehyde groups, and react with proteins.

In another embodiment, the acceptor molecule is a luminescent microsphere. These are typically made from polymers, which contain luminescent molecules (for example complexes of europium or platinum) incorporated into the polymer matrix, which can be conjugated to a variety of reagents.

Examples of non-fluorescent acceptor domains useful for the invention include quenchers such as DABCYL [4-((4-Dimethylamino) phenyl)azo]benzoic acid], DABSYL (Dimethylaminoazosulfonic acid), metal nanoparticles such as gold and silver, lack hole quenchers (BHQ) and QXL quenchers.

Chemiluminescent Donor Domain and Acceptor Domain Pairs

As used herein, the term "the separation and relative orientation of the chemiluminescent donor domain and the acceptor domain, in the presence and/or the absence of analyte, is within $\pm 50\%$ of the Forster distance" refers to the steady state RET measurements which can be carried out within a range of $\pm 50\%$ of R_0 . This phrase encompasses an efficiency of luminescence energy transfer from the chemiluminescent donor domain to the acceptor domain in the range of 10-90%. Outside of these distance limits it is still possible to estimate distance but the uncertainty is increased.

A criterion which should be considered in determining suitable pairings is the relative emission/fluorescence spectrum of the acceptor molecule compared to that of the donor. The emission spectrum of the donor should overlap with the absorbance spectrum of the acceptor molecule such that the light energy from the donor luminescence emission is at a wavelength that is able to excite the acceptor molecule and thereby promote acceptor molecule fluorescence when the two molecules are in a proper proximity and orientation with respect to one another. For example, it has been demonstrated that an *Renilla* luciferase/EGFP pairing is not as good as an *Renilla* luciferase/EYFP pairing based on observable emission spectral peaks (Xu, 1999; Wang, et al. (1997) in *Bioluminescence and Chemiluminescence: Molecular Reporting with Photons*, eds. Hastings et al. (Wiley, New York), pp. 419-422). To study potential pairing, protein fusions (for example) are prepared containing the selected bioluminescent protein and acceptor molecule and are tested, in the presence of an appropriate substrate.

It should also be confirmed that the donor and acceptor molecule do not spuriously associate with each other. This can be accomplished by, for example, separate co-expression of a bioluminescent protein and acceptor molecule in the same cells and then monitoring the luminescence spectrum in order to determine if BRET occurs. This may be achieved, for example, using the method of Xu et al. (1999). The selected bioluminescent protein and acceptor molecule form a suitable BRET pair if little or no BRET is observed.

The donor emission can be manipulated by modifications to the substrate. In the case of luciferases the substrate is coelenterazine. The rationale behind altering the donor

emission is to improve the resolution between donor emission and acceptor emissions. The original BRET system uses the *Renilla* luciferase as donor, EYFP (or Topaz) as the acceptor and coelenterazine h derivative as the substrate. These components when combined in a BRET assay, generate light in the 475-480 nm range for the bioluminescent protein and the 525-530 nm range for the acceptor molecule, giving a spectral resolution of 45-55 nm.

Unfortunately, *Renilla* luciferase generates a broad emission peak overlapping substantially the GFP emission, which in turn contributes to decrease the signal to noise of the system. One BRET system of the present invention, using coel400a as the *Renilla* luciferase substrate, provides broad spectral resolution between donor and acceptor emission wavelengths (~105 nm). *Renilla* luciferase with coel400a generates light between 390-400 nm and a GFP was prepared which absorbs light in this range and re-emits light at 505-508 nm. Because of this increase in spectral resolution between *Renilla* luciferase and GFP emissions, this BRET system provides an excellent biological tool to monitor small changes in conformation of a polypeptide of the invention. This is a significant improvement over the system described previously using the coelenterazine h derivative and EYFP, which has a wavelength difference between donor and acceptor of approximately 51 nm.

Various coelenterazine derivatives are known in the art, including coel400a, that generate light at various wavelengths (distinct from that generated by the wild type coelenterazine) as a result of *Renilla* luciferase activity. A worker skilled in the art would appreciate that because the light emission peak of the donor has changed, it is necessary to select an acceptor molecule which will absorb light at this wavelength and thereby permit efficient energy transfer. This can be done, for example by altering a GFP class 4 such that it becomes a class 3 or 1 GFP. Spectral overlapping between light emission of the donor and the light absorption peak of the acceptor is one condition among others for an efficient energy transfer. Class 3 and 1 GFPs are known to absorb light at 400 nm and reemit between 505-511 nm. This results in a wavelength difference between donor and acceptor emissions of approximately 111 nm.

Examples of further bioluminescent protein and acceptor molecule pairs are provided in Table 2.

Sensor Molecule

As used herein, the term "sensor molecule" refers to any molecule, complex of two or more covalently or non-covalently associated molecules, or two or more molecules which can be at least at some stage closely associated to enable RET between the donor and acceptor. Furthermore, if present, the two or more separate molecules which form the domain can be associated via an intermediate molecule. In one example, the sensor molecule can be a protein complex, where each subunit of the complex is non-covalently associated and the acceptor and domain may be on the same or different subunits of the protein complex. In another example, the sensor molecule is two separate nucleic acid strands, one labelled with the acceptor and the other labelled with the donor, such that hybridization to a target (analyte) results in the donor and acceptor being sufficiently close to result in RET. In this example, it can be considered that the sensor molecule is formed when it binds the analyte.

TABLE 2

Exemplary BRET bioluminescent proteins and acceptor molecule pairs.					
	BDP	Substrate	Substrate wavelength (peak)	Fluorescence acceptor molecule	Wavelength of acceptor (Ex/Em)
5	Rluc2	Native	470 nm	Venus	515/528 nm
10	Rluc8	coelenterazine			
	Rluc2	Native	470 nm	mOrange	548/562 nm
15	Rluc8	coelenterazine			
	Rluc2	Native	470 nm	EYFP/Topaz	514/527 nm
20	Rluc8	Coelenterazine			
	Rluc2	Native	470 nm	mCitrine	516/529 nm
25	Rluc8	Coelenterazine			
	Rluc2	Native	470 nm	YPet	517/530 nm
30	Rluc8	Coelenterazine			
	Rluc2	Native	470 nm	Fluorescein	495/519 nm
35	Rluc8	Coelenterazine			
	Rluc2	Native	470 nm	Acridine yellow	470/550 nm
40	Rluc8	Coelenterazine			
	Rluc2	Native	470 nm	Nile red	485/525 nm
45	Rluc8	Coelenterazine			
	Rluc2	Native	470 nm	R-Phycoerythrin	480/578
50	Rluc8	Coelenterazine			
	Rluc2	Native	470 nm	Red 613	480/613
55	Rluc8	Coelenterazine			
	Rluc2	Native	470 nm	TruRed	490/695
60	Rluc8	Coelenterazine			
	Rluc2	Native	470 nm	mOrange	548/562 nm
65	Rluc8	Coelenterazine			
	Rluc2	Native	470 nm	Venus	515/528 nm
70	Rluc8	Coelenterazine			
	Rluc2	Native	470 nm	mOrange	548/528 nm
75	Rluc8	Coelenterazine			
	Rluc2	Native	470 nm	EYFP/Topaz	514/527 nm
80	Rluc8	Coelenterazine			
	Rluc2	Native	470 nm	mCitrine	516/529 nm
85	Rluc8	Coelenterazine			
	Rluc2	Native	470 nm	YPet	517/530 nm
90	Rluc8	Coelenterazine			
	Rluc2	Native	470 nm	Fluorescein	490/525 nm
95	Rluc8	Coelenterazine			
	Rluc2	Native	470 nm	Acridine yellow	470/550 nm
100	Rluc8	Coelenterazine			
	Rluc2	Native	470 nm	Nile red	485/525 nm
105	Rluc8	Coelenterazine			
	Rluc2	Native	470 nm	R-Phycoerythrin	480/578
110	Rluc8	Coelenterazine			
	Rluc2	Native	470 nm	Red 613	480/613
115	Rluc8	Coelenterazine			
	Rluc2	Native	470 nm	TruRed	490/695
120	Rluc8	Coelenterazine			
	Rluc2	Native	470 nm	mOrange	548/562 nm
125	Rluc8	Coelenterazine			
	Rluc2	Native	470 nm	GFP2	396/508 nm
130	Rluc8	Coelenterazine			
	Rluc2	Native	470 nm	GFP10	400/510 nm
135	Rluc8	Coelenterazine			
	Rluc2	Native	470 nm	Wild type GFP	396 (475)/508 nm
140	Rluc8	Coelenterazine			
	Rluc2	Native	470 nm	TagBFP	402/457 nm
145	Rluc8	Coelenterazine			
	Rluc2	Native	470 nm	Cerulean/mCFP	433/475 nm
150	Rluc8	Coelenterazine			
	Rluc2	Native	470 nm	ECFP/CyPet	434/477 nm

TABLE 2-continued

Exemplary BRET bioluminescent proteins and acceptor molecule pairs.				
BDP	Substrate	Substrate wavelength (peak)	Fluorescence acceptor molecule	Wavelength of acceptor (Ex/Em)
Rluc	Coelenterazine	400 nm	Y66W	436/485 nm
Rluc2	400a			
Rluc8				
Rluc	Coelenterazine	400 nm	dKeima-Red	440/616 nm
Rluc2	400a			
Rluc8				
Rluc	Coelenterazine	400 nm	mKeima-Red	440/620 nm
Rluc2	400a			
Rluc8				
Rluc	Coelenterazine	400 nm	Quin-2	365/490 nm
Rluc2	400a			
Rluc8				
Rluc	Coelenterazine	400 nm	Pacific blue	403/551 nm
Rluc2	400a			
Rluc8				
Rluc	Coelenterazine	400 nm	Dansychloride	380/475 nm
Rluc2	400			
Rluc8				
Firefly luciferase	Luciferin	560 nm	Cyanine Cy3	575/605 nm
Firefly luciferase	Luciferin	560 nm	Texas red	590/615
Firefly luciferase	Luciferin	560 nm	TurboRed	553/574 nm
Firefly luciferase	Luciferin	560 nm	tdTomato	554/581 nm
Firefly luciferase	Luciferin	560 nm	TagRFP	555/584 nm
Firefly luciferase	Luciferin	560 nm	DsRed	557/592 nm
Firefly luciferase	Luciferin	560 nm	mRFP1	584/607 nm
Firefly luciferase	Luciferin	560 nm	mCherry	587/610 nm

The domain which binds the analyte (or candidate compound) may be any molecule as long as it can be appropriately associated with the donor and acceptor.

In an embodiment, the domain that binds the analyte is a protein or a nucleic acid. In a preferred embodiment, the domain is a protein. In an embodiment, the protein is a naturally occurring protein which binds one or more analytes (ligand), or a variant of the protein which retains analyte (ligand) binding activity. Examples include, but are not necessarily limited to, a receptor, odorant binding protein, pheromone-binding protein, enzyme (for example a protease, an oxidase, a phytase, a chitinase, an invertase, a lipase, a cellulase, a xylanase, a kinase, a phosphatase, an elongase, a transferase, a desaturase), ligand carrier or bacterial periplasmic binding protein. In an embodiment, the receptor is a G protein coupled receptor such as an odorant receptor or a taste receptor (for example a sweet, bitter or umami taste receptor, such as those described in Doty, 2012). In a further embodiment, the odorant receptor or taste receptor is from a nematode or vertebrate or is a mutant thereof.

In one embodiment, the sensor molecule is provided as a cell-free composition. As used herein, the term “cell free composition” refers to an isolated composition which contains few, if any, intact cells and which comprises the sensor molecule. Examples of cell free compositions include cell (such as yeast cell) extracts and compositions containing an isolated and/or recombinant sensor molecules (such as proteins). Methods for preparing cell-free compositions from cells are well-known in the art and are described in WO

2010/085844. In certain embodiments, the sensor molecule is embedded in a lipid bilayer such as of a liposome preparation, in cell or cell-free extract.

G Protein Coupled Receptors

5 As used herein, unless specified otherwise, the term “G protein coupled receptor” refers to a seven transmembrane receptor which signals through G proteins. The receptor may be a single subunit, or two or more receptor subunits. When two or more receptor subunits are present they may be the same, different, or a combination thereof (for example, two of one subunit and a single of another subunit). Furthermore, unless specified or implied otherwise the terms “G protein coupled receptor” and “subunit of a G protein coupled receptor”, or variations thereof, are used interchangeably.

15 As used herein, the term “odorant receptor”, “olfactory receptor”, “OR” or variations thereof refers to a polypeptide which, when present in a cell of an organism, is involved in chemosensory perception. In an embodiment, the cell is a neuron. Furthermore, the term “odorant receptor” or “olfactory receptor” refers to a polypeptide which binds an odorant ligand, or forms part of a protein complex that binds to an odorant ligand, resulting in a physiologic response.

20 As used herein, the term “forms part of” refers to the bioluminescent protein or acceptor molecule being located within the specified region of the G protein coupled receptor, or subunit thereof. This term also includes the possibility that the bioluminescent protein and/or acceptor molecule is attached to or binds the G protein coupled receptor but does not form a continuous chain of amino acids. In one embodiment, the bioluminescent protein or acceptor molecule completely replaces the specified region of the G protein coupled receptor. In another embodiment, some, but not all, of the specified region of the G protein coupled receptor is replaced. In yet another embodiment, none of the specified region of the G protein coupled receptor is replaced. As the skilled addressee will appreciate, the bioluminescent protein or acceptor molecule will not be inserted such that it makes the G protein coupled receptor portion of a polypeptide incapable of binding the analyte to result in a spatial change to the location and/or dipole orientation of the bioluminescent protein relative to the acceptor molecule.

40 G protein-coupled receptors (GPCRs) are also known as seven transmembrane receptors, 7TM receptors, serpentine receptors, heptahelical receptors, and G protein linked receptors (GPLR). GPCRs are a large protein family of transmembrane receptors that sense molecules outside the cell and activate inside signal transduction pathways and, ultimately, cellular responses. The ligands that bind and activate these receptors include light-sensitive compounds, odors, pheromones, hormones, and neurotransmitters, and vary in size from small molecules to peptides to large proteins. GPCRs are involved in many diseases, but are also the target of around half of all modern medicinal drugs. GPCRs can be grouped into at least 5 classes based on sequence homology and functional similarity:

- Class A rhodopsin-like,
- Class B secretin-like,
- Class C metabotropic/pheromone,
- Class D fungal pheromone, and
- Class E cAMP receptors.

60 Class A Rhodopsin like receptors include: Amine receptors: Acetylcholine, Alpha Adrenoceptors, Beta Adrenoceptors, Dopamine, Histamine, Serotonin, Octopamine, and Trace amine; Peptide receptors: Angiotensin, Bombesin, Bradykinin, C5a anaphylatoxin, Fmet-leu-phe, APJ like, Interleukin-8, Chemokine receptors (C—C Chemokine, C—X—C Chemokine, BONZO receptors (CXC6R),

C—X3—C Chemokine, and XC Chemokine), CCK receptors, Endothelin receptors, Melanocortin receptors, Neuropeptide Y receptors, Neurotensin receptors, Opioid receptors, Somatostatin receptors, Tachykinin receptors, (Substance P (NK1), Substance K (NK2), Neuromedin K (NK3), Tachykinin like 1, and Tachykinin like 2), Vasopressin-like receptors (Vasopressin, Oxytocin, and Conopressin), Galanin like receptors (Galanin, Allostatin, and GPCR 54), Proteinase-activated like receptors (e.g., Thrombin), Orexin & neuropeptide FF, Urotensin II receptors, Adrenomedullin (G10D) receptors, GPR37/endothelin B-like receptors, Chemokine receptor-like receptors, and Neuromedin U receptors; Hormone protein receptors: Follicle stimulating hormone, Lutropin-choriagonadotropic hormone, Thyrotropin, and Gonadotropin; (Rhod)opsin receptors; Olfactory receptors; Prostanoid receptors: Prostaglandin, Prostacyclin, and Thromboxane; Nucleotide-like receptors: Adenosine and Purinoceptors; Cannabis receptors; Platelet activating factor receptors; Gonadotropin-releasing hormone receptors; Thyrotropin-releasing hormone & Secretagogue receptors: Thyrotropin-releasing hormone, Growth hormone secretagogue, and Growth hormone secretagogue like; Melatonin receptors; Viral receptors; Lysosphingolipid & LPA (EDG) receptors; Leukotriene B4 receptor: Leukotriene B4 receptor BLT1 and Leukotriene B4 receptor BLT2; and Class A Orphan/other receptors: Platelet ADP & KI01 receptors, SREB, Mas protooncogene, RDC1, ORPH, LGR like (hormone receptors), GPR, GPR45 like, Cysteinyl leukotriene, Mas-related receptors (MRGs), and GP40 like receptors.

Class B (the secretin-receptor family) of the GPCRs includes receptors for polypeptide hormones (Calcitonin, Corticotropin releasing factor, Gastric inhibitory peptide, Glucagon, Glucagon-like peptide-1, -2, Growth hormone-releasing hormone, Parathyroid hormone, PACAP, Secretin, Vasoactive intestinal polypeptide, Diuretic hormone, EMR1, Latrophilin), molecules thought to mediate intercellular interactions at the plasma membrane (Brain-specific angiogenesis inhibitor (BAI)) and a group of *Drosophila* proteins (Methuselah-like proteins) that regulate stress responses and longevity.

Class C Metabotropic glutamate/pheromone receptors include Metabotropic glutamate, Metabotropic glutamate group I, Metabotropic glutamate group II, Metabotropic glutamate group III, Metabotropic glutamate other, Extracellular calcium-sensing, Putative pheromone Receptors, GABA-B, GABA-B subtype 1, GABA-B subtype 2, and Orphan GPRC5 receptors.

Sensor molecules useful for the invention may comprise G protein coupled receptors which, when expressed in a cell the N-terminus of the receptor is outside the cell and the C-terminus is inside the cell. The person skilled in the art is aware of suitable techniques for detecting the orientation of a transmembrane protein. Such techniques comprise but are not limited to crystallography, NMR-studies, modeling studies as well as microscopy techniques, like immunolabeling combined with detergent permeabilisation controls for light or electron microscopy preparation, fragment complementation tagging of two polypeptides and the like.

In a preferred embodiment, the G protein coupled receptor is a Class A GPCR. In a further preferred embodiment, the class A (rhodopsin-like) GPCR is an odorant receptor, dopamine receptor, muscarinic receptor or an adrenergic receptor, more preferably an odorant receptor. The odorant receptor can be from any source as long as when expressed in a cell the N-terminus of the receptor is outside the cell and the C-terminus is inside the cell. Examples include, but are

not limited to, a chordate receptor, a nematode receptor, or a biologically active variant or fragment of any one thereof. Examples of chordate receptors include, but are not limited to mammalian receptors, avian receptors and fish receptors. In a preferred embodiment, the odorant receptor is a nematode receptor or biologically active variant or fragment thereof. In an embodiment, the nematode receptor is a *Caenorhabditis elegans* receptor, or biologically active variant or fragment thereof. Examples of odorant receptors that can be used to produce polypeptides of the invention and/or used in the methods of the invention are described in Buck and Axel (1991), Robertson (1998 and 2001), Aloni et al. (2006), Feldmesser (2006), Olender et al. (2004a and b), Glusman et al. (2000a, 2000b and 2001), Fuchs et al. (2001), Pilpel and Lancet (1999), Sharon et al. (1998), Zozulya et al. (2001), Niimura and Nei (2003), Lander et al. (2001), Zhang and Firestein (2002), Young et al. (2002), and Fredriksson and Schioth (2005). Furthermore, a comprehensive list of odorant receptors are available from the SenseLab website (<http://senselab.med.yale.edu>).

In other embodiments, the GPCR is a Class B or Class C receptor, with Class C being more preferred of these two embodiments.

In a particularly preferred embodiment, the G protein coupled receptor comprises seven transmembrane domains.

The bioluminescent protein can form part of the first, third, fifth non-transmembrane loops (domains) or the C-terminus of the G protein coupled receptor (or polypeptide of the invention). The acceptor molecule also can form part of the first, third, fifth non-transmembrane loops (domains) or the C-terminus of the G protein coupled receptor (or polypeptide of the invention). Each of these regions is intracellular when the G protein coupled receptor is expressed and present in a cell.

The acceptor molecule cannot be in the same region as the bioluminescent protein when part of the same molecule (namely, the same single polypeptide chain), however, the acceptor molecule can be in the equivalent region as the bioluminescent protein when the G protein coupled receptor is present as a dimer or higher multimer. For example, the bioluminescent protein can form part of the C-terminus of one subunit of the receptor, and the acceptor molecule can form part of the C-terminus of another subunit of the receptor. In this example, the subunit to which the label is associated can be the same or different, for instance the two subunits can be identical apart from one labelled with the bioluminescent protein and the other labelled with the acceptor molecule.

In one embodiment, the bioluminescent protein forms part of the third non-transmembrane loop of the GPCR subunit, and the acceptor molecule forms part of the fifth non-transmembrane loop. In an alternate embodiment, the acceptor molecule forms part of the third non-transmembrane loop of the GPCR subunit, and the bioluminescent protein forms part of the fifth non-transmembrane loop.

In another embodiment, the bioluminescent protein forms part of the first non-transmembrane loop of the GPCR subunit, and the acceptor molecule forms part of the third non-transmembrane loop. In another embodiment, the acceptor molecule forms part of the first non-transmembrane loop of the GPCR subunit, and the bioluminescent protein forms part of the third non-transmembrane loop.

In a preferred embodiment, the bioluminescent protein forms part of the fifth non-transmembrane loop of the GPCR subunit, and the acceptor molecule forms part of the C-terminus. In an alternate embodiment, the acceptor molecule

forms part of the fifth non-transmembrane loop of the GPCR subunit, and the bioluminescent protein forms part of the C-terminus.

In another embodiment, the G protein coupled receptor comprises at least two subunits, where the bioluminescent protein forms part of the third non-transmembrane loop of a first subunit, and the acceptor molecule forms part of the fifth non-transmembrane loop of a second subunit. In an alternate embodiment, the acceptor molecule forms part of the third non-transmembrane loop of a first subunit, and the bioluminescent protein forms part of the fifth non-transmembrane loop of a second subunit.

In another embodiment, the G protein coupled receptor comprises at least two subunits, where the bioluminescent protein forms part of the first non-transmembrane loop of a first subunit, and the acceptor molecule forms part of the third non-transmembrane loop of a second subunit. In another embodiment, the acceptor molecule forms part of the first non-transmembrane loop of a first subunit, and the bioluminescent protein forms part of the third non-transmembrane loop of a second subunit.

In another embodiment, the G protein coupled receptor comprises at least two subunits, where the bioluminescent protein forms part of the fifth non-transmembrane loop of a first subunit, and the acceptor molecule forms part of the C-terminus of a second subunit. In an alternate embodiment, the acceptor molecule forms part of the fifth non-transmembrane loop of a first subunit, and the bioluminescent protein forms part of the C-terminus of a second subunit.

In another embodiment, the G protein coupled receptor comprises at least two subunits and the donor and acceptor molecule are in the same site of the first and second subunits respectively.

In an embodiment, the bioluminescent protein or acceptor molecule is located after the second amino acid of the fifth transmembrane domain and before the second amino acid before the beginning of sixth transmembrane domain. In another embodiment, the bioluminescent protein or acceptor molecule is located after about amino acid 8 after the fifth transmembrane domain or after about amino acid 22 after the fifth transmembrane domain. In a further embodiment, the bioluminescent protein or acceptor molecule is inserted about 10 or 12 amino acids before the sixth transmembrane domain. Most preferably, the bioluminescent protein or acceptor molecule is located in the middle of the third non-transmembrane loop (domain).

With regard to the C-terminus, it is preferred that about 5 to 25 amino acids of the natural C-terminus remain at the end of seventh transmembrane domain. Preferably, the bioluminescent protein or acceptor molecule is inserted after about the 16 or 20 amino acids after the seventh transmembrane.

Turning to the location of the bioluminescent protein or acceptor molecule in the first non-transmembrane loop (domain), it is preferred that said label is inserted about two amino acids after the end of first transmembrane domain and about two amino acids before the beginning of the second transmembrane domain. Most preferably, the bioluminescent protein or acceptor molecule is located in the middle of the first non-transmembrane loop (domain).

In a further embodiment, the bioluminescent protein can form part of the N-terminus, second, fourth, or sixth non-transmembrane loops (domains) of the G protein coupled receptor (or polypeptide of the invention). The acceptor molecule also can form part of the N-terminus, second, fourth, or sixth non-transmembrane loops (domains) of the G protein coupled receptor (or polypeptide of the invention),

however, it cannot be in the same region as the bioluminescent protein when part of the same molecule. Each of these regions is extracellular when the G protein coupled receptor is expressed and present in a cell.

The GPCR may be a non-naturally occurring chimera of two or more different GPCRs. In particular, this enables a transduction cassette to be produced where portions of one receptor are always present in the chimera into which other portions of a wide variety of GPCRs are inserted depending on the compound to be detected.

In one embodiment, the subunit comprises the N-terminus and at least a majority of the first transmembrane domain of a first G protein coupled receptor subunit, at least a majority of the first non-transmembrane loop through to at least a majority of the fifth transmembrane domain of a second G protein coupled receptor subunit, and at least a majority of the fifth non-transmembrane loop through to the C-terminal end of the first G protein coupled receptor subunit.

In another embodiment, the subunit comprises the N-terminus through to at least a majority of the fifth transmembrane domain of a first G protein coupled receptor subunit, and at least a majority of the fifth non-transmembrane loop through to the C-terminal end of a second G protein coupled receptor subunit.

As used herein, the term "at least a majority" of a specified portion (domain) of a G protein coupled receptor, refers to at least 51%, more preferably at least 75% and even more preferably at least 90% of the specified region.

The skilled person can readily determine the N-terminal end, transmembrane domains, non-transmembrane loops (domains) and C-terminus of a G protein coupled. For example, a variety of bioinformatics approaches may be used to determine the location and topology of transmembrane domains in a protein, based on its amino acid sequence and similarity with known transmembrane domain of G protein coupled receptors. Alignments and amino acid sequence comparisons are routinely performed in the art, for example, by using the BLAST program or the CLUSTAL W program. Based on alignments with known transmembrane domain-containing proteins, it is possible for one skilled in the art to predict the location of transmembrane domains. Furthermore, the 3 dimensional structures of some membrane-spanning proteins are known, for example, the seven transmembrane C-protein coupled rhodopsin photoreceptor structure has been solved by x-ray crystallography. Based on analyses and comparisons with such 3D structures, it may be possible to predict the location and topology of transmembrane domains in other membrane proteins. There are also many programs available for predicting the location and topology of transmembrane domains in proteins. For example, one may use one or a combination of the TMPred (Hofmann and Stoffel, 1993), which predicts membrane spanning proteins segments; TopPred (von Heijne et al., 1992) which predicts the topology of membrane proteins; PREDATOR (Frishman and Argos, 1997), which predicts secondary structure from single and multiple sequences; TMAP (Persson and Argos, 1994), which predicts transmembrane regions of proteins from multiply aligned sequences; and ALOM2 (Klien et al., 1984), which predicts transmembrane regions from single sequences.

In accordance with standard nomenclature, the numbering of the transmembrane domains and non-transmembrane loops (domains) is relative to the N-terminus of the polypeptide.

Variants of *C. elegans* str-112 (SEQ ID NO:41) and/or str-113 (SEQ ID NO:42) which bind 2-pentanone include, but are not limited to, molecules which are at least 90%

identical to str-112 (SEQ ID NO:41) and/or str-113 (SEQ ID NO:42), biologically active fragments which are at least 90% identical to str-112 (SEQ ID NO:41) and/or str-113 (SEQ ID NO:42), and fusion proteins thereof such as str-114/113 (SEQ ID NO:43). As the skilled person would appreciate, when determining the % identity, sections of the proteins comprising labels, such as the acceptor and donor in SEQ ID NOs 13, 14, 18, 27, 28 and 30, are preferably ignored.

Nucleic Acids

In one embodiment, the domain (or molecule of interest) is a nucleic acid. As the skilled addressee would be aware, there are many detection systems which rely on nucleic acid binding which would be adapted for use in the methods of the invention.

Molecular beacons (MBs) have been extensively researched in the construction of probes useful for detecting specific nucleic acids in homogenous solutions. MBs consist of a single stranded nucleic acid sequence that possesses a stem and loop structure and is labelled with BRET components at the 5' and 3' ends. The close proximity of the 5' and 3' ends came energy transfer to occur. The target DNA sequence hybridises with the probe nucleic acid sequence forcing the BRET components to move apart and causing the BRET ratio to decrease. Although a combination of fluorophore-acceptor pairs have been investigated the method is flawed by requiring an excitation source which could cause autofluorescence of the nucleic acids. Replacing the fluorophore with a bioluminescent protein overcomes this problem.

In another example, an acceptor and donor can be conjugated to two different antisense oligonucleotides, each complementary to different portions of the same target nucleic acid sequence. The different portions of the target sequences are located in closely within the target nucleic acid sequence. BRET components are brought into close proximity upon hybridisation to the target nucleic acid resulting in an increase in the BRET ratio.

In a further example, in the absence of target nucleic acid, acceptor and donor labelled complementary oligonucleotide probes hybridise causing energy transfer. In the presence of target nucleic acid, the target and donor labelled compete to hybridise with the acceptor protein thus lowering the BRET ratio. The decrease in BRET ratio can be correlated with the amount of total nucleic acid present in the sample.

Uses

The present invention can be used to detect the presence or absence or concentration of a wide variety of analytes including small volatile and non-volatile organic molecules, macromolecules, and biological particles and cells. The invention is compatible with almost any biological recognition element that can be functionally coupled to a chemiluminescence transduction system, including G-protein coupled and other receptors, binding proteins, enzymes, peptides and nucleic acid molecules. Examples of uses of microfluidic methods and systems of the invention are described in Li and Lin (2009), Mark et al. (2010), Theberge et al. (2010), Mohammed and Desmulliez (2011), Esch et al. (2011), Yeo et al. (2011), Noh et al. (2011) and Godin et al. (2008).

In a particularly preferred embodiment, the analyte is an odorant. Typically, the odorant will be a volatile organic or inorganic compound or inorganic gas that may be detected by chemosensory odorant receptors of at least one organism. These may include amino- and/or sulfhydryl-containing compounds, carboxylic acids, alcohols, aldehydes, alkanes, alkenes, aromatic compounds, esters, terpenes or terpene-

derivatives, ethers, CO₂ etc. as well as compounds bearing combinations of these features.

Odorants may be indicative of some biological or chemical state of value or of interest to humans. Such indications may include:

The sensory appeal, quality or safety of food and beverages, pharmaceuticals or related materials.

The health, nutritional or exercise status of humans or animals.

The presence or absence of hazardous substances, including pathogens.

The progress or status of industrial processes.

An environmental contamination or state.

The sensory appeal, quality or safety of perfumes, fragrances or other cosmetics.

In a particularly preferred embodiment, the analyte does not bind the donor or acceptor domain.

In another embodiment, the method may be used for screening for a compound which binds the sensor molecule.

As the skilled person would appreciate this allows the methods to be used in, for example, drug discovery and/or development. More specifically, the domain to which the analyte binds is a target for potential therapeutics. Thus, in this embodiment it is preferred that the domain bound by the analyte is a clinically important molecule such as, but are not limited to, an adrenergic receptor, a serotonin receptor, a dopamine receptor, metabotropic/glutamate receptor, a GABA receptor, a vomeronasal receptor, a taste receptor, or a secretin-like receptor.

As another example, a method of the invention could be used to detect spoilage of milk such as ultra-high temperature (UHT) processed milk. In this example, the sensor molecule can be a molecule cleaved by a bacterial protease that causes, at least in part, milk spoilage. For instance, the sensor molecule may comprise a region of a milk protein, such as κ -casein, which is cleaved by the protease(s) labelled with the chemiluminescent donor domain and an acceptor domain.

As the skilled person would be aware, the present invention can also be multiplexed. In this system, two or more different sensor molecules are provided which bind different compounds. Each different sensor molecule includes a different donor and/or acceptor molecule such that they emit at different wavelengths to enable the detection and quantification of different target compounds.

EXAMPLES

Example 1—Performance of a Hybrid BRET System in a Microfluidic System for Thrombin Cleavage Assay

Materials and Methods BRET System

A combination of BRET¹ and BRET² techniques was used and referred to herein as hybrid BRET. Specifically, RLuc with native coelenterazine substrate was used as the bioluminescent donor and GFP² as the acceptor molecule. The donor and acceptor were linked by a peptide sequence containing the thrombin cleavage site (LQGS_LVPR↓GSLQ (RG)) (GFP²-RG-RLuc) and expressed in *E. coli*. Thrombin cleavage of the cleavage site resulted in a change in the hybrid BRET signal. The mechanism of BRET system is shown in FIG. 1A.

Materials

GFP²-RG-RLuc biosensor was expressed and purified as reported previously (Dacres et al. 2009a). The purified

fusion protein was in thrombin cleavage buffer (10 mM Tris (pH 8.0), 100 mM NaCl, 1 mM EDTA). The final concentration of the native coelenterazine substrate (Biosynth) used for microfluidic based assays was 58.6 μ M and 5 μ M for plate-reader based assays. 1 unit (U)/ μ l thrombin protease (Amersham Biosciences) solution was prepared in 1 \times phosphate buffer saline (PBS).

Microfluidic Chip Fabrication and Experimental Set-Up

Simultaneous dual emission hybrid BRET measurements were carried out both in a microplate using a SpectraMax M2 spectrofluorimeter (Molecular Devices) and in the microfluidics apparatus described below. Spectral scans of BRET constructs were recorded using the luminescence scan mode between 400 and 650 nm on addition of 5 μ M native coelenterazine substrate to 1 μ M of biosensor.

For the microchip BRET measurements, a simple Y-shape microchannel microchip (FIG. 1B), 70 μ m wide and 50 μ m high was fabricated from polydimethylsiloxane (PDMS) using standard photolithography. The chip design was completed in a commercial drawing package (Adobe Illustrator CS4) and the design pattern was printed on a transparency mask (5,080 dpi, Allardice). Master patterns of the microfluidic devices were fabricated using a laminar dry film resist (Shipley 5038). Multiple layers of resist were laminated at 113 $^{\circ}$ C. onto a substrate of polished stainless steel. The channels were lithographically patterned using a collimated UV source (λ =350-450 nm) operated at 20 mJ/cm² and a transparency film mask. After exposure, the test pattern was developed in a 20% Na₂CO₃ solution.

The pattern in resist was subsequently replicated as a Nickel shim using an initial sputter deposition of 100 nm Ni followed by electroplating to a thickness of 150 μ m. Then a 10/1 (w/w) ratio of PDMS and curing agent was poured over the shim, degassed and baked overnight at 75 $^{\circ}$ C. The device was cut and peeled off the shim and then exposed to air plasma for 10 minutes. The PDMS was then immediately sealed with a glass slide; after baking for three hours at 75 $^{\circ}$ C., the PDMS adhered strongly to the surface of the glass and the PDMS glass microchip was ready to use.

A schematic of the set-up for microfluidic measurement is shown in FIG. 1C. A nEMESYS high pressure pump system (Cetoni, Germany) was used to pump the fluids from two SGE syringes (Supelco) with 50 μ l capacity onto the microchip. The flow rates of both streams were 20 μ l/h. The microchip was placed on a microscope (Nikon Eclipse TE2000-U) stage for visualization and measurement. A sapphire laser (488 nm, Coherent) was used to locate the detection spot. Emitted bioluminescence was collected with a 20 \times objective (Plan Fluor, Nikon). Bandpass filters (Nikon) of 515 nm-555 nm for GFP² and 430 nm-455 nm for RLuc were used for the two channels. De-magnification lenses (Nikon C-0.45 \times) were used to focus light emitted from each channel onto the photomultiplier tube (Hamamatsu H7421). Integration time was 200 ms for data acquisition for each channel of light. The measurement position was varied along the main channel starting at the first confluence of the input channels ($x=0$) to the end of microchip.

Thrombin Assay

Various concentrations of thrombin were added to purified GFP²-RG-RLuc biosensor and incubated at 30 $^{\circ}$ C. for 90 minutes. To measure the extent of thrombin cleavage the sample mixture following incubation and the native CLZ solution were pumped from separate syringes into the two inlet channels and allowed to flow through the main channel. Diffusion between the two streams induced a BRET reaction at the interface. Recombinant hirudin from yeast (Sigma)

was incubated with thrombin at room temperature for ten minutes prior to the protease assay.

Sodium Dodecyl Sulfate Polyacrylamide Gel Electrophoresis (SDS-PAGE)

To confirm complete thrombin cleavage of the GFP²-RG-RLuc biosensor, SDS-PAGE analysis was carried out. Proteins (2.5 μ g) were diluted in 1 \times sample loading buffer (Invitrogen) for SDS-gel electrophoresis in a 12% Bis-Tris gel with MOPS running buffer (NuPAGE, Invitrogen). Bands were stained with Fast StainTM (Fisher) and then visualised.

Data Analysis

Using the microplate spectrometer, hybrid BRET ratios were calculated as the ratio of bioluminescence emissions measured at 500 nm and 470 nm. Using the microchip system, the hybrid BRET ratio was calculated as ratio of the long wavelength emission (515 nm-555 nm) to the short wavelength emission (430 nm-455 nm) (Pfleger and Eidne, 2006). To allow comparison between the two different detection systems, the Hybrid BRET ratios were normalized by expressing them as a multiple of the BRET ratio without added thrombin, in the same measurement system. All data are reported as means \pm standard deviation (SD). Two-tailed unpaired t-tests were performed using Graphpad prism (version 5.00 for Windows, Graphpad Software, San Diego, Calif., USA). Statistical significance is defined as $p < 0.05$.

Result

Effect of Thrombin on BRET Spectra and Ratio

The bioluminescent spectrum of the thrombin biosensor before thrombin treatment was bimodal with a peak at 470 nm representing RLuc emission and a second peak at 500 nm representing GFP² emission (FIG. 2A). This indicates energy transfer from the excited state of native coelenterazine to GFP². Upon thrombin cleavage the green component of the spectrum was reduced, demonstrating that thrombin cleavage of the thrombin biosensor had reduced the efficiency of energy transfer between donor and acceptor.

SDS-PAGE (FIG. 2B) confirmed that following thrombin treatment, the fusion protein was cleaved into two components with molecular weights of 32.4 KDa and 36.4 KDa (Lane 5, FIG. 2B) corresponding to His-tagged GFP² and untagged RLuc. Pre-incubation of the BRET biosensor with hirudin inhibited the formation of the two components demonstrating thrombin specificity (Lane 6).

The effect of thrombin on the biosensor cleavage was quantified using the change in BRET^{Hz} ratio. Following thrombin cleavage, the BRET^{Hz} ratio decreased significantly ($P=0.0009$), by approximately 32%, from 1.11 \pm 0.06 to 0.75 \pm 0.04. The hybrid BRET ratio of 0.79 \pm 0.05 following thrombin cleavage was not significantly different ($P=0.3309$) from those obtained by mixing 1 μ M each of RLuc and GFP² (FIG. 3, control). Pre-addition of hirudin prevented the thrombin induced reduction in the BRET^{Hz} ratio of 1.08 \pm 0.14. This was not significantly different to the ratio measured without thrombin ($P=0.7663$).

On-Chip BRET Measurement

To optimize the flow conditions for detecting the BRET biosensor, a series of experiments were carried out to image and quantify the BRET luminance at different locations, flow rates and biosensor concentrations (FIG. 5). In the initial stage of contact of the two fluid streams of fusion protein and substrate, the diffusion layer was narrow and only a small volume of the liquid emitted bioluminescence (data not shown). The intensity of the bioluminescence was also low (\sim 457) but significantly higher than the background (\sim 2.3). From $x=1$ to 5 mm, the bioluminescence intensities remained almost constant but there was a significant

increase at $x=7$ mm. This increase may reflect increased mixing in the region. Regardless of the intensity of the bioluminescence, the $BRET^{FF}$ ratio remained almost constant (~ 5.2) throughout the entire measurement region. To benchmark the on-chip measurements, the BRET ratios were compared with the microplate data measured using a commercial BRET detection instrument. The relative changes of BRET ratio, i.e. BRET ratio measured with thrombin vs that measured without, are very consistent between microchip and microplate measurements (to within $\pm 4\%$).

The effect of varying flow rate and biosensor concentration on the $BRET^{FF}$ ratio was also investigated (FIG. 6). The flow rate dependence was measured at two locations, $x=0$ and 4.9 mm (FIG. 6a). At $x=0$, the $BRET^{FF}$ ratio was also constant (to within $\pm 1.1\%$) for the range of flow rates studied, i.e. 20-60 $\mu\text{l/h}$. At $x=4.9$ mm, there was a slightly larger variation (to within $\pm 2\%$) of the BRET ratio due to the change in flow conditions. However, the overall uncertainty between the two measurement locations was within $\pm 5\%$. FIG. 6b shows hybrid BRET ratio as a function of the biosensor concentration. Even though the uncertainty for low protein concentration was relatively high (e.g. standard deviation = 7.7% at 1.49 μM biosensor concentration), the overall variation in mean $BRET^{FF}$ ratios varied less than with biosensor concentration, i.e. a standard deviation of 2.7%. The small variation in the $BRET^{FF}$ ratio under different measurement conditions is an important finding since it means that the completeness of the $BRET^{FF}$ reaction is not crucial for quantification as long as bioluminescence can be measured. Although more complete mixing would be predicted to increase the luminosity of the system our data imply that it would have little effect in $BRET^{FF}$ ratio. This potentially simplifies the design requirements of microfluidic devices for BRET-based detection, at least for the levels of thrombin concentration considered in the study.

Effect of Thrombin Concentration

Using a flow rate of 20 $\mu\text{l/h}$ and biosensor concentration 2.972 μM (FIG. 6) with the measurement fixed at $x=2.1$ mm (FIG. 5) we compared the microchip and the microplate systems for measuring thrombin using a range of thrombin concentrations (FIG. 7). The $BRET^{FF}$ ratio changed linearly with increasing concentrations of thrombin up to 0.24 nM for microfluidic measurements and 2.7 nM for microplate measurements. At higher concentrations, the change of BRET ratio is much less pronounced due to the saturation of thrombin. In the low thrombin concentration regions, calibrations were linear with R^2 values exceeding 0.995. Comparison of the gradients of the calibrations revealed that the microfluidic method is 4.7 times more sensitive to changing thrombin concentrations than the microplate method. The detection limits for thrombin are 27 pM for the microchip-based technique compared to 310 pM using the microplate-based technique. The microchip-based $BRET^{FF}$ system has a detection limit intermediate between the values calculated for the $BRET^2$ and $BRET^1$ microplate-based assays of 15 μM and 53 μM , respectively (Dacres et al. 2009a).

Conclusion

Bioluminescence resonance energy transfer method has been demonstrated for the first time in a flow format using a fluid phase thrombin-sensitive biosensor. The $BRET^{FF}$ technique used is a combination of $BRET^1$ and $BRET^2$ which allows testing of the $BRET^2$ components with measurable luminosity. The BRET reaction and detection were carried out in a Y-shape microchannel network in a microchip. Experiments quantified the effects of measurement location, flow rate and biosensor concentration. These fac-

tors affected the bioluminescence intensities in both optical channels but not the $BRET^{FF}$ ratio. The microchip-based technique showed an improved sensitivity for detecting thrombin compared to an equivalent microplate-based technique measured with a commercial instrument. The detection limits for thrombin were 27 pM for the microchip-based technique compared to 310 pM using the microplate-based technique.

Example 2—Preference of BRET in a Microfluidic System

In a $BRET^2$ system, *Renilla* luciferase (RLuc) with coelenterazine 400a (CLZ400A) substrate was used as the photon donor and GFP² was used as the acceptor molecule. As the luminescence of $BRET^2$ is 100-fold smaller than that of the $BRET^{1-5}$, the $BRET^2$ reaction requires efficient mixing at optimal temperature, detection chamber size, flow rates and concentrations to produce highest bioluminescence signal. Thus, this system is used to evaluate different mixing mechanisms (FIG. 8), reaction chamber designs and reaction conditions.

PDMS chips with a Y-shaped microchannel with three mixing elements (FIG. 8), with a rectangular cross section in the microchannels (200 μm in width and 30 μm in height) was used to monitor $BRET^2$ assays. The detection chambers with different diameter and height were located at the end of the microchannels. The emitting bioluminescence was collected by a multimode optical fiber located underneath the detection chamber. The emissions will be split by dichroic block and going through two band pass filters corresponding to emission band of the donor (430 nm-455 nm) and the emission band of the acceptor (515 nm-555 nm) before going into two corresponding photomultiplier tubes (Hamamatsu H7421).

The method involves flowing the protein solution in one the inlet of the Y-shaped channel and flowing coelenterazine 400a substrate in another inlet of the channel.

The method requires efficient mixing of the protein flow and the substrate flow by the passive mixing elements at a suitable flow rate.

The method aims to collect as high bioluminescence signal as possible by varying mixing elements, chamber size, protein and substrate concentration, flow rate, temperature etc. As a result, the optimum microfluidic mixing chip design and reaction conditions will be obtained and be translated into other BRET assays.

In order to enhance the efficiency, a fluidic chip integrated with a large optical detection chamber is used. By locating an optical fibre under the chamber the light emitted from $BRET^2$ reaction is collected and transmitted to the detection sub-system (FIG. 9). This approach ensures minimal losses and therefore high sensitivity and allows simultaneous capture of minute changes in emission levels at two wavelengths.

The inventors tested the detection sensitivity using a sensor protein capable of detecting a model protease (thrombin). The results indicated five fold improvement in $BRET^2$ detection sensitivity in comparison to commercially available microplate readers. In these tests we also confirmed that the detection limit was less than 20 pM.

FIG. 10 shows sample data from the sensitivity tests. Emission counts for GFP and RLuc are indicated with green (top line in the first panel, bottom line in the second panel) and blue lines (bottom line in the first panel, top line in the second panel) respectively. The raw data are shown for the no thrombin blank and the condition with 270 pM thrombin.

The ratio between emission levels (BRET² ratio:GFP/RLuc) indicates an approximately tenfold change in response to digestion of the sensor with 270 pM of thrombin.

FIG. 11 shows the response of the sensor when the thrombin concentration is varied from 0 to 270 pM. The figure also indicates results when the same experiment was repeated with a commercially available instrument. The sensitivity (slope) is five fold higher in the microfluidic system. The calculated limit of detection is less than 20 pM.

The BRET² ratio was measured with a two-inlet microfluidic device upon mixing sensor protein (1 μM) with a preparation involving thrombin (540 nM) and substrate (12.5 μM). Control experiment was carried out by mixing sensor protein (1 μM) with substrate (12.5 μM). Approximately 75% decrease in BRET² signal was measured for on-chip reaction at input flow rate of 50 μL/hr (FIG. 12).

Example 3—Performance of a BRET² Based Odorant Sensor in a Microfluidic System

The BRET² system is more suitable for measuring ligand-induced molecular re-arrangements in GPCRs compared to FRET (WO 2010/085844) or standard BRET. This is because the 6.8 Å separation of the BRET pair in preferred GPCR constructs (Dacres et al., 2010 and 2011) is well matched to the Förster distance of the BRET² donor and acceptor combination. However, one tradeoff is the low quantum yield for the RLuc donor when using BRET² chemistry. This results in fewer photons being available for detection. The use of RLuc2 and 8 mutations has been shown to improve the quantum yield (De et al., 2007) of the BRET² system whilst only having minimal effects on the Förster distance of the BRET² system (FIG. 1). The present inventors replaced RLuc with RLuc2 or RLuc8 in a OGOR sensor in an attempt to increase photon yield without detriment to the sensitivity of the odorant assay. FIG. 18 shows the transduction scheme for diacetyl detection using OGOR2 incorporating RLuc2.

Materials and Methods

Construction of BRET²-GPCR Sensors Incorporating Tagged *C. elegans* Odorant Receptors

Chimaeric BRET² tagged odorant receptors have the BRET² components inserted into the third intracellular loop (IC3) and at the C-terminus of the *C. elegans* odorant receptor with green fluorescent protein, GFP² at IC3 and *Renilla* luciferase, RLuc at the C-terminus of the protein (OGOR). Using site-directed mutagenesis the RLuc2 mutations were introduced into the pYES-DEST-52 OGOR sequence. Primers 1 and 2 (Table 3) were used to introduce the mutation C124A and primer pair 3 and 4 was used to introduce the M185V mutation to make the construct named OGOR2 (FIG. 18, SEQ ID NO:1, SEQ ID NO-2).

TABLE 3

Primers for introducing the RLuc2 mutations. C124A and M185V, into the pYES-DEST52-OGOR sequence.	
Primer name	Sequence
1 C124A	CACGACTGGGGCGCCCTGGCCTTCCACTAC (SEQ ID NO: 7)
2 C124A Antisense	GTAGTGGAAAGGCCAGGGCGCGCCCCAGTCGTG (SEQ ID NO: 8)
3 M185V	CTTCTTCGTGGAGACCGTGCTGCCAGCAAGATC (SEQ ID NO: 9)

TABLE 3-continued

Primers for introducing the RLuc2 mutations. C124A and M185V, into the pYES-DEST52-OGOR sequence.	
Primer name	Sequence
4 M185V Antisense (SEQ ID NO: 10)	GATCTTGCTGGGCGACGCGTCTCCACGAAGAAG (SEQ ID NO: 10)

OGOR2 Sample Preparation

Yeast colonies were inoculated in 10 mL SCMM-U (*S. cerevisiae* minimal media, composition per 200 mL: 1.34 g yeast extract without amino acids and 0.38 g yeast supplementation media without uracil) supplemented with 2% glucose and incubated overnight at 28° C. An aliquot of the overnight culture was used to inoculate SCMM-U supplemented with 2% raffinose and 2% galactose to a final O.D.₆₀₀ of 0.4 and incubated for an additional 72 h at 15° C. with shaking at 200 rpm.

Cell cultures were centrifuged at 1500×g for 5 minutes at 4° C. Cells were resuspended in 1 mL of sterile water and centrifuged for 1 minute at 10,000×g. Cells were resuspended in 4 mL phosphate buffer solution (PBS). The cells were lysed by French press (~18000 psi) and cellular debris was removed by centrifugation at 15000×g (4° C.) for 15 minutes. Following this the supernatant fraction was centrifuged at 40,000 rpm (Beckman Coulter L-80 ultra-centrifuge) for 1 hour at 4° C. The supernatant was decanted and the membrane pellet was resuspended in 1 mL of PBS and stored at 4° C. for 48 hrs.

Diacetyl Assay

All ligand solutions were prepared directly in water. The OGOR concentration was normalized using GFP² intensity at 510 nm. Assays were carried out in 96-well plates (Perkin-Elmer) in a total volume of 100 μL in phosphate buffered saline. OGOR was incubated with each ligand for 45 minutes at 28° C. in wells sealed with Topseal-A™ (Packard).

Plate-Reader Measurements

Following the incubation, Coelenterazine 400a substrate (Biosynth) was added to a final concentration of 5 μM. Simultaneous dual emission BRET² measurements were recorded with a POLARstar OPTIMA microplate reader (BMG LabTech) using the BRET² emission filter set, comprising an RLuc/Clz400a emission filter (410 nm bandpass 80 nm) and a GFP² emission filter (515 nm bandpass 30nm), with gains set set to 3300 and 4095, respectively, for the two channels, with an integration time of 0.5s.

Endpoint On-Chip Microfluidic Measurements

Endpoint microfluidic assays were carried out on-chip in two inlet microfluidic mixer devices integrated with an optical detection chamber. Coelenterazine 400a substrate (Biosynth) was prepared to a final concentration 12.5 μM and introduced in first inlet. OGOR and OGOR2 membrane pellets were resuspended in 1 mL of PBS, diluted as required and incubated at 28° C. for 45 minutes with diacetyl solution at concentrations ranging from 1 aM-1 μM. The preparation was introduced in the second inlet. On-chip mixing was initiated with an input flow rate of 400 μL/hr for each inlet. BRET² measurements were recorded using two photomultiplier tubes, one equipped with an RLuc/Clz400a emission filter (410 nm bandpass 80 nm) and the other with GFP² emission filter (515 nm bandpass 30 nm). The optical output was collected using an optical fiber with 1 mm core diameter aligned with an on-chip optical detection chamber.

Real-Time On-Chip Microfluidic Measurements

On-chip real-time measurements were carried out in a three-inlet microfluidic mixer device integrated with an optical detection chamber. The first inlet was used to introduce Coelenterazine 400a substrate (Biosynth), which was prepared to give a final concentration of 12.5 μM in PBS. The second inlet contained diacetyl (2,3-butanedione) diluted to give a final concentration of 1 fM in PBS, or PBS only as a control. The third inlet was used to introduce sensor protein suspension, which was prepared by resuspending the membrane pellet describe above in 1 mL of PBS and further diluting as required. The on-chip mixing was initiated by using input flow rates ranging from 50-400 $\mu\text{L}/\text{hr}$. BRET² measurements were recorded using two photomultiplier tubes, one equipped with an RLuc/Clz400a emission filter (410 nm bandpass 80 nm) and the other with GFP² emission filter (515 nm bandpass 30 nm). The optical output was collected using an optical fiber with 1 mm core diameter aligned with an on-chip optical detection chamber.

Analyzer

BRET² signals were calculated as the ratio of emission intensity at 515 nm to that at 410 nm. All data are reported as the mean \pm standard deviation (SD) or mean \pm standard error of the mean (SEM) as described in the text. Curves were fitted with log [agonist] vs response curves with variable slopes following normalization of data, using Graphpad Prism version 5.03 for Windows. Two-tailed unpaired t-tests were carried out in Graphpad prism. Statistical significance was defined as $p < 0.05$.

Results

Intensity

Introducing the RLuc2 mutation into OGOR increased the bioluminescence intensity by a factor of approximately ~ 150 from 1766 ± 125 RLU for OGOR to 272886 ± 26754 RLU for OGOR2 (FIG. 19). This mutant version of OGOR therefore showed potential for facilitating BRET² detection of odorant binding by OGOR2 on a microfluidic chip. This prediction was confirmed by on chip measurements. The RLuc2 mutation increased the bioluminescence intensity by a factor of approximately ~ 126 from 6.45 ± 2.9 RLU to 809.74 ± 116 RLU (FIG. 20).

Demonstration of Odorant Binding by OGOR2 in a Multi-well Plate

There was a 21.4% decrease in BRET² signal upon addition of 1 μM diacetyl to membrane preparations containing OGOR2 (FIG. 21) in the wells of a microplate. The diacetyl-induced change in the BRET² signal is significantly different ($P = 0.0136$) from the control response to water. The percentage change in the signal in response to diacetyl is smaller than seen with the original OGOR sensor (32%) incorporating native RLuc. However, there was less variance in the blank measurements for OGOR2, $1.0 \pm 7.0\%$ ($n = 3$) compared with $1.0 \pm 13.5\%$ ($n = 4$) for OGOR. Therefore the OGOR2 sensor is potentially capable of detecting lower concentrations of diacetyl than the OGOR sensor because detection limit is calculated as the blank signal $\pm 3 \times \text{S.D.}$

The OGOR2 response to diacetyl (FIG. 22) is dose-dependent, with a linear range (spanning six log units, from 10^{-18} to 10^{-12} M (FIG. 22). The calculated EC_{50} value is 11.4 nM diacetyl. This is two orders of magnitude lower than for the OGOR response in a microwell, suggesting improved sensitivity for diacetyl.

Detection of Diacetyl Binding by OGOR2 Using a Microfluidic Endpoint Assay

Following incubation of 10 fM diacetyl with membrane suspensions containing OGOR2, microfluidic on-chip mea-

surements showed a 36.9% decrease in BRET² signal (FIG. 23). The decrease in the BRET² signal was 1.5 fold greater than equivalent measurements made using a plate reader (FIG. 21). This indicates that microfluidic measurements using the OGOR family of biosensors are potentially more sensitive, *sensu stricto*, than plate reader measurements.

The concentration-dependent response of OGOR2, spans 2 log units from 10-18 to 10-16 M (FIG. 24). The calculated EC_{50} value is approximately ~ 10 nM diacetyl.

This Level is in Good Agreement with Plate-Reader Measurements (FIG. 22).

Real-time on-chip detection of odorant binding by OGOR2 with a microfluidic device Real-time on-chip measurements showed a 27.4% decrease in the BRET² ratio following on-chip mixing of 1 fM diacetyl with 290 nM of protein and 12.5 μM substrate at input flow rates of 50, 100, 200 and 300 $\mu\text{L}/\text{hr}$ (FIGS. 25 and 26).

Example 4—Performance of a BRET² Based Periplasmic Binding Protein Sensor in a Microfluidic System

Periplasmic binding proteins (PBPs) form a large and diverse family of soluble proteins found in bacteria. PBPs bind a diverse range of chemically disparate species including carbohydrates, amino acids, and neurotransmitters, metals and ions to name a few (Medintz et al., 2006). Although PBPs are unrelated at the primary sequence they all undergo a large ligand-induced conformational rearrangement commonly referred to as the 'venus-fly-trap' mechanism (Sharff et al., 1992 and 1993; Spurlino et al., 1991).

The measured distance between a FRET tagged N and C terminus of MBP of 6.93 nm (Park et al., 2009) is of a similar scale to the measured distance within the GPCR suggesting that BRET may be a better option compared to FRET for measuring distance in this range. Measurement of ligand binding by a PBP on a microfluidic chip could lead to a generic transduction platform with a wide range of applications areas including security, food and drink quality control, environmental and health-care. The inventors chose MBP as the initial test of this concept because it is a well-characterised member of the PBP superfamily and potentially representative of all PBPs. The BRET² transduction mechanism for maltose binding by periplasmic protein MBP is shown in FIG. 27. This sensor is a proof-of-concept for all PBPs with a similar structure and/or ligand binding mechanism to MBP. It is well known that the affinity of MBP-based biosensors for maltose can be altered by targeted mutations of the MBP domain. A similar approach is applicable to other PBPs.

Materials and Methods

Construction of BRET Proteins

RLuc2 was amplified by polymerase chain reaction (PCR) and cloned into pGEM®-T Easy vector (Promega, Australia). This resulted in a BstBI site being introduced downstream of the amplified gene and a XhoI restriction site directly upstream from the amplified gene. DNA sequencing confirmed the correct amplicon sequence. The amplicon was inserted into the BstBI and XhoI sites of pRSET GFP²-FL1-RLuc (Dacres et al, 2010) replacing RLuc to give pRSET GFP²-FL1-RLuc2.

MBP was amplified and ligated into the pGEM®-T Easy vector. During this process, a BstBI site was inserted upstream of the amplified gene and a PstI site downstream. MBP was restriction cloned into the PstI and BstBI sites of the pRSET GFP²-FL1-RLuc2 replacing the FL1 sequence with MBP to generate pRSET GFP²-MBP-RLuc2.

The W140 mutation was introduced into pRSET GFP²—MBP—RLuc2 using site-directed mutagenesis (Stratagene) using primers C1 (CA-GATGTCGCGTATGCCGAC) (SEQ ID NO:11) and C2 (GTACGCACGGCATAACGCGAAAGCGGACATCTG) (SEQ ID NO:12). Nucleotide and amino acid sequences for BRET² tagged MBP receptor provided a SEQ ID NOs: 3 to 6).

Expression and Purification of BRET² Proteins

Proteins were expressed in *E. coli* strain BL21 DE3 (Novagen). An overnight culture was grown from a single colony in LB (10 g tryptone, 5 g yeast extract, 5 g NaCl (pH 7.4)) containing 100 µg/mL ampicillin and 2% glucose at 37° C., 200 rpm. Expression was induced by inoculating 500 mL LB containing 100 µg/mL ampicillin to an A₆₀₀ of 0.1 and incubating at 37° C. (200 rpm) for 3.5 hours followed by overnight incubation at 22° C. (200 rpm). Cells were harvested 24 hr after inoculation.

For protein purification, cells were harvested by centrifugation at 4335×g (4° C.) for 15 minutes and resuspended in equilibration buffer (50 mM sodium phosphate buffer, 300 mM NaCl, pH 7.0). The cells suspension was passed through a homogeniser (Avestin emulsiflex C3 (ATA Scientific, Australia)) at a pressure of ~22000 psi and the soluble protein fractions were isolated by centrifugation at 15000×g (4° C.) for 15 minutes. Proteins were purified using cobalt affinity chromatography according to the supplied instructions (BD Talon (BD Biosciences, Clontech, Australia)). Following elution of the purified protein with 150 mM imidazole, the sample was dialysed against 50 mM Tris (pH 8), 100 mM NaCl, and 1 mM EDTA using a cellulose membrane (12,000 molecular weight cut off (Sigma)). Aliquots of 500 µL protein were snap frozen on dry ice and stored at ~80° C. Protein concentrations were determined by absorbance at 280 nm and calculated according to the method of Gill and von Hippel (1989).

Spectral Scans

All spectral scans were recorded with a SpectraMax M2 plate-reading spectrofluorimeter (Molecular Devices, Australia). The reactions were carried out in 96-well plates (Perkin-Elmer, Australia). Bioluminescence scans of BRET² constructs were recorded using the luminescence scan mode scanning between 360 and 650 nm with 20 nm intervals. End-Point On-Chip Microfluidic Measurement

On-chip measurements were carried out with microfluidic mixers with two inlets, a passive micromixer and an integrated optical detection chamber. BRET² measurements were recorded by using two photo multiplier tubes one equipped with an RLuc/Clz400a emission filter (410 nm bandpass 80 nm) and the other with a GFP² emission filter (515 nm bandpass 30m). The optical emission was collected by using an optical fiber with 1 mm core diameter aligned with on-chip optical detection chamber through a dichroic mirror.

Real-Time On-Chip Microfluidic Measurements

Real-time on-chip measurements were carried out with microfluidic mixers with three inlets, a passive micromixer and an integrated optical detection chamber. BRET² measurements were recorded by using two photo multiplier tubes one equipped with an RLuc/Clz400a emission filter (410 nm bandpass 80 nm) and the other with a GFP² emission filter (515 nm bandpass 30 nm). The optical emission was collected using an optical fiber with 1 mm core diameter aligned with on-chip optical detection chamber through a dichroic mirror.

BRET Protein Assays

1 µM purified protein was used for all the energy transfer assays (final volume of 100 µL). 1 µM purified protein was prepared by diluting the protein in phosphate buffer solution (PBS, 0.058 M Na₂H₂PO₄, 0.017 NaH₂PO₄, 0.068 M NaCl (pH 7.4)). Purified protein was incubated with the sugar dissolved in double deionised water or water for 30 minutes at 28° C. Following incubation 16.67 µM coelenterazine 400a was added and the signal was recorded immediately.

On-chip BRET Protein Assays

For on-chip assays 1 µM purified protein was incubated with 1 mM maltose solution at 28° C. for 40 minutes. The preparation was then mixed on-chip with 5 µM coelenterazine 400a and the optical signal was recorded from the detection chamber. The control experiments was carried out by incubating protein preparations with water and mixing on the chip under the same conditions. The results were compared to determine the percentage change in BRET² signal upon addition of maltose and extended to determine the maltose sensitivity.

Real-Time On-Chip BRET Protein Assays

For real-time assays the protein preparation, maltose and the substrate were mixed on the chip simultaneously. 1 µM purified protein was mixed with 1 mM maltose solution and 5 µM coelenterazine 400a substrate solution. The optical signal was recorded from the detection chamber. The on-chip reaction time was controlled by varying the flow rate. The change in the BRET² signal was measured for different reaction times and results were compared with a control experiment with water.

BRET Ratio Determinations

BRET ratios were calculated as the ratio of maximum acceptor emission intensity to maximum donor emission intensity.

Real-time On-chip Detection of Maltose

A y-shaped chip with two input channels and a serpentine common channel of length 18 mm was used. The cross-sectional dimensions of the common channel were 0.2 mm×0.035 mm. The BRET reaction chamber was Ø=4 mm and H=1 mm. There was no mirror on the upper surface of the chamber. Light was captured and transferred to the standard dichroic detector using a bifurcated light guide with input (trunk diameter of 6 mm and NA=0.59). PMT gate time was 500 milliseconds. Two different flow rates were tested: 200 µL per hour and 400 µL in the common channel.

Input A was prepared to contain 1 µM maltose and 31.25 µM Clz400a substrate or in the case of the negative control, 31.25 µM Clz400a substrate only. Input B contained 1 µM GMR sensor. A and B were pumped into separate arms of the Y-shaped microfluidic chip at input flow rates of 100 µL/hour or 200 µL/hour to give common channel flow rates of 200 µL/hour or 400 µL/hour, respectively. Total residence times were estimated at approximately 230 seconds in the first case and 115 seconds in the latter case. BRET² ratios were determined on the average data collected from 200-250 seconds after flow was commenced.

Data Analysis

All data analysis was carried out using GraphPad Prism (version 5 for Windows, Graphpad Software, San Diego, Calif., USA). All data will be reported as means± standard deviation (SD) unless otherwise stated in the text. Two-tailed unpaired t-tests will be performed using Graphpad prism. Statistical significance is defined as p<0.05.

Results

Maltose Detection by MBP BRET Ratio—Plate Reader Assay

The selectivity of the BRET tagged MBP protein was determined by testing the response to a range of sugars

including monosaccharides, disaccharides and trisaccharides (FIG. 28). Only maltose ($P=0.001$) and maltotriose ($P=0.02$) produced significant ($P<0.05$) changes in the BRET signal from the BRET tagged MBP. The BRET biosensor did not respond to glucose, fructose, sucrose or raffinose. Fehr et al. (2002) demonstrated that the FRET biosensor was able to detect maltose and a range of maltose oligosaccharides but did not specifically recognise any pentoses, hexoses, sugar alcohols, disaccharides or trisaccharides that do not contain the α -1,4-glucosidic link. The amplitude of the change in BRET ratio decreased from 29.65% to 17.03% with increasing length of the maltose chain from two units (maltose) to three (maltotriose) (FIG. 28). This is in agreement with reduced closing movement in the presence of larger α 1,4-oligomaltoside chains as demonstrated by electroparamagnetic resonance (EPR) studies (Hall et al., 1997) and FRET measurements (Fehr et al., 2002). Comparison of the relative size of the BRET² response to that of the FRET response reported in the literature (Fehr et al., 2002) demonstrated that substitution of BRET components for FRET components can increase the dynamic range of the biosensor resulting in signal changes of $29.65\pm 1.11\%$ for BRET compared to $\sim 12\%$ for FRET (Fehr et al., 2002). The inventors expect the signal change for classic BRET² would be of the same order as that for FRET, based on the similarities in Forster distance.

Introduction of the W140A mutant into GFP²—MBP—RLuc2 abolished the BRET² response to maltose (FIG. 28). No significant difference ($P=0.63$) was observed between the BRET² response to either water or maltose. The W140A mutant has a dissociation constant higher than 100 mM for maltose and was previously used as a control for the FRET tagged MBP when applied to monitoring the uptake of maltose into yeast (Fehr et al., 2002). The lack of response of the W140A mutant to maltose indicates that the effect of maltose on the BRET² ratio of GFP²—MBP—RLuc2 is not due to a direct interaction between maltose and the BRET components themselves. These results confirm the potential suitability of the GFP²—MBP—RLUC2 (GMR) and similar sensors in a BRET² based microfluidic chip assay.

Response Time

The BRET² response increased with increasing incubation time until 30 minutes when the response reached a maximum (FIG. 29). Thirty minutes was used for further assays. In the present microplate assay format it is not possible to record the BRET² response in real-time but real-time maltose assay could be carried out using a microfluidic chip format.

Sensitivity

The BRET² tagged MBP biosensor was capable of quantifying different concentrations of maltose spanning three log units ranging from 1×10^{-8} M to 3.16×10^{-6} M with an EC_{50} of 3.71×10^{-7} M (FIG. 30a). The response of the FRET tagged MBP receptor is linear only over two log units ranging from 0.26 – 21.12 μ M with an EC_{50} of 3.24 μ M.

On-Chip Assay Measurements

Sensitivity assays were carried out on a two input microfluidic mixing device (FIG. 8b) with a serpentine common channel of $L=18$ mm. The BRET reaction chamber was $\varnothing=4$ mm and $H=1$ mm with no mirror. A bifurcated light guide was used with a 6 mm trunk and $NA=0.59$. 1 μ M GMR sensor was incubated with maltose at concentrations ranging from 10^{-9} to 10^{-3} M for 40 min at 28° C. The incubated sample and 31.25 μ M Clz400a substrate were each pumped onto the chip at input flow rates of 400 μ l/hr. The trunk end of the light guide was used to collect signal from the BRET reaction chamber. Two branches of the light guide were

directed toward to two sets of filter blocks (410/80 for blue, 515/30 for green) in front of two PMTs. The BRET² signal was measured at each concentration. The experiment was repeated on each of three days, using the same batch of GMR sensor. Nine chips were used, one for each concentration tested, across all three days. The log concentration response curve for on-chip detection was effectively identical to that of the previous plate based measurements as was the $EC_{50}=2.2\times 10^{-7}$ M (FIG. 30b).

The specificity of the sensor for maltose over the saccharides glucose and sucrose was investigated on chip. The amplitudes of the emissions were high with RLuc/Clz400a signals in the range of 10000 to 25000 counts/gate (500 ms) and GFP² signal in the range of 2000 to 10000 counts/gate (500 ms). In the absence of analyte, the BRET² ratio was 0.225. Binding of maltose (FIG. 52) resulted in a large change in BRET² ratio with a mean BRET² ratio of 0.35 for 0.1 mM maltose, an increase over the no sugar control of 52%. Reactions with glucose and sucrose resulted in 7 and 15% increases in BRET² ratio, respectively, confirming that the selectivity of the BRET²-based sensor for maltose is maintained in a microfluidic format.

Real-Time On-Chip Detection of Maltose

As the inventors have previously shown for protease and volatile detection, the invention is capable of mixing sample with sensor and substrate on chip, so that the entire detection reaction can be performed in a continuous flow format on the chip. The inventors demonstrated that this works with three inputs: sample, sensor and the coelenterazine 400A substrate using OGOR2 sensor and diacetyl (FIG. 26) and using two inputs for thrombin (see, for example, FIG. 51). The inventors extended this work to show that the same process works with the BRET-based maltose sensor. In this case, for convenience, the inventors also used a two input microfluidic chip. The coelenterazine substrate and a sample solution containing maltose (or a negative control without maltose) were premixed and pumped into one input and the GMR sensor solution was pumped into the other input.

Signals were detected approximately 40 seconds after initiating flow at both flow rates but stabilised more quickly (60 seconds vs approximately 130 seconds) in the case of the faster flow rate (200 μ L per hour inputs) (FIG. 67). Total luminance was strong and easily detected 1000-1500 counts/gate for RLuc/Clz400a and 6000-7000 counts/gate for GFP² at 100 μ l/hr or 2000-3000 counts/gate for RLuc/Clz400a and 7000-9000 counts/gate for GFP² at 200 μ l/hr.

Once stabilised, 1 μ M maltose was easily distinguished from control at both flow rates (FIG. 64), with the slower flow rate giving a change in BRET² ratio of $\approx 20\%$ and the faster flow rate showing a change of $\approx 27\%$.

Example 5—Comparison of Bioluminescent Signal Collection with and without Fiber Optical Switch

One of the highly preferred requirements of the instrument for use in the invention is multiplexing, meaning the instrument must be able to detect several analytes nearly at the same time (i.e. with very small time delay between one analyte to the next one). To reduce the cost and space as well as weight of the instrument, optical fiber switch could be used to enable multiplexing. In an embodiment, several input optical fibers will concurrently collect bioluminescent signal from at least six detection chambers. The optical switch will then connect one particular input fiber for a short period of time (few hundred milliseconds) to the single output fiber which connects to the optical blocks for splitting and band-passing the signal into two photomultiplier tubes

(PMT). In the same fashion, the switch will turn on the next input fiber. In the current example, the switch takes 50 ms to change between input fibers. Optical switching inevitably introduces optical losses in the collected signal. Thus, this experiment was done to confirm if it is possible to collect signal through the optical switch and calculate the amount of signal loss due to optical switching.

Experimental Setup

The experimental setup is shown in FIG. 31. FIG. 31A shows the set-up without the optical switch. A single fiber was manipulated to align below the optical detection chamber of the microfluidic chip. The fiber is then connected directly to the optical blocks. FIG. 31B shows the set-up with the optical switch. A Leoni 1×9 mol fiber optical switch was used. The 9 inputs are terminated by the sub miniature A (SMA) connectors while the single output fiber is terminated by ferrule connector (FC). A stainless plate was machined to contain an array of SMA receptacles allowing connection of optical fibers from the bottom. On the top of the plate sat the microfluidic chip with optical chamber aligned at the tip of the fiber. For this experiment one input fiber was used. The output fiber was then connected to the optical blocks.

Materials and Methods

Endpoint microfluidic assays were carried out on-chip in two inlet microfluidic mixer devices integrated with an optical detection chamber. Coelenterazine 400a substrate (Biosynth) was prepared to a final concentration 12.5 μM TE buffer (10 mM Tris (pH 8.0) 100 mM NaCl, 1 mM EDTA) and introduced in first inlet. GTR membrane protein was diluted in TE buffer (10 mM Tris (pH 8.0), 100 mM NaCl, 1 mM EDTA) at concentration of 1 μM. The prepared GTR solution was introduced in the second inlet. On-chip mixing was initiated with an input flow rate of 400 μl/hr for each inlet. BRET2 measurements were recorded using two photomultiplier tubes, one equipped with an RLuc/Clz400a emission filter (410 nm bandpass 80 nm) and the other with GFP² emission filter (515 nm bandpass 30 nm). The optical output was collected using one single input fiber for both cases in FIG. 31. The gate time was 500 ms.

Result

FIG. 32 shows the real-time bioluminescent signal in the RLuc/Clz400 channel collected without and with optical switching for three runs. The GFP also shows similar behaviour (data not shown). From these results, it is confirmed that bioluminescent signal has been successfully passed through the optical switch. In terms of loss, FIG. 33 compares the luminescent signals collected without and with optical switch in both RLuc/Clz400a and GFP channels. The loss due to the optical switch for the RLuc/Clz400a channel was 40% while for the GFP channel it was 28%.

Example 6—Optimisation of Overall System Luminance and Photon Detection Efficiency

One of the important features of the invention is its ability to detect very low levels of analyte in real time with economical use of reagents. One of the keys to achieving this is to generate the maximum number of photons per unit volume of sensor solution. Incorporation of improvements like the RLuc2 mutation assist with this. It is also vital to minimise loss of photons in the optical detection system. High photon detection efficiency permits a desirable combination of response time, reagent economy and signal to noise ratio. Increasing the volume of the BRET reaction chamber and the common channels tends to increase the available light signal, which improves the signal to noise ratio but reduces the time resolution of the system. In-

creasing the flow rate in the device, other things being equal, improves the time resolution of the device but reduces its reagent economy and the signal to noise ratio. It is also vital to minimise losses in the optical detection system. A number of alternative experimental set ups were developed to improve the photon detection efficiency.

Experimental Set Up

On-chip measurements were carried out with a microfluidic chip similar to that shown in FIG. 31A with two inlets, a passive mixing element and a detection chamber. An aluminium mirror was placed on top of the reaction chamber to enhance the BRET signal. BRET emissions were recorded using two photo multiplier tubes one equipped with an RLuc/Clz400a emission filter (410 nm bandpass 80 nm) and the other with a GFP² emission filter (515 nm bandpass 30 nm).

A number of variations were compared with the original set up (FIG. 31A). The diameter of the reaction chamber was increased to 4 mm (FIG. 34A) from an original diameter of 2 mm. The height of the reaction chamber was varied between 1 and 2 mm. A single optical fiber of diameter 0.4-1.0 mm (FIG. 31A) was replaced with a liquid light guide or fibre-optic bundle of 5 mm core diameter NA=0.59, feeding into a dichroic block (FIG. 34A), or a bifurcated light guide of trunk core diameter 6 mm branch core diameter of 4 mm (FIG. 37) or a multifurcated light guide of trunk core diameter 8 mm and branch core diameter 4 mm (FIGS. 38 and 40).

Materials and Methods

OGOR2 sensor solution was prepared at day 4 in PBS at high (100 and 50 times) dilution ratios from stock solution. Clz400a was prepared in PBS at 31.25 μM. When diacetyl was included, it was added to the OGOR2 sensor solution at a final concentration of 1 μM. For the control experiment, only DI water was added. The sensor tubes without and with diacetyl were both incubated at 28° C. in 30 min.

Results

Light collection was compared between the original system with fiber diameter 1.0 mm and the modified system using a single 5 mm core liquid light guide (FIG. 35). At a 100 fold dilution of sensor, the original system had high noise levels and neither the RLuc2 nor the GFP² signals could be discriminated from noise. In contrast, using the liquid light guide, background noise levels were substantially lower and both emission channels could be clearly discriminated from noise by approximately 50 seconds after switching the system on. Maximum signal levels were achieved by approximately 200 seconds after reagent pumping commenced. It should be noted that because the newer configuration has a BRET reaction chamber volume 4 fold greater than the original one, it takes up to 100 seconds longer for the signal to saturate in this condition. Nevertheless, discrimination from baseline can be detected by 50 seconds. Similar results were observed for the 50 times dilution ratio (results not shown). With the improved system, it was possible to detect analyte using OGOR2 at 50× and 100× dilutions (FIG. 36).

If each microfluidic channel has a dedicated photodetector then a scheme such as that shown in (FIG. 37), in which each microfluidic channel is interfaced with a bifurcated light guide that channels light into a pair of photomultipliers or equivalent detectors, is a suitable arrangement. Comparison of this arrangement with a dichroic block shows that it may have better photon detection efficiency and signal to noise characteristics under otherwise comparable conditions (FIG. 39).

If light guides (core diameter ≥ 1.0 mm) are used instead of optical fibres (core diameter ≤ 1.0) it is difficult to obtain a suitable optical switch for time domain switching of the optical detection system between different microfluidic channels. In this case, a shutter box may be used. An example of a suitable optical architecture is shown in FIG. 38. Light collected from the multichannel chip is directed to the shutter box and the output is channeled to the optical detector via a multifurcated fiber bundle. The shutters are located in the input side of the multifurcated fiber bundle allowing software selection of the sequence of channels and the duration of monitoring.

A suitable multifurcated light guide arrangement is shown in FIG. 40. Results obtained comparing this arrangement with channel-specific bifurcated light guides (FIG. 37) indicate that the dichroic filter gives an $8\times$ higher signal in the GFP channel and a $6.6\times$ higher signal in the RLuc channel compared with bifurcated light guides (FIG. 41). The BRET² ratio was 4.67 ± 0.07 with the dichroic filter and 3.85 ± 0.25 for the bifurcated arrangement.

Example 7—Examples of Suitable Valve and Solid State-Based Photodetector

A very wide variety of vacuum based and solid state sensors are commercially available, which can be interfaced with the microfluidic chip in order to measure the light produced by the BRET reaction. FIG. 42 illustrates a high counting efficiency, high gain, low dark-noise assembly using traditional vacuum tubes. FIG. 43 illustrates a high photon detection efficiency, high gain, low dark-noise assembly implemented using solid-state technology. Many variants on these two approaches are available.

Example 8—Experimental and Theoretical Optimisation of Diffusional Mixing in the Microfluidic Chip

Laminar flow conditions may pertain in a microfluidic chip of typical dimensions used in this invention. In this case mixing occurs principally by diffusion and may require slow flow rates and long residence times to approach completion. Slow flow rates are undesirable because they result in a slower time to first detection of analyte or analytes than would otherwise be the case. This limitation may be overcome by forcing turbulent mixing, using for example more complex microfluidic geometries and/or pulsatile flow and/or micromechanical mixing and/or acoustic and/or electrokinetic means. All of these methods, whilst feasible, potentially involve additional engineering complexity and cost. The inventors therefore investigated simple passive design features that can enhance diffusive mixing in a laminar flow environment.

Experimental Setup

For investigations with dyes, the inventors used a three inlet microfluidic network (FIG. 44). Thrombin detection experiments used a two-inlet microfluidic network, with Y-shaped geometry (FIG. 31a). The BRET reaction chamber (not shown) was either 2 mm or 4 mm in diameter. The dimensions of all microchannels were 200 μm wide by 35 μm deep. In the original (side-by-side) set up, the channels contacted each other along their vertical (35 μm) sides and were fabricated with a serpentine mixing region approximately 28 mm long (FIG. 44). In a modified (pancake stack) set up (FIG. 45), the two input channels were 30 μm deep and 600 μm wide and were stacked on top of each other, in contact via their horizontal (600 μm) sides to form a linear

common channel 600 μm wide and 60 μm deep. The length of the common channel was 20 mm.

For dye experiments, solutions of food dyes were drawn from three input microchannels using a single pump in withdrawal mode at flow rates of 30-300 μL per hour. For thrombin sensing experiments we used 12.5 μM coelenterazine A substrate, which was premixed with the test concentration of thrombin and pumped into one arm of the Y-shaped microchannel. 1 μM of a BRET² based thrombin biosensor, prepared as previously described (Dacres et al., 2009b) was pumped into the other arm of the microchannel. Input channel flow rates were varied from 50-400 μL per hour. The limits of detection were estimated informally as the lowest concentration of thrombin for which the operator could discern a change in the BRET² ratio at a input reagent flow rate of 50 μL per hour.

Results

As shown in FIG. 44, using a side-by-side configuration, flow is laminar at high flow rates (common channel flow rate=300 μL hour), corresponding to residence times of 2.35 seconds, and there is little or no observable mixing. Flow remains laminar at lower flow rates (common channel flow rate=30 μL per hour) corresponding to a residence time of 23.5 seconds, but significant diffusional mixing can be detected over this period.

Calculations of Residence Times

i) For withdrawal flow rates of 300 μL per hour and the three input network:

Volume of the serpentine region is 0.2 mm \times 0.035 mm \times 28 mm \Rightarrow 0.196 μL .

Flow rate in the common channel is 300 μL per hour. 0.196/300=6.53 $\times 10^{-4}$ hours=2.352 seconds.

ii) For input flow rates of 30 μL per hour.

The residence time is 10 \times longer, i.e. 23.52 seconds.

iii) For the side by side stack:

Volume of the serpentine region is 0.2 mm \times 0.035 mm \times 28 mm \Rightarrow 0.196 μL . Flow rate in the common channel is 100 μL per hour.

0.196/100=1.96 $\times 10^{-3}$ hours=7.056 seconds.

Volume of the BRET reaction chamber ($\pi 1^2 \times 1$ mm³)=3.14 μL

Flow rate is 100 μL per hour. 3.14/100=0.0314 per hour=113 seconds

Total residence time is 120 seconds.

iv) For the pancake stack

Volume of channel is 0.6 mm \times 0.06 \times 20 mm \Rightarrow 0.72 μL . Flow rate in the channel is

100 μL per hour 0.72/100=7.2 $\times 10^{-3}$ per hour=25.92 seconds

Volume of the BRET reaction chamber ($\pi 2^2 \times 1$ mm³)=12.6 μL

Flow rate is 100 μL per hour. 12.6/100=0.126 per hour=452 seconds.

Total residence time is 478 seconds or 7 minutes 58 seconds.

The thrombin assay is very sensitive to sub-optimal mixing because both the analyte and the sensor are macromolecules with slow diffusion coefficients and also because thrombin ($k_{cat}\approx 85$ s⁻¹) has to process a large number of sensors by proteolytic cleavage before a signal can be detected and this takes time.

Using a traditional side-by-side network, with a flow rate of 50 μL per hour in each input arm, the lowest concentration of thrombin observable in real time (120 seconds) was 540 nM. Using a pancake stack network at the same flow rate (478 second residence time) 27 nM thrombin could be detected easily (FIG. 46). Thrombin was detected down to 14 nM, the lowest concentration tested. After adjusting for

the fourfold difference in residence times there is at least a tenfold benefit in detecting a lower concentration of thrombin for the pancake stack.

The inventors attribute this improvement to improved diffusional mixing in the pancake stack architecture. They therefore compared the length of microfluidic channels (28 mm in the side-by-side example and 20 mm in the pancake stack example) with the theoretical distance required for complete mixing in these different configurations.

Calculation of distance required for complete diffusional mixing

L: Channel length (mm)

Q: Volumetric flow rate (l/hr) or (mm³/s)

$$Q=200 \mu\text{l/hr}=200 \text{ mm}^3/\text{hr}=0.055 \text{ mm}^3/\text{s}$$

D: Diffusion coefficient (for thrombin) $D=4.16 \cdot 10^{-5} \text{ mm}^2/\text{s}$

U: average velocity in channel (mm/s)=Q/width×height (channel cross sectional area)

X: Diffusional distance travelled in period t is estimated by $X^2=tD$.

The X value for complete mixing depends on the channel configuration. Assuming a two-input channel architecture, for the side-by-side design, X is half the common channel width and, for the pancake stack design, X is half the channel height.

$$\begin{aligned} \text{Residence time for complete mixing} &= L/U = X^2/D \\ D &\Rightarrow QX^2/\text{width} \times \text{height} \times D \end{aligned}$$

Therefore:

1. Current (side-by-side) design where:

H (Channel Height)=34 μm =0.034 mm and

W (Channel Width)=200 μm =0.2 mm

$$L \approx QH^2/4WHD = 0.055 \text{ mm}^3/\text{s} \times 0.04 \text{ mm}^2/4 \times 0.2 \text{ mm} \times 0.034 \text{ mm} \times 4.16 \cdot 10^{-5}$$

mm²/s=1944 mm

2. Current (pancake stack) design where:

H (Channel Height)=60 μm =0.060 mm and

W (Channel Width)=600 μm =0.6 mm

$$L \approx QH^2/4WHD = 0.055 \text{ mm}^3/\text{s} \times 3.6 \cdot 10^{-3} \text{ mm}^2/4 \times 0.6 \text{ mm} \times 0.06 \text{ mm} \times 4.16 \cdot 10^{-5} \text{ mm}^2/\text{s} = 33 \text{ mm}$$

3. Optimised (pancake stack) design where:

H (Channel Height)=14 μm =14×10⁻³ mm and

W (Channel Width)=1200 μm =1.2 mm

$$L \approx QH^2/4WHD = 0.055 \text{ mm}^3/\text{s} \times 196 \cdot 10^{-6} \text{ mm}^2/4 \times 1.2 \text{ mm} \times 14 \cdot 10^{-3} \text{ mm} \times 4.16 \cdot 10^{-5} \text{ mm}^2/\text{s} = 3.9 \text{ mm}$$

Therefore the side-by-side stack provides only 28 mm (i.e. 1.4%) of the 1944 mm required for complete mixing whereas the pancake stack arrangement tested provided 20 (i.e. 61%) of the 33 mm required for complete mixing. Calculations demonstrate that with minor additional changes it would be feasible to arrange for diffusive mixing to be complete within 7.7 mm i.e. less than 40% of the length available in the current design.

Example 9—Improvements to Microfluidic Network Designs and Pumping Arrangements

Microfluidic networks where the lengths of multiple reagent input channels connected to a common port vary as, for example in FIG. 14, had poor reliability (results not shown) because of the tendency for the differences in back pressure to prevent flow in longer channels, routing all flow through shorter channels. These designs are also very susceptible to blocking by bubbles, for similar reasons. The inventors therefore tested a number of different design

features and pumping arrangements to improve the reliability of the multichannel device.

Experimental Setup for Paired Symmetrical Microfluidic Sensors

In one example (FIG. 47), the inventors designed a network with a bilaterally symmetrical parallel channel layout to obtain two simultaneous reactions using two different sensors. This arrangement can be replicated to obtain any even number of sensor channels.

The inventors demonstrated fluid flow on the chip using food-colouring dye at two flow rates (FIG. 48). Diffusive mixing was largely complete at a flow rate of 150 $\mu\text{l/hr}$, whereas at 1500 $\mu\text{l/hr}$ the input streams remained largely separate.

Flow was continuous and even along both arms of the network and blockage occurred less frequently than with asymmetric designs. Nevertheless, this design is still susceptible to blockage or uneven flow if a bubble or other obstruction lodges in one of the two parallel arms. The inventors therefore investigated other approaches for driving the sample and reagents through the microfluidic network.

It is desirable that each common channel has its own dedicated pressure source(s) that is/are not shared with any other common channel. This means that, should there be variation in the backpressures in the network for any reason, then flow cannot be diverted to a different common channel. Unfortunately, when operating in positive pressure mode, observation of this principle would mean that each common channel requires three dedicated pumps: one each for the sensor, substrate and sample, resulting in a system with complex and potentially expensive engineering requirements. An elegant and superior alternative is to drive the reagents through individual common channels using a single dedicated pump operating in suction (negative) mode. This only requires a single pump per common channel, as shown in FIG. 49. The quality of laminar flow in a network driven by suction pressure is even and reliable as shown in FIG. 44. In the worst case, blockage or partial obstruction in one common channel or the microfluidic channels leading into it only affects that sensor channel.

An ancillary benefit of providing a dedicated source(s) of pressure for each common microfluidic channel (and therefore for each different sensor) is that it allows the simultaneous operation of multiple sensor channels independently of each other with potentially different flow rates and consequently different balances between speed and sensitivity (FIG. 50). This might for example, allow two or more channels to use the same sensor at different flow rates in order to give a range of different limits of detection and time constants. Another option is to operate several channels with different sensors, at different flow rates optimised for each sensor. An extreme example of this would be to run completely different sensor types such as a GPCR-based volatile sensor and a protease sensor in parallel on the same chip, with the same or different samples, and tailor the flow rates for the very different reaction kinetics of the two reaction classes. It would also be possible to use suction pumping, as described here, to support the use of different types or dilutions of sample or substrate chemistry on the same chip at the same time.

Use of suction mode is fully compatible with the concept of providing reagents in simple disposable cartridges on the inlet side of the network. Changing cartridges would allow simple and rapid switching of applications or targets, using the same basic hardware. An additional advantage is that the

need to decontaminate the pumping device, between samples or after analyte detection is minimised in the suction mode.

The inventors performed an additional experiment incorporating the preferred light collection and detection setup from Example 6 together with the preferred suction mode pumping of this Example and a BRET²-based thrombin sensor from Example 2. In this experiment, we used a simple Y-shaped microfluidic network with a serpentine common channel having dimensions of 0.2 mm×0.035 mm×28 mm. The BRET reaction chamber was Ø=2 mm and height 1 mm, giving a volume of 3.14 µL. Light from the reaction chamber was fed into one branch of a four-branch fiberoptic bundle and thence into a 25.4 mm (1 inch) diameter optical block for simultaneous dual wavelength measurement with a dedicated dichroic filter and two PMTs. The chip was primed with buffer and 50 µL input reservoirs were loaded with 50 µL of 1 µM GTR thrombin sensor and 50 µL of 12.5 µM coelenterazine 400a substrate. Flow was started using negative pressure (suction mode) at the outlet with a common channel flow rate of 200 µL/hr=0.055 µL/sec. Under these conditions, the BRET reaction chamber residence time was 57 seconds.

As shown in FIG. 51, after startup was complete, the system generated very strong signals in both optical channels with excellent signal to noise ratios (compare with FIG. 10a). Based on the rate at which signal develops and the BRET reaction chamber residence time, for a chamber with diameter 2 mm, we estimate that a minimum chamber height of 300 µm would still give measurable signals above background (FIG. 51c). At the specified flow rate, this would correspond to a reaction mixture integration time of approximately 20 seconds. A chamber diameter of 4 mm, would potentially allow the chamber height to be reduced to 75 µm, whilst retaining the same signal strength and reaction mixture integration time.

Example 10—Example of Application of the Invention to Beverages and Other Fluids, Including Prophetic Example of Predicting Plasmin Spoilage of UHT Milk Background

The invention is readily applicable to any analytes that will dissolve in water or an aqueous solution, including volatile chemicals that will partition into an aqueous solution. Analytes that are already present in an aqueous liquid, including milk, fruit juices, other beverages and bodily fluids including blood serum are especially amenable to detection because there is no need for a preliminary gas-liquid partition prior to analyte measurement.

A simple example of an application in this area includes prediction of spoilage of UHT milk. Proteases from bacteria that have been killed by UHT treatment may cause increased viscosity, gelation, and bitterness in whole and skimmed UHT milk during storage, thereby leading to loss of shelf-life. Specifically, it is proteolysis of casein by plasmin that causes these problems in UHT milk. Commonly used assays for detecting proteases are slow and are insufficiently sensitive to easily detect the very low levels of protease that can result in spoilage of UHT milk after 6-9 months or more of storage at ambient temperature. The invention could measure such very low levels of plasmin in UHT milk with great sensitivity and in real time. It would be applicable to an in-line monitoring in a commercial setting. This will allow estimation of product shelf life and identify any need for additional processing prior to packaging. Based on our previous BRET² sensors for thrombin and caspase proteases,

we would construct a biosensor for detection of plasmin activity in milk, by incorporating the target peptide sequence, preferably Lysine-X (where X=Lysine, Tyrosine, Valine or Glutamic acid), into the linker between BRET donor and acceptor (FIG. 53). This sensor would be incorporated into a version of the invention suitable for on-farm and in-factory use. However, because we did not have such a sensor readily to hand, we used some existing sensors, including one that detects thrombin, to demonstrate the feasibility of using our method to detect proteases in milk or indeed other commercially or medically important fluids such as orange juice and mammalian serum.

Method

In one experiment, we used the GFP²-FL₁-RLuc2 construct described by Dacres et al. (2012) diluted 1/125 (i.e. ≈0.5 µM) with 5 µM coelenterazine A in PBS or in various dilutions of full fat “Canberra Milk” brand milk, “Just Juice” reconstituted orange juice and mammalian blood or serum.

In another experiment, the inventors used the GTR BRET²-based thrombin sensor described in Examples 1 and 2 with RLuc replaced by RLuc2 (GFP²-RG-RLuc2 (GTR2)), construct described by Dacres et al. (2012) diluted 1/100 (≈0.5 µM) with 5 µM coelenterazine A in thrombin cleavage buffer or various dilutions of milk, orange juice or serum. Thrombin cleavage of GTR2 in various dilutions of milk, orange juice or serum was assessed by spiking the samples with 2 units of exogenous thrombin to simulate an endogenous protease. Serum was prepared from mammalian heparinized (250 IU/ml) blood samples. To prepare serum blood sample were left undisturbed at room temperature for 30 minutes and then centrifuged at 1,000-2,000×g for 15 minutes. The supernatant is designated serum. The serum samples were maintained at 2-8° C. while handling. All experiments were performed in 100 µL final volume in a microwell plate and BRET² signals were read in a Polarstar Optima microplate reader (BMG Labtech) as described previously.

Results

Preliminary results, using GFP²-FL₁-RLuc2, demonstrated that the BRET² chemistry functions well in the aqueous environment of whole milk and orange juice, diluted 1/10 with PBS (FIG. 54). FIG. 55 shows the time dependent decay of the BRET² signal of GFP²-FL₁-RLuc2 in whole milk

Results using GTR2 demonstrate that the BRET² chemistry also functions in serum when diluted 1/10 in thrombin cleavage buffer (FIGS. 56 and 57). Bioluminescence activity was completely recovered when diluted 1/500 for serum, 1/50 for orange and 1/10 for milk in thrombin assay buffer compared to resuspension in thrombin assay buffer alone (FIG. 56). The BRET² ratio was higher for all serum dilutions compared to buffer except for 1/1000 dilutions in buffer (FIG. 57a). When resuspended in orange the BRET² ratio was higher when diluted 1/10 in buffer compared to buffer alone but was a consistent value for all other dilutions (FIG. 57 b). Only GTR2 resuspended in undiluted milk resulted in a BRET² ratio higher than when resuspended in buffer alone compared to all other milk dilutions (FIG. 57c).

Thrombin activity was detected in 1/10 dilutions of milk and orange juice (FIG. 58). In serum a 1/100 dilution of the serum sample in buffer resulted in thrombin activity. All dilutions resulting in thrombin activity produced significant changes (P<0.0001) in the BRET² ratio compared to samples without addition of thrombin. Thrombin activity in serum diluted 1/1000, orange diluted 1/100 and milk diluted 1/100

in buffer resulted in BRET² signal changes not significantly different ($P>0.25$) from those generated in thrombin cleavage buffer.

Example 11—Demonstration of Gas Liquid Transfer of Volatiles Using a Wetted Wall Cyclone

One of the advantages of the invention is that it can be applied to detection of volatile analytes. However, because the sensors are necessarily dissolved or suspended in aqueous solution, volatile analytes must partition from the gas phase into aqueous solution before they are available to contact the sensors. The inventors set out to demonstrate the feasibility of transferring volatile chemicals from air to liquid in a format compatible with the invention. There are a number of methods that could be used rapidly to equilibrate ambient air or target headspace with an aqueous based sample liquid, including gas in liquid bubbling or misting. However, the inventors selected a wetted-wall cyclone to demonstrate the concept because suitable equipment is available commercially.

Experimental Set Up for Initial Tests

Initial tests were completed using the SASS2400 wetted-wall cyclone (Research International). The internal fan draws air at 40 L/min and equilibrates it with 1 mL water. To compensate for evaporation, the sample level is monitored and replenished from a 1300 mL reservoir of de-ionised water.

The sample chemical was placed in a 1.7-2 mL eppendorf tube. A hole was drilled in an 80 mm section of aluminium tubing to mount the tube in the inlet port of the SASS2400 (similar to FIG. 59). Sampling time for these tests was inclusive of fan start-up and sample liquid filling times.

Method

Two consecutive runs were done for each test, to give a total volume of 2 mL of sample. Tests were done following the time kinetics of re-absorption of oxygen into de-ionised water that had been de-oxygenated by sparging with nitrogen and with acetaldehyde and phenol. Oxygen concentration was measured with an oxygen electrode. Volatile concentrations in the SASS2400 sample fluid were estimated by liquid or gas chromatography, relative to standards.

Results

The wetted wall action of the sampler exposes a large area of the sample fluid to the sampled air flow and was very efficient in re-oxygenating the nitrogen sparged sample (FIG. 60). At the earliest time point that could be measured with this equipment, 80% saturation with oxygen was achieved within about 7 seconds and the process was complete in under 60 seconds.

Phenol was detected in the SASS2400 sample at the earliest time point measured (FIG. 61) and continued to accumulate in an approximately linear fashion with time up to the last sample point at 60 seconds.

Using this protocol, results obtained with acetaldehyde were unreliable with the concentration decreasing with using longer sampling times. The inventors attributed this to the very volatile nature of acetaldehyde and its propensity to degas rapidly from the sample reservoir.

Modified Equipment Setup

In order to improve the time resolution of experiments at early time points, the inventors modified the equipment to allow rapid re-direction of the input airflow after the SASS2400 fan was up to speed and the sample chamber had been filled, which takes up to about 12 seconds, usually about 9 seconds.

The fan in the SASS2400 is designed to draw in air from ambient around the device. Restricting the airflow through narrow or excessive lengths of plumbing could affect the designed airflow of 40 L/min and switching of the air path needs to be fast so the sampling times are consistent (FIG. 63). Solenoid valves or butterfly valves were considered less than ideal because of their effects on air-flow. A 3-way L port pneumatically operated ball valve (BLS3L6B) was chosen to allow rapid switching of air intake from room air to room air plus the volatile specimen (FIG. 60). The valve was connected with 1" BSP fittings for minimal constriction for the air flow and as it is a 3-way valve there was minimal additional plumbing required and the valve could be mounted very close to the SASS2400 air inlet. The valve was driven through a double acting solenoid and a 12 solenoid (ENS 1275) connected to a 6 Bar air supply.

A microcontroller circuit controlled the operation of the solenoid valve. The operating time is programmable and was set to 15 seconds. No digital output was available from the SASS2400 to synchronise the microcontroller so it was triggered by a manual push button activated at the start of the SASS2400 test cycle. The response of the 3-way valve was below one second.

All testing was done in a fume hood because of the nature of the volatile samples. Specimens could not simply be placed near the inlet of the 3-way valve as specimen concentration drawn into the SASS2400 may have varied with any air-flow change in the fume hood. A 1/4 inch pvc barb fitting was attached to the specimen inlet side of the solenoid (FIG. 62). A hole to mount a 2 ml safe-lock conical tube was drilled on the lower side of the PVC fitting 20 mm in from the end furthest from the solenoid. The air-flow at this point should be constant at 40 L/s due to the fan in the SASS2400. Specimens to be tested were placed in 1.7-2 ml safe-lock conical tubes with the lids removed. The conical tubes were filled to the upper rim at the start of each test. The constant surface area exposed to the air-flow should ensure a constant rate of evaporation within each test cycle.

Modified Test Procedure

All experiments were conducted in a fume hood. Personal protection equipment including gowns, gloves, shoe covers and a full face mask were used.

After powering up and establishing a computer connection, the SASS2400 was set to run for 20 seconds, drawing only from room air with no sample exposure, to flush the system. The solenoid and valves were not active at this stage. The solenoid and its control circuitry were powered up and several operations of the solenoid valve were run to ensure that air pressure was adequate for quick operation of the valve.

The SASS was programmed for the duration of the test run. This was the desired exposure time for sampling plus an addition fifteen seconds for initial fan start-up during which the 3-way air intake valve was switched away from the specimen.

A clean 8 mL sample bottle was placed in the collection position on the front of the sampler. 0.6 mL of de-ionised water was placed in a new 2 ml sample vial ready to take the sample after the test. Temperature, humidity and atmospheric pressure were recorded.

The lid was removed from a clean 2 mL safe-lock tube. Phenol specimens were placed in the safe lock tube, filling it as close as possible to the rim, before placing the tube in the mounting hole. For liquid specimens the tube was placed in its mount and then filled with specimen. Care was taken

to ensure that the liquid was filled to the rim of the specimen tube so that a consistent surface area of the liquid was exposed to the air-flow.

The SASS2400 and the delay trigger for the solenoid were activated simultaneously. After fifteen seconds the specimen was switched into the SASS2400 air intake. At the end of the sampling time, the fan was switched off and the sample was pumped to a 8 ml collection bottle on the front of the SASS2400 for 20 seconds to ensure that all of the sample was transferred to the sample bottle.

At the end of each test cycle the SASS2400 was programmed to run an internal peristaltic pump for 20 seconds to transfer the 1 mL test sample into an 8 ml bottle fitted to the front of the SASS2400. 0.8 mL of the sample was transferred from the collection bottle to the analysis vial and a further 0.6 mL of de-ionised water was used to fill the vial before it was sealed and sent for analysis. Tests were nm for acetaldehyde and phenol for sampling times from 5 seconds to 600 seconds and sent for chromatographic analysis.

Results Using New Procedure

Mean phenol concentration was 7.7 $\mu\text{g/mL}$ (i.e. ≈ 8 ppm v/v) in the SASS2400 sample after only 15 seconds exposure to ≈ 1 gram sample of phenol with a $\text{O}=\text{6}$ mm surface area. Phenol is an example of a highly volatile compound with a vapour pressure= 0.474×10^{-4} atmospheres at 20°C . Even after only a few seconds exposure, acetaldehyde concentrations in the sample vial were off-scale (i.e. \gg mg/L) demonstrating very rapid partition of acetaldehyde into the water. Rapid uptake and equilibration of these volatile organic compounds demonstrate the feasibility of the wetted wall cyclone as a gas-liquid transfer module prior to on-chip microfluidic detection.

Example 12—Additional GPCR Volatile Sensor Developed

The inventors previously described the construction of a BRET²-based diacetyl sensor by inserting RLuc or RLuc2 and GFP² domains into the sequence of the odr-10 diacetyl receptor from *C. elegans*. This sensor was expressed in *S. cerevisiae* and a crude membrane suspension was prepared and demonstrated to respond with exquisite sensitivity and selectivity for diacetyl in a plate based assay and also in the microfluidic format described in Example 3 above. As noted however, one of the advantages of the current invention is that multiple microfluidic sensor channels can be operated simultaneously in order to detect multiple individual analytes or, with appropriate selection of sensors, to provide a chemical fingerprint of a complex sample. To enable this it is necessary to derive a number of compatible volatile sensors with distinct specificities. The inventors therefore selected five additional putative chemoreceptor cDNAs from *C. elegans* as starting points for the engineering of novel BRET²-based sensors. The inventors also constructed a chimera between str-113 and str-114 in order to demonstrate the feasibility of deriving sensors that are synthetic molecular hybrids of naturally occurring receptors, with potentially novel ligand specificity that is not available readily from naturally occurring sequences.

SGSRs are chimaeras of *C. elegans* str-112, str-113, str-114, str-115, str-116 and str-114/113 with the BRET² tags GFP² and RLuc or RLuc2 inserted in the third intracellular loop and at the C-terminus, respectively. The positions of the third intracellular loops of STR proteins were predicted using "TMAP" an algorithm from "The Biology Workbench" (a web-based tool for prediction of transmembrane

segments <http://seqtool.sdsc.edu>). These were named SGSR-112, SGSR-113, SGSR-114/113, SGSR-114, SGSR-115 and SGSR-116.

Method for Design and Construction of BRET² Tagged *C. elegans* Str Odorant Receptors

Except for SGSR-112, which was commercially synthesised, SGSR expression cassettes were designed and made by introducing multiple restriction sites into the relevant gene-specific PCR primers. PCR products containing those sites were cloned into TOPO PCR vectors (Invitrogen) and then digested with the corresponding restriction enzymes (REs) and ligated into the expression cassettes. Some alterations were made to suit particular genes if they possessed one or more RE sites used by the cassettes.

RE sites for str fragment 1 were NcoI (5') and BspEI (3'), for GFP² are BspEI and SalI, for str fragment 2 are SalI and KpnI/EcoRI as EcoRI cuts Str116 fragment2, and, for *Renilla* luciferase, KpnI/EcoRI and NotI.

The SGSR 114/113 chimera was constructed by modifying *C. elegans* SGSR-113 (by replacing the first fragment of str-13, 113-1 using the restriction sites NcoI and BspEI in the cassette with the corresponding fragment of str-114, str-114-1). Str114-1 contains the first 720 str-114 nucleotides of, corresponding to its first 240 amino acids and was amplified by high fidelity PCR using primers incorporating the restriction sites, NcoI at the 5' end and BspEI at the 3' end.

All constructs were confirmed to be error free by restriction digestion and DNA sequencing.

The amino acid sequences of GFP² RLuc labelled SGSR-112, SGSR-113, SGSR-114, SGSR-115, SGSR-116 and SGSR-114/113 receptors are provided as SEQ ID NOs 13 to 18 respectively, whereas the corresponding open reading frames are provided as SEQ ID NOs 19 to 24 respectively. Results with Additional Six Sensors

All SGSR yeast membrane preps had strong GFP² and BRET² signals after induction by galactose at 15°C . for 72 hours and all of them showed changes in BRET² ratio when exposed to a medium conditioned with OP50 *E. coli* bacteria (a food source for *C. elegans*) compared to LB medium alone. The inventors selected a number of specific volatiles (including 1-hexanol, 1 butanol, butane-2,3-dione, 3-hydroxybutanone, 2-pentanone and 2 nonanone) for further testing based on GC-MS analysis of the headspace of OP50 bacteria grown on LB. The volatile ligand, 2-pentanone, tested positive for three of these sensors SGSR-112, SGSR-113 and SGSR-114/113 (FIG. 64). This is the first time that a volatile ligand (or indeed any ligand) has been identified for a BRET-based GPCR sensor, in the absence of prior knowledge of the ligand based on research with the unmodified parental GPCR. It is a demonstration of the utility of the BRET system for do-orphaning receptors generally and *C. elegans* chemoreceptors in particular.

Concentration-response characteristics (FIG. 65) indicate an EC₅₀ likely to be in the picomolar range. Not only does this reduce to practice the process of engineering, do-orphaning and characterising novel volatile sensors, it also demonstrates, at least in the case of SGSR-112 a viable method for do-orphaning the parental native receptors, the first time this has been achieved for almost 20 years.

The BRET² tagged SGSR-114/113 and SGSR-113 sensors responded to a range of volatile ligands including alcohols and ketones (FIG. 64). The inventors identified six volatile ligands for SGSR-114/113 and four for SGSR-113. The SGSR-112 response to 2-pentanone was linear over 9 log units from 1×10^{-14} M to 1×10^{-5} M with an EC₅₀ of 1.5×10^{-10} M (1.3 ppt) (FIG. 65). This broad concentration-

dependency is consistent with the response of the BRET² tagged ODR-10 which was also linear over 9 log units and also the response of the whole organism.

The inventors quantified the sensitivity of, SGSR-114/113 in vitro, for two of its ligands, 2-pentanone and diacetyl and of SGSR-113 to 1-hexanol (FIG. 66). The BRET² tagged Str114/113 receptor can detect parts per quadrillion (sub pM) levels of diacetyl and parts per billion levels (nM) levels of 2-pentanone and the Str-113 receptor can detect parts per billion (nM) levels of 1-hexanol. These would be particularly useful semi-broad sensors for use in the invention.

Construction of BRET² Tagged *C. elegans* Odorant Receptors with *RLuc2*

Following do-orphaning of the five additional natural and one chimaeric BRET² tagged sensors, which was accomplished in a plate based assay, the inventors incorporated the *RLuc2* mutations into each of them. This was required because, as described above, the *RLuc2* variant has been shown to be much brighter and therefore essential for practical use at a microfluidic scale.

The BRET² components were inserted into the third intracellular loop (IC3) and at the C-terminus of the *C. elegans* odorant receptor with green fluorescent protein, GFP² at IC3 and *Renilla* luciferase, *RLuc* at the C-terminus of the protein. Using site-directed mutagenesis the *RLuc2* mutations were introduced into the pYES-DEST-52 BRET² tagged odorant receptor sequence. Primers 1 and 2 (Table 3) were used to introduce the mutation C124A and primer pair 3 and 4 were used to introduce the M185 V mutation. The *RLuc2* mutations were introduced into all of the sensors based on OGOR, Str-112, Str-113, Str-114, Str-114/113, Str-115 and Str-116 as well as an additional model receptor called OGOR mutant which contains the original odr-10 mutation (H110Y) identified by Sengupta et al. (1996) that has previously been shown previously to be unresponsive to diacetyl.

The amino acid sequence of GFP² *RLuc2* labelled OGOR, OGOR mutant, SGSR-112, SGSR-113, SGSR-114, SGSR-114/113 SGSR-115 and SGSR-116 and receptors are provided as SEQ ID NOs 25 to 32 respectively, whereas the corresponding open reading frames are provided as SEQ ID NOs 33 to 40 respectively.

It will be appreciated by persons skilled in the art that numerous variations and/or modifications may be made to the invention as shown in the specific embodiments without departing from the spirit or scope of the invention as broadly described. The present embodiments are, therefore, to be considered in all respects as illustrative and not restrictive.

The present application claims priority from U.S. 61/624, 899 filed 16 Apr. 2012, and AU 2013204332 filed 12 Apr. 2013, the entire contents of both of which are incorporated herein by reference.

All publications discussed and/or referenced herein are incorporated herein in their entirety.

Any discussion of documents, acts, materials, devices, articles or the like which has been included in the present specification is solely for the purpose of providing a context for the present invention. It is not to be taken as an admission that any or all of these matters form part of the prior art base or were common general knowledge in the field relevant to the present invention as it existed before the priority date of each claim of this application.

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gagcaccaag acaagatcaa ggccatcgtc catgctgaga gtgctggtga cgtgatcgag 2340
tcctgggacg agtggcctga catcagggag gatatgccc tgatcaagag cgaagagggc 2400
gagaaaatgg tgcttgagaa taactcttc gtcgagaccg tgctcccaag caagatcatg 2460
cggaaaactg agcctgagga gttcgtgccc tacctggagc cattcaagga gaagggcgag 2520
gttagacggc ctaccctctc ctggcctcgc gagatccctc tcgttaaggg aggcaagccc 2580
gacgtcgtcc agattgtccg caactacaac gcctacctc gggccagcga cgatctgcct 2640
aagatgttca tcgagtccga cctggggtc ttttccaacg ctattgtcga gggagctaag 2700
aagttcccta acaccaggtt cgtgaagggt aaggccctcc acttcagcca ggaggacgct 2760
ccagatgaaa tgggtaagta catcaagagc ttcgtggagc gcgtgctgaa gaacgagcag 2820
taa 2823

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<210> SEQ ID NO 4

<211> LENGTH: 940

<212> TYPE: PRT

<213> ORGANISM: Artificial Sequence

<220> FEATURE:

<223> OTHER INFORMATION: GFP2-MBP-RLuc2 fusion protein

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<400> SEQUENCE: 4

Met Val Ser Lys Gly Glu Glu Leu Phe Thr Gly Val Val Pro Ile Leu
 1 5 10 15
 Val Glu Leu Asp Gly Asp Val Asn Gly His Lys Phe Ser Val Ser Gly
 20 25 30
 Glu Gly Glu Gly Asp Ala Thr Tyr Gly Lys Leu Thr Leu Lys Phe Ile
 35 40 45
 Cys Thr Thr Gly Lys Leu Pro Val Pro Trp Pro Thr Leu Val Thr Thr
 50 55 60
 Leu Ser Tyr Gly Val Gln Cys Phe Ser Arg Tyr Pro Asp His Met Lys
 65 70 75 80
 Gln His Asp Phe Phe Lys Ser Ala Met Pro Glu Gly Tyr Val Gln Glu
 85 90 95
 Arg Thr Ile Phe Phe Lys Asp Asp Gly Asn Tyr Lys Thr Arg Ala Glu
 100 105 110
 Val Lys Phe Glu Gly Asp Thr Leu Val Asn Arg Ile Glu Leu Lys Gly
 115 120 125
 Ile Asp Phe Lys Glu Asp Gly Asn Ile Leu Gly His Lys Leu Glu Tyr
 130 135 140
 Asn Tyr Asn Ser His Asn Val Tyr Ile Met Ala Asp Lys Gln Lys Asn
 145 150 155 160
 Gly Ile Lys Val Asn Phe Lys Ile Arg His Asn Ile Glu Asp Gly Ser
 165 170 175
 Val Gln Leu Ala Asp His Tyr Gln Gln Asn Thr Pro Ile Gly Asp Gly
 180 185 190
 Pro Val Leu Leu Pro Asp Asn His Tyr Leu Ser Thr Gln Ser Ala Leu
 195 200 205
 Ser Lys Asp Pro Asn Glu Lys Arg Asp His Met Val Leu Leu Glu Phe
 210 215 220
 Val Thr Ala Ala Gly Ile Thr Leu Gly Met Asp Glu Leu Tyr Lys Leu
 225 230 235 240
 Gln Gly Gly Thr Gly Gly Gly Met Lys Ile Glu Glu Gly Lys Leu Val
 245 250 255
 Ile Trp Ile Asn Gly Asp Lys Gly Tyr Asn Gly Leu Ala Glu Val Gly
 260 265 270
 Lys Lys Phe Glu Lys Asp Thr Gly Ile Lys Val Thr Val Glu His Pro
 275 280 285
 Asp Lys Leu Glu Glu Lys Phe Pro Gln Val Ala Ala Thr Gly Asp Gly
 290 295 300
 Pro Asp Ile Ile Phe Trp Ala His Asp Arg Phe Gly Gly Tyr Ala Gln
 305 310 315 320
 Ser Gly Leu Leu Ala Glu Ile Thr Pro Asp Lys Ala Phe Gln Asp Lys
 325 330 335
 Leu Tyr Pro Phe Thr Trp Asp Ala Val Arg Tyr Asn Gly Lys Leu Ile
 340 345 350
 Ala Tyr Pro Ile Ala Val Glu Ala Leu Ser Leu Ile Tyr Asn Lys Asp
 355 360 365
 Leu Leu Pro Asn Pro Pro Lys Thr Trp Glu Glu Ile Pro Ala Leu Asp
 370 375 380
 Lys Glu Leu Lys Ala Lys Gly Lys Ser Ala Leu Met Phe Asn Leu Gln
 385 390 395 400
 Glu Pro Tyr Phe Thr Trp Pro Leu Ile Ala Ala Asp Gly Gly Tyr Ala

-continued

405					410					415					
Phe	Lys	Tyr	Glu	Asn	Gly	Lys	Tyr	Asp	Ile	Lys	Asp	Val	Gly	Val	Asp
			420					425					430		
Asn	Ala	Gly	Ala	Lys	Ala	Gly	Leu	Thr	Phe	Leu	Val	Asp	Leu	Ile	Lys
		435					440					445			
Asn	Lys	His	Met	Asn	Ala	Asp	Thr	Asp	Tyr	Ser	Ile	Ala	Glu	Ala	Ala
		450				455						460			
Phe	Asn	Lys	Gly	Glu	Thr	Ala	Met	Thr	Ile	Asn	Gly	Pro	Trp	Ala	Trp
465					470					475					480
Ser	Asn	Ile	Asp	Thr	Ser	Lys	Val	Asn	Tyr	Gly	Val	Thr	Val	Leu	Pro
				485					490						495
Thr	Phe	Lys	Gly	Gln	Pro	Ser	Lys	Pro	Phe	Val	Gly	Val	Leu	Ser	Ala
			500					505					510		
Gly	Ile	Asn	Ala	Ala	Ser	Pro	Asn	Lys	Glu	Leu	Ala	Lys	Glu	Phe	Leu
		515					520						525		
Glu	Asn	Tyr	Leu	Leu	Thr	Asp	Glu	Gly	Leu	Glu	Ala	Val	Asn	Lys	Asp
530						535					540				
Lys	Pro	Leu	Gly	Ala	Val	Ala	Leu	Lys	Ser	Tyr	Glu	Glu	Glu	Leu	Val
545					550					555					560
Lys	Asp	Pro	Arg	Ile	Ala	Ala	Thr	Met	Glu	Asn	Ala	Gln	Lys	Gly	Glu
				565					570						575
Ile	Met	Pro	Asn	Ile	Pro	Gln	Met	Ser	Ala	Phe	Trp	Tyr	Ala	Val	Arg
			580					585						590	
Thr	Ala	Val	Ile	Asn	Ala	Ala	Ser	Gly	Arg	Gln	Thr	Val	Asp	Glu	Ala
		595					600						605		
Leu	Lys	Asp	Ala	Gln	Thr	Ala	Leu	Lys	Asp	Ala	Gln	Thr	Gly	Gly	Gly
610						615							620		
Thr	Gly	Gly	Phe	Glu	Met	Ala	Ser	Lys	Val	Tyr	Asp	Pro	Glu	Gln	Arg
625					630						635				640
Lys	Arg	Met	Ile	Thr	Gly	Pro	Gln	Trp	Trp	Ala	Arg	Cys	Lys	Gln	Met
				645					650						655
Asn	Val	Leu	Asp	Ser	Phe	Ile	Asn	Tyr	Tyr	Asp	Ser	Glu	Lys	His	Ala
			660					665						670	
Glu	Asn	Ala	Val	Ile	Phe	Leu	His	Gly	Asn	Ala	Ala	Ser	Ser	Tyr	Leu
		675					680						685		
Trp	Arg	His	Val	Val	Pro	His	Ile	Glu	Pro	Val	Ala	Arg	Cys	Ile	Ile
690						695					700				
Pro	Asp	Leu	Ile	Gly	Met	Gly	Lys	Ser	Gly	Lys	Ser	Gly	Asn	Gly	Ser
705					710					715					720
Tyr	Arg	Leu	Leu	Asp	His	Tyr	Lys	Tyr	Leu	Thr	Ala	Trp	Phe	Glu	Leu
				725					730						735
Leu	Asn	Leu	Pro	Lys	Lys	Ile	Ile	Phe	Val	Gly	His	Asp	Trp	Gly	Ala
			740					745						750	
Ala	Leu	Ala	Phe	His	Tyr	Ser	Tyr	Glu	His	Gln	Asp	Lys	Ile	Lys	Ala
		755					760						765		
Ile	Val	His	Ala	Glu	Ser	Val	Val	Asp	Val	Ile	Glu	Ser	Trp	Asp	Glu
	770					775					780				
Trp	Pro	Asp	Ile	Glu	Glu	Asp	Ile	Ala	Leu	Ile	Lys	Ser	Glu	Glu	Gly
785					790						795				800
Glu	Lys	Met	Val	Leu	Glu	Asn	Asn	Phe	Phe	Val	Glu	Thr	Val	Leu	Pro
				805						810					815
Ser	Lys	Ile	Met	Arg	Lys	Leu	Glu	Pro	Glu	Glu	Phe	Ala	Ala	Tyr	Leu
			820					825							830

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Glu Pro Phe Lys Glu Lys Gly Glu Val Arg Arg Pro Thr Leu Ser Trp
 835 840 845
 Pro Arg Glu Ile Pro Leu Val Lys Gly Gly Lys Pro Asp Val Val Gln
 850 855 860
 Ile Val Arg Asn Tyr Asn Ala Tyr Leu Arg Ala Ser Asp Asp Leu Pro
 865 870 875 880
 Lys Met Phe Ile Glu Ser Asp Pro Gly Phe Phe Ser Asn Ala Ile Val
 885 890 895
 Glu Gly Ala Lys Lys Phe Pro Asn Thr Glu Phe Val Lys Val Lys Gly
 900 905 910
 Leu His Phe Ser Gln Glu Asp Ala Pro Asp Glu Met Gly Lys Tyr Ile
 915 920 925
 Lys Ser Phe Val Glu Arg Val Leu Lys Asn Glu Gln
 930 935 940

<210> SEQ ID NO 5
 <211> LENGTH: 2823
 <212> TYPE: DNA
 <213> ORGANISM: Artificial Sequence
 <220> FEATURE:
 <223> OTHER INFORMATION: Nucleotide sequence encoding GFP2-MBP-RLuc2
 W140A fusion protein

<400> SEQUENCE: 5

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atggtgagca agggcgagga gctgttcacc ggggtggtgc ccacccctggt cgagctggac   60
ggcgacgtaa acggccacaa gtccagcgtg tccggcgagg gcgagggcga tgccacctac   120
ggcaagctga ccctgaagtt catctgcacc accggcaagc tgcccgtgcc ctggcccacc   180
ctcgtgacca ccctgagcta cggcgtgcag tgcttcagcc gctaccccga ccacatgaag   240
cagcacgact tcttcaagtc cgccatgccc gaaggctacg tccaggagcg caccatcttc   300
ttcaaggacg acggcaacta caagaccgcc gccgaggtga agttcgaggg cgacaccctg   360
gtgaaccgca tcgagctgaa gggcatcgac ttcaaggagg acggcaacat cctggggcac   420
aagctggagt acaactacaa cagccacaac gtctatatca tggccgacaa gcagaagaac   480
ggcatcaagg tgaacttcaa gatccgccac aacatcgagg acggcagcgt gcagctcgcc   540
gaccactacc agcagaacac ccccatcggc gacggccccg tgctgctgcc cgacaaccac   600
tacctgagca cccagtcgcc cctgagcaaa gaccccaacg agaagcgcga tcacatggtc   660
ctgctggagt tcgtgaccgc cgccggggtc actctcgcca tggacgagct gtacaagctg   720
cagggtggta ccggaggcgg catgaaaatc gaagaaggtg aactggtaat ctggattaac   780
ggcgataaag gctataacgg tctcgctgaa gtcggtaaga aattcgagaa agataccgga   840
attaaagtca ccgttgagca tccggataaa ctggaagaga aattcccaca ggttgccgca   900
actggcgatg gccctgacat tatcttctgg gcacacgacc gctttggtgg ctacgctcaa   960
tctggcctgt tggtgaaat caccgccggac aaagcgttcc aggacaagct gtatccgttt  1020
acctgggatg ccgtacgtta caacggcaag ctgattgctt acccgatcgc tgttgaagcg  1080
ttatcgctga tttataacaa agatctgctg ccgaacccgc caaaaacctg ggaagagatc  1140
ccggcgctgg ataaagaact gaaagcgaag ggtaagagcg cgctgatggt caacctgcaa  1200
gaaccgtact tcacctggcc gctgattgct gctgacgggg gttatgcggt caagtatgaa  1260
aacggcaagt acgacattaa agacgtgggc gtggataacg ctggcgcgaa agcgggtctg  1320
accttctcgg ttgacctgat taaaaacaaa cacatgaatg cagacaccga ttactccatc  1380

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gcagaagctg cctttaataa aggcgaaaca gcgatgacca tcaacggccc gtgggcatgg 1440
tccaacatcg acaccagcaa agtgaattat ggtgtaacgg tactgcccac cttcaagggt 1500
caaccatcca aaccgttcgt tggcgtgctg agcgcaggta ttaacgcgcg cagtccgaac 1560
aaagagctgg caaaagagtt cctcgaaaac tatctgctga ctgatgaagg tctggaagcg 1620
gttaataaag acaaacggct gggtgccgta gcgctgaagt cttacgagga agagttgggt 1680
aaagatccgc gtattgcccg cactatggaa aacgcccaga aagtgaaat catgccgaac 1740
atcccgcaga tgtccgcttt cgcgatgcc gtgcgtactg cggatgatcaa cgccgccagc 1800
ggtcgtcaga ctgctgatga agccctgaaa gacgcgcaga ctgccctgaa agacgcgcag 1860
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aaacgcatga tcaactggcc tcagtgggtg gctcgtgca agcaaatgaa cgtgctggac 1980
tccttcacca actactatga ttccgagaag cacgcccaga acgcccgtgat tttctgcat 2040
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agatgcatca tccctgatct gatcggaatg ggtaagtccg gcaagagcgg gaatggctca 2160
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aagaaaatca tctttgtggg ccacgactgg ggggctgctc tggccttca ctactcctac 2280
gagcaccaag acaagatcaa ggccatcgtc catgctgaga gtgtcgtgga cgtgatcgag 2340
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gagaaaatgg tgcttgagaa taacttcttc gtcgagacgg tgctcccaag caagatcatg 2460
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aagttcccta acaccgagtt cgtgaagggt aagggcctcc acttcagcca ggaggacgct 2760
ccagatgaaa tgggtaagta catcaagagc ttcgtggagc gcgtgctgaa gaacgagcag 2820
taa 2823

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<210> SEQ ID NO 6

<211> LENGTH: 940

<212> TYPE: PRT

<213> ORGANISM: Artificial Sequence

<220> FEATURE:

<223> OTHER INFORMATION: GFP2-MBP-RLuc2 W140A fusion protein

<400> SEQUENCE: 6

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Met Val Ser Lys Gly Glu Glu Leu Phe Thr Gly Val Val Pro Ile Leu
1           5           10           15
Val Glu Leu Asp Gly Asp Val Asn Gly His Lys Phe Ser Val Ser Gly
20          25          30
Glu Gly Glu Gly Asp Ala Thr Tyr Gly Lys Leu Thr Leu Lys Phe Ile
35          40          45
Cys Thr Thr Gly Lys Leu Pro Val Pro Trp Pro Thr Leu Val Thr Thr
50          55          60
Leu Ser Tyr Gly Val Gln Cys Phe Ser Arg Tyr Pro Asp His Met Lys
65          70          75          80
Gln His Asp Phe Phe Lys Ser Ala Met Pro Glu Gly Tyr Val Gln Glu
85          90          95
Arg Thr Ile Phe Phe Lys Asp Asp Gly Asn Tyr Lys Thr Arg Ala Glu

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100				105				110							
Val	Lys	Phe	Glu	Gly	Asp	Thr	Leu	Val	Asn	Arg	Ile	Glu	Leu	Lys	Gly
	115						120					125			
Ile	Asp	Phe	Lys	Glu	Asp	Gly	Asn	Ile	Leu	Gly	His	Lys	Leu	Glu	Tyr
	130					135					140				
Asn	Tyr	Asn	Ser	His	Asn	Val	Tyr	Ile	Met	Ala	Asp	Lys	Gln	Lys	Asn
	145				150					155					160
Gly	Ile	Lys	Val	Asn	Phe	Lys	Ile	Arg	His	Asn	Ile	Glu	Asp	Gly	Ser
				165					170					175	
Val	Gln	Leu	Ala	Asp	His	Tyr	Gln	Gln	Asn	Thr	Pro	Ile	Gly	Asp	Gly
			180					185					190		
Pro	Val	Leu	Leu	Pro	Asp	Asn	His	Tyr	Leu	Ser	Thr	Gln	Ser	Ala	Leu
		195					200						205		
Ser	Lys	Asp	Pro	Asn	Glu	Lys	Arg	Asp	His	Met	Val	Leu	Leu	Glu	Phe
	210					215					220				
Val	Thr	Ala	Ala	Gly	Ile	Thr	Leu	Gly	Met	Asp	Glu	Leu	Tyr	Lys	Leu
	225				230					235					240
Gln	Gly	Gly	Thr	Gly	Gly	Gly	Met	Lys	Ile	Glu	Glu	Gly	Lys	Leu	Val
				245					250					255	
Ile	Trp	Ile	Asn	Gly	Asp	Lys	Gly	Tyr	Asn	Gly	Leu	Ala	Glu	Val	Gly
			260					265						270	
Lys	Lys	Phe	Glu	Lys	Asp	Thr	Gly	Ile	Lys	Val	Thr	Val	Glu	His	Pro
		275					280					285			
Asp	Lys	Leu	Glu	Glu	Lys	Phe	Pro	Gln	Val	Ala	Ala	Thr	Gly	Asp	Gly
	290					295				300					
Pro	Asp	Ile	Ile	Phe	Trp	Ala	His	Asp	Arg	Phe	Gly	Gly	Tyr	Ala	Gln
	305				310					315					320
Ser	Gly	Leu	Leu	Ala	Glu	Ile	Thr	Pro	Asp	Lys	Ala	Phe	Gln	Asp	Lys
				325					330					335	
Leu	Tyr	Pro	Phe	Thr	Trp	Asp	Ala	Val	Arg	Tyr	Asn	Gly	Lys	Leu	Ile
			340					345						350	
Ala	Tyr	Pro	Ile	Ala	Val	Glu	Ala	Leu	Ser	Leu	Ile	Tyr	Asn	Lys	Asp
		355					360						365		
Leu	Leu	Pro	Asn	Pro	Pro	Lys	Thr	Trp	Glu	Glu	Ile	Pro	Ala	Leu	Asp
	370					375					380				
Lys	Glu	Leu	Lys	Ala	Lys	Gly	Lys	Ser	Ala	Leu	Met	Phe	Asn	Leu	Gln
	385				390					395					400
Glu	Pro	Tyr	Phe	Thr	Trp	Pro	Leu	Ile	Ala	Ala	Asp	Gly	Gly	Tyr	Ala
				405					410					415	
Phe	Lys	Tyr	Glu	Asn	Gly	Lys	Tyr	Asp	Ile	Lys	Asp	Val	Gly	Val	Asp
			420					425					430		
Asn	Ala	Gly	Ala	Lys	Ala	Gly	Leu	Thr	Phe	Leu	Val	Asp	Leu	Ile	Lys
		435					440						445		
Asn	Lys	His	Met	Asn	Ala	Asp	Thr	Asp	Tyr	Ser	Ile	Ala	Glu	Ala	Ala
	450					455					460				
Phe	Asn	Lys	Gly	Glu	Thr	Ala	Met	Thr	Ile	Asn	Gly	Pro	Trp	Ala	Trp
	465				470					475					480
Ser	Asn	Ile	Asp	Thr	Ser	Lys	Val	Asn	Tyr	Gly	Val	Thr	Val	Leu	Pro
				485					490					495	
Thr	Phe	Lys	Gly	Gln	Pro	Ser	Lys	Pro	Phe	Val	Gly	Val	Leu	Ser	Ala
			500						505				510		
Gly	Ile	Asn	Ala	Ala	Ser	Pro	Asn	Lys	Glu	Leu	Ala	Lys	Glu	Phe	Leu
		515					520						525		

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Glu Asn Tyr Leu Leu Thr Asp Glu Gly Leu Glu Ala Val Asn Lys Asp
 530 535 540

Lys Pro Leu Gly Ala Val Ala Leu Lys Ser Tyr Glu Glu Glu Leu Val
 545 550 555 560

Lys Asp Pro Arg Ile Ala Ala Thr Met Glu Asn Ala Gln Lys Gly Glu
 565 570 575

Ile Met Pro Asn Ile Pro Gln Met Ser Ala Phe Ala Tyr Ala Val Arg
 580 585 590

Thr Ala Val Ile Asn Ala Ala Ser Gly Arg Gln Thr Val Asp Glu Ala
 595 600 605

Leu Lys Asp Ala Gln Thr Ala Leu Lys Asp Ala Gln Thr Gly Gly Gly
 610 615 620

Thr Gly Gly Phe Glu Met Ala Ser Lys Val Tyr Asp Pro Glu Gln Arg
 625 630 635 640

Lys Arg Met Ile Thr Gly Pro Gln Trp Trp Ala Arg Cys Lys Gln Met
 645 650 655

Asn Val Leu Asp Ser Phe Ile Asn Tyr Tyr Asp Ser Glu Lys His Ala
 660 665 670

Glu Asn Ala Val Ile Phe Leu His Gly Asn Ala Ala Ser Ser Tyr Leu
 675 680 685

Trp Arg His Val Val Pro His Ile Glu Pro Val Ala Arg Cys Ile Ile
 690 695 700

Pro Asp Leu Ile Gly Met Gly Lys Ser Gly Lys Ser Gly Asn Gly Ser
 705 710 715 720

Tyr Arg Leu Leu Asp His Tyr Lys Tyr Leu Thr Ala Trp Phe Glu Leu
 725 730 735

Leu Asn Leu Pro Lys Lys Ile Ile Phe Val Gly His Asp Trp Gly Ala
 740 745 750

Ala Leu Ala Phe His Tyr Ser Tyr Glu His Gln Asp Lys Ile Lys Ala
 755 760 765

Ile Val His Ala Glu Ser Val Val Asp Val Ile Glu Ser Trp Asp Glu
 770 775 780

Trp Pro Asp Ile Glu Glu Asp Ile Ala Leu Ile Lys Ser Glu Glu Gly
 785 790 795 800

Glu Lys Met Val Leu Glu Asn Asn Phe Phe Val Glu Thr Val Leu Pro
 805 810 815

Ser Lys Ile Met Arg Lys Leu Glu Pro Glu Glu Phe Ala Ala Tyr Leu
 820 825 830

Glu Pro Phe Lys Glu Lys Gly Glu Val Arg Arg Pro Thr Leu Ser Trp
 835 840 845

Pro Arg Glu Ile Pro Leu Val Lys Gly Gly Lys Pro Asp Val Val Gln
 850 855 860

Ile Val Arg Asn Tyr Asn Ala Tyr Leu Arg Ala Ser Asp Asp Leu Pro
 865 870 875 880

Lys Met Phe Ile Glu Ser Asp Pro Gly Phe Phe Ser Asn Ala Ile Val
 885 890 895

Glu Gly Ala Lys Lys Phe Pro Asn Thr Glu Phe Val Lys Val Lys Gly
 900 905 910

Leu His Phe Ser Gln Glu Asp Ala Pro Asp Glu Met Gly Lys Tyr Ile
 915 920 925

Lys Ser Phe Val Glu Arg Val Leu Lys Asn Glu Gln
 930 935 940

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<210> SEQ ID NO 7
<211> LENGTH: 33
<212> TYPE: DNA
<213> ORGANISM: Artificial Sequence
<220> FEATURE:
<223> OTHER INFORMATION: Primer

<400> SEQUENCE: 7

cacgactggg ggcgcgcctt gcccttcac tac 33

<210> SEQ ID NO 8
<211> LENGTH: 33
<212> TYPE: DNA
<213> ORGANISM: Artificial Sequence
<220> FEATURE:
<223> OTHER INFORMATION: Primer

<400> SEQUENCE: 8

gtagtgaag gccagggcgc cccccagtc gtg 33

<210> SEQ ID NO 9
<211> LENGTH: 34
<212> TYPE: DNA
<213> ORGANISM: Artificial Sequence
<220> FEATURE:
<223> OTHER INFORMATION: Primer

<400> SEQUENCE: 9

cttcttctg gagaccgtgc tgcccagaa gatc 34

<210> SEQ ID NO 10
<211> LENGTH: 34
<212> TYPE: DNA
<213> ORGANISM: Artificial Sequence
<220> FEATURE:
<223> OTHER INFORMATION: Primer

<400> SEQUENCE: 10

gatcttgctg ggcagcagc tctccagaa gaag 34

<210> SEQ ID NO 11
<211> LENGTH: 32
<212> TYPE: DNA
<213> ORGANISM: Artificial Sequence
<220> FEATURE:
<223> OTHER INFORMATION: Primer

<400> SEQUENCE: 11

cagatgtccg cttctgcgta tgccgtgcgt ac 32

<210> SEQ ID NO 12
<211> LENGTH: 32
<212> TYPE: DNA
<213> ORGANISM: Artificial Sequence
<220> FEATURE:
<223> OTHER INFORMATION: Primer

<400> SEQUENCE: 12

gtacgcacgg catacgcgaa agcggacatc tg 32

<210> SEQ ID NO 13
<211> LENGTH: 896
<212> TYPE: PRT
<213> ORGANISM: Artificial Sequence
<220> FEATURE:
<223> OTHER INFORMATION: GFP2-str-112 SGSR-RLuc fusion protein

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<400> SEQUENCE: 13

Met Ser Gly Gln Leu Trp Leu Ala Leu Val Asp Ala Ala Asp Met Val
 1 5 10 15
 Gly Phe Thr Leu Thr Ile Ser Ile Asn Ile Ile Leu Leu Gly Leu Ile
 20 25 30
 Arg Thr Arg Gly Lys Thr Leu Gly Thr Tyr Lys Tyr Leu Met Ser Phe
 35 40 45
 Phe Ser Phe Phe Ser Ile Phe Tyr Ala Ile Val Glu Ser Ile Leu Arg
 50 55 60
 Pro Ile Met His Ile Glu Asn Thr Thr Phe Phe Leu Ile Ser Arg Lys
 65 70 75 80
 Arg Phe Asp Tyr Ser Thr Arg Leu Gly Lys Ile Asn Ser Ala Phe Tyr
 85 90 95
 Cys Ala Cys Phe Ala Thr Ser Phe Val Leu Ser Ala Val His Phe Val
 100 105 110
 Tyr Arg Tyr Phe Ala Ala Cys Lys Pro Asn Leu Leu Arg Leu Phe Asn
 115 120 125
 Leu Pro His Leu Leu Leu Trp Pro Leu Met Cys Ser Ile Pro Val Thr
 130 135 140
 Ala Trp Ala Ser Val Ser Tyr Phe Leu Tyr Pro Asp Thr Glu Tyr Thr
 145 150 155 160
 Glu Ala Ala Val Thr Tyr Val Leu Lys Thr His Tyr Glu Val Ile Lys
 165 170 175
 Lys Glu Asn Val Ser Tyr Ile Ala Tyr Val Tyr Tyr Gln Tyr Glu Asn
 180 185 190
 Gly Glu Arg His Ile Tyr Ile Lys Asn Leu Leu Gly Cys Phe Val His
 195 200 205
 Tyr Phe Val Met Ser Met Thr Phe Val Val Val Phe Tyr Cys Gly Phe
 210 215 220
 Ser Thr Trp Trp Thr Ile Arg Glu His Arg Gly Ala Ser Asp Arg Thr
 225 230 235 240
 Met Val Ser Lys Gly Glu Glu Leu Phe Thr Gly Val Val Pro Ile Leu
 245 250 255
 Val Glu Leu Asp Gly Asp Val Asn Gly His Lys Phe Ser Val Ser Gly
 260 265 270
 Glu Gly Glu Gly Asp Ala Thr Tyr Gly Lys Leu Thr Leu Lys Phe Ile
 275 280 285
 Cys Thr Thr Gly Lys Leu Pro Val Pro Trp Pro Thr Leu Val Thr Thr
 290 295 300
 Leu Thr Tyr Gly Val Gln Cys Phe Ser Arg Tyr Pro Asp His Met Lys
 305 310 315 320
 Gln His Asp Phe Phe Lys Ser Ala Met Pro Glu Gly Tyr Val Gln Glu
 325 330 335
 Arg Thr Ile Phe Phe Lys Asp Asp Gly Asn Tyr Lys Thr Arg Ala Glu
 340 345 350
 Val Lys Phe Glu Gly Asp Thr Leu Val Asn Arg Ile Glu Leu Lys Gly
 355 360 365
 Ile Asp Phe Lys Glu Asp Gly Asn Ile Leu Gly His Lys Leu Glu Tyr
 370 375 380
 Asn Tyr Asn Ser His Asn Val Tyr Ile Met Ala Asp Lys Gln Lys Asn
 385 390 395 400
 Gly Ile Lys Val Asn Phe Lys Ile Arg His Asn Ile Glu Asp Gly Ser

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405					410					415					
Val	Gln	Leu	Ala	Asp	His	Tyr	Gln	Gln	Asn	Thr	Pro	Ile	Gly	Asp	Gly
			420					425					430		
Pro	Val	Leu	Leu	Pro	Asp	Asn	His	Tyr	Leu	Ser	Thr	Gln	Ser	Ala	Leu
		435					440					445			
Ser	Lys	Asp	Pro	Asn	Glu	Lys	Arg	Asp	His	Met	Val	Leu	Leu	Glu	Phe
	450					455					460				
Val	Thr	Ala	Ala	Gly	Ile	Thr	Leu	Gly	Met	Asp	Glu	Leu	Tyr	Lys	Arg
465					470					475					480
His	Leu	His	Arg	Gln	Leu	Phe	Lys	Ala	Leu	Val	Phe	Gln	Thr	Leu	Val
				485					490						495
Pro	Ser	Ile	Phe	Met	Tyr	Ile	Pro	Thr	Gly	Val	Met	Phe	Ile	Ala	Pro
			500					505					510		
Phe	Phe	Asp	Ile	Asn	Leu	Asn	Ala	Asn	Ala	Asn	Phe	Ile	Val	Phe	Cys
		515					520					525			
Ser	Phe	Leu	Tyr	Pro	Gly	Leu	Asp	Pro	Leu	Ile	Leu	Ile	Phe	Ile	Ile
	530					535					540				
Arg	Glu	Phe	Arg	Val	Thr	Ile	Leu	Asn	Ile	Ile	Arg	Gly	Asn	Glu	Arg
545					550					555					560
Gly	Asn	Ala	Val	Gly	Glu	Ala	Tyr	Ser	Thr	Ser	Arg	Ile	Lys	Ser	Ser
				565					570						575
Gln	Pro	Ala	Ala	Val	Asn	Leu	Ser	Gly	Met	Thr	Ser	Lys	Val	Tyr	Asp
			580					585					590		
Pro	Glu	Gln	Arg	Lys	Arg	Met	Ile	Thr	Gly	Pro	Gln	Trp	Trp	Ala	Arg
		595					600					605			
Cys	Lys	Gln	Met	Asn	Val	Leu	Asp	Ser	Phe	Ile	Asn	Tyr	Tyr	Asp	Ser
	610					615					620				
Glu	Lys	His	Ala	Glu	Asn	Ala	Val	Ile	Phe	Leu	His	Gly	Asn	Ala	Ala
625					630					635					640
Ser	Ser	Tyr	Leu	Trp	Arg	His	Val	Val	Pro	His	Ile	Glu	Pro	Val	Ala
				645					650						655
Arg	Cys	Ile	Ile	Pro	Asp	Leu	Ile	Gly	Met	Gly	Lys	Ser	Gly	Lys	Ser
		660						665					670		
Gly	Asn	Gly	Ser	Tyr	Arg	Leu	Leu	Asp	His	Tyr	Lys	Tyr	Leu	Thr	Ala
		675					680						685		
Trp	Phe	Glu	Leu	Leu	Asn	Leu	Pro	Lys	Lys	Ile	Ile	Phe	Val	Gly	His
	690					695						700			
Asp	Trp	Gly	Ala	Cys	Leu	Ala	Phe	His	Tyr	Ser	Tyr	Glu	His	Gln	Asp
705					710					715					720
Lys	Ile	Lys	Ala	Ile	Val	His	Ala	Glu	Ser	Val	Val	Asp	Val	Ile	Glu
				725					730						735
Ser	Trp	Asp	Glu	Trp	Pro	Asp	Ile	Glu	Glu	Asp	Ile	Ala	Leu	Ile	Lys
			740					745					750		
Ser	Glu	Glu	Gly	Glu	Lys	Met	Val	Leu	Glu	Asn	Asn	Phe	Phe	Val	Glu
		755					760					765			
Thr	Met	Leu	Pro	Ser	Lys	Ile	Met	Arg	Lys	Leu	Glu	Pro	Glu	Glu	Phe
	770					775						780			
Ala	Ala	Tyr	Leu	Glu	Pro	Phe	Lys	Glu	Lys	Gly	Glu	Val	Arg	Arg	Pro
785					790					795					800
Thr	Leu	Ser	Trp	Pro	Arg	Glu	Ile	Pro	Leu	Val	Lys	Gly	Gly	Lys	Pro
				805					810						815
Asp	Val	Val	Gln	Ile	Val	Arg	Asn	Tyr	Asn	Ala	Tyr	Leu	Arg	Ala	Ser
			820					825							830

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Asp Asp Leu Pro Lys Met Phe Ile Glu Ser Asp Pro Gly Phe Phe Ser
 835 840 845

Asn Ala Ile Val Glu Gly Ala Lys Lys Phe Pro Asn Thr Glu Phe Val
 850 855 860

Lys Val Lys Gly Leu His Phe Ser Gln Glu Asp Ala Pro Asp Glu Met
 865 870 875 880

Gly Lys Tyr Ile Lys Ser Phe Val Glu Arg Val Leu Lys Asn Glu Gln
 885 890 895

<210> SEQ ID NO 14
 <211> LENGTH: 897
 <212> TYPE: PRT
 <213> ORGANISM: Artificial Sequence
 <220> FEATURE:
 <223> OTHER INFORMATION: GFP2-str-113 SGSR-RLuc fusion protein

<400> SEQUENCE: 14

Met Ser Asp Arg His Trp Leu Asp Ile Thr Thr Tyr Ser Asp His Ile
 1 5 10 15

Gly Phe Thr Ile Ser Thr Ile Ala Asn Phe Val Leu Ile Leu Leu Leu
 20 25 30

Val Phe Arg Pro Thr Lys Ser Tyr Gly Ser Tyr Lys Tyr Leu Met Ile
 35 40 45

Thr Phe Cys Val Phe Ser Leu Phe Tyr Thr Ser Ile Glu Thr Phe Leu
 50 55 60

Arg Pro Leu Ile His Ile Tyr Asp Asn Thr Ile Phe Val Ile Gln Arg
 65 70 75 80

Lys Arg Phe Gln Tyr Ser Glu Gly Thr Ala Arg Ala Ile Ser Ser Thr
 85 90 95

Tyr Cys Gly Cys Tyr Ala Met Ser Phe Thr Leu Phe Ala Val His Phe
 100 105 110

Val Tyr Arg Tyr Tyr Ala Ala Cys Lys Pro Asp Asn Leu Arg Tyr Phe
 115 120 125

Gln Gly Cys Tyr Phe Val Ala Trp Val Phe Gly Ala Met Ala Val Ala
 130 135 140

Ala Ser Trp Gly Phe Ala Ala Phe Ile Leu Tyr Pro Glu Thr Glu Arg
 145 150 155 160

Thr Arg Thr Ala Leu Ile His Val Ile Gln Thr Ser Tyr Glu Leu Asp
 165 170 175

Pro Glu Trp Val Gly Asn Val Pro Tyr Ser Tyr Trp Arg Thr Glu Asn
 180 185 190

Gly Val Glu Tyr Leu Asn Pro Arg Asn Val Ile Gly Ile Phe Gln His
 195 200 205

Gly Val Ile Met Ile Leu Ser Phe Gly Thr Val Phe Tyr Cys Gly Phe
 210 215 220

Asn Thr Tyr Lys Thr Leu Asn Gly Ser Leu Gly Val Ser Glu Lys Thr
 225 230 235 240

Ser Gly Met Val Ser Lys Gly Glu Glu Leu Phe Thr Gly Val Val Pro
 245 250 255

Ile Leu Val Glu Leu Asp Gly Asp Val Asn Gly His Lys Phe Ser Val
 260 265 270

Ser Gly Glu Gly Glu Gly Asp Ala Thr Tyr Gly Lys Leu Thr Leu Lys
 275 280 285

Phe Ile Cys Thr Thr Gly Lys Leu Pro Val Pro Trp Pro Thr Leu Val
 290 295 300

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Thr Thr Leu Ser Tyr Gly Val Gln Cys Phe Ser Arg Tyr Pro Asp His
 305 310 315 320
 Met Lys Gln His Asp Phe Phe Lys Ser Ala Met Pro Glu Gly Tyr Val
 325 330 335
 Gln Glu Arg Thr Ile Phe Phe Lys Asp Asp Gly Asn Tyr Lys Thr Arg
 340 345 350
 Ala Glu Val Lys Phe Glu Gly Asp Thr Leu Val Asn Arg Ile Glu Leu
 355 360 365
 Lys Gly Ile Asp Phe Lys Glu Asp Gly Asn Ile Leu Gly His Lys Leu
 370 375 380
 Glu Tyr Asn Tyr Asn Ser His Asn Val Tyr Ile Met Ala Asp Lys Gln
 385 390 395 400
 Lys Asn Gly Ile Lys Val Asn Phe Lys Ile Arg His Asn Ile Glu Asp
 405 410 415
 Gly Ser Val Gln Leu Ala Asp His Tyr Gln Gln Asn Thr Pro Ile Gly
 420 425 430
 Asp Gly Pro Val Leu Leu Pro Asp Asn His Tyr Leu Ser Thr Gln Ser
 435 440 445
 Ala Leu Ser Lys Asp Pro Asn Glu Lys Arg Asp His Met Val Leu Leu
 450 455 460
 Glu Phe Val Thr Ala Ala Gly Ile Thr Leu Gly Met Asp Glu Leu Tyr
 465 470 475 480
 Lys Val Asp Lys Glu Met His Thr Gln Leu Phe Lys Ala Leu Val Leu
 485 490 495
 Gln Thr Ile Ile Pro Thr Thr Leu Met Tyr Ile Pro Thr Thr Met Leu
 500 505 510
 Phe Val Thr Pro Phe Val Gly Leu Asn Ile Gly Cys Tyr Gly Asn Ile
 515 520 525
 Thr Thr Ala Thr Val His Leu Tyr Pro Gly Ile Asp Pro Val Val Leu
 530 535 540
 Ile Phe Ile Ile Arg Asp Phe Arg Gln Thr Ile Leu Arg Pro Phe Arg
 545 550 555 560
 Cys Phe Tyr Arg Ser Asn Ser Val Glu Asn Thr Ala Thr Ile Arg Gln
 565 570 575
 Tyr Gln Gln Ser Ser Ser Lys Gly Ser Arg Met Thr Ser Lys Val Tyr
 580 585 590
 Asp Pro Glu Gln Arg Lys Arg Met Ile Thr Gly Pro Gln Trp Trp Ala
 595 600 605
 Arg Cys Lys Gln Met Asn Val Leu Asp Ser Phe Ile Asn Tyr Tyr Asp
 610 615 620
 Ser Glu Lys His Ala Glu Asn Ala Val Ile Phe Leu His Gly Asn Ala
 625 630 635 640
 Ala Ser Ser Tyr Leu Trp Arg His Val Val Pro His Ile Glu Pro Val
 645 650 655
 Ala Arg Cys Ile Ile Pro Asp Leu Ile Gly Met Gly Lys Ser Gly Lys
 660 665 670
 Ser Gly Asn Gly Ser Tyr Arg Leu Leu Asp His Tyr Lys Tyr Leu Thr
 675 680 685
 Ala Trp Phe Glu Leu Leu Asn Leu Pro Lys Lys Ile Ile Phe Val Gly
 690 695 700
 His Asp Trp Gly Ala Cys Leu Ala Phe His Tyr Ser Tyr Glu His Gln
 705 710 715 720

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Asp Lys Ile Lys Ala Ile Val His Ala Glu Ser Val Val Asp Val Ile
      725                               730                735
Glu Ser Trp Asp Glu Trp Pro Asp Ile Glu Glu Asp Ile Ala Leu Ile
      740                               745                750
Lys Ser Glu Glu Gly Glu Lys Met Val Leu Glu Asn Asn Phe Phe Val
      755                               760                765
Glu Thr Met Leu Pro Ser Lys Ile Met Arg Lys Leu Glu Pro Glu Glu
      770                               775                780
Phe Ala Ala Tyr Leu Glu Pro Phe Lys Glu Lys Gly Glu Val Arg Arg
      785                               790                795                800
Pro Thr Leu Ser Trp Pro Arg Glu Ile Pro Leu Val Lys Gly Gly Lys
      805                               810                815
Pro Asp Val Val Gln Ile Val Arg Asn Tyr Asn Ala Tyr Leu Arg Ala
      820                               825                830
Ser Asp Asp Leu Pro Lys Met Phe Ile Glu Ser Asp Pro Gly Phe Phe
      835                               840                845
Ser Asn Ala Ile Val Glu Gly Ala Lys Lys Phe Pro Asn Thr Glu Phe
      850                               855                860
Val Lys Val Lys Gly Leu His Phe Ser Gln Glu Asp Ala Pro Asp Glu
      865                               870                875                880
Met Gly Lys Tyr Ile Lys Ser Phe Val Glu Arg Val Leu Lys Asn Glu
      885                               890                895

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Gln

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<210> SEQ ID NO 15
<211> LENGTH: 904
<212> TYPE: PRT
<213> ORGANISM: Artificial Sequence
<220> FEATURE:
<223> OTHER INFORMATION: GFP2-str-114 SGSR-RLuc fusion protein

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<400> SEQUENCE: 15

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Met Ser Asp Ile Tyr Trp Ile Gln Ile Thr Glu Val Cys Ser Phe Val
 1      5      10
Gly Phe Met Leu Ser Val Leu Gly Asn Ser Thr Leu Leu Val Leu Leu
 20      25      30
Ser Gly Lys Ser Ile Asp Gly Ile Gly Thr Tyr Arg Tyr Leu Met Ile
 35      40      45
Thr Phe Cys Val Phe Ser Leu Leu Phe Thr Ile Leu Glu Asp Phe Ile
 50      55      60
Arg Pro Leu Met His His Tyr Asn Asn Thr Ile Ile Val Leu Gln Arg
 65      70      75      80
Lys Arg Phe Gln Phe Ser Asp Ser Thr Ala Arg Ile Leu Thr Val Ser
 85      90      95
Tyr Cys Gly Cys Phe Ala Met Cys Phe Val Met Phe Ala Val His Phe
 100     105     110
Ile Tyr Arg Tyr Leu Val Ala Cys His Pro Thr Lys Leu His Tyr Phe
 115     120     125
Arg Pro Lys Asn Phe Ile Phe Trp Leu Ser Gly Met Leu Phe Ile Ala
 130     135     140
Gly Ser Trp Val Ala Ile Ala Tyr Val Phe Phe Gln Glu Asp Leu Glu
 145     150     155     160
Thr Arg Thr Asp Leu Val Phe Ile Leu Ser Thr Cys Tyr Asn Leu Thr
 165     170     175
Pro Asp Asp Val Gly His Val Pro Tyr Ala Phe Tyr Lys Thr Gln Gly

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180					185					190					
Asn	Thr	Arg	Val	Ile	Arg	Trp	Asp	Asn	Met	Ile	Gly	Val	Ile	His	His
		195					200					205			
Met	Ile	Val	Met	Thr	Ile	Ser	Ile	Ser	Ala	Val	Phe	Tyr	Phe	Gly	Ile
	210					215					220				
Lys	Thr	Tyr	Thr	Arg	Ile	Met	Ser	Phe	Lys	Gly	Lys	Ser	Gln	Lys	Thr
	225					230					235				240
Ser	Gly	Met	Val	Ser	Lys	Gly	Glu	Glu	Leu	Phe	Thr	Gly	Val	Val	Pro
				245					250					255	
Ile	Leu	Val	Glu	Leu	Asp	Gly	Asp	Val	Asn	Gly	His	Lys	Phe	Ser	Val
			260						265					270	
Ser	Gly	Glu	Gly	Glu	Gly	Asp	Ala	Thr	Tyr	Gly	Lys	Leu	Thr	Leu	Lys
		275						280					285		
Phe	Ile	Cys	Thr	Thr	Gly	Lys	Leu	Pro	Val	Pro	Trp	Pro	Thr	Leu	Val
	290					295					300				
Thr	Thr	Leu	Ser	Tyr	Gly	Val	Gln	Cys	Phe	Ser	Arg	Tyr	Pro	Asp	His
	305					310					315				320
Met	Lys	Gln	His	Asp	Phe	Phe	Lys	Ser	Ala	Met	Pro	Glu	Gly	Tyr	Val
				325					330					335	
Gln	Glu	Arg	Thr	Ile	Phe	Phe	Lys	Asp	Asp	Gly	Asn	Tyr	Lys	Thr	Arg
			340						345					350	
Ala	Glu	Val	Lys	Phe	Glu	Gly	Asp	Thr	Leu	Val	Asn	Arg	Ile	Glu	Leu
			355						360					365	
Lys	Gly	Ile	Asp	Phe	Lys	Glu	Asp	Gly	Asn	Ile	Leu	Gly	His	Lys	Leu
	370					375					380				
Glu	Tyr	Asn	Tyr	Asn	Ser	His	Asn	Val	Tyr	Ile	Met	Ala	Asp	Lys	Gln
	385					390					395				400
Lys	Asn	Gly	Ile	Lys	Val	Asn	Phe	Lys	Ile	Arg	His	Asn	Ile	Glu	Asp
				405					410					415	
Gly	Ser	Val	Gln	Leu	Ala	Asp	His	Tyr	Gln	Gln	Asn	Thr	Pro	Ile	Gly
			420						425					430	
Asp	Gly	Pro	Val	Leu	Leu	Pro	Asp	Asn	His	Tyr	Leu	Ser	Thr	Gln	Ser
		435							440					445	
Ala	Leu	Ser	Lys	Asp	Pro	Asn	Glu	Lys	Arg	Asp	His	Met	Val	Leu	Leu
	450								455					460	
Glu	Phe	Val	Thr	Ala	Ala	Gly	Ile	Thr	Leu	Gly	Met	Asp	Glu	Leu	Tyr
	465								470					475	480
Lys	Val	Asp	Lys	Asp	Leu	Gln	Asn	Gln	Phe	Phe	Thr	Ala	Leu	Val	Ala
				485					490					495	
Gln	Thr	Val	Val	Pro	Leu	Ile	Phe	Met	Phe	Ile	Pro	Asn	Met	Val	Leu
			500						505					510	
Thr	Thr	Ala	Ala	Leu	Ile	Asp	Gly	Thr	Phe	Gly	Ser	Trp	Ala	Asn	Ile
		515							520					525	
Thr	Val	Val	Met	Asn	His	Leu	Tyr	Pro	Ala	Ala	Asp	Pro	Phe	Val	Ile
	530								535					540	
Leu	Phe	Ile	Ile	Lys	Gly	Phe	Arg	Asn	Ser	Ile	Arg	Asn	Val	Ile	Tyr
	545					550					555				560
Arg	Cys	Thr	Lys	Thr	Lys	Lys	Ala	Ser	Val	Ser	Ser	Val	Val	Arg	Gly
				565					570					575	
Ile	Glu	Ala	Gln	Ser	Lys	Lys	Gln	Ser	Phe	Ser	Arg	Val	Asp	Ile	Ser
			580						585					590	
Arg	Met	Thr	Ser	Lys	Val	Tyr	Asp	Pro	Glu	Gln	Arg	Lys	Arg	Met	Ile
				595					600					605	

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Thr Gly Pro Gln Trp Trp Ala Arg Cys Lys Gln Met Asn Val Leu Asp
 610 615 620

Ser Phe Ile Asn Tyr Tyr Asp Ser Glu Lys His Ala Glu Asn Ala Val
 625 630 635 640

Ile Phe Leu His Gly Asn Ala Ala Ser Ser Tyr Leu Trp Arg His Val
 645 650 655

Val Pro His Ile Glu Pro Val Ala Arg Cys Ile Ile Pro Asp Leu Ile
 660 665 670

Gly Met Gly Lys Ser Gly Lys Ser Gly Asn Gly Ser Tyr Arg Leu Leu
 675 680 685

Asp His Tyr Lys Tyr Leu Thr Ala Trp Phe Glu Leu Leu Asn Leu Pro
 690 695 700

Lys Lys Ile Ile Phe Val Gly His Asp Trp Gly Ala Cys Leu Ala Phe
 705 710 715 720

His Tyr Ser Tyr Glu His Gln Asp Lys Ile Lys Ala Ile Val His Ala
 725 730 735

Glu Ser Val Val Asp Val Ile Glu Ser Trp Asp Glu Trp Pro Asp Ile
 740 745 750

Glu Glu Asp Ile Ala Leu Ile Lys Ser Glu Glu Gly Glu Lys Met Val
 755 760 765

Leu Glu Asn Asn Phe Phe Val Glu Thr Met Leu Pro Ser Lys Ile Met
 770 775 780

Arg Lys Leu Glu Pro Glu Glu Phe Ala Ala Tyr Leu Glu Pro Phe Lys
 785 790 795 800

Glu Lys Gly Glu Val Arg Arg Pro Thr Leu Ser Trp Pro Arg Glu Ile
 805 810 815

Pro Leu Val Lys Gly Gly Lys Pro Asp Val Val Gln Ile Val Arg Asn
 820 825 830

Tyr Asn Ala Tyr Leu Arg Ala Ser Asp Asp Leu Pro Lys Met Phe Ile
 835 840 845

Glu Ser Asp Pro Gly Phe Phe Ser Asn Ala Ile Val Glu Gly Ala Lys
 850 855 860

Lys Phe Pro Asn Thr Glu Phe Val Lys Val Lys Gly Leu His Phe Ser
 865 870 875 880

Gln Glu Asp Ala Pro Asp Glu Met Gly Lys Tyr Ile Lys Ser Phe Val
 885 890 895

Glu Arg Val Leu Lys Asn Glu Gln
 900

<210> SEQ ID NO 16
 <211> LENGTH: 890
 <212> TYPE: PRT
 <213> ORGANISM: Artificial Sequence
 <220> FEATURE:
 <223> OTHER INFORMATION: GFP2-str-115 SGSR-RLuc fusion protein

<400> SEQUENCE: 16

Met Thr Asp Gln His Trp Val Ile Ile Thr Asp Ile Ala Gly Pro Ile
 1 5 10 15

Gly Phe Ser Met Ser Ile Phe Ser Asn Ser Ile Leu Leu Phe Leu Ile
 20 25 30

Phe Ser His Ser Ser Pro Ile Lys Gly Pro Tyr Lys Arg Met Leu Ile
 35 40 45

Val Phe Cys Ile Phe Thr Val Phe Tyr Ser Phe Val Glu Val Met Leu
 50 55 60

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Gln Pro Leu Ile His Ile Tyr Asp Asp Thr Leu Phe Leu Ile His Arg
 65 70 75 80
 Lys Arg Ile Asp Leu Pro Lys Trp Leu Thr Arg Leu Val Pro Thr Thr
 85 90 95
 Tyr Cys Trp Cys Tyr Ala Met Ser Phe Ser Leu Phe Ala Leu Gln Phe
 100 105 110
 Leu Tyr Arg Tyr Val Ala Val Cys Lys Pro Gln Tyr Val Asp Leu Phe
 115 120 125
 Val Gly Cys His Phe Tyr Ala Trp Val Val Leu Ile Leu Ser Leu Ala
 130 135 140
 Thr Ser Trp Gly Leu Thr Ala Ala Phe Met Phe Pro Gln Thr Asp Arg
 145 150 155 160
 Thr Thr Glu Ile Phe Leu His Ile Ile Tyr Ser Ser Tyr Asp Leu Glu
 165 170 175
 Pro Tyr Trp Thr Asp Tyr Val Ala Tyr Lys Tyr Phe Asp Thr Asp Glu
 180 185 190
 Asn Asn Val Arg Trp Val Asn Val Leu Ser Phe Phe Gly Val Leu Gln
 195 200 205
 His Gly Ile Val Ile Thr Leu Ser Phe Gly Thr Leu Tyr Tyr Cys Gly
 210 215 220
 Ile Asn Thr Tyr Leu Lys Ile Lys Lys His Thr Gly Thr Ser Asn Arg
 225 230 235 240
 Thr Ser Gly Met Val Ser Lys Gly Glu Glu Leu Phe Thr Gly Val Val
 245 250 255
 Pro Ile Leu Val Glu Leu Asp Gly Asp Val Asn Gly His Lys Phe Ser
 260 265 270
 Val Ser Gly Glu Gly Glu Gly Asp Ala Thr Tyr Gly Lys Leu Thr Leu
 275 280 285
 Lys Phe Ile Cys Thr Thr Gly Lys Leu Pro Val Pro Trp Pro Thr Leu
 290 295 300
 Val Thr Thr Leu Ser Tyr Gly Val Gln Cys Phe Ser Arg Tyr Pro Asp
 305 310 315 320
 His Met Lys Gln His Asp Phe Phe Lys Ser Ala Met Pro Glu Gly Tyr
 325 330 335
 Val Gln Glu Arg Thr Ile Phe Phe Lys Asp Asp Gly Asn Tyr Lys Thr
 340 345 350
 Arg Ala Glu Val Lys Phe Glu Gly Asp Thr Leu Val Asn Arg Ile Glu
 355 360 365
 Leu Lys Gly Ile Asp Phe Lys Glu Asp Gly Asn Ile Leu Gly His Lys
 370 375 380
 Leu Glu Tyr Asn Tyr Asn Ser His Asn Val Tyr Ile Met Ala Asp Lys
 385 390 395 400
 Gln Lys Asn Gly Ile Lys Val Asn Phe Lys Ile Arg His Asn Ile Glu
 405 410 415
 Asp Gly Ser Val Gln Leu Ala Asp His Tyr Gln Gln Asn Thr Pro Ile
 420 425 430
 Gly Asp Gly Pro Val Leu Leu Pro Asp Asn His Tyr Leu Ser Thr Gln
 435 440 445
 Ser Ala Leu Ser Lys Asp Pro Asn Glu Lys Arg Asp His Met Val Leu
 450 455 460
 Leu Glu Phe Val Thr Ala Ala Gly Ile Thr Leu Gly Met Asp Glu Leu
 465 470 475 480

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Tyr Lys Val Asp Arg Cys Ile Gln Leu Gln Leu Phe Arg Ala Leu Val
 485 490 495
 Ala Gln Thr Ile Leu Pro Met Phe Met Met Tyr Ile Pro Val Gly Phe
 500 505 510
 Met Phe Ala Cys Pro Tyr Phe Asp Leu Gln Leu Gly Ala Tyr Thr Asn
 515 520 525
 Tyr Gln Thr Val Met Ala Gln Leu Tyr Pro Gly Ile Asp Pro Phe Val
 530 535 540
 Met Leu Phe Leu Ile Asp Ser Tyr Arg Ile Thr Ile Phe Gly Trp Leu
 545 550 555 560
 Cys Pro Arg Phe Val Tyr Val Lys Pro Met His Ser Thr Tyr Thr Leu
 565 570 575
 Thr Ser Arg Met Thr Ser Lys Val Tyr Asp Pro Glu Gln Arg Lys Arg
 580 585 590
 Met Ile Thr Gly Pro Gln Trp Trp Ala Arg Cys Lys Gln Met Asn Val
 595 600 605
 Leu Asp Ser Phe Ile Asn Tyr Tyr Asp Ser Glu Lys His Ala Glu Asn
 610 615 620
 Ala Val Ile Phe Leu His Gly Asn Ala Ala Ser Ser Tyr Leu Trp Arg
 625 630 635 640
 His Val Val Pro His Ile Glu Pro Val Ala Arg Cys Ile Ile Pro Asp
 645 650 655
 Leu Ile Gly Met Gly Lys Ser Gly Lys Ser Gly Asn Gly Ser Tyr Arg
 660 665 670
 Leu Leu Asp His Tyr Lys Tyr Leu Thr Ala Trp Phe Glu Leu Leu Asn
 675 680 685
 Leu Pro Lys Lys Ile Ile Phe Val Gly His Asp Trp Gly Ala Cys Leu
 690 695 700
 Ala Phe His Tyr Ser Tyr Glu His Gln Asp Lys Ile Lys Ala Ile Val
 705 710 715 720
 His Ala Glu Ser Val Val Asp Val Ile Glu Ser Trp Asp Glu Trp Pro
 725 730 735
 Asp Ile Glu Glu Asp Ile Ala Leu Ile Lys Ser Glu Glu Gly Glu Lys
 740 745 750
 Met Val Leu Glu Asn Asn Phe Phe Val Glu Thr Met Leu Pro Ser Lys
 755 760 765
 Ile Met Arg Lys Leu Glu Pro Glu Glu Phe Ala Ala Tyr Leu Glu Pro
 770 775 780
 Phe Lys Glu Lys Gly Glu Val Arg Arg Pro Thr Leu Ser Trp Pro Arg
 785 790 795 800
 Glu Ile Pro Leu Val Lys Gly Gly Lys Pro Asp Val Val Gln Ile Val
 805 810 815
 Arg Asn Tyr Asn Ala Tyr Leu Arg Ala Ser Asp Asp Leu Pro Lys Met
 820 825 830
 Phe Ile Glu Ser Asp Pro Gly Phe Phe Ser Asn Ala Ile Val Glu Gly
 835 840 845
 Ala Lys Lys Phe Pro Asn Thr Glu Phe Val Lys Val Lys Gly Leu His
 850 855 860
 Phe Ser Gln Glu Asp Ala Pro Asp Glu Met Gly Lys Tyr Ile Lys Ser
 865 870 875 880
 Phe Val Glu Arg Val Leu Lys Asn Glu Gln
 885 890

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<210> SEQ ID NO 17
<211> LENGTH: 906
<212> TYPE: PRT
<213> ORGANISM: Artificial Sequence
<220> FEATURE:
<223> OTHER INFORMATION: GFP2-str-116 SGSR-RLuc fusion protein

<400> SEQUENCE: 17

Met Thr Asp Arg Arg Trp Val Ala Ile Thr Asp Ile Ala Gly Pro Ile
1          5          10          15
Gly Phe Thr Met Ser Ile Phe Ser Asn Ser Val Leu Leu Ser Leu Ile
20          25          30
Phe Ser Ser Ser Ser Pro Ile Lys Gly Ala Tyr Lys Asn Met Leu Ile
35          40          45
Val Leu Cys Ile Phe Thr Met Phe Tyr Ser Phe Val Glu Ile Met Leu
50          55          60
Gln Pro Leu Ile His Ile Tyr Asp Asp Thr Leu Phe Leu Ile His Arg
65          70          75          80
Lys Arg Phe Asp Leu Ser Lys Gly Ile Thr Arg Leu Ile Pro Thr Thr
85          90          95
Tyr Cys Trp Cys Tyr Ala Met Ser Phe Ser Leu Phe Ala Leu Gln Phe
100         105         110
Leu Tyr Arg Tyr Val Ala Val Cys Lys Pro His Leu Val Val Phe Phe
115         120         125
Thr Gly Cys Tyr Phe Tyr Tyr Trp Leu Ala Leu Ile Leu Ser Leu Ala
130         135         140
Thr Ser Trp Gly Leu Thr Ala Ala Phe Met Phe Pro Gln Thr Asn Arg
145         150         155         160
Thr Thr Glu Ser Phe Asn Tyr Val Ile Lys Thr Ser Tyr Asp Leu Asp
165         170         175
Pro Tyr Trp Thr Asp Tyr Val Ala Tyr Lys Tyr Phe Asp Thr Asp Glu
180         185         190
Asn His Val Arg Trp Val Asn Val Leu Ser Leu Phe Gly Val Leu Gln
195         200         205
His Gly Leu Val Ile Thr Leu Ser Phe Gly Thr Leu Phe Tyr Cys Gly
210         215         220
Ile Lys Thr Tyr Leu Ser Ile Thr Glu His Val Gly Met Ser Ser Lys
225         230         235         240
Thr Ser Gly Met Val Ser Lys Gly Glu Glu Leu Phe Thr Gly Val Val
245         250         255
Pro Ile Leu Val Glu Leu Asp Gly Asp Val Asn Gly His Lys Phe Ser
260         265         270
Val Ser Gly Glu Gly Glu Gly Asp Ala Thr Tyr Gly Lys Leu Thr Leu
275         280         285
Lys Phe Ile Cys Thr Thr Gly Lys Leu Pro Val Pro Trp Pro Thr Leu
290         295         300
Val Thr Thr Leu Ser Tyr Gly Val Gln Cys Phe Ser Arg Tyr Pro Asp
305         310         315         320
His Met Lys Gln His Asp Phe Phe Lys Ser Ala Met Pro Glu Gly Tyr
325         330         335
Val Gln Glu Arg Thr Ile Phe Phe Lys Asp Asp Gly Asn Tyr Lys Thr
340         345         350
Arg Ala Glu Val Lys Phe Glu Gly Asp Thr Leu Val Asn Arg Ile Glu
355         360         365
Leu Lys Gly Ile Asp Phe Lys Glu Asp Gly Asn Ile Leu Gly His Lys

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370					375					380					
Leu	Glu	Tyr	Asn	Tyr	Asn	Ser	His	Asn	Val	Tyr	Ile	Met	Ala	Asp	Lys
385					390					395					400
Gln	Lys	Asn	Gly	Ile	Lys	Val	Asn	Phe	Lys	Ile	Arg	His	Asn	Ile	Glu
			405						410					415	
Asp	Gly	Ser	Val	Gln	Leu	Ala	Asp	His	Tyr	Gln	Gln	Asn	Thr	Pro	Ile
			420					425						430	
Gly	Asp	Gly	Pro	Val	Leu	Leu	Pro	Asp	Asn	His	Tyr	Leu	Ser	Thr	Gln
		435					440						445		
Ser	Ala	Leu	Ser	Lys	Asp	Pro	Asn	Glu	Lys	Arg	Asp	His	Met	Val	Leu
		450				455						460			
Leu	Glu	Phe	Val	Thr	Ala	Ala	Gly	Ile	Thr	Leu	Gly	Met	Asp	Glu	Leu
465					470					475					480
Tyr	Lys	Val	Asp	Arg	Ser	Leu	Gln	Leu	Gln	Leu	Phe	Arg	Ala	Leu	Val
				485					490						495
Ala	Gln	Thr	Cys	Leu	Pro	Met	Leu	Met	Met	Tyr	Met	Pro	Ile	Gly	Phe
			500					505						510	
Met	Phe	Ser	Cys	Pro	Tyr	Phe	Asp	Leu	Gln	Leu	Gly	Ala	Val	Thr	Asn
		515					520						525		
Tyr	Gln	Thr	Val	Met	Ala	Gln	Leu	Tyr	Pro	Gly	Ile	Asp	Pro	Phe	Met
		530				535						540			
Leu	Leu	Phe	Leu	Ile	Asn	Ala	Tyr	Arg	Lys	Thr	Val	Leu	Ser	Leu	Ile
545					550						555				560
Cys	Pro	Asn	Phe	Ile	Gln	Lys	Lys	Tyr	Val	Gln	Thr	Ala	Thr	Thr	Arg
				565					570						575
Asp	Gly	Thr	Asp	Ala	Ser	Ala	Thr	Met	Asn	Ser	Val	Lys	Ser	Thr	Gln
			580					585						590	
Leu	Ser	Arg	Met	Thr	Ser	Lys	Val	Tyr	Asp	Pro	Glu	Gln	Arg	Lys	Arg
		595					600						605		
Met	Ile	Thr	Gly	Pro	Gln	Trp	Trp	Ala	Arg	Cys	Lys	Gln	Met	Asn	Val
		610				615							620		
Leu	Asp	Ser	Phe	Ile	Asn	Tyr	Tyr	Asp	Ser	Glu	Lys	His	Ala	Glu	Asn
625					630					635					640
Ala	Val	Ile	Phe	Leu	His	Gly	Asn	Ala	Ala	Ser	Ser	Tyr	Leu	Trp	Arg
				645					650						655
His	Val	Val	Pro	His	Ile	Glu	Pro	Val	Ala	Arg	Cys	Ile	Ile	Pro	Asp
			660						665					670	
Leu	Ile	Gly	Met	Gly	Lys	Ser	Gly	Lys	Ser	Gly	Asn	Gly	Ser	Tyr	Arg
		675					680						685		
Leu	Leu	Asp	His	Tyr	Lys	Tyr	Leu	Thr	Ala	Trp	Phe	Glu	Leu	Leu	Asn
		690				695							700		
Leu	Pro	Lys	Lys	Ile	Ile	Phe	Val	Gly	His	Asp	Trp	Gly	Ala	Cys	Leu
705					710					715					720
Ala	Phe	His	Tyr	Ser	Tyr	Glu	His	Gln	Asp	Lys	Ile	Lys	Ala	Ile	Val
				725						730					735
His	Ala	Glu	Ser	Val	Val	Asp	Val	Ile	Glu	Ser	Trp	Asp	Glu	Trp	Pro
			740						745					750	
Asp	Ile	Glu	Glu	Asp	Ile	Ala	Leu	Ile	Lys	Ser	Glu	Glu	Gly	Glu	Lys
		755					760							765	
Met	Val	Leu	Glu	Asn	Asn	Phe	Phe	Val	Glu	Thr	Met	Leu	Pro	Ser	Lys
		770					775						780		
Ile	Met	Arg	Lys	Leu	Glu	Pro	Glu	Glu	Phe	Ala	Ala	Tyr	Leu	Glu	Pro
785					790					795					800

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Phe Lys Glu Lys Gly Glu Val Arg Arg Pro Thr Leu Ser Trp Pro Arg
805 810 815

Glu Ile Pro Leu Val Lys Gly Gly Lys Pro Asp Val Val Gln Ile Val
820 825 830

Arg Asn Tyr Asn Ala Tyr Leu Arg Ala Ser Asp Asp Leu Pro Lys Met
835 840 845

Phe Ile Glu Ser Asp Pro Gly Phe Phe Ser Asn Ala Ile Val Glu Gly
850 855 860

Ala Lys Lys Phe Pro Asn Thr Glu Phe Val Lys Val Lys Gly Leu His
865 870 875 880

Phe Ser Gln Glu Asp Ala Pro Asp Glu Met Gly Lys Tyr Ile Lys Ser
885 890 895

Phe Val Glu Arg Val Leu Lys Asn Glu Gln
900 905

<210> SEQ ID NO 18
<211> LENGTH: 901
<212> TYPE: PRT
<213> ORGANISM: Artificial Sequence
<220> FEATURE:
<223> OTHER INFORMATION: GFP2-str-113/114 SGSR-RLuc fusion protein

<400> SEQUENCE: 18

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Gly Phe Met Leu Ser Val Leu Gly Asn Ser Thr Leu Leu Val Leu Leu
20 25 30

Ser Gly Lys Ser Ile Asp Gly Ile Gly Thr Tyr Arg Tyr Leu Met Ile
35 40 45

Thr Phe Cys Val Phe Ser Leu Leu Phe Thr Ile Leu Glu Asp Phe Ile
50 55 60

Arg Pro Leu Met His His Tyr Asn Asn Thr Ile Ile Val Leu Gln Arg
65 70 75 80

Lys Arg Phe Gln Phe Ser Asp Ser Thr Ala Arg Ile Leu Thr Val Ser
85 90 95

Tyr Cys Gly Cys Phe Ala Met Cys Phe Val Met Phe Ala Val His Phe
100 105 110

Ile Tyr Arg Tyr Leu Val Ala Cys His Pro Thr Lys Leu His Tyr Phe
115 120 125

Arg Pro Lys Asn Phe Ile Phe Trp Leu Ser Gly Met Leu Phe Ile Ala
130 135 140

Gly Ser Trp Val Ala Ile Ala Tyr Val Phe Phe Gln Glu Asp Leu Glu
145 150 155 160

Thr Arg Thr Asp Leu Val Phe Ile Leu Ser Thr Cys Tyr Asn Leu Thr
165 170 175

Pro Asp Asp Val Gly His Val Pro Tyr Ala Phe Tyr Lys Thr Gln Gly
180 185 190

Asn Thr Arg Val Ile Arg Trp Asp Asn Met Ile Gly Val Ile His His
195 200 205

Met Ile Val Met Thr Ile Ser Ile Ser Ala Val Phe Tyr Phe Gly Ile
210 215 220

Lys Thr Tyr Thr Arg Ile Met Ser Phe Lys Gly Lys Ser Gln Lys Thr
225 230 235 240

Ser Gly Met Val Ser Lys Gly Glu Glu Leu Phe Thr Gly Val Val Pro
245 250 255

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Ile Leu Val Glu Leu Asp Gly Asp Val Asn Gly His Lys Phe Ser Val
 260 265 270
 Ser Gly Glu Gly Glu Gly Asp Ala Thr Tyr Gly Lys Leu Thr Leu Lys
 275 280 285
 Phe Ile Cys Thr Thr Gly Lys Leu Pro Val Pro Trp Pro Thr Leu Val
 290 295 300
 Thr Thr Leu Ser Tyr Gly Val Gln Cys Phe Ser Arg Tyr Pro Asp His
 305 310 315 320
 Met Lys Gln His Asp Phe Phe Lys Ser Ala Met Pro Glu Gly Tyr Val
 325 330 335
 Gln Glu Arg Thr Ile Phe Phe Lys Asp Asp Gly Asn Tyr Lys Thr Arg
 340 345 350
 Ala Glu Val Lys Phe Glu Gly Asp Thr Leu Val Asn Arg Ile Glu Leu
 355 360 365
 Lys Gly Ile Asp Phe Lys Glu Asp Gly Asn Ile Leu Gly His Lys Leu
 370 375 380
 Glu Tyr Asn Tyr Asn Ser His Asn Val Tyr Ile Met Ala Asp Lys Gln
 385 390 395 400
 Lys Asn Gly Ile Lys Val Asn Phe Lys Ile Arg His Asn Ile Glu Asp
 405 410 415
 Gly Ser Val Gln Leu Ala Asp His Tyr Gln Gln Asn Thr Pro Ile Gly
 420 425 430
 Asp Gly Pro Val Leu Leu Pro Asp Asn His Tyr Leu Ser Thr Gln Ser
 435 440 445
 Ala Leu Ser Lys Asp Pro Asn Glu Lys Arg Asp His Met Val Leu Leu
 450 455 460
 Glu Phe Val Thr Ala Ala Gly Ile Thr Leu Gly Met Asp Glu Leu Tyr
 465 470 475 480
 Lys Val Asp Lys Glu Met His Thr Gln Leu Phe Lys Ala Leu Val Leu
 485 490 495
 Gln Thr Ile Ile Pro Thr Thr Leu Met Tyr Ile Pro Thr Thr Met Leu
 500 505 510
 Phe Val Thr Pro Phe Val Gly Leu Asn Ile Gly Cys Tyr Gly Asn Ile
 515 520 525
 Thr Thr Ala Thr Val His Leu Tyr Pro Gly Ile Asp Pro Val Val Leu
 530 535 540
 Ile Phe Ile Ile Arg Asp Phe Arg Gln Thr Ile Leu Arg Pro Phe Arg
 545 550 555 560
 Cys Phe Tyr Arg Ser Asn Ser Val Glu Asn Thr Ala Thr Ile Arg Gln
 565 570 575
 Tyr Gln Gln Ser Ser Ser Lys Gly Ser Arg Glu Phe Gly Thr Met Ala
 580 585 590
 Ser Lys Val Tyr Asp Pro Glu Gln Arg Lys Arg Met Ile Thr Gly Pro
 595 600 605
 Gln Trp Trp Ala Arg Cys Lys Gln Met Asn Val Leu Asp Ser Phe Ile
 610 615 620
 Asn Tyr Tyr Asp Ser Glu Lys His Ala Glu Asn Ala Val Ile Phe Leu
 625 630 635 640
 His Gly Asn Ala Ala Ser Ser Tyr Leu Trp Arg His Val Val Pro His
 645 650 655
 Ile Glu Pro Val Ala Arg Cys Ile Ile Pro Asp Leu Ile Gly Met Gly
 660 665 670

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Lys Ser Gly Lys Ser Gly Asn Gly Ser Tyr Arg Leu Leu Asp His Tyr
 675 680 685

Lys Tyr Leu Thr Ala Trp Phe Glu Leu Leu Asn Leu Pro Lys Lys Ile
 690 695 700

Ile Phe Val Gly His Asp Trp Gly Ala Ala Leu Ala Phe His Tyr Ser
 705 710 715 720

Tyr Glu His Gln Asp Lys Ile Lys Ala Ile Val His Ala Glu Ser Val
 725 730 735

Val Asp Val Ile Glu Ser Trp Asp Glu Trp Pro Asp Ile Glu Glu Asp
 740 745 750

Ile Ala Leu Ile Lys Ser Glu Glu Gly Glu Lys Met Val Leu Glu Asn
 755 760 765

Asn Phe Phe Val Glu Thr Val Leu Pro Ser Lys Ile Met Arg Lys Leu
 770 775 780

Glu Pro Glu Glu Phe Ala Ala Tyr Leu Glu Pro Phe Lys Glu Lys Gly
 785 790 795 800

Glu Val Arg Arg Pro Thr Leu Ser Trp Pro Arg Glu Ile Pro Leu Val
 805 810 815

Lys Gly Gly Lys Pro Asp Val Val Gln Ile Val Arg Asn Tyr Asn Ala
 820 825 830

Tyr Leu Arg Ala Ser Asp Asp Leu Pro Lys Met Phe Ile Glu Ser Asp
 835 840 845

Pro Gly Phe Phe Ser Asn Ala Ile Val Glu Gly Ala Lys Lys Phe Pro
 850 855 860

Asn Thr Glu Phe Val Lys Val Lys Gly Leu His Phe Ser Gln Glu Asp
 865 870 875 880

Ala Pro Asp Glu Met Gly Lys Tyr Ile Lys Ser Phe Val Glu Arg Val
 885 890 895

Leu Lys Asn Glu Gln
 900

<210> SEQ ID NO 19
 <211> LENGTH: 2694
 <212> TYPE: DNA
 <213> ORGANISM: Artificial Sequence
 <220> FEATURE:
 <223> OTHER INFORMATION: Nucleotide sequence encoding GFP2-str-112
 SGSR-RLuc fusion protein

<400> SEQUENCE: 19

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ggtacttaca agtacttgat gtctttcttt tctttctttt ctattttcta tgcaatcggt    180
gaatctatct tgagaccaat catgcatatc gaaaacacta catttttctt aatctccaga    240
aagagattcg attacagtac tagattgggt aaaattaatt cagctttcta ctgtgcttgt    300
ttcgcaacat ccttcgtttt gactgcagtt catttcgttt acagatactt cgctgcttgt    360
aagcctaatt tgttgagatt gtttaactta cctcatttgt tattgtggcc attgatgtgt    420
tcaattcctg ttactgcttg ggcactctgt tcatactttt tgtaccaga tacagaatat    480
accgaagctg cagttaccta tgttttgaag actcattacg aagttattaa aaaggaaaac    540
gtttcttaca ttgcttacgt ttactaccaa tacgaaaacg gtgaaagaca tatctatatt    600
aaaaacttat tgggttgttt cgttcattac ttcgttatgt ctatgacatt cgttgttgtt    660
ttctattgtg gtttctcaac ttggtggaca attagagaac atagaggtgc ttccgataga    720
    
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acaatggta gtaagggta agaattatc accggtgtg tccaatfff ggttgaatta 780
gatggtgacg ttaatggtca taaatfffcc gttagtgggtg aaggtgaagg tgacgcaaca 840
tacggtaaat tgacctgaa gtttatfffgt accactggta aattgccagt tccttgccca 900
accttggta caacctaac ttatggtgtt caatgffff ccagataccc tgatcatatg 960
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ttggttaaca gaatcgaatt gaagggtatc gatttcaagg aagatggtaa catcttgggt 1140
cataagtgg aatacaatta caactcccat aacgtttaca tcatggctga taagcaaaag 1200
aatggtatta aagttaactt caagatcaga cataacatcg aagatggttc agttcaattg 1260
gcagatcatt accaacaata caccctatt ggtgacggtc ctgffffgtt gccagataac 1320
cattacttat caactcaatc cgctttgagt aaggatccaa acgaaaagag agatcatatg 1380
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aactactacg attcagaaaa gcctgctgaa aacgctggtt tttcttgcg tggtaacgct 1920
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atcttctgtg gtcctgattg ggtgtctgtt ttggcatttc attactctta cgaacatcaa 2160
gataaaatta aggtatcgt tcatgcagaa tccgttgttg atgttattga aagttgggat 2220
gaatggccag atatcgaaga agatctcgt ttaattaagt ccgaagaagg tgaaaagatg 2280
gttttgaaa acaactffff cgttgaaact atgttgccta gtaagatcat gagaaagttg 2340
gaacctgaag aatttctctc atatttggaa ccattcaaac aaaaggggtg agttagaaga 2400
cctacattat cttggcctag agaaattcca ttggttaaag gtggtaaacc agatgttgtt 2460
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aacacagaat tctgtaaggt taagggtttg catttctctc aagaagatgc tccagatgaa 2640
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<210> SEQ ID NO 20

<211> LENGTH: 2694

<212> TYPE: DNA

<213> ORGANISM: Artificial Sequence

<220> FEATURE:

<223> OTHER INFORMATION: Nucleotide sequence encoding GFP2-str-113
SGSR-RLuc fusion protein

<400> SEQUENCE: 20

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gaaacttttt	tgagacctct	catccatatac	tacgacaata	cgatcttcgt	gattcagcgc	240
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tacgccatga	gcttcacct	gttcgccgtc	cactttgtct	accgttacta	tgcggcttgc	360
aaacccgaca	acctccgtta	cttccaagga	tgtacttttg	tgcgatgggt	attcggagca	420
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ggaaatgttc	catatagcta	ttggcgca	gaaaacggag	tggaatacct	gaatcctcgc	600
aacgtcatcg	ggatctttca	acacggcgtc	atcatgatcc	tctccttcgg	aacagtcttc	660
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cccaccctga gctggcccag agagatcccc ctggtgaagg gcggaagcc cgacgtggtg	2460
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aacaccgagt tcgtgaaggt gaagggcctg cacttcagcc aggaggacgc ccccgacgag	2640
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<210> SEQ ID NO 21
 <211> LENGTH: 2715
 <212> TYPE: DNA
 <213> ORGANISM: Artificial Sequence
 <220> FEATURE:
 <223> OTHER INFORMATION: Nucleotide sequence encoding GFP2-str-114
 SGSR-RLuc fusion protein

<400> SEQUENCE: 21

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ggcacctatc ggtacttgat gatcactttc tgcgttttca gtttattatt tacgatatta	180
gaggatttta tcagaccgct gatgcatcac tataacaata ccataattgt tttacaacgc	240
aagcggtttc agttttctga ttcaacggct agaactctga cagtctctta ctgcgctgt	300
ttcgcgatgt gcttcgtgat gttcgcggtt catttcatct atcgatatct agttgcttgt	360
cacccgacaa aattgcaact ttttcgacct aaaaatttca ttttctggct gtcgagcatg	420
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accaggacgg atttggattt tattttgtca acttggtata atttaacgcc agatgatgtc	540
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aagaacggca tcaaggtgaa cttcaagatc cgcacaaca tcgaggacgg cagcgtgcag	1260
ctcgcgacc actaccagca gaacaccccc atcggcgacg gcccgtgct gctgcccagc	1320
aaccactacc tgagcaccca gtccgcccctg agcaaaagacc ccaacgagaa gcgcatcac	1380
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aaggtcgaca aggatctoca gaatcaattt ttcactgtct tagttgtca aaccgtagtc	1500
cctctgattt tcattgttat cccaaatag gtgctcacta cggcagccct tatagatggc	1560
acatttggct catgggccc aattactgta gttatgaatc atttgcctcc ggctgcccag	1620
ccattcgtta tactgttcat tattaagggg ttccggaata gtattagaaa tgttatatat	1680
cgctgcacaa aaacgaaaaa agcatcgggt agctcagtg tccgtggtat tgaggetcaa	1740

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agcaagaaac aatctttttc tcgagttgat atttctagaa tgaccagcaa ggtgtacgac 1800
cccgagcaga ggaagaggat gatcaccggc cccagtggt gggccagggt caagcagatg 1860
aacgtgctgg acagcttcat caactactac gacagcgaga agcacgccga gaacgccgtg 1920
atcttcctgc acggcaacgc cgctagcagc tacctgtgga ggcacgtggt gccccacatc 1980
gagcccggtg ccaggtgcat catccccgat ctgatcgcca tgggcaagag cggcaagagc 2040
ggcaacggca gctacaggct gctggaccac tacaagtacc tgaccgcctg gttcgagctc 2100
ctgaacctgc ccaagaagat catctctgtg ggccaagact ggggcgcctg cctggccttc 2160
cactacagct acgagcacca ggacaagatc aaggccatcg tgcacgccga gagcgtgggtg 2220
gacgtgatcg agagctggga cgagtgcca gacatcgagg aggacatgc cctgatcaag 2280
agcgaggagg gcgagaagat ggtgctggag aacaacttct tcgtggagac catgctgccc 2340
agcaagatca tgagaaagct ggagcccagag gagttcgccg cctacctgga gccctcaag 2400
gagaagggcg aggtgagaag acccaccctg agctggccca gagagatccc cctggtgaa 2460
ggcggcaagc ccgacgtggt gcagatcgtg agaaactaca acgcctacct gagagccagc 2520
gacgacctgc ccaagatggt catcgagagc gaccccggt tcttcagcaa cgccatcgtg 2580
gagggcgcca agaagttccc caacaccgag ttcgtgaagg tgaagggcct gcacttcagc 2640
caggaggacg cccccgacga gatgggcaag tacatcaaga gcttcgtgga gagagtgctg 2700
aagaacgagc agtaa 2715

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<210> SEQ ID NO 22
<211> LENGTH: 2673
<212> TYPE: DNA
<213> ORGANISM: Artificial Sequence
<220> FEATURE:
<223> OTHER INFORMATION: Nucleotide sequence encoding GFP2-str-115
SGSR-RLuc fusion protein

<400> SEQUENCE: 22

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```

atgactgac aacactgggt tattatcaca gatattgctg gtccaatcgg attttcaatg 60
tccatttttt caaactctat tcttttgttt ttgatatttt cacattcacc tccaataaaa 120
ggtccataca aacgaatgct catagtattt tgcataattt ccgtattcta ctcatgttc 180
gaagtcacgc ttcagccact aatccatatt tacgacgaca ctttattttt gattcatcga 240
aagagaatag acttgccaaa atggttaaca cgtttggttc ctactaccta ttgttggtgt 300
tacgcaatga gtttttcctt gtttgatta caatttttat atagatatgt ggcagtatgc 360
aaaccgcaat atgttgatct ttttgcgga tgcactttt atgcttgggt agttttgatc 420
ttatcactag ccacgagctg gggactcact gcagettcca tgttcccaca aaccgaccga 480
acaactgaaa ttttttgca cataatttat agttcatatg acttgagacc ttattggaca 540
gattatgttg cttataaata ctttgatact gatgagaata atgtgagatg ggtcaatggt 600
cttagttttt tcggtgtcct tcagcacggg attgtaatta ctctaagttt tggcacccct 660
tattattgtg gcatcaacac gtatctcaaa ataaaaaac aactggaac atcaaacaga 720
acttccggaa tggtagcaaa gggcgaggag ctgttcaccg ggggtggtgc catcctggtc 780
gagctggaag cgcacgtaaa cgccacaag ttcagcgtgt ccggcgaggg cgagggcgat 840
gccacctacg gcaagctgac cctgaagttc atctgcacca ccggcaagct gcccgtgccc 900
tggccccccc tcgtgaccac cctgagctac ggcgtgcagt gcttcagccg ctaccccgac 960
cacatgaagc agcacgactt cttcaagtcc gccatgcccg aaggctacgt ccaggagcgc 1020

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accatcttct tcaaggacga cggcaactac aagacccgcg ccgaggtgaa gttcgagggc 1080
gacaccctgg tgaaccgcat cgagctgaag ggcacogact tcaaggagga cggcaacatc 1140
ctggggcaca agctggagta caactacaac agccacaacg tctatatcat ggccgacaag 1200
cagaagaacg gcatcaaggt gaacttcaag atccgccaca acatcgagga cggcagcgtg 1260
cagctcgcgc accactacca gcagaacacc cccatcggcg acggccccgt gctgctgccc 1320
gacaaccact acctgagcac ccagtcggcc ctgagcaaag accccaacga gaagcgcgat 1380
cacatggtcc tgctggagtt cgtgaccgcc gccgggatca ctctcgcat ggacgagctg 1440
tacaaggtcg accgatgtat tcaactacaa cttttcagag ctctggttgc acagacaatt 1500
ttaccaatgt tcatgatgta tattccggtt ggtttcatgt ttgcatgtcc atattttgac 1560
ttgcaattag gtgcatacac caattatcaa acagtcatgg cacaaactta tccgggaatc 1620
gaccatttg tgatgctggt tttgatagat tcttatagaa taacaatatt tggatggtta 1680
tgtccaagat ttgtttatgt aaagccgatg cattccacat acaccctaac ttctagaatg 1740
accagcaagg tgtacgacc cgagcagagg aagaggatga tcaccggccc ccagtgggtg 1800
gccaggtgca agcagatgaa cgtgctggac agcttcatca actactacga cagcgagaag 1860
cacgcccaga acgcccgtgat cttcctgcac ggcaacgccc ctagcagcta cctgtggagg 1920
cacgtggtgc cccacatcga gcccggtggc aggtgcatca tccccgatct gatcggcatg 1980
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ggcgccctgcc tggccttcca ctacagctac gaccaccagg acaagatcaa ggccatcgtg 2160
cacgcccaga gcgtggtgga cgtgatcag agctgggacg agtggccaga catcgaggag 2220
gacatcgccc tgatcaagag cgaggagggc gagaagatgg tgctggagaa caacttcttc 2280
gtggagacca tgctgcccag caagatcag agaaagctgg agcccagga gttcgcgcc 2340
tacctggagc ccttcaagga gaagggcagc gtgagaagac ccaccctgag ctggcccaga 2400
gagatcccc tggtgaaggg cggcaagccc gacgtggtgc agatcgtgag aaactacaac 2460
gcctacctga gagccagcga cgacctgccc aagatgttca tcgagagcga ccccggttc 2520
ttcagcaacg ccacgtgga gggcgccaag aagttccca acaccgagtt cgtgaaggtg 2580
aagggcctgc acttcagcca ggaggacgcc cccgacgaga tgggcaagta catcaagagc 2640
ttcgtggaga gagtgtgaa gaacgagcag taa 2673

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<210> SEQ ID NO 23

<211> LENGTH: 2721

<212> TYPE: DNA

<213> ORGANISM: Artificial Sequence

<220> FEATURE:

<223> OTHER INFORMATION: Nucleotide sequence encoding GFP2-str-116
SGSR-RLuc fusion protein

<400> SEQUENCE: 23

```

atgaccgatc gtcgctgggt cgctattacg gacattgccg gaccgattgg gttcacaatg 60
tcaatTTTTT cgaactcggg gctgttatcg ttgatattct caagcagctc tccaattaaa 120
ggagcttaca aaaatatggt gatagtgttg tgatattca ctatgttcta ctcttttgtt 180
gaaataatgc ttcaaccggt gattcatatt tatgatgaca cgctgttctt gatccaccgg 240
aaaagatttg acctgtctaa aggaattaca cgtttgatac ctacaacata ttgttggtgt 300
tatgcaatga gtttctcatt attcgcctc cagttttgt acagatatgt ggcagtttgc 360

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aaacctcact tagttgTTTT ttttactgga tgctatttct attattgggtt ggcactcacc	420
ttatcacttg ctacaagttg ggggcttact gcagctttta tggtoeccga aaccaatcga	480
acaactgaaa gcttcaacta cgtaataaaa acttcttatg acttagatcc ttattggacg	540
gattatgttg cctataaata ttttgacacc gatgagaatc atgtgagatg ggtgaatgtt	600
cttagtttat ttggagtctt gcagcacgga ttagtaatta cgttgagttt tggaacctta	660
ttctactgtg gaattaaaac ttactcagc attactgaac atgttggaat gtccagcaag	720
acctccgga tggtgagcaa gggcgaggag ctggtcaccg ggggtgtgcc catcctggtc	780
gagctggacg gcgacgtaaa cggccacaag ttcagcgtgt ccggcgaggg cgagggcgat	840
gccacctacg gcaagctgac cctgaagtcc atctgcacca ccggcaagct gccctgtccc	900
tggcccacc tcgtgaccac cctgagctac ggcgtgcagt gcttcagccg ctaccccgac	960
cacatgaagc agcacgactt cttcaagtcc gccatgcccg aaggctacgt ccaggagcgc	1020
accatcttct tcaaggacga cggcaactac aagaccgcg ccgaggtgaa gttcgagggc	1080
gacacctgg tgaaccgcat cgagctgaag ggcatcgact tcaaggagga cggcaacatc	1140
ctggggcaca agctggagta caactacaac agccacaacg tctatatcat ggccgacaag	1200
cagaagaacg gcacaaagt gaacttcaag atccgccaca acatcgagga cggcagcgtg	1260
cagctcgcg accactacca gcagaacacc cccatcggcg acggcccgt gctgctgccc	1320
gacaaccact acctgagcac ccagtcgcc ctgagcaaaag accccaacga gaagcgcgat	1380
cacatggtcc tgctggagtt cgtgaccgcc gccgggatca ctctcgcat ggacgagctg	1440
tacaagtg accgaagtct tcaactcaa ctattccgtg ctttagttgc tcagacatgt	1500
cttccaatgc tcattgatga catgccaaata ggattcatgt tttcttgccc ttactttgat	1560
ttgcaacttg gagcagtcac aaactatcaa accgtcatgg cacagttata cccaggaatc	1620
gaccattta tgttgctatt tcttattaac gcctacagaa agacagtgtt aagcttgatc	1680
tgctctaatt ttatccagaa aaaatatgtt caaacggcaa ctactcgtga tggcacagat	1740
gcctcggcaa caatgaatc tgttaaatct acacagttat ctagaatgac cagcaaggtg	1800
tacgaccccg agcagaggaa gaggatgatc accggcccc agtgggtggc caggtgcaag	1860
cagatgaacg tgctggacag cttcatcaac tactacgaca gcgagaagca cgcgagaa	1920
gccgtgatct tcctgcacgg caacgcgct agcagctacc tgtggaggca cgtggtgccc	1980
cacatcgagc ccgtggccag gtgcacatc cccgatctga tcggcatggg caagagcggc	2040
aagagcggca acggcagcta caggctgctg gaccactaca agtacctgac cgcctggttc	2100
gagctcctga acctgcccga gaagatcacc ttcgtgggcc acgactgggg cgcctgctg	2160
gccttccact acagctacga gcaccaggac aagatcaagg ccatcgtgca cgcgagagc	2220
gtggtggacg tgatcgagag ctgggacgag tggccagaca tcgaggagga catcgccctg	2280
atcaagagcg agggggcgga gaagatggtg ctggagaaca acttctctgt ggagaccatg	2340
ctgcccagca agatcatgag aaagctggag cccgaggagt tcgccccta cctggagccc	2400
ttcaaggaga agggcgaggt gagaagacc accctgagct ggcccagaga gatcccctg	2460
gtgaaggcg gcaagcccga cgtggtgcag atcgtgagaa actacaacgc ctacctgaga	2520
gccagcgacg acctgcccga gatgttcac gagagcgacc ccggcttctt cagcaacgcc	2580
atcgtggagg gcgccaagaa gttcccac accgagttcg tgaaggtgaa gggcctgac	2640
ttcagccagg aggacgcccc cgacgagatg ggcaagtaca tcaagagctt cgtggagaga	2700
gtgctgaaga acgacagta a	2721

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<210> SEQ ID NO 24
 <211> LENGTH: 2706
 <212> TYPE: DNA
 <213> ORGANISM: Artificial Sequence
 <220> FEATURE:
 <223> OTHER INFORMATION: Nucleotide sequence encoding GFP2-str-113/114
 SGSr-RLuc fusion protein

<400> SEQUENCE: 24

```

atgtccgata tatactggat acaaattact gaagtttgct ccttcgtcgg atttatgctc    60
tcagttctag ggaacagtac acttttagta ctgctcagtg gaaaatccat agatggaatt    120
ggcacctatc ggtacttgat gatcactttc tgcgttttca gtttattatt tacgatatta    180
gaggatttta tcagaccgct gatgcatcac tataacaata ccataattgt tttacaacgc    240
aagcggtttc agtttttga ttcaacggct agaactctga cagtctctta ctgcggctgt    300
ttcgcgatgt gcttcgtgat gttcgcggtt catttcatct atcgatatct agttgcttgt    360
caccgcacaa aattgcaact ttttcgacc aaaaatttca ttttctggct gtccggcatg    420
ttattcatag caggaagctg ggttgcaatt gcatatgtct ttttcaaga agacctagaa    480
accaggacgg atttggattt tattttgtca acttggtata atttaacgcc agatgatgtc    540
ggacatgtac cgtatgcttt ttacaaaact caaggaaata caccagtaat tcgatgggat    600
aacatgattg gagtaattca tcatatgata gttatgacaa tctctataag tgccgttttc    660
tactttggca ttaaaaccta cactcgaata atgagtttca agggaaaatc ccagaaaacc    720
tccggaatgg tgagcaaggg cgaggagctg ttcaccgggg tggtgcccat cctggtcgag    780
ctggacggcg acgtaaaccg ccacaagttc agcgtgtccg gcgagggcga gggcgatgcc    840
acctacggca agctgaccct gaagttcacc tgcaccaccg gcaagctgcc cgtgccctgg    900
cccaccctcg tgaccaccct gagctacggc gtgcagtgct tcagccgcta ccccgaccac    960
atgaagcagc acgacttctt caagtcgcc atgcccgaag gctacgtcca ggagcgcacc   1020
atcttcttca aggacgacgg caactacaag acccgcgccc aggtgaagtt cgagggcgac   1080
accctggtga accgcatcga gctgaagggc atcgacttca aggaggacgg caacatcctg   1140
gggcacaagc tggagtacaa ctacaacagc cacaacgtct atatcatggc cgacaagcag   1200
aagaacggca tcaaggtgaa cttcaagatc cgcacaaca tcgaggacgg cagcgtgcag   1260
ctcgcgacc actaccagca gaacaccccc atcggcgacg gccccgtgct gctgcccagc   1320
aaccactacc tgagcaccca gtccgcccctg agcaaagacc ccaacgagaa gcgcgatcac   1380
atggtcctgc tggagtctgt gaccgcgccc gggatcactc tcggcatgga cgagctgtac   1440
aaggtcgaca aagaaatgca cacccaattg ttcaaggcct tggttctaca gactatcacc   1500
cctactacac taatgtacat cccgacaacc atgctctttg tcacccatt cgttggactc   1560
aacatcggct gttacggcaa catcactact gccaccgtcc atttgtatcc tgggaattgac   1620
ccagtcgctt tgatctttat aatccgagac ttccggcaaa cgattttaag accattcaga   1680
tgcttctacc gttcaaatag tgcgaaaac actgccacca taaggcaata ccagcagagc   1740
agctccaaag gatctagaga attcggtagc atggcttcca aggtgtacga ccccgagcaa   1800
cgcaaacgca tgatcactgg gctcagtggt tgggctcgtc gcaagcaaat gaacgtgctg   1860
gactccttca tcaactacta tgattccgag aagcacgccc agaacgcccg gatTTTTctg   1920
catggtaacg ctgcctccag ctacctgtgg aggcacgtcg tgctccatc cgagcccgtg   1980
gctagatgca tcaccctga tctgatcgga atgggtaagt ccggcaagag cgggaatggc   2040
  
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tcataatgcc tcctggatca ctacaagtac ctcaccgctt ggctogagct gctgaacctt 2100
ccaaagaaaa tcattttgt gggccaagac tggggggctg ctctggcctt tcaactactcc 2160
tacgagcacc aagacaagat caaggccatc gtccatgctg agagtgtcgt ggacgtgatc 2220
gagtctctggg acgagtggcc tgacatcgag gaggatatcg ccctgatcaa gagcgaagag 2280
ggcgagaaaa tgggtgctga gaataacttc ttcgtcgaga ccgtgctccc aagcaagatc 2340
atgcggaaac tggagcctga ggagttcgtc gctacactgg agccattcaa ggagaagggc 2400
gaggttagac ggctaccct ctctggcct cgcgagatcc ctctcgttaa gggaggcaag 2460
cccgacgtcg tccagattgt ccgcaactac aacgcctacc ttcgggccag cgacgatctg 2520
cctaagatgt tcacgagtc cgaccctggg ttcttttcca acgctattgt cgagggagct 2580
aagaagttcc ctaacaccga gttcgtgaag gtgaagggcc tccacttcag ccaggaggac 2640
gctccagatg aaatgggtaa gtacatcaag agcttcgtgg agcgcgtgct gaagaacgag 2700
cagtaa 2706

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<210> SEQ ID NO 25
<211> LENGTH: 889
<212> TYPE: PRT
<213> ORGANISM: Artificial Sequence
<220> FEATURE:
<223> OTHER INFORMATION: GFP2-OGOR-RLuc2 protein

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<400> SEQUENCE: 25

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Met Ser Gly Glu Leu Trp Ile Thr Leu Val Asp Thr Ala Asp Ile Val
1          5          10          15
Gly Val Thr Leu Thr Phe Cys Val Asn Ile Val Leu Leu Gly Leu Leu
20          25          30
Lys Thr Arg Gly Lys Asn Leu Gly Thr Tyr Lys Tyr Leu Met Ala Phe
35          40          45
Phe Ser Val Phe Ser Ile Phe Tyr Ala Ile Ile Glu Phe Ile Leu Arg
50          55          60
Pro Ile Met His Ile Glu Asn Thr Thr Phe Phe Leu Ile Ser Arg Lys
65          70          75          80
Arg Phe Asn Tyr Ser Thr Lys Leu Gly Lys Ile Asn Ser Ala Phe Tyr
85          90          95
Cys Ala Cys Phe Ala Thr Ser Phe Val Val Ser Gly Val His Phe Val
100         105         110
Tyr Arg Tyr Phe Ala Thr Cys Lys Pro Asn Leu Leu Arg Leu Phe Asn
115        120        125
Leu Pro Thr Leu Leu Leu Trp Pro Leu Gly Cys Ser Val Pro Val Thr
130        135        140
Met Trp Ala Ser Val Ser Tyr Phe Leu Tyr Pro Asp Thr Glu Tyr Thr
145        150        155        160
Glu Ala Ala Val Thr Asn Val Leu Asn Asn His Tyr Asn Trp Ile Lys
165        170        175
Lys Glu Asn Val Ser Tyr Ile Ala Tyr Val Tyr Tyr Gln Tyr Glu Asn
180        185        190
Gly Val Arg His Ile Tyr Leu Lys Asn Leu Leu Gly Cys Phe Val His
195        200        205
Tyr Phe Val Met Ser Met Thr Phe Val Val Met Phe Tyr Cys Gly Tyr
210        215        220
Ala Thr Trp Lys Thr Met Asn Glu His Lys Asp Val Ser Asp Arg Thr
225        230        235        240

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Ile Gly Met Gly Lys Ser Gly Lys Ser Gly Asn Gly Ser Tyr Arg Leu
 660 665 670
 Leu Asp His Tyr Lys Tyr Leu Thr Ala Trp Phe Glu Leu Leu Asn Leu
 675 680 685
 Pro Lys Lys Ile Ile Phe Val Gly His Asp Trp Gly Ala Ala Leu Ala
 690 695 700
 Phe His Tyr Ser Tyr Glu His Gln Asp Lys Ile Lys Ala Ile Val His
 705 710 715 720
 Ala Glu Ser Val Val Asp Val Ile Glu Ser Trp Asp Glu Trp Pro Asp
 725 730 735
 Ile Glu Glu Asp Ile Ala Leu Ile Lys Ser Glu Glu Gly Glu Lys Met
 740 745 750
 Val Leu Glu Asn Asn Phe Phe Val Glu Thr Val Leu Pro Ser Lys Ile
 755 760 765
 Met Arg Lys Leu Glu Pro Glu Glu Phe Ala Ala Tyr Leu Glu Pro Phe
 770 775 780
 Lys Glu Lys Gly Glu Val Arg Arg Pro Thr Leu Ser Trp Pro Arg Glu
 785 790 795 800
 Ile Pro Leu Val Lys Gly Gly Lys Pro Asp Val Val Gln Ile Val Arg
 805 810 815
 Asn Tyr Asn Ala Tyr Leu Arg Ala Ser Asp Asp Leu Pro Lys Met Phe
 820 825 830
 Ile Glu Ser Asp Pro Gly Phe Phe Ser Asn Ala Ile Val Glu Gly Ala
 835 840 845
 Lys Lys Phe Pro Asn Thr Glu Phe Val Lys Val Lys Gly Leu His Phe
 850 855 860
 Ser Gln Glu Asp Ala Pro Asp Glu Met Gly Lys Tyr Ile Lys Ser Phe
 865 870 875 880
 Val Glu Arg Val Leu Lys Asn Glu Gln
 885

<210> SEQ ID NO 26

<211> LENGTH: 889

<212> TYPE: PRT

<213> ORGANISM: Artificial Sequence

<220> FEATURE:

<223> OTHER INFORMATION: GFP2-OGOR-RLuc2 mutant protein

<400> SEQUENCE: 26

Met Ser Gly Glu Leu Trp Ile Thr Leu Val Asp Thr Ala Asp Ile Val
 1 5 10 15
 Gly Val Thr Leu Thr Phe Cys Val Asn Ile Val Leu Leu Gly Leu Leu
 20 25 30
 Lys Thr Arg Gly Lys Asn Leu Gly Thr Tyr Lys Tyr Leu Met Ala Phe
 35 40 45
 Phe Ser Val Phe Ser Ile Phe Tyr Ala Ile Ile Glu Phe Ile Leu Arg
 50 55 60
 Pro Ile Met His Ile Glu Asn Thr Thr Phe Phe Leu Ile Ser Arg Lys
 65 70 75 80
 Arg Phe Asn Tyr Ser Thr Lys Leu Gly Lys Ile Asn Ser Ala Phe Tyr
 85 90 95
 Cys Ala Cys Phe Ala Thr Ser Phe Val Val Ser Gly Val Tyr Phe Val
 100 105 110
 Tyr Arg Tyr Phe Ala Thr Cys Lys Pro Asn Leu Leu Arg Leu Phe Asn
 115 120 125

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Leu Pro Thr Leu Leu Leu Trp Pro Leu Gly Cys Ser Val Pro Val Thr
 130 135 140
 Met Trp Ala Ser Val Ser Tyr Phe Leu Tyr Pro Asp Thr Glu Tyr Thr
 145 150 155 160
 Glu Ala Ala Val Thr Asn Val Leu Asn Asn His Tyr Asn Trp Ile Lys
 165 170 175
 Lys Glu Asn Val Ser Tyr Ile Ala Tyr Val Tyr Tyr Gln Tyr Glu Asn
 180 185 190
 Gly Val Arg His Ile Tyr Leu Lys Asn Leu Leu Gly Cys Phe Val His
 195 200 205
 Tyr Phe Val Met Ser Met Thr Phe Val Val Met Phe Tyr Cys Gly Tyr
 210 215 220
 Ala Thr Trp Lys Thr Met Asn Glu His Lys Asp Val Ser Asp Arg Thr
 225 230 235 240
 Met Val Ser Lys Gly Glu Glu Leu Phe Thr Gly Val Val Pro Ile Leu
 245 250 255
 Val Glu Leu Asp Gly Asp Val Asn Gly His Lys Phe Ser Val Ser Gly
 260 265 270
 Glu Gly Glu Gly Asp Ala Thr Tyr Gly Lys Leu Thr Leu Lys Phe Ile
 275 280 285
 Cys Thr Thr Gly Lys Leu Pro Val Pro Trp Pro Thr Leu Val Thr Thr
 290 295 300
 Leu Ser Tyr Gly Val Gln Cys Phe Ser Arg Tyr Pro Asp His Met Lys
 305 310 315 320
 Gln His Asp Phe Phe Lys Ser Ala Met Pro Glu Gly Tyr Val Gln Glu
 325 330 335
 Arg Thr Ile Phe Phe Lys Asp Asp Gly Asn Tyr Lys Thr Arg Ala Glu
 340 345 350
 Val Lys Phe Glu Gly Asp Thr Leu Val Asn Arg Ile Glu Leu Lys Gly
 355 360 365
 Ile Asp Phe Lys Glu Asp Gly Asn Ile Leu Gly His Lys Leu Glu Tyr
 370 375 380
 Asn Tyr Asn Ser His Asn Val Tyr Ile Met Ala Asp Lys Gln Lys Asn
 385 390 395 400
 Gly Ile Lys Val Asn Phe Lys Ile Arg His Asn Ile Glu Asp Gly Ser
 405 410 415
 Val Gln Leu Ala Asp His Tyr Gln Gln Asn Thr Pro Ile Gly Asp Gly
 420 425 430
 Pro Val Leu Leu Pro Asp Asn His Tyr Leu Ser Thr Gln Ser Ala Leu
 435 440 445
 Ser Lys Asp Pro Asn Glu Lys Arg Asp His Met Val Leu Leu Glu Phe
 450 455 460
 Val Thr Ala Ala Gly Ile Thr Leu Gly Met Asp Glu Leu Tyr Lys Arg
 465 470 475 480
 Ala Leu Gln Lys Gln Leu Phe Lys Ala Leu Val Leu Gln Thr Leu Ile
 485 490 495
 Pro Thr Ile Phe Met Tyr Ala Pro Thr Gly Val Met Phe Ile Ala Pro
 500 505 510
 Phe Phe Asp Val Asn Leu Asn Ala Asn Ala Asn Phe Ile Val Phe Cys
 515 520 525
 Ser Phe Leu Tyr Pro Gly Leu Asp Pro Leu Ile Leu Ile Leu Ile Ile
 530 535 540
 Arg Asp Phe Arg Arg Thr Ile Phe Asn Phe Leu Cys Gly Lys Lys Asn

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545		550		555		560									
Ser	Val	Asp	Glu	Ser	Arg	Ser	Thr	Thr	Arg	Ala	Asn	Leu	Ser	Gln	Val
				565					570					575	
Pro	Thr	Met	Thr	Ser	Lys	Val	Tyr	Asp	Pro	Glu	Gln	Arg	Lys	Arg	Met
			580					585					590		
Ile	Thr	Gly	Pro	Gln	Trp	Trp	Ala	Arg	Cys	Lys	Gln	Met	Asn	Val	Leu
		595					600					605			
Asp	Ser	Phe	Ile	Asn	Tyr	Tyr	Asp	Ser	Glu	Lys	His	Ala	Glu	Asn	Ala
610					615						620				
Val	Ile	Phe	Leu	His	Gly	Asn	Ala	Ala	Ser	Ser	Tyr	Leu	Trp	Arg	His
625					630						635				640
Val	Val	Pro	His	Ile	Glu	Pro	Val	Ala	Arg	Cys	Ile	Ile	Pro	Asp	Leu
			645						650					655	
Ile	Gly	Met	Gly	Lys	Ser	Gly	Lys	Ser	Gly	Asn	Gly	Ser	Tyr	Arg	Leu
		660						665					670		
Leu	Asp	His	Tyr	Lys	Tyr	Leu	Thr	Ala	Trp	Phe	Glu	Leu	Leu	Asn	Leu
		675					680					685			
Pro	Lys	Lys	Ile	Ile	Phe	Val	Gly	His	Asp	Trp	Gly	Ala	Ala	Leu	Ala
690						695					700				
Phe	His	Tyr	Ser	Tyr	Glu	His	Gln	Asp	Lys	Ile	Lys	Ala	Ile	Val	His
705					710					715					720
Ala	Glu	Ser	Val	Val	Asp	Val	Ile	Glu	Ser	Trp	Asp	Glu	Trp	Pro	Asp
				725						730					735
Ile	Glu	Glu	Asp	Ile	Ala	Leu	Ile	Lys	Ser	Glu	Glu	Gly	Glu	Lys	Met
			740						745					750	
Val	Leu	Glu	Asn	Asn	Phe	Phe	Val	Glu	Thr	Val	Leu	Pro	Ser	Lys	Ile
			755				760						765		
Met	Arg	Lys	Leu	Glu	Pro	Glu	Glu	Phe	Ala	Ala	Tyr	Leu	Glu	Pro	Phe
770						775					780				
Lys	Glu	Lys	Gly	Glu	Val	Arg	Arg	Pro	Thr	Leu	Ser	Trp	Pro	Arg	Glu
785					790					795					800
Ile	Pro	Leu	Val	Lys	Gly	Gly	Lys	Pro	Asp	Val	Val	Gln	Ile	Val	Arg
				805					810						815
Asn	Tyr	Asn	Ala	Tyr	Leu	Arg	Ala	Ser	Asp	Asp	Leu	Pro	Lys	Met	Phe
			820						825					830	
Ile	Glu	Ser	Asp	Pro	Gly	Phe	Phe	Ser	Asn	Ala	Ile	Val	Glu	Gly	Ala
			835				840						845		
Lys	Lys	Phe	Pro	Asn	Thr	Glu	Phe	Val	Lys	Val	Lys	Gly	Leu	His	Phe
850						855						860			
Ser	Gln	Glu	Asp	Ala	Pro	Asp	Glu	Met	Gly	Lys	Tyr	Ile	Lys	Ser	Phe
865					870					875					880
Val	Glu	Arg	Val	Leu	Lys	Asn	Glu	Gln							
				885											

<210> SEQ ID NO 27
 <211> LENGTH: 897
 <212> TYPE: PRT
 <213> ORGANISM: Artificial Sequence
 <220> FEATURE:
 <223> OTHER INFORMATION: GFP2-str-112 SGSR-RLuc2 mutant protein

<400> SEQUENCE: 27
 Met Gly Ser Gly Gln Leu Trp Leu Ala Leu Val Asp Ala Ala Asp Met
 1 5 10 15
 Val Gly Phe Thr Leu Thr Ile Ser Ile Asn Ile Ile Leu Leu Gly Leu

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20					25					30					
Ile	Arg	Thr	Arg	Gly	Lys	Thr	Leu	Gly	Thr	Tyr	Lys	Tyr	Leu	Met	Ser
	35						40					45			
Phe	Phe	Ser	Phe	Phe	Ser	Ile	Phe	Tyr	Ala	Ile	Val	Glu	Ser	Ile	Leu
	50					55					60				
Arg	Pro	Ile	Met	His	Ile	Glu	Asn	Thr	Thr	Phe	Phe	Leu	Ile	Ser	Arg
	65					70					75				80
Lys	Arg	Phe	Asp	Tyr	Ser	Thr	Arg	Leu	Gly	Lys	Ile	Asn	Ser	Ala	Phe
				85					90					95	
Tyr	Cys	Ala	Cys	Phe	Ala	Thr	Ser	Phe	Val	Leu	Ser	Ala	Val	His	Phe
		100						105					110		
Val	Tyr	Arg	Tyr	Phe	Ala	Ala	Cys	Lys	Pro	Asn	Leu	Leu	Arg	Leu	Phe
		115						120					125		
Asn	Leu	Pro	His	Leu	Leu	Leu	Trp	Pro	Leu	Met	Cys	Ser	Ile	Pro	Val
	130						135				140				
Thr	Ala	Trp	Ala	Ser	Val	Ser	Tyr	Phe	Leu	Tyr	Pro	Asp	Thr	Glu	Tyr
	145					150					155				160
Thr	Glu	Ala	Ala	Val	Thr	Tyr	Val	Leu	Lys	Thr	His	Tyr	Glu	Val	Ile
				165					170					175	
Lys	Lys	Glu	Asn	Val	Ser	Tyr	Ile	Ala	Tyr	Val	Tyr	Tyr	Gln	Tyr	Glu
			180						185					190	
Asn	Gly	Glu	Arg	His	Ile	Tyr	Ile	Lys	Asn	Leu	Leu	Gly	Cys	Phe	Val
		195						200					205		
His	Tyr	Phe	Val	Met	Ser	Met	Thr	Phe	Val	Val	Val	Phe	Tyr	Cys	Gly
	210					215						220			
Phe	Ser	Thr	Trp	Trp	Thr	Ile	Arg	Glu	His	Arg	Gly	Ala	Ser	Asp	Arg
	225					230					235				240
Thr	Met	Val	Ser	Lys	Gly	Glu	Glu	Leu	Phe	Thr	Gly	Val	Val	Pro	Ile
				245					250					255	
Leu	Val	Glu	Leu	Asp	Gly	Asp	Val	Asn	Gly	His	Lys	Phe	Ser	Val	Ser
			260					265						270	
Gly	Glu	Gly	Glu	Gly	Asp	Ala	Thr	Tyr	Gly	Lys	Leu	Thr	Leu	Lys	Phe
		275					280						285		
Ile	Cys	Thr	Thr	Gly	Lys	Leu	Pro	Val	Pro	Trp	Pro	Thr	Leu	Val	Thr
	290					295					300				
Thr	Leu	Thr	Tyr	Gly	Val	Gln	Cys	Phe	Ser	Arg	Tyr	Pro	Asp	His	Met
	305					310					315				320
Lys	Gln	His	Asp	Phe	Phe	Lys	Ser	Ala	Met	Pro	Glu	Gly	Tyr	Val	Gln
				325					330					335	
Glu	Arg	Thr	Ile	Phe	Phe	Lys	Asp	Asp	Gly	Asn	Tyr	Lys	Thr	Arg	Ala
			340					345						350	
Glu	Val	Lys	Phe	Glu	Gly	Asp	Thr	Leu	Val	Asn	Arg	Ile	Glu	Leu	Lys
		355					360						365		
Gly	Ile	Asp	Phe	Lys	Glu	Asp	Gly	Asn	Ile	Leu	Gly	His	Lys	Leu	Glu
	370					375					380				
Tyr	Asn	Tyr	Asn	Ser	His	Asn	Val	Tyr	Ile	Met	Ala	Asp	Lys	Gln	Lys
	385					390					395				400
Asn	Gly	Ile	Lys	Val	Asn	Phe	Lys	Ile	Arg	His	Asn	Ile	Glu	Asp	Gly
				405					410					415	
Ser	Val	Gln	Leu	Ala	Asp	His	Tyr	Gln	Gln	Asn	Thr	Pro	Ile	Gly	Asp
				420					425					430	
Gly	Pro	Val	Leu	Leu	Pro	Asp	Asn	His	Tyr	Leu	Ser	Thr	Gln	Ser	Ala
		435						440						445	

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Leu Ser Lys Asp Pro Asn Glu Lys Arg Asp His Met Val Leu Leu Glu
 450 455 460
 Phe Val Thr Ala Ala Gly Ile Thr Leu Gly Met Asp Glu Leu Tyr Lys
 465 470 475 480
 Arg His Leu His Arg Gln Leu Phe Lys Ala Leu Val Phe Gln Thr Leu
 485 490 495
 Val Pro Ser Ile Phe Met Tyr Ile Pro Thr Gly Val Met Phe Ile Ala
 500 505 510
 Pro Phe Phe Asp Ile Asn Leu Asn Ala Asn Ala Asn Phe Ile Val Phe
 515 520 525
 Cys Ser Phe Leu Tyr Pro Gly Leu Asp Pro Leu Ile Leu Ile Phe Ile
 530 535 540
 Ile Arg Glu Phe Arg Val Thr Ile Leu Asn Ile Ile Arg Gly Asn Glu
 545 550 555 560
 Arg Gly Asn Ala Val Gly Glu Ala Tyr Ser Thr Ser Arg Ile Lys Ser
 565 570 575
 Ser Gln Pro Ala Ala Val Asn Leu Ser Gly Met Thr Ser Lys Val Tyr
 580 585 590
 Asp Pro Glu Gln Arg Lys Arg Met Ile Thr Gly Pro Gln Trp Trp Ala
 595 600 605
 Arg Cys Lys Gln Met Asn Val Leu Asp Ser Phe Ile Asn Tyr Tyr Asp
 610 615 620
 Ser Glu Lys His Ala Glu Asn Ala Val Ile Phe Leu His Gly Asn Ala
 625 630 635 640
 Ala Ser Ser Tyr Leu Trp Arg His Val Val Pro His Ile Glu Pro Val
 645 650 655
 Ala Arg Cys Ile Ile Pro Asp Leu Ile Gly Met Gly Lys Ser Gly Lys
 660 665 670
 Ser Gly Asn Gly Ser Tyr Arg Leu Leu Asp His Tyr Lys Tyr Leu Thr
 675 680 685
 Ala Trp Phe Glu Leu Leu Asn Leu Pro Lys Lys Ile Ile Phe Val Gly
 690 695 700
 His Asp Trp Gly Ala Ala Leu Ala Phe His Tyr Ser Tyr Glu His Gln
 705 710 715 720
 Asp Lys Ile Lys Ala Ile Val His Ala Glu Ser Val Val Asp Val Ile
 725 730 735
 Glu Ser Trp Asp Glu Trp Pro Asp Ile Glu Glu Asp Ile Ala Leu Ile
 740 745 750
 Lys Ser Glu Glu Gly Glu Lys Met Val Leu Glu Asn Asn Phe Phe Val
 755 760 765
 Glu Thr Val Leu Pro Ser Lys Ile Met Arg Lys Leu Glu Pro Glu Glu
 770 775 780
 Phe Ala Ala Tyr Leu Glu Pro Phe Lys Glu Lys Gly Glu Val Arg Arg
 785 790 795 800
 Pro Thr Leu Ser Trp Pro Arg Glu Ile Pro Leu Val Lys Gly Gly Lys
 805 810 815
 Pro Asp Val Val Gln Ile Val Arg Asn Tyr Asn Ala Tyr Leu Arg Ala
 820 825 830
 Ser Asp Asp Leu Pro Lys Met Phe Ile Glu Ser Asp Pro Gly Phe Phe
 835 840 845
 Ser Asn Ala Ile Val Glu Gly Ala Lys Lys Phe Pro Asn Thr Glu Phe
 850 855 860

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Val Lys Val Lys Gly Leu His Phe Ser Gln Glu Asp Ala Pro Asp Glu
865 870 875 880

Met Gly Lys Tyr Ile Lys Ser Phe Val Glu Arg Val Leu Lys Asn Glu
885 890 895

Gln

<210> SEQ ID NO 28

<211> LENGTH: 901

<212> TYPE: PRT

<213> ORGANISM: Artificial Sequence

<220> FEATURE:

<223> OTHER INFORMATION: SFP2-str-113 SGSR-RLuc2 mutant protein

<400> SEQUENCE: 28

Met Ser Asp Arg His Trp Leu Asp Ile Thr Thr Tyr Ser Asp His Ile
1 5 10 15

Gly Phe Thr Ile Ser Thr Ile Ala Asn Phe Val Leu Ile Leu Leu Leu
20 25 30

Val Phe Arg Pro Thr Lys Ser Tyr Gly Ser Tyr Lys Tyr Leu Met Ile
35 40 45

Thr Phe Cys Val Phe Ser Leu Phe Tyr Thr Ser Ile Glu Thr Phe Leu
50 55 60

Arg Pro Leu Ile His Ile Tyr Asp Asn Thr Ile Phe Val Ile Gln Arg
65 70 75 80

Lys Arg Phe Gln Tyr Ser Glu Gly Thr Ala Arg Ala Ile Ser Ser Thr
85 90 95

Tyr Cys Gly Cys Tyr Ala Met Ser Phe Thr Leu Phe Ala Val His Phe
100 105 110

Val Tyr Arg Tyr Tyr Ala Ala Cys Lys Pro Asp Asn Leu Arg Tyr Phe
115 120 125

Gln Gly Cys Tyr Phe Val Ala Trp Val Phe Gly Ala Met Ala Val Ala
130 135 140

Ala Ser Trp Gly Phe Ala Ala Phe Ile Leu Tyr Pro Glu Thr Glu Arg
145 150 155 160

Thr Arg Thr Ala Leu Ile His Val Ile Gln Thr Ser Tyr Glu Leu Asp
165 170 175

Pro Glu Trp Val Gly Asn Val Pro Tyr Ser Tyr Trp Arg Thr Glu Asn
180 185 190

Gly Val Glu Tyr Leu Asn Pro Arg Asn Val Ile Gly Ile Phe Gln His
195 200 205

Gly Val Ile Met Ile Leu Ser Phe Gly Thr Val Phe Tyr Cys Gly Phe
210 215 220

Asn Thr Tyr Lys Thr Leu Asn Gly Ser Leu Gly Val Ser Glu Lys Thr
225 230 235 240

Ser Gly Met Val Ser Lys Gly Glu Glu Leu Phe Thr Gly Val Val Pro
245 250 255

Ile Leu Val Glu Leu Asp Gly Asp Val Asn Gly His Lys Phe Ser Val
260 265 270

Ser Gly Glu Gly Glu Gly Asp Ala Thr Tyr Gly Lys Leu Thr Leu Lys
275 280 285

Phe Ile Cys Thr Thr Gly Lys Leu Pro Val Pro Trp Pro Thr Leu Val
290 295 300

Thr Thr Leu Ser Tyr Gly Val Gln Cys Phe Ser Arg Tyr Pro Asp His
305 310 315 320

Met Lys Gln His Asp Phe Phe Lys Ser Ala Met Pro Glu Gly Tyr Val

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325					330					335					
Gln	Glu	Arg	Thr	Ile	Phe	Phe	Lys	Asp	Asp	Gly	Asn	Tyr	Lys	Thr	Arg
			340					345					350		
Ala	Glu	Val	Lys	Phe	Glu	Gly	Asp	Thr	Leu	Val	Asn	Arg	Ile	Glu	Leu
		355					360					365			
Lys	Gly	Ile	Asp	Phe	Lys	Glu	Asp	Gly	Asn	Ile	Leu	Gly	His	Lys	Leu
	370					375					380				
Glu	Tyr	Asn	Tyr	Asn	Ser	His	Asn	Val	Tyr	Ile	Met	Ala	Asp	Lys	Gln
385					390					395					400
Lys	Asn	Gly	Ile	Lys	Val	Asn	Phe	Lys	Ile	Arg	His	Asn	Ile	Glu	Asp
				405					410					415	
Gly	Ser	Val	Gln	Leu	Ala	Asp	His	Tyr	Gln	Gln	Asn	Thr	Pro	Ile	Gly
			420					425						430	
Asp	Gly	Pro	Val	Leu	Leu	Pro	Asp	Asn	His	Tyr	Leu	Ser	Thr	Gln	Ser
		435					440						445		
Ala	Leu	Ser	Lys	Asp	Pro	Asn	Glu	Lys	Arg	Asp	His	Met	Val	Leu	Leu
450						455					460				
Glu	Phe	Val	Thr	Ala	Ala	Gly	Ile	Thr	Leu	Gly	Met	Asp	Glu	Leu	Tyr
465					470					475					480
Lys	Val	Asp	Lys	Glu	Met	His	Thr	Gln	Leu	Phe	Lys	Ala	Leu	Val	Leu
				485					490						495
Gln	Thr	Ile	Ile	Pro	Thr	Thr	Leu	Met	Tyr	Ile	Pro	Thr	Thr	Met	Leu
			500					505						510	
Phe	Val	Thr	Pro	Phe	Val	Gly	Leu	Asn	Ile	Gly	Cys	Tyr	Gly	Asn	Ile
		515					520						525		
Thr	Thr	Ala	Thr	Val	His	Leu	Tyr	Pro	Gly	Ile	Asp	Pro	Val	Val	Leu
530						535					540				
Ile	Phe	Ile	Ile	Arg	Asp	Phe	Arg	Gln	Thr	Ile	Leu	Arg	Pro	Phe	Arg
545					550					555					560
Cys	Phe	Tyr	Arg	Ser	Asn	Ser	Val	Glu	Asn	Thr	Ala	Thr	Ile	Arg	Gln
				565					570					575	
Tyr	Gln	Gln	Ser	Ser	Ser	Lys	Gly	Ser	Arg	Glu	Phe	Gly	Thr	Met	Thr
			580					585						590	
Ser	Lys	Val	Tyr	Asp	Pro	Glu	Gln	Arg	Lys	Arg	Met	Ile	Thr	Gly	Pro
		595					600						605		
Gln	Trp	Trp	Ala	Arg	Cys	Lys	Gln	Met	Asn	Val	Leu	Asp	Ser	Phe	Ile
610						615						620			
Asn	Tyr	Tyr	Asp	Ser	Glu	Lys	His	Ala	Glu	Asn	Ala	Val	Ile	Phe	Leu
625					630					635					640
His	Gly	Asn	Ala	Ala	Ser	Ser	Tyr	Leu	Trp	Arg	His	Val	Val	Pro	His
				645					650					655	
Ile	Glu	Pro	Val	Ala	Arg	Cys	Ile	Ile	Pro	Asp	Leu	Ile	Gly	Met	Gly
			660					665						670	
Lys	Ser	Gly	Lys	Ser	Gly	Asn	Gly	Ser	Tyr	Arg	Leu	Leu	Asp	His	Tyr
		675					680						685		
Lys	Tyr	Leu	Thr	Ala	Trp	Phe	Glu	Leu	Leu	Asn	Leu	Pro	Lys	Lys	Ile
	690					695						700			
Ile	Phe	Val	Gly	His	Asp	Trp	Gly	Ala	Ala	Leu	Ala	Phe	His	Tyr	Ser
705					710					715					720
Tyr	Glu	His	Gln	Asp	Lys	Ile	Lys	Ala	Ile	Val	His	Ala	Glu	Ser	Val
				725					730					735	
Val	Asp	Val	Ile	Glu	Ser	Trp	Asp	Glu	Trp	Pro	Asp	Ile	Glu	Glu	Asp
			740					745						750	

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Ile Ala Leu Ile Lys Ser Glu Glu Gly Glu Lys Met Val Leu Glu Asn
 755 760 765

Asn Phe Phe Val Glu Thr Val Leu Pro Ser Lys Ile Met Arg Lys Leu
 770 775 780

Glu Pro Glu Glu Phe Ala Ala Tyr Leu Glu Pro Phe Lys Glu Lys Gly
 785 790 795 800

Glu Val Arg Arg Pro Thr Leu Ser Trp Pro Arg Glu Ile Pro Leu Val
 805 810 815

Lys Gly Gly Lys Pro Asp Val Val Gln Ile Val Arg Asn Tyr Asn Ala
 820 825 830

Tyr Leu Arg Ala Ser Asp Asp Leu Pro Lys Met Phe Ile Glu Ser Asp
 835 840 845

Pro Gly Phe Phe Ser Asn Ala Ile Val Glu Gly Ala Lys Lys Phe Pro
 850 855 860

Asn Thr Glu Phe Val Lys Val Lys Gly Leu His Phe Ser Gln Glu Asp
 865 870 875 880

Ala Pro Asp Glu Met Gly Lys Tyr Ile Lys Ser Phe Val Glu Arg Val
 885 890 895

Leu Lys Asn Glu Gln
 900

<210> SEQ ID NO 29
 <211> LENGTH: 908
 <212> TYPE: PRT
 <213> ORGANISM: Artificial Sequence
 <220> FEATURE:
 <223> OTHER INFORMATION: GFP2-str-114 SGSR-RLuc2 mutant protein

<400> SEQUENCE: 29

Met Ser Asp Ile Tyr Trp Ile Gln Ile Thr Glu Val Cys Ser Phe Val
 1 5 10 15

Gly Phe Met Leu Ser Val Leu Gly Asn Ser Thr Leu Leu Val Leu Leu
 20 25 30

Ser Gly Lys Ser Ile Asp Gly Ile Gly Thr Tyr Arg Tyr Leu Met Ile
 35 40 45

Thr Phe Cys Val Phe Ser Leu Leu Phe Thr Ile Leu Glu Asp Phe Ile
 50 55 60

Arg Pro Leu Met His His Tyr Asn Asn Thr Ile Ile Val Leu Gln Arg
 65 70 75 80

Lys Arg Phe Gln Phe Ser Asp Ser Thr Ala Arg Ile Leu Thr Val Ser
 85 90 95

Tyr Cys Gly Cys Phe Ala Met Cys Phe Val Met Phe Ala Val His Phe
 100 105 110

Ile Tyr Arg Tyr Leu Val Ala Cys His Pro Thr Lys Leu His Tyr Phe
 115 120 125

Arg Pro Lys Asn Phe Ile Phe Trp Leu Ser Gly Met Leu Phe Ile Ala
 130 135 140

Gly Ser Trp Val Ala Ile Ala Tyr Val Phe Phe Gln Glu Asp Leu Glu
 145 150 155 160

Thr Arg Thr Asp Leu Val Phe Ile Leu Ser Thr Cys Tyr Asn Leu Thr
 165 170 175

Pro Asp Asp Val Gly His Val Pro Tyr Ala Phe Tyr Lys Thr Gln Gly
 180 185 190

Asn Thr Arg Val Ile Arg Trp Asp Asn Met Ile Gly Val Ile His His
 195 200 205

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Met Ile Val Met Thr Ile Ser Ile Ser Ala Val Phe Tyr Phe Gly Ile
 210 215 220
 Lys Thr Tyr Thr Arg Ile Met Ser Phe Lys Gly Lys Ser Gln Lys Thr
 225 230 235 240
 Ser Gly Met Val Ser Lys Gly Glu Glu Leu Phe Thr Gly Val Val Pro
 245 250 255
 Ile Leu Val Glu Leu Asp Gly Asp Val Asn Gly His Lys Phe Ser Val
 260 265 270
 Ser Gly Glu Gly Glu Gly Asp Ala Thr Tyr Gly Lys Leu Thr Leu Lys
 275 280 285
 Phe Ile Cys Thr Thr Gly Lys Leu Pro Val Pro Trp Pro Thr Leu Val
 290 295 300
 Thr Thr Leu Ser Tyr Gly Val Gln Cys Phe Ser Arg Tyr Pro Asp His
 305 310 315 320
 Met Lys Gln His Asp Phe Phe Lys Ser Ala Met Pro Glu Gly Tyr Val
 325 330 335
 Gln Glu Arg Thr Ile Phe Phe Lys Asp Asp Gly Asn Tyr Lys Thr Arg
 340 345 350
 Ala Glu Val Lys Phe Glu Gly Asp Thr Leu Val Asn Arg Ile Glu Leu
 355 360 365
 Lys Gly Ile Asp Phe Lys Glu Asp Gly Asn Ile Leu Gly His Lys Leu
 370 375 380
 Glu Tyr Asn Tyr Asn Ser His Asn Val Tyr Ile Met Ala Asp Lys Gln
 385 390 395 400
 Lys Asn Gly Ile Lys Val Asn Phe Lys Ile Arg His Asn Ile Glu Asp
 405 410 415
 Gly Ser Val Gln Leu Ala Asp His Tyr Gln Gln Asn Thr Pro Ile Gly
 420 425 430
 Asp Gly Pro Val Leu Leu Pro Asp Asn His Tyr Leu Ser Thr Gln Ser
 435 440 445
 Ala Leu Ser Lys Asp Pro Asn Glu Lys Arg Asp His Met Val Leu Leu
 450 455 460
 Glu Phe Val Thr Ala Ala Gly Ile Thr Leu Gly Met Asp Glu Leu Tyr
 465 470 475 480
 Lys Val Asp Lys Asp Leu Gln Asn Gln Phe Phe Thr Ala Leu Val Ala
 485 490 495
 Gln Thr Val Val Pro Leu Ile Phe Met Phe Ile Pro Asn Met Val Leu
 500 505 510
 Thr Thr Ala Ala Leu Ile Asp Gly Thr Phe Gly Ser Trp Ala Asn Ile
 515 520 525
 Thr Val Val Met Asn His Leu Tyr Pro Ala Ala Asp Pro Phe Val Ile
 530 535 540
 Leu Phe Ile Ile Lys Gly Phe Arg Asn Ser Ile Arg Asn Val Ile Tyr
 545 550 555 560
 Arg Cys Thr Lys Thr Lys Lys Ala Ser Val Ser Ser Val Val Arg Gly
 565 570 575
 Ile Glu Ala Gln Ser Lys Lys Gln Ser Phe Ser Arg Val Asp Ile Ser
 580 585 590
 Arg Glu Phe Gly Thr Met Thr Ser Lys Val Tyr Asp Pro Glu Gln Arg
 595 600 605
 Lys Arg Met Ile Thr Gly Pro Gln Trp Trp Ala Arg Cys Lys Gln Met
 610 615 620

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Asn Val Leu Asp Ser Phe Ile Asn Tyr Tyr Asp Ser Glu Lys His Ala
 625 630 635 640

Glu Asn Ala Val Ile Phe Leu His Gly Asn Ala Ala Ser Ser Tyr Leu
 645 650 655

Trp Arg His Val Val Pro His Ile Glu Pro Val Ala Arg Cys Ile Ile
 660 665 670

Pro Asp Leu Ile Gly Met Gly Lys Ser Gly Lys Ser Gly Asn Gly Ser
 675 680 685

Tyr Arg Leu Leu Asp His Tyr Lys Tyr Leu Thr Ala Trp Phe Glu Leu
 690 695 700

Leu Asn Leu Pro Lys Lys Ile Ile Phe Val Gly His Asp Trp Gly Ala
 705 710 715 720

Ala Leu Ala Phe His Tyr Ser Tyr Glu His Gln Asp Lys Ile Lys Ala
 725 730 735

Ile Val His Ala Glu Ser Val Val Asp Val Ile Glu Ser Trp Asp Glu
 740 745 750

Trp Pro Asp Ile Glu Glu Asp Ile Ala Leu Ile Lys Ser Glu Glu Gly
 755 760 765

Glu Lys Met Val Leu Glu Asn Asn Phe Phe Val Glu Thr Val Leu Pro
 770 775 780

Ser Lys Ile Met Arg Lys Leu Glu Pro Glu Glu Phe Ala Ala Tyr Leu
 785 790 795 800

Glu Pro Phe Lys Glu Lys Gly Glu Val Arg Arg Pro Thr Leu Ser Trp
 805 810 815

Pro Arg Glu Ile Pro Leu Val Lys Gly Gly Lys Pro Asp Val Val Gln
 820 825 830

Ile Val Arg Asn Tyr Asn Ala Tyr Leu Arg Ala Ser Asp Asp Leu Pro
 835 840 845

Lys Met Phe Ile Glu Ser Asp Pro Gly Phe Phe Ser Asn Ala Ile Val
 850 855 860

Glu Gly Ala Lys Lys Phe Pro Asn Thr Glu Phe Val Lys Val Lys Gly
 865 870 875 880

Leu His Phe Ser Gln Glu Asp Ala Pro Asp Glu Met Gly Lys Tyr Ile
 885 890 895

Lys Ser Phe Val Glu Arg Val Leu Lys Asn Glu Gln
 900 905

<210> SEQ ID NO 30
 <211> LENGTH: 901
 <212> TYPE: PRT
 <213> ORGANISM: Artificial Sequence
 <220> FEATURE:
 <223> OTHER INFORMATION: GFP2-str-113/114 SGSR-RLuc2 mutant protein

<400> SEQUENCE: 30

Met Ser Asp Ile Tyr Trp Ile Gln Ile Thr Glu Val Cys Ser Phe Val
 1 5 10 15

Gly Phe Met Leu Ser Val Leu Gly Asn Ser Thr Leu Leu Val Leu Leu
 20 25 30

Ser Gly Lys Ser Ile Asp Gly Ile Gly Thr Tyr Arg Tyr Leu Met Ile
 35 40 45

Thr Phe Cys Val Phe Ser Leu Leu Phe Thr Ile Leu Glu Asp Phe Ile
 50 55 60

Arg Pro Leu Met His His Tyr Asn Asn Thr Ile Ile Val Leu Gln Arg
 65 70 75 80

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Lys Arg Phe Gln Phe Ser Asp Ser Thr Ala Arg Ile Leu Thr Val Ser
 85 90 95
 Tyr Cys Gly Cys Phe Ala Met Cys Phe Val Met Phe Ala Val His Phe
 100 105 110
 Ile Tyr Arg Tyr Leu Val Ala Cys His Pro Thr Lys Leu His Tyr Phe
 115 120 125
 Arg Pro Lys Asn Phe Ile Phe Trp Leu Ser Gly Met Leu Phe Ile Ala
 130 135 140
 Gly Ser Trp Val Ala Ile Ala Tyr Val Phe Phe Gln Glu Asp Leu Glu
 145 150 155 160
 Thr Arg Thr Asp Leu Val Phe Ile Leu Ser Thr Cys Tyr Asn Leu Thr
 165 170 175
 Pro Asp Asp Val Gly His Val Pro Tyr Ala Phe Tyr Lys Thr Gln Gly
 180 185 190
 Asn Thr Arg Val Ile Arg Trp Asp Asn Met Ile Gly Val Ile His His
 195 200 205
 Met Ile Val Met Thr Ile Ser Ile Ser Ala Val Phe Tyr Phe Gly Ile
 210 215 220
 Lys Thr Tyr Thr Arg Ile Met Ser Phe Lys Gly Lys Ser Gln Lys Thr
 225 230 235 240
 Ser Gly Met Val Ser Lys Gly Glu Glu Leu Phe Thr Gly Val Val Pro
 245 250 255
 Ile Leu Val Glu Leu Asp Gly Asp Val Asn Gly His Lys Phe Ser Val
 260 265 270
 Ser Gly Glu Gly Glu Gly Asp Ala Thr Tyr Gly Lys Leu Thr Leu Lys
 275 280 285
 Phe Ile Cys Thr Thr Gly Lys Leu Pro Val Pro Trp Pro Thr Leu Val
 290 295 300
 Thr Thr Leu Ser Tyr Gly Val Gln Cys Phe Ser Arg Tyr Pro Asp His
 305 310 315 320
 Met Lys Gln His Asp Phe Phe Lys Ser Ala Met Pro Glu Gly Tyr Val
 325 330 335
 Gln Glu Arg Thr Ile Phe Phe Lys Asp Asp Gly Asn Tyr Lys Thr Arg
 340 345 350
 Ala Glu Val Lys Phe Glu Gly Asp Thr Leu Val Asn Arg Ile Glu Leu
 355 360 365
 Lys Gly Ile Asp Phe Lys Glu Asp Gly Asn Ile Leu Gly His Lys Leu
 370 375 380
 Glu Tyr Asn Tyr Asn Ser His Asn Val Tyr Ile Met Ala Asp Lys Gln
 385 390 395 400
 Lys Asn Gly Ile Lys Val Asn Phe Lys Ile Arg His Asn Ile Glu Asp
 405 410 415
 Gly Ser Val Gln Leu Ala Asp His Tyr Gln Gln Asn Thr Pro Ile Gly
 420 425 430
 Asp Gly Pro Val Leu Leu Pro Asp Asn His Tyr Leu Ser Thr Gln Ser
 435 440 445
 Ala Leu Ser Lys Asp Pro Asn Glu Lys Arg Asp His Met Val Leu Leu
 450 455 460
 Glu Phe Val Thr Ala Ala Gly Ile Thr Leu Gly Met Asp Glu Leu Tyr
 465 470 475 480
 Lys Val Asp Lys Glu Met His Thr Gln Leu Phe Lys Ala Leu Val Leu
 485 490 495
 Gln Thr Ile Ile Pro Thr Thr Leu Met Tyr Ile Pro Thr Thr Met Leu

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500					505					510					
Phe	Val	Thr	Pro	Phe	Val	Gly	Leu	Asn	Ile	Gly	Cys	Tyr	Gly	Asn	Ile
	515						520					525			
Thr	Thr	Ala	Thr	Val	His	Leu	Tyr	Pro	Gly	Ile	Asp	Pro	Val	Val	Leu
	530					535					540				
Ile	Phe	Ile	Ile	Arg	Asp	Phe	Arg	Gln	Thr	Ile	Leu	Arg	Pro	Phe	Arg
545					550					555					560
Cys	Phe	Tyr	Arg	Ser	Asn	Ser	Val	Glu	Asn	Thr	Ala	Thr	Ile	Arg	Gln
				565					570						575
Tyr	Gln	Gln	Ser	Ser	Ser	Lys	Gly	Ser	Arg	Glu	Phe	Gly	Thr	Met	Thr
			580					585						590	
Ser	Lys	Val	Tyr	Asp	Pro	Glu	Gln	Arg	Lys	Arg	Met	Ile	Thr	Gly	Pro
		595					600					605			
Gln	Trp	Trp	Ala	Arg	Cys	Lys	Gln	Met	Asn	Val	Leu	Asp	Ser	Phe	Ile
610						615						620			
Asn	Tyr	Tyr	Asp	Ser	Glu	Lys	His	Ala	Glu	Asn	Ala	Val	Ile	Phe	Leu
625					630					635					640
His	Gly	Asn	Ala	Ala	Ser	Ser	Tyr	Leu	Trp	Arg	His	Val	Val	Pro	His
				645					650						655
Ile	Glu	Pro	Val	Ala	Arg	Cys	Ile	Ile	Pro	Asp	Leu	Ile	Gly	Met	Gly
			660					665						670	
Lys	Ser	Gly	Lys	Ser	Gly	Asn	Gly	Ser	Tyr	Arg	Leu	Leu	Asp	His	Tyr
		675				680						685			
Lys	Tyr	Leu	Thr	Ala	Trp	Phe	Glu	Leu	Leu	Asn	Leu	Pro	Lys	Lys	Ile
	690					695					700				
Ile	Phe	Val	Gly	His	Asp	Trp	Gly	Ala	Ala	Leu	Ala	Phe	His	Tyr	Ser
705					710					715					720
Tyr	Glu	His	Gln	Asp	Lys	Ile	Lys	Ala	Ile	Val	His	Ala	Glu	Ser	Val
				725					730						735
Val	Asp	Val	Ile	Glu	Ser	Trp	Asp	Glu	Trp	Pro	Asp	Ile	Glu	Glu	Asp
			740					745					750		
Ile	Ala	Leu	Ile	Lys	Ser	Glu	Glu	Gly	Glu	Lys	Met	Val	Leu	Glu	Asn
		755					760					765			
Asn	Phe	Phe	Val	Glu	Thr	Val	Leu	Pro	Ser	Lys	Ile	Met	Arg	Lys	Leu
	770					775						780			
Glu	Pro	Glu	Glu	Phe	Ala	Ala	Tyr	Leu	Glu	Pro	Phe	Lys	Glu	Lys	Gly
785					790					795					800
Glu	Val	Arg	Arg	Pro	Thr	Leu	Ser	Trp	Pro	Arg	Glu	Ile	Pro	Leu	Val
				805					810						815
Lys	Gly	Gly	Lys	Pro	Asp	Val	Val	Gln	Ile	Val	Arg	Asn	Tyr	Asn	Ala
			820					825					830		
Tyr	Leu	Arg	Ala	Ser	Asp	Asp	Leu	Pro	Lys	Met	Phe	Ile	Glu	Ser	Asp
		835					840						845		
Pro	Gly	Phe	Phe	Ser	Asn	Ala	Ile	Val	Glu	Gly	Ala	Lys	Lys	Phe	Pro
	850					855							860		
Asn	Thr	Glu	Phe	Val	Lys	Val	Lys	Gly	Leu	His	Phe	Ser	Gln	Glu	Asp
865					870					875					880
Ala	Pro	Asp	Glu	Met	Gly	Lys	Tyr	Ile	Lys	Ser	Phe	Val	Glu	Arg	Val
				885					890						895
Leu	Lys	Asn	Glu	Gln											
			900												

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<211> LENGTH: 890
<212> TYPE: PRT
<213> ORGANISM: Artificial Sequence
<220> FEATURE:
<223> OTHER INFORMATION: GFP2-str-115 SGSR-RLuc2 mutant protein

<400> SEQUENCE: 31
Met Thr Asp Gln His Trp Val Ile Ile Thr Asp Ile Ala Gly Pro Ile
1          5          10          15
Gly Phe Ser Met Ser Ile Phe Ser Asn Ser Ile Leu Leu Phe Leu Ile
20          25          30
Phe Ser His Ser Ser Pro Ile Lys Gly Pro Tyr Lys Arg Met Leu Ile
35          40          45
Val Phe Cys Ile Phe Thr Val Phe Tyr Ser Phe Val Glu Val Met Leu
50          55          60
Gln Pro Leu Ile His Ile Tyr Asp Asp Thr Leu Phe Leu Ile His Arg
65          70          75          80
Lys Arg Ile Asp Leu Pro Lys Trp Leu Thr Arg Leu Val Pro Thr Thr
85          90          95
Tyr Cys Trp Cys Tyr Ala Met Ser Phe Ser Leu Phe Ala Leu Gln Phe
100         105         110
Leu Tyr Arg Tyr Val Ala Val Cys Lys Pro Gln Tyr Val Asp Leu Phe
115         120         125
Val Gly Cys His Phe Tyr Ala Trp Val Val Leu Ile Leu Ser Leu Ala
130         135         140
Thr Ser Trp Gly Leu Thr Ala Ala Phe Met Phe Pro Gln Thr Asp Arg
145         150         155         160
Thr Thr Glu Ile Phe Leu His Ile Ile Tyr Ser Ser Tyr Asp Leu Glu
165         170         175
Pro Tyr Trp Thr Asp Tyr Val Ala Tyr Lys Tyr Phe Asp Thr Asp Glu
180         185         190
Asn Asn Val Arg Trp Val Asn Val Leu Ser Phe Phe Gly Val Leu Gln
195         200         205
His Gly Ile Val Ile Thr Leu Ser Phe Gly Thr Leu Tyr Tyr Cys Gly
210         215         220
Ile Asn Thr Tyr Leu Lys Ile Lys Lys His Thr Gly Thr Ser Asn Arg
225         230         235         240
Thr Ser Gly Met Val Ser Lys Gly Glu Glu Leu Phe Thr Gly Val Val
245         250         255
Pro Ile Leu Val Glu Leu Asp Gly Asp Val Asn Gly His Lys Phe Ser
260         265         270
Val Ser Gly Glu Gly Glu Gly Asp Ala Thr Tyr Gly Lys Leu Thr Leu
275         280         285
Lys Phe Ile Cys Thr Thr Gly Lys Leu Pro Val Pro Trp Pro Thr Leu
290         295         300
Val Thr Thr Leu Ser Tyr Gly Val Gln Cys Phe Ser Arg Tyr Pro Asp
305         310         315         320
His Met Lys Gln His Asp Phe Phe Lys Ser Ala Met Pro Glu Gly Tyr
325         330         335
Val Gln Glu Arg Thr Ile Phe Phe Lys Asp Asp Gly Asn Tyr Lys Thr
340         345         350
Arg Ala Glu Val Lys Phe Glu Gly Asp Thr Leu Val Asn Arg Ile Glu
355         360         365
Leu Lys Gly Ile Asp Phe Lys Glu Asp Gly Asn Ile Leu Gly His Lys
370         375         380

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Leu Glu Tyr Asn Tyr Asn Ser His Asn Val Tyr Ile Met Ala Asp Lys
 385 390 395 400
 Gln Lys Asn Gly Ile Lys Val Asn Phe Lys Ile Arg His Asn Ile Glu
 405 410 415
 Asp Gly Ser Val Gln Leu Ala Asp His Tyr Gln Gln Asn Thr Pro Ile
 420 425 430
 Gly Asp Gly Pro Val Leu Leu Pro Asp Asn His Tyr Leu Ser Thr Gln
 435 440 445
 Ser Ala Leu Ser Lys Asp Pro Asn Glu Lys Arg Asp His Met Val Leu
 450 455 460
 Leu Glu Phe Val Thr Ala Ala Gly Ile Thr Leu Gly Met Asp Glu Leu
 465 470 475 480
 Tyr Lys Val Asp Arg Cys Ile Gln Leu Gln Leu Phe Arg Ala Leu Val
 485 490 495
 Ala Gln Thr Ile Leu Pro Met Phe Met Met Tyr Ile Pro Val Gly Phe
 500 505 510
 Met Phe Ala Cys Pro Tyr Phe Asp Leu Gln Leu Gly Ala Tyr Thr Asn
 515 520 525
 Tyr Gln Thr Val Met Ala Gln Leu Tyr Pro Gly Ile Asp Pro Phe Val
 530 535 540
 Met Leu Phe Leu Ile Asp Ser Tyr Arg Ile Thr Ile Phe Gly Trp Leu
 545 550 555 560
 Cys Pro Arg Phe Val Tyr Val Lys Pro Met His Ser Thr Tyr Thr Leu
 565 570 575
 Thr Ser Arg Met Thr Ser Lys Val Tyr Asp Pro Glu Gln Arg Lys Arg
 580 585 590
 Met Ile Thr Gly Pro Gln Trp Trp Ala Arg Cys Lys Gln Met Asn Val
 595 600 605
 Leu Asp Ser Phe Ile Asn Tyr Tyr Asp Ser Glu Lys His Ala Glu Asn
 610 615 620
 Ala Val Ile Phe Leu His Gly Asn Ala Ala Ser Ser Tyr Leu Trp Arg
 625 630 635 640
 His Val Val Pro His Ile Glu Pro Val Ala Arg Cys Ile Ile Pro Asp
 645 650 655
 Leu Ile Gly Met Gly Lys Ser Gly Lys Ser Gly Asn Gly Ser Tyr Arg
 660 665 670
 Leu Leu Asp His Tyr Lys Tyr Leu Thr Ala Trp Phe Glu Leu Leu Asn
 675 680 685
 Leu Pro Lys Lys Ile Ile Phe Val Gly His Asp Trp Gly Ala Ala Leu
 690 695 700
 Ala Phe His Tyr Ser Tyr Glu His Gln Asp Lys Ile Lys Ala Ile Val
 705 710 715 720
 His Ala Glu Ser Val Val Asp Val Ile Glu Ser Trp Asp Glu Trp Pro
 725 730 735
 Asp Ile Glu Glu Asp Ile Ala Leu Ile Lys Ser Glu Glu Gly Glu Lys
 740 745 750
 Met Val Leu Glu Asn Asn Phe Phe Val Glu Thr Val Leu Pro Ser Lys
 755 760 765
 Ile Met Arg Lys Leu Glu Pro Glu Glu Phe Ala Ala Tyr Leu Glu Pro
 770 775 780
 Phe Lys Glu Lys Gly Glu Val Arg Arg Pro Thr Leu Ser Trp Pro Arg
 785 790 795 800

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Glu Ile Pro Leu Val Lys Gly Gly Lys Pro Asp Val Val Gln Ile Val
 805 810 815
 Arg Asn Tyr Asn Ala Tyr Leu Arg Ala Ser Asp Asp Leu Pro Lys Met
 820 825 830
 Phe Ile Glu Ser Asp Pro Gly Phe Phe Ser Asn Ala Ile Val Glu Gly
 835 840 845
 Ala Lys Lys Phe Pro Asn Thr Glu Phe Val Lys Val Lys Gly Leu His
 850 855 860
 Phe Ser Gln Glu Asp Ala Pro Asp Glu Met Gly Lys Tyr Ile Lys Ser
 865 870 875 880
 Phe Val Glu Arg Val Leu Lys Asn Glu Gln
 885 890

<210> SEQ ID NO 32
 <211> LENGTH: 906
 <212> TYPE: PRT
 <213> ORGANISM: Artificial Sequence
 <220> FEATURE:
 <223> OTHER INFORMATION: GFP2-str-116 SGSR-RLuc2 mutant protein

<400> SEQUENCE: 32

Met Thr Asp Arg Arg Trp Val Ala Ile Thr Asp Ile Ala Gly Pro Ile
 1 5 10 15
 Gly Phe Thr Met Ser Ile Phe Ser Asn Ser Val Leu Leu Ser Leu Ile
 20 25 30
 Phe Ser Ser Ser Ser Pro Ile Lys Gly Ala Tyr Lys Asn Met Leu Ile
 35 40 45
 Val Leu Cys Ile Phe Thr Met Phe Tyr Ser Phe Val Glu Ile Met Leu
 50 55 60
 Gln Pro Leu Ile His Ile Tyr Asp Asp Thr Leu Phe Leu Ile His Arg
 65 70 75 80
 Lys Arg Phe Asp Leu Ser Lys Gly Ile Thr Arg Leu Ile Pro Thr Thr
 85 90 95
 Tyr Cys Trp Cys Tyr Ala Met Ser Phe Ser Leu Phe Ala Leu Gln Phe
 100 105 110
 Leu Tyr Arg Tyr Val Ala Val Cys Lys Pro His Leu Val Val Phe Phe
 115 120 125
 Thr Gly Cys Tyr Phe Tyr Tyr Trp Leu Ala Leu Ile Leu Ser Leu Ala
 130 135 140
 Thr Ser Trp Gly Leu Thr Ala Ala Phe Met Phe Pro Gln Thr Asn Arg
 145 150 155 160
 Thr Thr Glu Ser Phe Asn Tyr Val Ile Lys Thr Ser Tyr Asp Leu Asp
 165 170 175
 Pro Tyr Trp Thr Asp Tyr Val Ala Tyr Lys Tyr Phe Asp Thr Asp Glu
 180 185 190
 Asn His Val Arg Trp Val Asn Val Leu Ser Leu Phe Gly Val Leu Gln
 195 200 205
 His Gly Leu Val Ile Thr Leu Ser Phe Gly Thr Leu Phe Tyr Cys Gly
 210 215 220
 Ile Lys Thr Tyr Leu Ser Ile Thr Glu His Val Gly Met Ser Ser Lys
 225 230 235 240
 Thr Ser Gly Met Val Ser Lys Gly Glu Glu Leu Phe Thr Gly Val Val
 245 250 255
 Pro Ile Leu Val Glu Leu Asp Gly Asp Val Asn Gly His Lys Phe Ser
 260 265 270

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Val Ser Gly Glu Gly Glu Gly Asp Ala Thr Tyr Gly Lys Leu Thr Leu
 275 280 285
 Lys Phe Ile Cys Thr Thr Gly Lys Leu Pro Val Pro Trp Pro Thr Leu
 290 295 300
 Val Thr Thr Leu Ser Tyr Gly Val Gln Cys Phe Ser Arg Tyr Pro Asp
 305 310 315 320
 His Met Lys Gln His Asp Phe Phe Lys Ser Ala Met Pro Glu Gly Tyr
 325 330 335
 Val Gln Glu Arg Thr Ile Phe Phe Lys Asp Asp Gly Asn Tyr Lys Thr
 340 345 350
 Arg Ala Glu Val Lys Phe Glu Gly Asp Thr Leu Val Asn Arg Ile Glu
 355 360 365
 Leu Lys Gly Ile Asp Phe Lys Glu Asp Gly Asn Ile Leu Gly His Lys
 370 375 380
 Leu Glu Tyr Asn Tyr Asn Ser His Asn Val Tyr Ile Met Ala Asp Lys
 385 390 395 400
 Gln Lys Asn Gly Ile Lys Val Asn Phe Lys Ile Arg His Asn Ile Glu
 405 410 415
 Asp Gly Ser Val Gln Leu Ala Asp His Tyr Gln Gln Asn Thr Pro Ile
 420 425 430
 Gly Asp Gly Pro Val Leu Leu Pro Asp Asn His Tyr Leu Ser Thr Gln
 435 440 445
 Ser Ala Leu Ser Lys Asp Pro Asn Glu Lys Arg Asp His Met Val Leu
 450 455 460
 Leu Glu Phe Val Thr Ala Ala Gly Ile Thr Leu Gly Met Asp Glu Leu
 465 470 475 480
 Tyr Lys Val Asp Arg Ser Leu Gln Leu Gln Leu Phe Arg Ala Leu Val
 485 490 495
 Ala Gln Thr Cys Leu Pro Met Leu Met Met Tyr Met Pro Ile Gly Phe
 500 505 510
 Met Phe Ser Cys Pro Tyr Phe Asp Leu Gln Leu Gly Ala Val Thr Asn
 515 520 525
 Tyr Gln Thr Val Met Ala Gln Leu Tyr Pro Gly Ile Asp Pro Phe Met
 530 535 540
 Leu Leu Phe Leu Ile Asn Ala Tyr Arg Lys Thr Val Leu Ser Leu Ile
 545 550 555 560
 Cys Pro Asn Phe Ile Gln Lys Lys Tyr Val Gln Thr Ala Thr Thr Arg
 565 570 575
 Asp Gly Thr Asp Ala Ser Ala Thr Met Asn Ser Val Lys Ser Thr Gln
 580 585 590
 Leu Gly Thr Met Thr Ser Lys Val Tyr Asp Pro Glu Gln Arg Lys Arg
 595 600 605
 Met Ile Thr Gly Pro Gln Trp Trp Ala Arg Cys Lys Gln Met Asn Val
 610 615 620
 Leu Asp Ser Phe Ile Asn Tyr Tyr Asp Ser Glu Lys His Ala Glu Asn
 625 630 635 640
 Ala Val Ile Phe Leu His Gly Asn Ala Ala Ser Ser Tyr Leu Trp Arg
 645 650 655
 His Val Val Pro His Ile Glu Pro Val Ala Arg Cys Ile Ile Pro Asp
 660 665 670
 Leu Ile Gly Met Gly Lys Ser Gly Lys Ser Gly Asn Gly Ser Tyr Arg
 675 680 685
 Leu Leu Asp His Tyr Lys Tyr Leu Thr Ala Trp Phe Glu Leu Leu Asn

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690			695			700									
Leu	Pro	Lys	Lys	Ile	Ile	Phe	Val	Gly	His	Asp	Trp	Gly	Ala	Ala	Leu
705				710				715							720
Ala	Phe	His	Tyr	Ser	Tyr	Glu	His	Gln	Asp	Lys	Ile	Lys	Ala	Ile	Val
			725					730							735
His	Ala	Glu	Ser	Val	Val	Asp	Val	Ile	Glu	Ser	Trp	Asp	Glu	Trp	Pro
			740					745							750
Asp	Ile	Glu	Glu	Asp	Ile	Ala	Leu	Ile	Lys	Ser	Glu	Glu	Gly	Glu	Lys
			755					760							765
Met	Val	Leu	Glu	Asn	Asn	Phe	Phe	Val	Glu	Thr	Val	Leu	Pro	Ser	Lys
			770					775							780
Ile	Met	Arg	Lys	Leu	Glu	Pro	Glu	Glu	Phe	Ala	Ala	Tyr	Leu	Glu	Pro
			785					790							800
Phe	Lys	Glu	Lys	Gly	Glu	Val	Arg	Arg	Pro	Thr	Leu	Ser	Trp	Pro	Arg
				805						810					815
Glu	Ile	Pro	Leu	Val	Lys	Gly	Gly	Lys	Pro	Asp	Val	Val	Gln	Ile	Val
			820					825							830
Arg	Asn	Tyr	Asn	Ala	Tyr	Leu	Arg	Ala	Ser	Asp	Asp	Leu	Pro	Lys	Met
			835					840							845
Phe	Ile	Glu	Ser	Asp	Pro	Gly	Phe	Phe	Ser	Asn	Ala	Ile	Val	Glu	Gly
			850					855							860
Ala	Lys	Lys	Phe	Pro	Asn	Thr	Glu	Phe	Val	Lys	Val	Lys	Gly	Leu	His
			865					870							880
Phe	Ser	Gln	Glu	Asp	Ala	Pro	Asp	Glu	Met	Gly	Lys	Tyr	Ile	Lys	Ser
				885						890					895
Phe	Val	Glu	Arg	Val	Leu	Lys	Asn	Glu	Gln						
			900							905					

<210> SEQ ID NO 33

<211> LENGTH: 2670

<212> TYPE: DNA

<213> ORGANISM: Artificial Sequence

<220> FEATURE:

<223> OTHER INFORMATION: Nucleotide sequence encoding GFP2-OGOR-Rluc2 fusion

<400> SEQUENCE: 33

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atgtcgggag aattgtggat taccctagtt gacacagcgg acattgtcgg cgtcacccctc   60
accttctgtg tcaacattgt tcttctogga cttctgaaaa cacgtggaaa aaacttgggc   120
acttataaat atctcatggc gtttttctca gtattctcga ttttttacgc catcatcgag   180
ttcatattac gacctataat gcatattgag aacaccactt tctttttgat ctcaaggaaa   240
agattcaact actccaccaa acttgaaaa atcaactctg cgttttactg tgcttgtttt   300
gccaccagtt ttgtgtctc aggagttcac ttgtttatc gatattttgc aacttgcaaa   360
ccgaatctac ttcgtttgtt caacttgcca actcttctac tttggcact tggttgcaat   420
gtaccctgga caatgtggc tagtgtctca tatttttgt atccagatac cgagtacacg   480
gaagcggctg tcaccaatgt actaaataac cactataact ggatcaaaaa ggagaatgta   540
tcgtacattg catacgtcta ttaccaatac gaaaacggag taaggcatat ctacctcaaa   600
aacttgcttg gatgctttgt tcattacttt gtcattgtcga tgacgtttgt tgtgatgttc   660
tactgaggat atgccacgtg gaaaactatg aatgaacaca aggatgtatc tgatagaact   720
atggtgagca agggcgagga gctgttcacc ggggtggtgc ccatcctggt cgagctggac   780
ggcgacgtaa acggccacaa gttcagcgtg tccggcgagg gcgagggcga tgccacctac   840

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ggcaagctga ccctgaagtt catctgcacc accggcaagc tgeccgtgcc ctggcccacc 900
ctcgtgacca ccctgagcta cggcgtgcag tgcttcagcc gctaccccga ccacatgaag 960
cagcacgact tcttcaagtc cgccatgccc gaaggctacg tccaggagcg caccatcttc 1020
ttcaaggacg acggcaacta caagaccgcc gccgaggta agttcgaggg cgacaccctg 1080
gtgaaccgca tcgagctgaa gggcatcgac ttcaaggagg acggcaacat cctggggcac 1140
aagctggagt acaactacaa cagccacaac gtctatatca tggccgacaa gcagaagaac 1200
ggcatcaagg tgaacttcaa gatccgccac aacatcgagg acggcagcgt gcagctcgcc 1260
gaccactacc agcagaacac ccccatcggc gacggccccc tgctgctgcc cgacaaccac 1320
tacctgagca cccagtcgcg cctgagcaaa gaccccaacg agaagcgcga tcacatggtc 1380
ctgctggagt tcgtgaccgc cgccgggatc actctcgcca tggacgagct gtacaagcga 1440
gcgctacaga aacaactttt caaagcttta gttcttcaga cactcatccc aactatcttc 1500
atgtacgccc caactggagt catgttcatc gcaccgtttt ttgacgtgaa tttgaatgca 1560
aacgccaatt tcattgtggt ttgctcattt ctgtacccgg gactcgatcc actcattctg 1620
atthttgatca ttcgtgattt ccgaagaaca atattcaatt tcttgtgtgg aaagaaaaac 1680
agtgttgatg aatcccgtc gacaacaaga gccaatttgt ctcaagtcc gacgatgacc 1740
agcaagggtg acgaccocga gcagaggaag aggatgatca ccggccccc gtgggtgggc 1800
aggtgcaagc agatgaacgt gctggacagc ttcatacaact actacgacag cgagaagcac 1860
gccgagaacg ccgtgatctt cctgcacggc aacgcgcgta gcagctacct gtggaggcac 1920
gtggtgcccc acatcgagcc cgtggccagg tgcatcatcc ccgatctgat cggcatgggc 1980
aagagcggca agagcggcaa cggcagctac aggctgctgg accactacaa gtacctgacc 2040
gcctggttcg agctcctgaa cctgcccagg aagatcatct tcgtgggcca cgactggggc 2100
gccgcccctg ccttccaacta cagctacgag caccaggaca agatcaaggc catcgtgcac 2160
gccgagagcg tgggtgacgt gatcgagagc tgggacgagt ggcagacat cgaggaggac 2220
atcgcccctg tcaagagcga ggagggcgag aagatgggtc tggagaacaa cttcttcgtg 2280
gagaccgtgc tgcccagcaa gatcatgaga aagctggagc ccgaggagtt cgccgcctac 2340
ctggagccct tcaaggagaa gggcgagggt agaagaccca ccctgagctg gccagagag 2400
atccccctgg tgaagggcgg caagcccgcac gtggtgcaga tcgtgagaaa ctacaacgcc 2460
tacctgagag ccagcgaaga cctgcccagg atgttcatcg agagcgaccc cggctttctt 2520
agcaacgcca tcgtggaggg cgccaagaag ttccccacaa ccgagttcgt gaaggtgaag 2580
ggcctgcact tcagccagga ggacgcccc gacgagatgg gcaagtacat caagagcttc 2640
gtggagagag tgctgaagaa cgagcagtaa 2670

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<210> SEQ ID NO 34

<211> LENGTH: 2670

<212> TYPE: DNA

<213> ORGANISM: Artificial Sequence

<220> FEATURE:

<223> OTHER INFORMATION: Nucleotide sequence encoding GFP2-OGOR-RLuc2 mutant protein

<400> SEQUENCE: 34

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atgtcgggag aattgtggat taccctagtt gacacagcgg acattgtcgg cgtcaccctc 60
accttctgtg tcaacattgt tcttctcgga cttctgaaaa cacgtggaaa aaacttgggc 120
acttataaat atctcatggc gttttttctca gtattctcga ttttttacgc catcatcgag 180

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ttcatattac	gacctataat	gcatattgag	aacaccactt	tctttttgat	ctcaaggaaa	240
agattcaact	actccaccaa	acttgaaaa	atcaactctg	cgttttactg	tgcttgttt	300
gccaccagtt	ttgttgtctc	aggagtttat	tttgtttatc	gatattttgc	aacttgcaaa	360
cogaatctac	ttcgtttggt	caacttgcca	actctttctac	tttggccact	tggttgcagt	420
gtacccggtga	caatgtgggc	tagtgtctca	tattttttgt	atccagatac	cgagtacacg	480
gaagcggctg	tcaccaatgt	actaaataac	cactataact	ggatcaaaaa	ggagaatgta	540
tcgtacattg	catacgtota	ttaccaatac	gaaaacggag	taaggcatat	ctacctcaaa	600
aacttgcttg	gatgctttgt	tcattaactt	gtcatgtcga	tgacgtttgt	tgtgatgttc	660
tactgcggtat	atgccacgtg	gaaaactatg	aatgaacaca	aggatgtatc	tgatagaact	720
atggtgagca	aggcggagga	gctgttcacc	gggtggtgc	ccatcctggt	cgagctggac	780
ggcgacgtaa	acggccacaa	gttcagcgtg	tccggcgagg	gcgagggcga	tgccacctac	840
ggcaagctga	ccctgaagtt	catctgcacc	accggcaagc	tgcccgtgcc	ctggcccacc	900
ctcgtgacca	ccctgagcta	cggcgtgcag	tgcttcagcc	gctaccccga	ccacatgaag	960
cagcacgact	tcttcaagtc	cgccatgcc	gaaggctacg	tccaggagcg	caccatcttc	1020
ttcaaggacg	acggcaacta	caagaccgc	gccgaggtga	agttcgaggg	cgacaccctg	1080
gtgaaccgca	tcgagctgaa	gggcatcgac	ttcaaggagg	acggcaacat	cctggggcac	1140
aagctggagt	acaactacaa	cagccacaac	gtctatatca	tggccgacaa	gcagaagaac	1200
ggcatcaagg	tgaacttcaa	gatccgccac	aacatcgagg	acggcagcgt	gcagctcgcc	1260
gaccactacc	agcagaacac	ccccatcggc	gacggccccg	tgctgctgcc	cgacaaccac	1320
tacctgagca	cccagtcgpc	cctgagcaaa	gaccccaacg	agaagcgcca	tcacatggtc	1380
ctgctggagt	tcgtgaccgc	cgccgggatc	actctcgcca	tggacgagct	gtacaagcga	1440
gogctacaga	aacaactttt	caaagcttta	gttcttcaga	cactcatccc	aactatcttc	1500
atgtacgccc	caactggagt	catgttcatc	gcaccgtttt	ttgacgtgaa	tttgaatgca	1560
aacgccaatt	tcattgtggt	ttgctcattt	ctgtaccggg	gactcgatcc	actcattctg	1620
atthtgatca	ttcgtgattt	ccgaagaaca	atattcaatt	tcttgtgtgg	aaagaaaaac	1680
agtgttgatg	aatccccgctc	gacaacaaga	gccaatthtgt	ctcaagttcc	gacgatgacc	1740
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aggtgcaagc	agatgaaagt	gctggacagc	ttcatcaact	actacgacag	cgagaagcac	1860
gccgagaacg	ccgtgatctt	cctgcacggc	aacgcccgta	gcagctacct	gtggaggcac	1920
gtggtgcccc	acatcgagcc	cgtggccagg	tgcatcatcc	ccgatctgat	cggtatgggc	1980
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gccgcccctgg	ccttccacta	cagctacgag	caccaggaca	agatcaaggc	catcgtgcac	2160
gccgagagcg	tggtggacgt	gatcgagagc	tgggacgagt	ggccagacat	cgaggaggac	2220
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agcaacgcc	tcgtggagg	cgccaagaag	ttccccaca	ccgagttcgt	gaaggtgaag	2580
ggcctgcact	tcagccagga	ggacgcccc	gacgagatgg	gcaagtacat	caagagcttc	2640
gtggagagag	tgctgaagaa	cgagcagtaa				2670

<210> SEQ ID NO 35
 <211> LENGTH: 2714
 <212> TYPE: DNA
 <213> ORGANISM: Artificial Sequence
 <220> FEATURE:
 <223> OTHER INFORMATION: Nucleotide sequence encoding GFP2-str-112
 SGSR-RLuc2 mutant protein

<400> SEQUENCE: 35

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ggttcataca	agtacctgat	gatcacattc	tgctgttca	gcctctttta	cacctccatt	180
gaaacttttt	tgagacctct	catccatatac	tacgacaata	cgatcttcgt	gattcagcgc	240
aagagattcc	agtactccga	gggtaccgct	agagccattt	catcgacctc	ctgaggctgc	300
tacgccatga	gcttcacct	gttcgacctc	cactttgtct	accgttacta	tgcggcttgc	360
aaaccgaca	acctccgcta	cttccaagga	tgctactttg	tcgcatgggt	attcggagca	420
atggcggtgg	cgggagctg	ggggctcgca	gcgtttatct	tgtaccggga	gaccgagagg	480
accaggacgg	cgttgatata	cgatcacaac	acatcctatg	agctggatcc	cgagtgggtg	540
ggaaatgttc	catatagcta	ttggcgcaac	gaaaacggag	tggaatacct	gaatcctcgc	600
aacgtcatcg	ggatctttca	acacggcgct	atcatgatcc	tctccttcgg	aacagtcttc	660
tactgcggat	tcaaacctta	taagactttg	aacggaagtc	tgggggtgtc	tgaaaaaaca	720
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tgcttctacc	gttcaaatag	tgctgaaaac	actgccacca	taaggcaata	ccagcagagc	1740
agctccaaag	gatctagaga	atccggtacc	atgaccagca	aggtgtacga	ccccgagcag	1800
aggaagagga	tgatcaccgg	ccccagtggt	tgggccaggt	gcaagcagat	gaacgtgctg	1860

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gacagcttca tcaactacta cgacagcgag aagcacgccc agaacgccgt gatcttctg 1920
cacggcaacg ccgctagcag ctacctgtgg aggcacgtgg tgccccacat cgagcccgtg 1980
gccaggtgca tcattcccga tctgatcggc atgggcaaga gcggaagag cggcaacggc 2040
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cccaagaaga tcattctcgt gggccaacgac tggggcgccc ccctggcctt cactacagc 2160
tacgagcacc aggacaagat caaggccatc gtgcacgccc agagcgtggt ggacgtgatc 2220
gagagctggg acgagtgggc agacatcgag gaggacatcg ccctgatcaa gagcggaggag 2280
ggcgagaaga tgggtgctgga gaacaacttc ttcgtggaga ccgtgctgcc cagcaagatc 2340
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aagaagtcc ccaacaccga gttcgtgaag gtgaagggcc tgcacttcag ccaggaggac 2640
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cagtaagcgg ccgc 2714

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<210> SEQ ID NO 36
<211> LENGTH: 2714
<212> TYPE: DNA
<213> ORGANISM: Artificial Sequence
<220> FEATURE:
<223> OTHER INFORMATION: Nucleotide sequence encoding GFP2-str-113
SGSR-RLuc2 mutant protein

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<400> SEQUENCE: 36
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ggttcataca agtacctgat gatcacattc tgcgtgttca gcctctttta cacctccatt 180
gaaacttttt tgagacctct catccatata tacgacaata cgatcttctg gattcagcgc 240
aagagattcc agtactccga gggtagcgtc agagccattt catcgacctc ctgcccgtgc 300
tacgccatga gcttcaccct gttcgcgctc cactttgtct accgttacta tgcggcttgc 360
aaaccgaca acctccgtta ctccaagga tgcacttttg tcgcatgggt attcggagca 420
atggcgggtg cggcgagctg ggggttcgca gcgtttatct tgtaccggga gaccgagagg 480
accaggacgg cgttgatata cgtcatataa acatcctatg agctggatcc cgagtgggtg 540
ggaaatgttc catatagcta ttggcgcaca gaaaacggag tggaatacct gaatcctcgc 600
aacgtcatcg ggatctttca acacggcgtc atcatgatcc tctccttcgg aacagtcttc 660
tactgcggat tcaaacctta taagactttg aacggaagtc tgggggtgct tgaaaaaaca 720
tccggaatgg tgagcaaggg cgaggagctg ttcaccgggg tgggtgcccac cctggtcgag 780
ctggacggcg acgtaaacgg ccacaagttc agcgtgtccg gcgagggcga gggcgatgcc 840
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cccaccctcg tgaccacctt gagctacggc gtgcagtgtc tcagccgcta ccccgaccac 960
atgaagcagc acgacttctt caagtccgcc atgcccgaag gctacgtcca ggagcgcacc 1020
atcttcttca aggacgacgg caactacaag acccgcgccc aggtgaagtt cgagggcgac 1080
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gggcacaagc tggagtagaa ctacaacagc cacaacgtct atatcatggc cgacaagcag 1200
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ctcggcgacc actaccagca gaacaccccc atcggcgacg gccccgtgct gctgcccgac 1320
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cctactacac taatgtacat cccgacaacc atgctctttg tcaccccatt cgttggactc 1560
aacatcggct gttacggcaa catcactact gccacgctcc atttgtatcc tgggaattgac 1620
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cccaagatgt tcacgagag cgaccccggc ttcttcagca acgcatcgt ggaggggccc 2580
aagaagtcc ccaacaccga gttcgtgaag gtgaagggcc tgcacttcag ccaggaggac 2640
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cagtaagcgg ccgc 2714

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<210> SEQ ID NO 37
<211> LENGTH: 2714
<212> TYPE: DNA
<213> ORGANISM: Artificial Sequence
<220> FEATURE:
<223> OTHER INFORMATION: Nucleotide sequence encoding GFP2-str-114
SGSR-RLuc2 mutant protein

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<400> SEQUENCE: 37
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ggttcataca agtacctgat gatcacatc tgcgtgttca gcctctttta cacctccatt 180
gaaacttttt tgagacctct catccatc taccgacaata cgatcttctg gattcagcgc 240
aagagattcc agtactccga gggtagcctc agagccattt catcgacctc ctgoggtgct 300
tacgcatgca gcttcaccct gttcgcgctc cactttgtct accgttacta tgcggcttgc 360
aaacccgaca acctccgtta cttccaagga tgctactttg tcgcatgggt attcggagca 420

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atggcgggtg cggcgagctg ggggttcgca gcgtttatc tgtaccggga gaccgagagg	480
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ggaaatgttc catatagcta ttggcgcaca gaaaacggag tggaaacct gaatcctcgc	600
aacgtcatcg ggatcttca acacggcgtc atcatgatcc tctccttcgg aacagtcttc	660
tactgcggtt tcaacactta taagactttg aacggaagtc tgggggtgtc tgaaaaaaca	720
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<210> SEQ ID NO 38
<211> LENGTH: 2714
<212> TYPE: DNA
<213> ORGANISM: Artificial Sequence
<220> FEATURE:
<223> OTHER INFORMATION: Nucleotide sequence encoding GFP2-str-113/114
      SGRS-RLuc2 mutant protein

<400> SEQUENCE: 38
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gccaggtgca tcatccccga tctgatcggc atgggcaaga gcggcaagag cggcaacggc      2040
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gagagctggg acgagtggcc agacatcgag gaggacatcg ccctgatcaa gagcgaggag 2280
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cccgacgtgg tgcagatcgt gagaaactac aacgcctacc tgagagccag cgacgacctg 2520
cccaagatgt tcatcgagag cgaccccgcc ttcttcagca acgccaatcgt ggagggcgcc 2580
aagaagttcc ccaacaccga gttcgtgaag gtgaagggcc tgcacttcag ccaggaggac 2640
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<210> SEQ ID NO 39
<211> LENGTH: 2673
<212> TYPE: DNA
<213> ORGANISM: Artificial Sequence
<220> FEATURE:
<223> OTHER INFORMATION: Nucleotide sequence encoding GFP2-str-115
    SGSR-RLuc2 mutant protein

<400> SEQUENCE: 39

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ggtccatata aacgaatgct catagtattt tgcataatta ccgtattcta ctcaattgtc 180
gaagtcatgc ttcagccact aatccatatt tacgaogaca ctttattttt gattcatcga 240
aagagaatag acttgccaaa atggttaaca cgtttggttc ctactaccta ttgttggtgt 300
tacgcaatga gtttttcctt gtttgatta caatttttat atagatatgt ggcagtatgc 360
aaaccgcaat atggtgatct ttttgcgga tgtcactttt atgcttgggt agttttgatc 420
ttatcactag ccacgagctg gggactcact gcagctttca tgttcccaca aaccgaccga 480
acaactgaaa tttttttgca cataatttat agttcatatg acttgagacc ttattggaca 540
gattatgttg cttataaata ctttgatact gatgagaata atgtgagatg ggtcaatggt 600
cttagttttt tcggtgtcct tcagcacggg attgtaatta ctctaagttt tggcaccctt 660
tattattgtg gcatcaacac gtatctcaaa ataaaaaaaa acactggaac atcaaacaga 720
acttccggaa tggtgagcaa gggcgaggag ctgttcaccg ggggtggtgcc catcctggtc 780
gagctggaag gcgacgtaaa cggccacaag ttcagcgtgt ccggcgaggg cgagggcgat 840
gccacctacg gcaagctgac cctgaagtgc atctgcacca ccggcaagct gccctgtccc 900
tggccccacc tcgtgaccac cctgagctac ggcgtgcagt gcttcagccg ctacccccag 960
cacatgaagc agcaccgact cttcaagtcc gccatgcccg aaggetacgt ccaggagcgc 1020
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gacaccctgg tgaaccgcat cgagctgaag ggcacogact tcaaggagga cggcaacatc 1140
ctggggcaca agctggagta caactacaac agccacaacg tctatatcat ggccgacaag 1200
cagaagaacg gcatcaaggt gaacttcaag atccgccaca acatcgagga cggcagcgtg 1260
cagctcgcgg accactacca gcagaacacc cccatcgccg acggccccgt gctgctgccc 1320
gacaaccact acctgagcac ccagtcgcc ctgagcaaaag accccaacga gaagcgcgat 1380

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cacatggtcc	tgctggagtt	cgtgaccgcc	gccgggatca	ctctcggeat	ggacgagctg	1440
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ttaccaatgt	tcatgatgta	tattcccggt	ggtttcatgt	ttgcatgtcc	atattttgac	1560
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gaccatttg	tgatgctggt	ttgatagat	tcttatagaa	taacaatatt	tggatggtta	1680
tgtccaagat	ttgtttatgt	aaagccgatg	cattccacat	acaccctaac	ttctagaatg	1740
accagcaagg	tgtacgacct	cgagcagagg	aagaggatga	tcaccggccc	ccagtgggtg	1800
gccaggtgca	agcagatgaa	cgtgctggac	agcttcatca	actactacga	cagcgagaag	1860
cacgccgaga	acgccgtgat	cttcctgcac	ggcaacgccg	ctagcagcta	cctgtggagg	1920
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ggcaagagcg	gcaagagcgg	caacggcagc	tacaggtgct	tggaccacta	caagtactct	2040
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ttcagcaacg	ccatcgtgga	ggcgccaag	aagttcccca	acaccgagtt	cgtgaagggtg	2580
aagggcctgc	acttcagcca	ggaggacgcc	cccgcagaga	tgggcaagta	catcaagagc	2640
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<210> SEQ ID NO 40
 <211> LENGTH: 2729
 <212> TYPE: DNA
 <213> ORGANISM: Artificial Sequence
 <220> FEATURE:
 <223> OTHER INFORMATION: Nucleotide sequence encoding GFP2-str-116
 SGSR-RLuc2 mutant protein

<400> SEQUENCE: 40						
atgaccgatc	gctcgtgggt	cgctattacg	gacattgccg	gaccgattgg	gttcacaatg	60
tcaatttttt	cgaactcggg	gctgttatcg	ttgatattct	caagcagctc	tccaattaaa	120
ggagcttaca	aaaatatggt	gatagtgttg	tgtatattca	ctatgttcta	ctcttttggt	180
gaaataatgc	ttcaaccggt	gattcatatt	tatgatgaca	cgctgttctt	gatccaccgg	240
aaaagatttg	acctgtctaa	aggaattaca	cgtttgatac	ctacaacata	ttgttggtgt	300
tatgcaatga	gtttctcatt	attcgccctc	cagtttttgt	acagatatgt	ggcagtttgc	360
aaacctcact	tagttgtttt	ttttactgga	tgctatttct	attattgggt	ggcactcatc	420
ttatcacttg	ctacaagttg	ggggcttact	gcagctttta	tgttcccgca	aaccaatcga	480
acaactgaaa	gcttcaacta	cgtaataaaa	acttcttatg	acttagatcc	ttattggacg	540
gattatgttg	cctataaata	ttttgacacc	gatgagaatc	atgtgagatg	ggtgaatggt	600
cttagtttat	ttggagtctt	gcagcacgga	ttagtaatta	cgttgagttt	tggaaacctta	660
ttctactgtg	gaattaaaac	ttatctcagc	attactgaac	atgttggaat	gtccagcaag	720

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acctccgaa tggtagcaa gggcgaggag ctgttcaccg gggtagtgcc catcctggtc 780
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gccacctacg gcaagctgac cctgaagttc atctgcacca cggcaagct gccctgtccc 900
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cacatgaagc agcaccgactt cttcaagtcc gccatgcccc aaggctacgt ccaggagcgc 1020
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tacgaccccg agcagaggaa gaggatgatc accggcccc agtggtgggc caggtgcaag 1860
cagatgaacg tgctggacag cttcatcaac tactacgaca gcgagaagca cgcgagaaac 1920
gccgtgatct tcctgcacgg caacgcgct agcagctacc tgtggaggca cgtggtgccc 1980
cacatcgagc ccgtggccag gtcgcatcacc cccgatctga tcggcatggg caagagcggc 2040
aagagcggca acggcagcta caggctgctg gaccactaca agtacctgac cgctgggttc 2100
gagctcctga acctgcccaa gaagatcacc ttcgtgggcc acgactgggg cgccgcctg 2160
gccttccact acagctacga gcaccaggac aagatcaagg ccatcgtgca cgcgagagc 2220
gtggtggacg tgatcgagag ctgggacgag tggccagaca tcgaggagga catcgccctg 2280
atcaagagcg aggagggcga gaagatggtg ctggagaaca acttctcgt ggagaccgtg 2340
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ttcaaggaga agggcgaggt gagaagacc accctgagct ggcccagaga gatccccctg 2460
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ttcagccagg aggaccccc cgacgagatg ggcaagtaca tcaagagctt cgtggagaga 2700
gtgctgaaga acgagcagta agcggcgcg 2729

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<210> SEQ ID NO 41

<211> LENGTH: 346

<212> TYPE: PRT

<213> ORGANISM: *Caenorhabditis elegans*

<400> SEQUENCE: 41

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Met Ser Gly Gln Leu Trp Leu Ala Leu Val Asp Ala Ala Asp Met Val
1           5           10           15

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Gly Phe Thr Leu Thr Ile Ser Ile Asn Ile Ile Leu Leu Gly Leu Ile
 20 25 30
 Arg Thr Arg Gly Lys Thr Leu Gly Thr Tyr Lys Tyr Leu Met Ser Phe
 35 40 45
 Phe Ser Phe Phe Ser Ile Phe Tyr Ala Ile Val Glu Ser Ile Leu Arg
 50 55 60
 Pro Ile Met His Ile Glu Asn Thr Thr Phe Phe Leu Ile Ser Arg Lys
 65 70 75 80
 Arg Phe Asp Tyr Ser Thr Arg Leu Gly Lys Ile Asn Ser Ala Phe Tyr
 85 90 95
 Cys Ala Cys Phe Ala Thr Ser Phe Val Leu Ser Ala Val His Phe Val
 100 105 110
 Tyr Arg Tyr Phe Ala Ala Cys Lys Pro Asn Leu Leu Arg Leu Phe Asn
 115 120 125
 Leu Pro His Leu Leu Leu Trp Pro Leu Met Cys Ser Ile Pro Val Thr
 130 135 140
 Ala Trp Ala Ser Val Ser Tyr Phe Leu Tyr Pro Asp Thr Glu Tyr Thr
 145 150 155 160
 Glu Ala Ala Val Thr Tyr Val Leu Lys Thr His Tyr Glu Val Ile Lys
 165 170 175
 Lys Glu Asn Val Ser Tyr Ile Ala Tyr Val Tyr Tyr Gln Tyr Glu Asn
 180 185 190
 Gly Glu Arg His Ile Tyr Ile Lys Asn Leu Leu Gly Cys Phe Val His
 195 200 205
 Tyr Phe Val Met Ser Met Thr Phe Val Val Val Phe Tyr Cys Gly Phe
 210 215 220
 Ser Thr Trp Trp Thr Ile Arg Glu His Arg Gly Ala Ser Asp Arg Thr
 225 230 235 240
 Arg His Leu His Arg Gln Leu Phe Lys Ala Leu Val Phe Gln Thr Leu
 245 250 255
 Val Pro Ser Ile Phe Met Tyr Ile Pro Thr Gly Val Met Phe Ile Ala
 260 265 270
 Pro Phe Phe Asp Ile Asn Leu Asn Ala Asn Ala Asn Phe Ile Val Phe
 275 280 285
 Cys Ser Phe Leu Tyr Pro Gly Leu Asp Pro Leu Ile Leu Ile Phe Ile
 290 295 300
 Ile Arg Glu Phe Arg Val Thr Ile Leu Asn Ile Ile Arg Gly Asn Glu
 305 310 315 320
 Arg Gly Asn Ala Val Gly Glu Ala Tyr Ser Thr Ser Arg Ile Lys Ser
 325 330 335
 Ser Gln Pro Ala Ala Val Asn Leu Ser Gly
 340 345

<210> SEQ ID NO 42

<211> LENGTH: 341

<212> TYPE: PRT

<213> ORGANISM: Caenorhabditis elegans

<400> SEQUENCE: 42

Met Ser Asp Arg His Trp Leu Asp Ile Thr Thr Tyr Ser Asp His Ile
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 Gly Phe Thr Ile Ser Thr Ile Ala Asn Phe Val Leu Ile Leu Leu Leu
 20 25 30
 Val Phe Arg Pro Thr Lys Ser Tyr Gly Ser Tyr Lys Tyr Leu Met Ile

-continued

Thr	Phe	Cys	Val	Phe	Ser	Leu	Phe	Tyr	Thr	Ser	Ile	Glu	Thr	Phe	Leu
50						55					60				
Arg	Pro	Leu	Ile	His	Ile	Tyr	Asp	Asn	Thr	Ile	Phe	Val	Ile	Gln	Arg
65				70					75						80
Lys	Arg	Phe	Gln	Tyr	Ser	Glu	Gly	Thr	Ala	Arg	Ala	Ile	Ser	Ser	Thr
				85					90					95	
Tyr	Cys	Gly	Cys	Tyr	Ala	Met	Ser	Phe	Thr	Leu	Phe	Ala	Val	His	Phe
		100						105					110		
Val	Tyr	Arg	Tyr	Tyr	Ala	Ala	Cys	Lys	Pro	Asp	Asn	Leu	Arg	Tyr	Phe
		115						120				125			
Gln	Gly	Cys	Tyr	Phe	Val	Ala	Trp	Val	Phe	Gly	Ala	Met	Ala	Val	Ala
130						135					140				
Ala	Ser	Trp	Gly	Phe	Ala	Ala	Phe	Ile	Leu	Tyr	Pro	Glu	Thr	Glu	Arg
145					150					155					160
Thr	Arg	Thr	Ala	Leu	Ile	His	Val	Ile	Gln	Thr	Ser	Tyr	Glu	Leu	Asp
				165					170						175
Pro	Glu	Trp	Val	Gly	Asn	Val	Pro	Tyr	Ser	Tyr	Trp	Arg	Thr	Glu	Asn
			180					185						190	
Gly	Val	Glu	Tyr	Leu	Asn	Pro	Arg	Asn	Val	Ile	Gly	Ile	Phe	Gln	His
		195					200					205			
Gly	Val	Ile	Met	Ile	Leu	Ser	Phe	Gly	Thr	Val	Phe	Tyr	Cys	Gly	Phe
210						215					220				
Asn	Thr	Tyr	Lys	Thr	Leu	Asn	Gly	Ser	Leu	Gly	Val	Ser	Glu	Lys	Thr
225					230					235					240
Lys	Glu	Met	His	Thr	Gln	Leu	Phe	Lys	Ala	Leu	Val	Leu	Gln	Thr	Ile
				245					250						255
Ile	Pro	Thr	Thr	Leu	Met	Tyr	Ile	Pro	Thr	Thr	Met	Leu	Phe	Val	Thr
				260					265					270	
Pro	Phe	Val	Gly	Leu	Asn	Ile	Gly	Cys	Tyr	Gly	Asn	Ile	Thr	Thr	Ala
		275						280				285			
Thr	Val	His	Leu	Tyr	Pro	Gly	Ile	Asp	Pro	Val	Val	Leu	Ile	Phe	Ile
290						295					300				
Ile	Arg	Asp	Phe	Arg	Gln	Thr	Ile	Leu	Arg	Pro	Phe	Arg	Cys	Phe	Tyr
305					310					315					320
Arg	Ser	Asn	Ser	Val	Glu	Asn	Thr	Ala	Thr	Ile	Arg	Gln	Tyr	Gln	Gln
				325					330						335
Ser	Ser	Ser	Lys	Gly											
			340												

<210> SEQ ID NO 43

<211> LENGTH: 351

<212> TYPE: PRT

<213> ORGANISM: Artificial Sequence

<220> FEATURE:

<223> OTHER INFORMATION: str113/114 chimeric protein

<400> SEQUENCE: 43

Met	Ser	Asp	Arg	His	Trp	Leu	Asp	Ile	Thr	Thr	Tyr	Ser	Asp	His	Ile
1				5					10					15	
Gly	Phe	Thr	Ile	Ser	Thr	Ile	Ala	Asn	Phe	Val	Leu	Ile	Leu	Leu	Leu
			20					25					30		
Val	Phe	Arg	Pro	Thr	Lys	Ser	Tyr	Gly	Ser	Tyr	Lys	Tyr	Leu	Met	Ile
		35						40				45			
Thr	Phe	Cys	Val	Phe	Ser	Leu	Phe	Tyr	Thr	Ser	Ile	Glu	Thr	Phe	Leu

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50	55	60
Arg Pro Leu Ile His Ile Tyr Asp Asn Thr Ile Phe Val Ile Gln Arg 65 70 75 80		
Lys Arg Phe Gln Tyr Ser Glu Gly Thr Ala Arg Ala Ile Ser Ser Thr 85 90 95		
Tyr Cys Gly Cys Tyr Ala Met Ser Phe Thr Leu Phe Ala Val His Phe 100 105 110		
Val Tyr Arg Tyr Tyr Ala Ala Cys Lys Pro Asp Asn Leu Arg Tyr Phe 115 120 125		
Gln Gly Cys Tyr Phe Val Ala Trp Val Phe Gly Ala Met Ala Val Ala 130 135 140		
Ala Ser Trp Gly Phe Ala Ala Phe Ile Leu Tyr Pro Glu Thr Glu Arg 145 150 155 160		
Thr Arg Thr Ala Leu Ile His Val Ile Gln Thr Ser Tyr Glu Leu Asp 165 170 175		
Pro Glu Trp Val Gly Asn Val Pro Tyr Ser Tyr Trp Arg Thr Glu Asn 180 185 190		
Gly Val Glu Tyr Leu Asn Pro Arg Asn Val Ile Gly Ile Phe Gln His 195 200 205		
Gly Val Ile Met Ile Leu Ser Phe Gly Thr Val Phe Tyr Cys Gly Phe 210 215 220		
Asn Thr Tyr Lys Thr Leu Asn Gly Ser Leu Gly Val Ser Glu Lys Thr 225 230 235 240		
Ser Gly Val Asp Lys Glu Met His Thr Gln Leu Phe Lys Ala Leu Val 245 250 255		
Leu Gln Thr Ile Ile Pro Thr Thr Leu Met Tyr Ile Pro Thr Thr Met 260 265 270		
Leu Phe Val Thr Pro Phe Val Gly Leu Asn Ile Gly Cys Tyr Gly Asn 275 280 285		
Ile Thr Thr Ala Thr Val His Leu Tyr Pro Gly Ile Asp Pro Val Val 290 295 300		
Leu Ile Phe Ile Ile Arg Asp Phe Arg Gln Thr Ile Leu Arg Pro Phe 305 310 315 320		
Arg Cys Phe Tyr Arg Ser Asn Ser Val Glu Asn Thr Ala Thr Ile Arg 325 330 335		
Gln Tyr Gln Gln Ser Ser Ser Lys Gly Ser Arg Glu Phe Gly Thr 340 345 350		

<210> SEQ ID NO 44
 <211> LENGTH: 1041
 <212> TYPE: DNA
 <213> ORGANISM: Caenorhabditis elegans

<400> SEQUENCE: 44

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acgatctcca tcaacatcat tctactgggg ctgattagaa cacgtggaaa aacgttgga	120
acgtacaaat acttgatgag cttcttctcg ttcttctcaa tcttttatgc aatcgttgaa	180
tctatattga gaccaataat gcatatcgaa aacacgacgt tctttctgat ttctcggaaa	240
cgcttcgatt actcaactcg ccttggtaaa atcaactctg cttctactg tgettgttt	300
gccacgagtt ttgtcctgtc tgcggtacac tttgtgtatc ggtactttgc cgettgc aaa	360
ccgaatctgc tacgcttgtt taaccttccg catcttttac tgtggccttt gatgtgttcg	420
attctctgta ctgcgtgggc aagtgtttct tactttttgt acccagacac cgagtacact	480

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gaagcagcag ttacatatgt tctgaaaaca cactacgagg tgatcaaaaa agaaaatgta 540
tcttatatcg catacgtata ctatcaatat gaaaatgggg agcgtcacat ctacataaaa 600
aatttgcttg gctgctttgt aactactctc gttatgtcaa tgacatttgt agttgtgttt 660
tactgcggat tttctacatg gtggacgatt cgtgagcacc gtggagcacc tgataggaca 720
cgtcacctgc atagacaatt gtttaaggca cttgtatttc aaaccttgt tccatcaata 780
tttatgtaca tcccaactgg tgctcatgtc atcgctccct ttttogecat caacctgaat 840
gccaatgcaa acttcatcgt tttttgctca tttctctatc caggctctga cccactaatt 900
ctcattttta tcattcgcga attcagggtc actattttga atatcatcag aggaaatgag 960
cggggaaatg ctgttgcgga agcatactca acttctcgaa taaaatcacc acaacctgca 1020
gctgttaatc tttctggata a 1041

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<210> SEQ ID NO 45
<211> LENGTH: 1026
<212> TYPE: DNA
<213> ORGANISM: Caenorhabditis elegans

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<400> SEQUENCE: 45

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atgtctgacc gtcattggct cgacatcacc acctactcag accacattgg gtttacgatt 60
tccaccatcg ccaatttcgt tctgatoctt ctgctagtct tccgaccgac caaatcatac 120
ggttcataca agtacctgat gatcacattc tgcgtgttca gcctctttta cacctccatt 180
gaaacttttt tgagacctct catccatata tacgacaata cgatcttcgt gattcagcgc 240
aagagattcc agtactccga gggtaaccgt agagccattt catcgacctc ctgaggctgc 300
tacgccatga gcttcacctt gttcgcctgc cactttgtct accgttacta tgcggcttgc 360
aaacccgaca acctccgtta ctccaagga tgctactttg tcgcatgggt attcggagca 420
atggcgggtg cggcgagctg ggggttcgca gcgtttatct tgtaccgga gaccgagagg 480
accaggacgg cgttgatata cgtcatataa acatcctatg agctggatcc cgagtgggtg 540
ggaaatgttc catatagcta ttggcgcaca gaaaacggag tggaatacct gaatcctcgc 600
aacgtcatcg ggatctttca acacggcgtc atcatgatcc tctccttcgg aacagtcttc 660
tactgcggat tcaaacctta taagactttg aacggaagtc tgggggtgct tgaaaaaaca 720
aaagaaatgc acaccaatg gttcaaggcc ttggttctac agactatcat ccctaetaca 780
ctaattgtaca tcccgacaac catgctcttt gtcaccccat tcggttgact caacatcggc 840
tgttacggca acatcactac tgccaccgtc catttgtatc ctggaattga cccagtcgtt 900
ttgatcttta taatccgaga ctcccgcaa acgattttaa gaccattcag atgcttctac 960
cgttcaaata gtgtcgaaaa cactgccacc ataaggcaat accagcagag cagctccaaa 1020
ggataa 1026

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<210> SEQ ID NO 46
<211> LENGTH: 1056
<212> TYPE: DNA
<213> ORGANISM: Artificial Sequence
<220> FEATURE:
<223> OTHER INFORMATION: str113/114 chimeric protein encoding sequence

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<400> SEQUENCE: 46

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atgtctgacc gtcattggct cgacatcacc acctactcag accacattgg gtttacgatt 60
tccaccatcg ccaatttcgt tctgatoctt ctgctagtct tccgaccgac caaatcatac 120

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ggttcataca agtacctgat gatcacattc tgcgtgttca gcctctttta cacctccatt	180
gaaacttttt tgagacctct catccatatac tacgacaata cgatcttcgt gattcagcgc	240
aagagattcc agtactccga gggtagcgc agagccattt catcgaccta ctgcggtgc	300
tacgccatga gcttcacct gttcgcgct cactttgtct accgttacta tgcggcttgc	360
aaacccgaca acctccgta ctccaagga tgctactttg tcgcatgggt attcggagca	420
atggcggtgg cggcgagctg ggggttcgca gcgtttattc tgtaccgga gaccgagag	480
accaggacgg cgttgatata cgtcatatac acatcctatg agctggatcc cgagtgggtg	540
ggaaatgttc catatagcta ttggcgca gaaaacggag tggaatacct gaatcctcgc	600
aacgtcatcg ggtactttca acacggcgtc atcatgatcc tctccttcgg aacagtcttc	660
tactgcggt tcaaacctta taagactttg aacggaagtc tgggggtgct tgaaaaaaca	720
tccggagtgc acaagaagt gcacacccaa ttggtcaagg ccttgggtct acagaactatc	780
atccctacta cactaatgta catcccgaca accatgctct ttgtcacccc attcgttga	840
ctcaacatcg gctgttacgg caacatcact actgccaccg tccatttga tcttgaatt	900
gaccagtcg ttttgatctt tataatccga gacttccggc aaacgatttt aagaccattc	960
agatgctctt accgttcaaa tagtgcgaa aacactgcca ccataaggca ataccagcag	1020
agcagctcca aaggatctag agaattcggc acctaa	1056

The invention claimed is:

1. A protease sensor molecule comprising a protease cleavable domain, a chemiluminescent donor domain and an acceptor domain, wherein the protease is capable of cleaving a milk protein, and wherein the spatial location and/or dipole orientation of the chemiluminescent donor domain relative to the acceptor domain is altered when the protease cleavable domain is cleaved by the protease, and wherein the chemiluminescent donor domain is a bioluminescent protein.

2. The sensor molecule according to claim 1, wherein the protease is capable of causing milk spoilage.

3. The protease sensor molecule according to claim 1, wherein the protease is a bacterial protease.

4. The protease sensor molecule according to claim 1, wherein the protease is plasmin.

5. The protease sensor molecule according to claim 1, wherein the protease cleavable domain comprises the amino acid sequence KZ, where Z is K, Y, V or E.

6. The protease sensor molecule according to claim 5, wherein the protease cleavable domain comprises the amino acid sequence LQXXXXXKZXLQ (SEQ ID NO:47), where Z is K, Y, V or E, and X is any amino acid.

7. The protease sensor molecule according to claim 1, wherein the milk protein is casein.

8. The protease sensor molecule according to claim 1, wherein the milk is ultra-high temperature (UHT) processed milk.

9. The protease sensor molecule according to claim 1, wherein the separation and relative orientation of the chemiluminescent donor domain and the acceptor domain in the absence of the protease is within $\pm 50\%$ of the Forster distance.

10. The protease sensor molecule according to claim 1, wherein the bioluminescent protein is a luciferase, a β -galactosidase, a lactamase, a horseradish peroxidase, an alkaline phosphatase, a β -glucuronidase or a β -glucosidase.

11. The protease sensor molecule according to claim 10, wherein the luciferase is a *Renilla* luciferase, a Firefly luciferase, a Coelenterate luciferase, a North American glow worm luciferase, a click beetle luciferase, a railroad worm luciferase, a bacterial luciferase, a *Gaussia* luciferase, Aequorin, an *Arachnocampa* luciferase, or a biologically active variant or fragment of any one, or chimera of two or more, thereof.

12. The protease sensor molecule according to claim 1, wherein the chemiluminescent donor domain is capable of modifying a substrate.

13. The protease sensor molecule according to claim 12, wherein the substrate is luciferin, calcium, coelenterazine, or a derivative or analogue of coelenterazine.

14. The protease sensor molecule according to claim 1, wherein the acceptor domain is a fluorescent acceptor domain.

15. The protease sensor molecule according to claim 12, wherein

i) the bioluminescent protein is a luciferase or a biologically active variant or fragment, and/or

ii) the substrate is luciferin, coelenterazine, or a derivative or analogue of coelenterazine, and/or

iii) the acceptor domain is green fluorescent protein (GFP), Venus, mOrange, or a biologically active variant or fragment of any one thereof.

16. The protease sensor molecule according to claim 15, wherein

i) the luciferase is a *Renilla* luciferase, the acceptor domain is GFP², and the substrate is coelenterazine 400a,

ii) the luciferase is a *Renilla* luciferase 2, the acceptor domain is GFP², and the substrate is coelenterazine 400a,

iii) the luciferase is a *Renilla* luciferase 8, the acceptor domain is GFP², and the substrate is coelenterazine 400a,

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- iv) the luciferase is a *Renilla* luciferase 2, the acceptor domain is Venus, and the substrate is coelenterazine,
 - v) the luciferase is a *Renilla* luciferase 8, the acceptor domain is Venus, and the substrate is coelenterazine,
 - vi) the luciferase is a *Renilla* luciferase 8.6-535, the acceptor domain is mOrange, and the substrate is coelenterazine, or
 - vii) the luciferase is a *Renilla* luciferase 8, the acceptor domain is mOrange, and the substrate is coelenterazine.
17. A method of classifying milk or cheese, the method comprising
- i) mixing the protease sensor molecule according claim 1, a substrate of the chemiluminescent donor, and the milk or the cheese,
 - ii) detecting modification of the substrate by the chemiluminescent donor, and
 - iii) classifying the milk or cheese based on the alteration in the spatial location and/or dipole orientation of the chemiluminescent donor domain relative to the acceptor domain,
- wherein the spatial location and/or dipole orientation of the chemiluminescent donor domain relative to the acceptor domain is altered when the protease cleavable domain is cleaved by the protease.
18. A method of classifying milk or cheese, the method comprising
- i) flowing through a microfluidic device comprising one or more microchannels,
 - a) the milk or the cheese,
 - b) a protease sensor molecule comprising a protease cleavable domain, a chemiluminescent donor

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- domain and an acceptor domain, wherein the separation and relative orientation of the chemiluminescent donor domain and the acceptor domain in the absence of the protease is within $\pm 50\%$ of the Forster distance,
 - c) a substrate of the chemiluminescent donor,
 - ii) mixing the protease sensor molecule, the substrate, and the milk or the cheese in the device, and
 - iii) detecting modification of the substrate by the chemiluminescent donor using an electro-optical sensing device,
 - iv) processing at least one signal from the electro-optical sensing device and correlating the pattern of electro-optical responses with one or more pre-determined characteristics of one or more samples of interest, and
 - v) classifying the quality and/or shelf life of the milk or the cheese based on the correlation of the pattern of responses,
- wherein the spatial location and/or dipole orientation of the chemiluminescent donor domain relative to the acceptor domain is altered when the protease cleavable domain is cleaved by the protease.
19. The method according to claim 18, wherein
- a) the protease sensor molecule is not fixed to the device, and/or
 - b) the method further comprises calculating as a ratio the energy transfer occurring between the chemiluminescent donor domain and the acceptor domain.

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